

**FINITE ELEMENT METHOD FOR FLUID FLOW OF MODELLING OF
THE DESCEMET MEMBRANE DETACHMENT AND
RHEMATOGENEOUS RETINAL DETACHMENT**

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DESCEMET MEMBRANE DETACHMENT AND RHEMATOGENEOUS
RETINAL DETACHMENT

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To my beloved
father, mother,
brother, sisters
&
my supervisors,
Assoc. Prof. Dr. Sharidan Shafie,
and
Dr. Zuhaila Ismail.

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ABSTRACT

A numerical computation of the ocular fluid mechanics incorporate with Descemet membrane detachment (DMD) and Rhegmatogenous retinal detachment (RRD) were presented. DMD and RRD are serious diseases of the human eye that might cause vision impairment and blindness. The developing mechanisms of both diseases are related to the fluid flow in the anterior chamber (AC) and vitreous cavity (VC) of the human eye. However, the measurement of the fluid data in the human eye is difficult due to the small size of the eye and extremely low velocity of the fluid flow. Therefore, mathematical models were proposed to investigate the fluid flow in the human eye with DMD and RRD respectively. The aqueous humour (AH) in the AC and the vitreous humour (VH) in the VC have similar properties to water. Thus the AH and VH were assumed as an incompressible Newtonian fluid. Navier-Stokes equations were applied to govern the fluid flow in AC and VC. In AC, the AH flow was driven by the buoyancy forces. The AH adjacent to the iris was heated and eventually rises as buoyant flow. While, the AH adjacent to the cornea becomes colder and heavier that it flows down in the direction of the gravitational force. In VC, the VH flow was induced by the movement of the eye. Finite element method was used to solve this problem. A source code (MATLAB) was constructed to run the iterative numerical procedure, to determine the approximate solutions and to display the results graphically. The results show that the circulation of the AH in the AC was affected by the types and location of the DMD. Additionally, change in the orientations (the direction of the gravitational force) and the shape (the area) of the AC do change the characteristics of the AH flow. On the other hand, the characteristic of the VH flows in the VC were dependent on the pattern and seriousness of the RRD. The VH flow in the VC were dominantly driven by the saccadic eye movement. It is observed that, the scale and location of the sclera buckling were the important factors that affect the outflow of the subretinal fluid flow into the VC.

ABSTRAK

Pengiraan berangka bagi mekanik bendalir okular yang melibatkan penanggalan membran Descemet (DMD) dan penanggalan retina jenis Rhegmatogenous (RRD) dipersembahkan. DMD dan RRD merupakan penyakit mata manusia yang serius berkemungkinan boleh menyebabkan gangguan penglihatan dan kebutaan. Mekanisme melaratnya kedua-dua penyakit ini berkait rapat dengan aliran bendalir di dalam *aqueous chamber* (AC) dan *vitreous chamber* (VC) mata manusia. Namun, pengukuran data bendalir di dalam mata manusia adalah sukar kerana saiz mata yang kecil dan halaju aliran bendalir yang amat rendah. Oleh itu, model matematik telah dicadangkan untuk menyelidik aliran bendalir di dalam mata manusia, masing-masing dengan DMD dan RRD. *Aqueous humour* (AH) dalam AC dan *vitreous humour* (VH) dalam VC mempunyai ciri-ciri yang serupa dengan air. Oleh itu AH dan VH diandaikan sebagai bendalir Newtonan tidak termampat. Persamaan Navier-Stokes telah digunakan untuk mentadbir aliran bendalir dalam AC dan VC. Dalam AC, aliran AH didorong oleh daya keapungan. AH bersebelahan dengan iris dipanaskan dan akhirnya akan meningkat sebagai aliran apung. Manakala, AH bersebelahan dengan kornea menjadi lebih sejuk dan lebih berat sehingga kemudiannya akan mengalir mengikuti arah daya graviti. Dalam VC, aliran VH diaruh oleh pergerakan mata. Kaedah unsur terhingga digunakan untuk menyelesaikan masalah ini. Satu kod sumber (MATLAB) telah dibina untuk melaksanakan prosedur berangka secara lelaran, bagi menentukan penyelesaian penghampiran dan memaparkan keputusan secara grafik. Keputusan menunjukkan peredaran AH di dalam AC dipengaruhi oleh jenis dan lokasi DMD. Di samping itu, perubahan orientasi (arah daya graviti) dan perubahan bentuk AC (keluasan) didapati mengubah ciri-ciri aliran AH. Sebaliknya, ciri-ciri aliran VH di dalam VC adalah bergantung kepada corak dan keseriusan RRD. Aliran VH di dalam VC didominasi oleh pergerakan mata sakadik. Diperhatikan bahawa, skala dan lokasi sklera melengkok adalah faktor penting yang mempengaruhi pengaliran keluar bendalir *subretinal* masuk ke dalam VC.

TABLE OF CONTENTS

CHAPTER	TITLE	PAGE
	DECLARATION	ii
	DEDICATION	iii
	ACKNOWLEDGEMENTS	iv
	ABSTRACT	v
	ABSTRAK	vi
	TABLE OF CONTENTS	vii
	LIST OF TABLES	xi
	LIST OF FIGURES	xii
	LIST OF SYMBOLS	xxii
	LIST OF APPENDICES	xxv
1	INTRODUCTION	1
	1.1 Introduction	1
	1.2 Research Background	2
	1.3 Statement of the Problem	7
	1.4 Objectives of the Study	8
	1.5 Scope of the Study	8
	1.6 Significant of the Study	9
	1.7 Outline of the Thesis	10
	1.8 Conclusions	11
2	LITERATURE REVIEW	12
	2.1 Introduction	12

2.2	Anatomy of Human Eye	13
2.2.1	Cornea	14
2.2.2	Iris and Pupil	15
2.2.3	Lens	16
2.2.4	Anterior Chamber and Aqueous Humour	17
2.2.5	Limbus and Ciliary Body	18
2.2.6	Sclera	19
2.2.7	Choroid	19
2.2.8	Retina	20
2.2.9	Vitreous Humour	21
2.3	Fluid Flow in Anterior Chamber	22
2.3.1	Descemet Membrane Detachment	27
2.3.2	Cornea Indentation	30
2.4	Fluid Flow in Vitreous Cavity	30
2.4.1	Rhegmatogeneous Retinal Detachment	31
2.4.2	Scleral Buckling	38
3	IMPLEMENTATION OF THE FINITE ELEMENT METHOD	41
3.1	Introduction	41
3.2	Finite Element Method	42
3.3	Standard Shape Functions of Taylor-Hood Element	43
3.4	Gaussian Quadrature	51
3.5	Nonlinear Equations	54
3.6	Navier-Stokes Equations	56
3.6.1	Finite Element Models of Navier-Stokes Equations	57
3.6.2	Linearization of Navier-Stokes Equations	61
3.7	Conclusions	64
4	COMPUTER IMPLEMENTATION OF FINITE ELEMENT METHOD	66
4.1	Introduction	66

4.2	Data Preparation	67
4.3	Construction of Global Matrix	72
4.4	Incorporating Boundary Conditions	75
4.5	Solutions	77
4.6	Applications of the Source Code	79
4.6.1	Mathematical Formulation	79
4.6.2	Finite Element Model of the Governing Equations	82
4.6.3	Linearization of the Governing Equations	83
4.6.4	Results and Discussion	86
4.7	Conclusions	93
5	DESCEMET MEMBRANE DETACHMENT	95
5.1	Introduction	95
5.2	Aqueous Humour Flow in the Aqueous Chamber	96
5.2.1	Finite Element Model of the Governing Equations	99
5.2.2	Linearization the Governing Equations	101
5.2.3	Mesh Test and Validation	104
5.3	Influence of the Types of DMD to the AH Flow in AC	109
5.3.1	Results and Discussion	113
5.4	Influence of the Cornea Indentation to the AH Flow in AC	123
5.4.1	Results and Discussion	126
5.5	Influence of the patient's orientation to the AH Flow in AC	132
5.5.1	Results and Discussion	133
5.6	Conclusions	140
6	RHEMATOGENOUS RETINAL DETACHMENT	141
6.1	Introduction	141

6.2	Liquefied Vitreous Humour Flow in the Vitreous Chamber	142
6.2.1	Finite Element Model of the Governing Equations	145
6.2.2	Linearization the Governing Equations	145
6.2.3	Mesh Test and Validation	147
6.3	Liquefied VH Flow through the Detached Retina in a Channel with Rigid Walls	152
6.3.1	Results and Discussion	155
6.4	Liquefied VH Flow through the Detached Retina in a Channel with One Moving Wall	168
6.4.1	Results and Discussion	169
6.5	Effect of SB to the Flow of Liquefied VH in VC with RRD	184
6.5.1	Results and Discussion	187
6.6	Conclusions	197
7	CONCLUSIONS	198
7.1	Summary of the Research	198
7.2	Recommendations for the Future Research	200
	REFERENCES	203
	Appendices A - J	217 - 266

LIST OF TABLES

TABLE NO.	TITLE	PAGE
4.1	The numbering of the node points that generated by <code>mesh2d</code>	69
4.2	The xy -coordinates of the geometry nodes that generated by <code>mesh2d</code>	70
4.3	The numbering of the node points for the quadratic triangular mesh	70
4.4	The xy - coordinates of the geometry nodes for the quadratic triangular mesh	71
4.5	The numbering of the global DOFs	74
4.6	Parameters for different mesh	87
4.7	Results for u - velocity at the geometric centre of the cavity	90
4.8	Results for v - velocity at the geometric centre of the cavity	90
5.1	Properties of the AH used in the model	97
5.2	Parameters for different mesh	104
5.3	Results for the maximum u - velocity and its location in the AC	106
5.4	The corresponding value of b to the value of a_1 considered	124
6.1	Properties of the VH used in the model	143
6.2	Parameters for different mesh	147
6.3	Results for the u - velocity at five randomly chosen location in the VC for Case 1	149
6.4	Results for the u - velocity at five randomly chosen location in the VC for Case 2	150

LIST OF FIGURES

FIGURE NO.	TITLE	PAGE
1.1	Structure of Human Eye (Kara, 2011)	2
2.1	Structure of the Cornea (Stephen and Allen, 2004)	15
2.2	Pupil and iris (Kara, 2011)	16
2.3	Flow of the aqueous humor from posterior chamber to anterior chamber and out the chamber through the trabecular meshwork (Jouzdani, 2013)	18
2.4	Structure of Retina	21
2.5	Descemet membrane detachment (Couch and Baratz, 2009)	28
2.6	Retinal detachment (Root, 2009)	32
3.1	Triangular Taylor-Hood element	44
3.2	Mapping the element in physical coordinate (x, y) to the normalized coordinate (ε, η)	46
3.3	6 points mapping from the physical coordinate to the normalized coordinate	53
4.1	Three main functional parts of computer implementation of FEM	67
4.2	Unstructured mesh for linear triangular element	68
4.3	Unstructured mesh for quadratic triangular element	71
4.4	The <code>node_condition</code> for the geometry shown in Figure 4.3	77
4.5	Flowchart of the computer programing	78
4.6	Lid cavity driven flow	80

4.7	(a) Basic region, lid cavity problem, (b) mesh 1, (c) mesh 2, (d) mesh 3, (e) mesh 4 and (f) mesh 5	88
4.8	The (a) v -velocity and (b) u -velocity profiles along a horizontal line passing through the geometric centre of the cavity with $Re = 100$ for mesh 1 = 2056 elements, mesh 2 = 4104 elements, mesh 3 = 8208 elements, mesh 4 = 13642 elements and mesh 5 = 16392 elements	89
4.9	Velocity contours and streamline for the lid driven cavity problem with $Re = 100$ for (a) the present source code and (b) COMSOL Multiphysics 5.0	91
4.10	Velocity contours and streamline for the lid driven cavity problem with $Re = 400$ for (a) the present source code and (b) COMSOL Multiphysics 5.0	92
4.11	Velocity contours and streamline for the lid driven cavity problem with $Re = 1000$ for (a) the present source code and (b) COMSOL Multiphysics 5.0	93
5.1	Schematic diagram of the AC	96
5.2	(a) The basic AC region and (b) mesh 1	105
5.3	The u - velocity profiles along a vertical line passing through the geometric centre of the cornea with mesh 1, mesh 2, mesh 3, mesh 4 and mesh 5	105
5.4	Velocity contour and streamline of the AH flow in the AC	107
5.5	Streamline plots given by (a) Ismail <i>et al.</i> (2012) and (b) Canning <i>et al.</i> (2002).	107
5.6	Velocity contour and streamline of the AH flow in the AC which computed by COMSOL Multiphysics 5.0	108
5.7	Isotherms plot of the AC by (a) the present source code and (b) COMSOL Multiphysics 5.0	108
5.8	Non-scrolled (a) planar and non-peripheral, (b) non-planar and non-peripheral, (c) planar and peripheral and (d) non-planar and peripheral, DMD	109

5.9	Scrolled (a) planar and non-peripheral, (b) non-planar and non-peripheral, (c) planar and peripheral and (d) non-planar and peripheral, upper DMD	110
5.10	Problem domain and boundary conditions of (a) non-scrolled planar and non-peripheral, DMD and (b) scrolled, planar and non-peripheral DMD	111
5.11	Extracting the piecewise-linear geometry nodes for (a) non-scrolled planar and non-peripheral, DMD and (b) scrolled, planar and non-peripheral DMD	112
5.12	Mesh for (a) non-scrolled planar and non-peripheral, DMD and (b) scrolled, planar and non-peripheral DMD	112
5.13	Velocity contour, streamline and isotherm of the AH flow in the AC for the case with the non-scrolled, non-peripheral, (a) planar and (b) non-planar upper DMD	115
5.14	Velocity contour, streamline and isotherm of the AH flow in the AC for the case with the non-scrolled, peripheral, (a) planar and (b) non-planar upper DMD	116
5.15	Velocity contour, streamline and isotherm of the AH flow in the AC for the case with the scrolled, non-peripheral, (a) planar and (b) non-planar upper DMD	117
5.16	Velocity contour, streamline and isotherm of the AH flow in the AC for the case with the scrolled, peripheral, (a) planar and (b) non-planar upper DMD	118
5.17	Velocity contour, streamline and isotherm of the AH flow in the AC for the case with the non-scrolled, non-peripheral, (a) planar and (b) non-planar lower DMD	119
5.18	Velocity contour, streamline and isotherm of the AH flow in the AC for the case with the non-scrolled, peripheral, (a) planar and (b) non-planar lower DMD	120
5.19	Velocity contour, streamline and isotherm of the AH flow in the AC for the case with the scrolled, non-peripheral, (a) planar and (b) non-planar lower DMD	121

5.20	Velocity contour, streamline and isotherm of the AH flow in the AC for the case with the scrolled, peripheral, (a) planar and (b) non-planar lower DMD	122
5.21	Problem domain and boundary conditions of the AH flow in the AC with cornea indentation	123
5.22	Mesh of the AH flow in the AC, where the cornea is indented with $a_I = 0.3$ mm, (a) without the DMD and (b) with non-scrolled, planar and non-peripheral DMD	125
5.23	Velocity contour, streamline and isotherm of the AH flow in the AC with the cornea indentation of (a) $a_I = 0.3$ mm, (b) $a_I = 0.4$ mm and (c) $a_I = 0.5$ mm	127
5.24	Velocity contour, streamline and isotherm of the AH flow in the AC with the cornea indentation of $a_I = 0.3$ mm and with the non-scrolled, non-peripheral, (a) planar and (b) non-planar upper DMD	128
5.25	Velocity contour, streamline and isotherm of the AH flow in the AC with the cornea indentation of $a_I = 0.3$ mm and with the scrolled, non-peripheral, (a) planar and (b) non-planar upper DMD	129
5.26	Velocity contour, streamline and isotherm of the AH flow in the AC with the cornea indentation of $a_I = 0.3$ mm and with the non-scrolled, non-peripheral, (a) planar and (b) non-planar lower DMD	130
5.27	Velocity contour, streamline and isotherm of the AH flow in the AC with the cornea indentation of $a_I = 0.3$ mm and with the scrolled, non-peripheral, (a) planar and (b) non-planar lower DMD	131
5.28	Problem domain and boundary conditions of the AH flow in the AC when the patient is in a sleeping position	132
5.29	Velocity contour of the AH flow in the AC with the patient in a sleeping position by (a) Kumar <i>et al.</i> (2006) and (b) Ooi (2009).	135

5.30	Velocity contour, streamline and isotherm of the AH flow in the AC with the patient in a sleeping position	135
5.31	Velocity contour, streamline and isotherm of the AH flow in the AC with non-scrolled, non-peripheral, (a) planar and (b) non-planar upper DMD when the patient is in sleeping position	136
5.32	Velocity contour, streamline and isotherm of the AH flow in the AC with the non-scrolled, peripheral, (a) planar and (b) non-planar upper DMD when the patient is in sleeping position	137
5.33	Velocity contour, streamline and isotherm of the AH flow in the AC with scrolled, non-peripheral, (a) planar and (b) non-planar upper DMD when the patient is in sleeping position	138
5.34	Velocity contour, streamline and isotherm of the AH flow in the AC with scrolled, peripheral, (a) planar and (b) non-planar upper DMD when the patient is in sleeping position	139
6.1	Schematic diagram of the VH in the VC for (a) between two rigid walls and (b) a stationary wall and an upper wall moving with a constant velocity	143
6.2	Mesh of the VH flow in the VC with mesh 1	148
6.3	The u - velocity profiles of the VH along a vertical line passing through the geometric centre of the VC with mesh1, mesh 2, mesh 3, mesh 4 and mesh 5 for (a) Case 1 and (b) Case 2	148
6.4	Velocity contour of the VH flow in the VC for Case 1 by (a) the present source code and (b) COMSOL Multiphysics 5.0	150
6.5	Streamline plots of the VH flow in the VC for Case 1 by (a) the present source code and (b) COMSOL Multiphysics 5.0	151

6.6	Velocity contour of the VH flow in the VC for Case 2 by (a) the present source code and (b) COMSOL Multiphysics 5.0	151
6.7	Streamline plots of the VH flow in the VC for Case 2 by (a) the present source code and (b) COMSOL Multiphysics 5.0	152
6.8	(a) Non-scrolled detached retina and (b) scrolled detached retina	153
6.9	Problem domain and boundary conditions of the liquefied VH flow in the VC for Case 1 with RRD at the bottom wall	153
6.10	Extracts the piecewise-linear geometry nodes for the scrolled RRD	154
6.11	Mesh for the scrolled RRD	154
6.12	Velocity contour of the VH flow in the VC with non-scrolled RRD for (a) $h_0 = 1$ mm , (b) $h_0 = 2$ mm and (c) $h_0 = 3$ mm .	156
6.13	Streamline of the VH flow in the VC with non-scrolled RRD for (a) $h_0 = 1$ mm , (b) $h_0 = 2$ mm and (c) $h_0 = 3$ mm	157
6.14	Velocity contour of the VH flow in the VC with scrolled RRD for (a) $h_0 = 1$ mm , (b) $h_0 = 2$ mm and (c) $h_0 = 3$ mm	158
6.15	Streamline of the VH flow in the VC with scrolled RRD for (a) $h_0 = 1$ mm , (b) $h_0 = 2$ mm and (c) $h_0 = 3$ mm	159
6.16	Velocity contour of the VH flow in the VC with opposite non-scrolled RRD for (a) $h_0 = 1$ mm , (b) $h_0 = 2$ mm and (c) $h_0 = 3$ mm	160
6.17	Streamline of the VH flow in the VC with opposite non-scrolled RRD for (a) $h_0 = 1$ mm , (b) $h_0 = 2$ mm and (c) $h_0 = 3$ mm	161

6.18	Velocity contour of the VH flow in the VC with opposite scrolled RRD for (a) $h_0 = 1$ mm , (b) $h_0 = 2$ mm and (c) $h_0 = 3$ mm	162
6.19	Streamline of the VH flow in the VC with opposite scrolled RRD for (a) $h_0 = 1$ mm , (b) $h_0 = 2$ mm and (c) $h_0 = 3$ mm	163
6.20	Velocity profile of the VH flow in the VC with non-scrolled RRD along a vertical line at (a) $x = -0.5$ mm , (b) $x = 0$ mm and (c) $x = 0.5$ mm	164
6.21	Velocity profile of the VH flow in the VC with scrolled RRD along a vertical line at (a) $x = -0.5$ mm , (b) $x = 0$ mm and (c) $x = 0.5$ mm .	165
6.22	Velocity profile of the VH flow in the VC with opposite non-scrolled RRD along a vertical line at (a) $x = -0.5$ mm , (b) $x = 0$ mm and (c) $x = 0.5$ mm .	166
6.23	Velocity profile of the VH flow in the VC with opposite scrolled RRD along a vertical line at (a) $x = -0.5$ mm , (b) $x = 0$ mm and (c) $x = 0.5$ mm	167
6.24	Problem domain and boundary conditions of the liquefied VH flow in the VC for Case 2 with RRD at the bottom wall	168
6.25	Comparison of the velocity profile of the VH flow which driven by 15°s^{-1} saccadic eye movement along a vertical line at $x = 0$ mm in the VC for cases with fluid entering and without fluid entering	170
6.26	Comparison of the velocity profile of the VH flow which driven by 100°s^{-1} saccadic eye movement along a vertical line at $x = 0$ mm in the VC for cases with fluid entering and without fluid entering	171

- 6.27 Comparison of the velocity profile of the VH flow which driven by $200\text{ }^{\circ}\text{s}^{-1}$ saccadic eye movement along a vertical line at $x=0\text{ mm}$ in the VC for cases with fluid entering and without fluid entering 171
- 6.28 Comparison of the velocity profile of the VH flow which driven by $400\text{ }^{\circ}\text{s}^{-1}$ saccadic eye movement along a vertical line at $x=0\text{ mm}$ in the VC for cases with fluid entering and without fluid entering 171
- 6.29 Velocity contour of the VH flow, which driven by the saccadic eye movement with velocity $400\text{ }^{\circ}\text{s}^{-1}$, in the VC with non-scrolled RRD for (a) $h_0 = 1\text{ mm}$, (b) $h_0 = 2\text{ mm}$ and (c) $h_0 = 3\text{ mm}$ 172
- 6.30 Streamline of the VH flow, which driven by the saccadic eye movement with velocity $400\text{ }^{\circ}\text{s}^{-1}$, in the VC with non-scrolled RRD for (a) $h_0 = 1\text{ mm}$, (b) $h_0 = 2\text{ mm}$ and (c) $h_0 = 3\text{ mm}$ 173
- 6.31 Velocity contour of the VH flow, which driven by the saccadic eye movement with velocity $400\text{ }^{\circ}\text{s}^{-1}$, in the VC with scrolled RRD for (a) $h_0 = 1\text{ mm}$, (b) $h_0 = 2\text{ mm}$ and (c) $h_0 = 3\text{ mm}$ 174
- 6.32 Streamline of the VH flow, which driven by the saccadic eye movement with velocity $400\text{ }^{\circ}\text{s}^{-1}$, in the VC with scrolled RRD for (a) $h_0 = 1\text{ mm}$, (b) $h_0 = 2\text{ mm}$ and (c) $h_0 = 3\text{ mm}$ 175
- 6.33 Velocity contour of the VH flow, which driven by the saccadic eye movement with velocity $400\text{ }^{\circ}\text{s}^{-1}$, in the VC with opposite non-scrolled RRD for (a) $h_0 = 1\text{ mm}$, (b) $h_0 = 2\text{ mm}$ and (c) $h_0 = 3\text{ mm}$ 176

- 6.34 Streamline of the VH flow, which driven by the saccadic eye movement with velocity $400 \text{ }^\circ\text{s}^{-1}$, in the VC with opposite non-scrolled RRD for (a) $h_0 = 1 \text{ mm}$, (b) $h_0 = 2 \text{ mm}$ and (c) $h_0 = 3 \text{ mm}$ 177
- 6.35 Velocity contour of the VH flow, which driven by the saccadic eye movement with velocity $400 \text{ }^\circ\text{s}^{-1}$, in the VC with opposite scrolled RRD for (a) $h_0 = 1 \text{ mm}$, (b) $h_0 = 2 \text{ mm}$ and (c) $h_0 = 3 \text{ mm}$ 178
- 6.36 Streamline of the VH flow, which driven by the saccadic eye movement with velocity $400 \text{ }^\circ\text{s}^{-1}$, in the VC with opposite scrolled RRD for (a) $h_0 = 1 \text{ mm}$, (b) $h_0 = 2 \text{ mm}$ and (c) $h_0 = 3 \text{ mm}$ 179
- 6.37 Velocity profile of the VH flow, which driven by the saccadic eye movement with velocity $400 \text{ }^\circ\text{s}^{-1}$, in the VC with non-scrolled RRD along a vertical line at (a) $x = -0.5 \text{ mm}$, (b) $x = 0 \text{ mm}$ and (c) $x = 0.5 \text{ mm}$ 180
- 6.38 Velocity profile of the VH flow, which driven by the saccadic eye movement with velocity $400 \text{ }^\circ\text{s}^{-1}$, in the VC with scrolled RRD along a vertical line at (a) $x = -0.5 \text{ mm}$, (b) $x = 0 \text{ mm}$ and (c) $x = 0.5 \text{ mm}$ 181
- 6.39 Velocity profile of the VH flow, which driven by the saccadic eye movement with velocity $400 \text{ }^\circ\text{s}^{-1}$, in the VC with opposite non-scrolled RRD along a vertical line at (a) $x = -0.5 \text{ mm}$, (b) $x = 0 \text{ mm}$ and (c) $x = 0.5 \text{ mm}$ 182
- 6.40 Velocity profile of the VH flow, which driven by the saccadic eye movement with velocity $400 \text{ }^\circ\text{s}^{-1}$, in the VC with opposite scrolled RRD along a vertical line at (a) $x = -0.5 \text{ mm}$, (b) $x = 0 \text{ mm}$ and (c) $x = 0.5 \text{ mm}$ 183
- 6.41 The domain of the liquefied VH flow pass through RRD and SB 184

6.42	The domain of the liquefied VH flow pass through RRD and SB when the SB is placed on (a) $x = -L/2$ and (b) $x = L/2$.	186
6.43	Mesh for the liquefied VH in the VC with RRD and SB	186
6.44	Velocity contour and streamline of the VH flow in the VC with RRD which has not been treated by SB	188
6.45	Velocity contour of the VH flow in the VC with RRD and has been treated by SB with size $a = 0.5$ mm and (a) $b = 0.5$ mm, (b) $b = 0.7$ mm and (c) $b = 0.9$ mm	189
6.46	Streamline of the VH flow in the VC with RRD and has been treated by SB with size $a = 0.5$ mm and (a) $b = 0.5$ mm, (b) $b = 0.7$ mm and (c) $b = 0.9$ mm	190
6.47	Velocity contour of the VH flow in the VC with RRD and has been treated by SB with size $a = 0.7$ mm and (a) $b = 0.5$ mm, (b) $b = 0.7$ mm and (c) $b = 0.9$ mm	191
6.48	Streamline of the VH flow in the VC with RRD and has been treated by SB with size $a = 0.7$ mm and (a) $b = 0.5$ mm, (b) $b = 0.7$ mm and (c) $b = 0.9$ mm	192
6.49	Velocity contour of the VH flow in the VC with RRD and has been treated by SB with size $a = 0.9$ mm and (a) $b = 0.5$ mm, (b) $b = 0.7$ mm and (c) $b = 0.9$ mm	193
6.50	Streamline of the VH flow in the VC with RRD and has been treated by SB with size $a = 0.9$ mm and (a) $b = 0.5$ mm, (b) $b = 0.7$ mm and (c) $b = 0.9$ mm	194
6.51	Velocity contour of the VH flow in the VC with RRD and has been treated by SB with size $a = 0.9$ mm and $b = 0.5$ mm at position (a) shift to the left and (b) shift to the right of y -axis	195
6.52	Streamline of the VH flow in the VC with RRD and has been treated by SB with size $a = 0.9$ mm and $b = 0.5$ mm at position (a) shift to the left and (b) shift to the right of y -axis	196

LIST OF SYMBOLS

A_{e_i}	-	surface area of a finite element
AC	-	Anterior Chamber
AH	-	Aqueous Humour
CS	-	control surface
CV	-	control volume
DOF	-	degree of freedom
DM	-	Descemet's Membrane
DMD	-	Descemet's Membrane Detachment
e	-	internal energy
e_i	-	element i
E	-	energy per unit mass
\vec{F}_{body}	-	body force
$\vec{F}_{surface}$	-	surface force
$F(\vec{x}, t)$	-	extensive property of a system
$f(\vec{x}, t)$	-	extensive property of a system per unit volume
\vec{g}	-	gravitational force
h	-	specific enthalpy
k	-	thermal conductivity
m	-	mass

\vec{n}	-	normal unit vector
$N_j^{e_i}$	-	shape function of 1D line element
P	-	pressure
P_a	-	normal atmospheric pressure
P_h	-	hydrostatic pressure
P_m	-	mean/dynamic pressure
Pr	-	Prandtl number
\vec{q}	-	heat flux vector
Q	-	internal heat source
RTT	-	Reynold Transport Theorem
RD	-	Retinal Detachment
RRD	-	Rhematogeneous Retinal Detachment
SB	-	Scleral Buckling
t	-	time
T	-	temperature of the fluid
T_p	-	temperature at the iris
T_c	-	temperature of the cornea
T_∞	-	temperature of the ambient medium
U	-	a typical velocity in human eye
U_0	-	a constant velocity
U_w	-	a velocity at the wall
u	-	velocity component of fluid phase in x -direction
v	-	velocity component of fluid phase in y -direction
$V(t)$	-	material volume

VH	-	Vitreous Humour
VC	-	Vitreous Cavity
w	-	velocity component of fluid phase in z -direction
$w_m(x)$	-	weight function
w_i	-	weight of Gauss Quadrature
μ	-	dynamic viscosity coefficient
ν	-	kinematic viscosity coefficient
σ_{ij}	-	stress tensor
τ_{ij}	-	viscous stress tensor
τ	-	tolerance value
ε_{ij}	-	strain rate tensor
β	-	thermal expansion
ρ	-	density of the fluid
$\psi_k^{e_i}$	-	shape function for 2D linear element
$\phi_j^{e_i}$	-	shape function for 2D quadratic element
δ_{ij}	-	Kronecker Delta
Γ_{e_i}	-	boundary curve of a finite element

LIST OF APPENDICES

APPENDIX	TITLE	PAGE
A	Evaluation of Shape Functions for the Taylor-Hood Element in Maple	217
B	Area of a Triangular Element	220
C	Gauss Quadrature Points	221
D	Evaluation of the Transformation Equations Using Maple	223
E	Dimensionless Governing Equations	225
F	Finite Element Source Code	227
G	Piecewise-linear Geometry Input of DMD	248
H	Algorithms	256
I	List of Published Scientific Papers	262
J	List of Conferences Participated	264

CHAPTER 1

INTRODUCTION

1.1 Introduction

The eye is an organ that enables a human being to see. The eye helps the human being to understand and interpret the world around them. Descemet's membrane detachment (DMD) and Rhegmatogenous retinal detachment (RRD) are diseases of the eye that might cause blindness. The formation of both diseases involves the fluid flow inside the eye. However, the small dimension of the human eye and the extremely low velocities of the ocular fluid flow make it difficult for in-vivo study on the human eye. Therefore, many aspects of fluid flow within the human eye have not yet been fully examined or quantitatively explained. Alternative, computational simulation of the ocular fluid flow is applied to understand the flow mechanisms in the human eye, especially when the eye has DMD and RRD. In this chapter, the background of the problem is explained. Then, the statement of the problem and the objectives of this research are highlighted. Some limitations and scopes of the research are also stated here. Finally, the significance of the study and the outline of the thesis are presented.

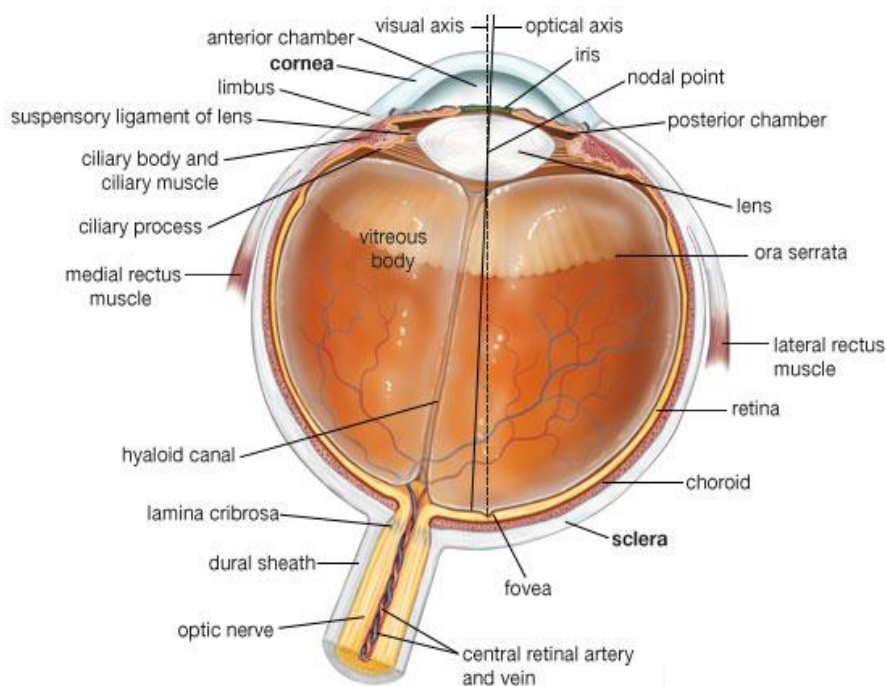


Figure 1.1 Structure of Human Eye (Kara, 2011).

1.2 Research Background

The clear dome like surface that exists at the front of a human eye is called as the cornea. The cornea covers the iris and the pupil, as shown in Figures 1.1. The region bounded by the cornea, the iris and the pupil is known as the anterior chamber (AC). There are three main layers and two auxiliary layers contained in the cornea, those are the epithelium, the stroma, the endothelium, the Browman layer and the Descemet membrane (DM). DM is a layer lies between the stroma and the endothelium layer of the cornea. DMD happens when DM is separated away from the stroma by the aqueous humour (AH) that flows into the space between the DM and the stroma through a tear or break on the DM. The detachment of DM may have serious adverse effects to the vision function of the human eye. Planar or non-planar, scrolled or non-scrolled and peripheral or non-peripheral with central corneal involvement are the types of DMD (Mulhern *et al.*, 1996; Menezo *et al.*, 2002; Potter and Zalatimo, 2005).

DMD due to cataract surgery, iridectomy, trabeculectomy, corneal transplantation, deep lamellar keratoplasty, holmium laser sclerostomy, alkali burn and viscocanalostomy have been reported by Mulhern *et al.* (1996), Potter and Zalatimo (2005), Hirano *et al.* (2002) and Ünlü and Aksünger (2000). Sevillano *et al.* (2008) reported the technique of curing of DMD caused by cataract surgery with sulphur hexafluoride injection. Potter and Zalatimo (2005) presented the case of treating scrolled DMD by injecting fourteen percent of intracameral perfluoropropane (C_3F_8) into AC.

Recently, Couch and Baratz (2009), investigated two cases of delayed bilateral DM and in one eye it was fixed surgically and the other eye improved spontaneously. They estimated that the spontaneous reattachment happens because of the buoyancy effects which cause the AH flow in AC. The spontaneous reattachment of DM has been supported by some observational and anecdotal evidences (Marcon *et al.*, 2002; Nouri *et al.*, 2002; Couch and Baratz, 2009; Ismail *et al.*, 2012). Fitt and Gonzalez (2006) had shown that under normal conditions the buoyancy effects due to the temperature gradient in AC enhance the AH to flow. Ismail *et al.* (2012) intended to explain the phenomena of the spontaneous reattachment and thus, developed a mathematical model to describe the AH flow in AC with DMD. They concluded that the temperature difference across the eye and the orientation of the patient may control the clinical outcomes for the DMD. Nonetheless, the model developed by Ismail *et al.* (2012) was based on the lubrication theory limit, which include a lot of simplification. Consequently, the model may only partially illuminate the behaviour of the fluid flow in AC. Therefore, in this thesis, fluid mechanical theory is applied to model the fluid flow in AC, in order to study the effect of the detached DM on the behaviour of the AH flow in AC.

DMD is categorized as planar or non-planar, scrolled or non-scrolled and peripheral or non-peripheral. Mackool and Holtz (1977) reported that non-planar detachments were difficult to reattach spontaneously compared to planar DMD. Assia *et al.* (1995) concluded that non-scrolled and non-planar DMD might be able to reattach spontaneously. And, Marcon *et al.* (2002) claimed that non-planar and non-scrolled DMD often reattach spontaneously if given enough time. These imply that the type of DMD may affect the AH flow, thus influencing the occurrence of the

spontaneous reattachment of DMD in AC. Therefore, a model is developed is used to analyse the effect of different types of DMD to the fluid flow in AC. As, Amini and Barocas (2009) had shown that cornea indentation changed the contour of the iris and altered the AC angle, which is the angle between the iris and the cornea. Hence, it is possible for the indentation of cornea to affect the AH flow, which is driven by the temperature difference in the AC of human eye. Thus, the effects of the cornea indentation of the AH flow dynamics are investigated as well. In addition, the DMD problem during the indentation is also discussed in this study.

Retinal detachment happens in human eye when retina peels away from the cellular layer, which is called choroid and located between the retina and the sclera (Cook *et al.*, 1995; Dyson *et al.*, 2004; Daniel and Wilkinson, 2009; Ismail, 2013). Depending on the mechanism of subretinal fluid accumulation, retinal detachment can be categorized into Rhegmatogenous, Exudative and Tractional (Dyson *et al.*, 2004; Daniel and Wilkinson, 2009; Ismail, 2013). Rhegmatogenous Retinal Detachment (RRD) may occur when the liquefied vitreous humour (VH) flow through a tear or break into the space between the retina and the retinal pigment epithelium. Consequently, the patient will become permanently blind in the affected eye because the detached retina lost the ability to function. Exudative retinal detachment and Tractional retinal detachment happen without a retina break. Exudative retinal detachment occurs when retina is pulled away by subretinal fluid which produced by a tumour or an inflammatory disorder. The retinal detachments caused by proliferative diabetic retinopathy, cicatricial retinopathy of prematurity, proliferative sickle retinopathy and penetrating trauma are called as Tractional retinal detachment.

Retina, sclera and choroid are the main layers of human eyes as shown in Figure 1.1. Retina is the innermost layer of these three layers. Sclera is the outermost layer of the human eye and choroid is the intermediate layer. Retina is one of the most important parts of the human eye and may be considered to be a part of the brain. It is a complex nervous structure that is responsible for the visual process. Retina has three layers of nerve cells and two layers of synaptic connections (Davson, 1980; Kolb, 2003; Ismail, 2013). The nerve cell layers are photoreceptors, inner nuclear and ganglion cells. The photoreceptor layer is the outermost layer in the retina against the pigment epithelium and the choroid, and consists of the sensitive layer of rods and cones. The

nuclear layer, which consists of 1 to 4 types of horizontal cells, 11 types of bipolar cells and 22 to 30 types of amacrine cells, lies between the photoreceptors and the ganglion cells. Then, in the innermost layer of the retina contains 20 types of the ganglion cells (Pirenne, 1967; Davson, 1980; Kolb, 2003).

Retina is also an important part in the visualization process because in the centre of the retina is a region with the highest visual acuity and it is named as fovea (Pirenne, 1967; Davson, 1980). When light passes through the cornea and the pupil to the lens, then it will be focused onto the fovea at the retina. To reach the photoreceptors, the light has to travel along the thickness of the retina. When the photoreceptors of the human eye receive the light, the light energy is transduced into electrical signals. Then, the electrical signals transmit back to the amacrine and the ganglion cells and the signals are propagated to the optic nerve by the axons of the ganglion cells. The optic nerve takes the ganglion cell axons to the brain for further visual processing (Pirenne, 1967; Davson, 1980; Kolb, 2003; Ismail, 2013).

RRD happens when the liquefied VH flows through a tear or break on the surface of the retina into the space between the retina and the retinal pigment epithelium (Daniel and Wilkinson, 2009; Ismail, 2013). The movement of the fluid in the subretinal space will pull the retina away from the choroid. To realize the mechanisms of the formation of the RRD, a number of researchers investigated the RRD problem clinically. Fatt and Shantinath (1971) reported that the RRD happen when there exist a hole in the retina. The mechanisms of the subretinal fluid in the pigment epithelium were discussed by Quintyn and Brasseur (2004). The recent trends in the managements of RRD can be found in the report prepared by Sodhi *et al.* (2008). However, few researchers studied the RRD problem mathematically. Gonzalez (2004) modelled the retinal detachment problem mathematically by assuming the detached retina as a free surface and the surface tension effect was taken into account. The effect of shear stress was neglected. In the study, the author found that the surface tension affect the progress of the retinal detachment.

More recently, Ismail (2013) considered the effect of pressure gradient to the fluid flow in the detached retina. A paradigm mathematical model was developed and solved by asymptotic method. The behaviour and the deformation of the detached

retina were analysed. So far, some pioneering experimental and analytical researches had been performed, but the findings are short of data for the movements of liquefied vitreous in the RRD. Besides that, the results obtained in the previous researches were probably incomplete. In those researches, assumptions were made to simplify the governing equations, so that the analytical solutions can be determined. Thus, the obtained results cannot fully represent the actual fluid flow in the human eye with RRD. In this research, full two dimensional Navier-Stokes equations are used to represent the fluid flow in VC with RRD. Finite element method is applied to obtain the numerical solutions and used to analyse the complex flow field in the eye with a detached retina.

There are various treatments for RRD and the most common treatment for uncomplicated RRD is scleral buckling (SB) (Sodhi *et al.*, 2008; Ismail, 2013). A SB is a piece of fascia lata, palmaris tendon, semi-hard plastic, silicone sponge, rubber, or donor sclera that ophthalmologist places on the outside of the sclera or the white of the eye to treat the RRD. Silicone is the most popular material used to make the sclera buckle because silicon is nontoxic and nonallergenic (Daniel and Wilkinson, 2009). To relieve the traction on the retina, the SB will be sewn within the sclera. Therefore, the retinal tear will settle against the wall of the eye, so that the chorioretinal adhesions can be formed to seal the retinal break (Daniel and Wilkinson, 2009; Ismail, 2013).

SB has gained attention of many researchers due to its popularities. The anatomic and visual results in an asymptomatic clinical RRD repaired by SB were reported by Greven *et al.* (1999). Foster *et al.* (2010) found that rapid eye movements facilitate more rapid retinal reattachment. They have used a commercial software, the COMSOL Multiphysics to simulate the influence of the SB on the flow of subretinal fluid in a physical model of retinal detachment. The physical principles behind the SB surgery were analysed. Motivated by the above study, in the present work, the effect of the SB on the movement of liquefied VH in the subspace between the detached retina and choroid is investigated.

1.3 Statement of the Problem

As explained earlier, the flow data inside AC and VC are difficult to obtain due to the small scale of both chambers. In addition, the complexities of flow measurements inside a living eye also are obstacles for obtaining the data. As an alternative method, computational simulation of the flow can be very useful in producing the needed understanding of the flow mechanisms inside the AC and VC. In this way, the behaviour of the fluid flow when the human eye has DMD and RRD diseases can be comprehended. Further, most of the studies in the literature were conducted by using perturbation or asymptotic methods and were incapable to solve the complex fluid flow model used to describe the fluid flow in the AC with DMD and the VC with RRD respectively. Numerical method is needed. Therefore, finite element method is proposed in this study to obtain the numerical results of the flow. Although the DMD is a rare ocular problem, it may induce the loss of vision. The influence of the type of DMD, the cornea indentation and the position of the patient, to the flow of AH in AC may improve the occurrence of the spontaneous reattachment phenomena. Apart from that, as the SB treatment is the most common way to treat RRD, the response of the liquefied VH to SB is valuable in order to increase the success rate of the treatment.

Some questions need to be answered in order to accomplish this study. How to develop the governing equations that describe the behaviour of the fluid flow in the AC and the VC respectively? How to model the fluid flow in the AC with DMD and the VC with RRD respectively? Is the finite element method able to solve the corresponding governing equations? How does AH flow behave in the AC with DMD? In what way do the type of the DMD, the cornea indentation and the position of the patient influence the AH flow in the AC? How does the liquefied VH flow behave in the VC with RRD? And what are the effects of the SB of the fluid field in VC with RRD? This research aims to answer these questions successfully.

1.4 Objectives of the Study

The aim of this research is to investigate the characteristics of fluid flow in the human eye with DMD and RRD respectively. This includes the construction of suitable mathematical models of the flow by considering an appropriate governing equation and the boundary conditions and then solve the resulting equations using finite element method. Specifically, the objectives of this study are:

1. To develop the appropriate governing equations that describe the fluid flow in the AC with DMD and the VC with RRD respectively.
2. To develop a source code in MATLAB in order to solve the corresponding governing equations by using finite element method.
3. To investigate the AH flow, driven by the temperature gradient, in the AC with DMD.
4. To investigate the influence of the types of DMD, the indentation of the cornea and the position of the patient on the fluid behaviour in the AC.
5. To investigate the fluid flow in the human eye with RRD, as a simple thin layer channel flow where a detachment is present in two cases:
 - (i) Both upper and bottom walls are not moving
 - (ii) With a moving upper wall
6. To investigate the influence of the SB, which is used to treat RRD, on the liquefied VH flow in the subspace between the detached retina and choroid.

1.5 Scope of the Study

The fluid flow in the human eye with DMD and RRD are analysed. The fluid in the AC and VC is considered as an incompressible Newtonian fluid. The governing equations are solved numerically by using finite element method. The MATLAB 2013

software is used for the computation of numerical results as well as for plotting the graph for visual display. The fluid flow in the AC which is driven by the temperature gradient, for the DMD problem is considered. The types of DMD to be considered in this thesis are planar, non-planar, scrolled and non-scrolled. Additionally, the effects of the indentation of the cornea and the position of the patient in the fluid flow in the AC are analysed. Normally, retinal detachment can be characterized as rhegmatogenous, tractional and exudative. The present study only focus on the RRD problem. This study is restricted to the effects of SB treatment. The effect of the scleral buckle on the outflow of the subretinal fluid through a hole in the retina is discussed.

1.6 Significance of the Study

The exact mechanism of RRD is complex and the picture of its development remains incomplete. Previous researches show only parts of the full puzzle. It is important to comprehend the development of the retinal detachment so that a new treatment method can be developed. It is hard to study the formation of the RRD in the real human eye. As a result, information on the RRD's formation is lacking. Thus, results obtained in this research fill up the incompleteness of the information. Wong *et al.* (1999) reported annual incidences of RRD in Singapore based on ethnicity. The results showed that 11.6 cases per 100,000 in the Chinese population, 7 cases among the Malays, and 3.9 cases for the Indians.

The annual incidence of RRD of 18.2 cases per 100,000 people, in the Netherlands was reported by Van de Put *et al.* (2013). The result showed that peak incidence occurred for 55-59 year olds with 52.5 cases per 100,000 people. The data show that population of RRD is huge. Therefore, a full understanding of the RRD's formation is essential for the prevention. Also as sclera buckling is the most common treatment for the RRD, it is important to increase the percentage of the successful treatment. The understanding of the dynamic effect of SB on retinal detachment is essential to reduce the percentage of treatment failure.

DMD is an uncommon disease in the eye, mostly occurs during cataract extraction. 50% of people between ages 65 and 74 and 70% of people over age 75 have cataract (Kara, 2011). Cloudy vision, glare, colour vision problems and double vision are some of the symptoms of cataract. To treat cataracts, surgery is normally performed to remove the affected lens and replace it by an artificial lens within the eye. The mechanism that causes the DM to tear from the stroma is unclear and the most popular hypothesis is that it is caused by the mechanical force applied to the cornea during surgery. This allows the AH to flow through the tear into the space between DM and the stroma and generate full DMD. An understanding of the role of the fluid flow in the devolving of full DMD is important. This will assist ophthalmologists to figure out better treatment to heal DMD.

The finite element analysis used in this research is originally applied in the structural engineering. The application of the method in this study explores the technique in the field of fluid mechanics. Furthermore, numerical model obtained in this research is expected to be also suitable for other fluid problems such as fluid flow in a sphere or fluid flow inside the Earth. In addition, the numerical results obtained in this study can be used to validate new results obtained.

1.7 Outline of the Thesis

This thesis contains seven chapters are included in this thesis. The statement of problems, objectives, scope and significance of the research make up the introduction as Chapter 1. The literature review of the interested problems is elaborated and established in Chapter 2. There are two sections in the chapter, the fluid flow in the AC and the fluid flow in the VC. The achievements of researchers on fluid flow in the human eye as well as the methods that used by them to accomplish the task are presented. The implementation of finite element method in solving the proposed problem is explained in Chapter 3 and 4. The fundamental procedures of using finite element method are given in Chapter 3. In additions, the Taylor-Hood element used to

mesh the domain and the iteration manner applied to solve the nonlinear equation are also explained in the chapter. The computer implementation of finite element method has been explored in Chapter 4. The verification of the source code also has been done and presented in the chapter.

The effect of the DMD to the fluid flow in AC is studied in Chapter 5. The effect of the different types of DMD, the shape of the AC and the position of the patient to the fluid flow are discussed. In Chapter 6, the RRD problem is demonstrated. Two cases are considered: (1) both upper and bottom walls are not moving and (2) with a moving upper wall, in order to analyse the behaviour of the fluid flow in the human eye with RRD. The alteration of the fluid flow due to the type of the RRD, the change of the gravity direction and the indented VC by the SB is explored and discussed. In the final chapter of this thesis, the summary of the research is presented. Additionally, some suggestions for the future study based on the present research are highlighted.

1.8 Conclusions

In this present chapter, the background of the problem, the statement of the problem, the objectives of the research, the scope of the research, significance of the study and the outline of the thesis are presented. The difficulties for in-vivo study on human eye lead researchers to use computational simulation of the ocular fluid flow to understand the flowing mechanical of the fluid in the human eye, especially in respect to the diseases of DMD and RRD. Six objectives are proposed to achieve in this thesis.

REFERENCES

- Abouali, O., Modareszadeh, A., Ghaffarieh, A., and Tu, J. (2012a). Investigation of saccadic eye movement effects on the fluid dynamic in the anterior chamber. *Journal of Biomechanical Engineering* 134.
- Abouali, O., Modareszadeh, A., Ghaffariyeh, A., and Tu, J. (2012b). Numerical simulation of the fluid dynamics in vitreous cavity due to saccadic eye movement. *Medical Engineering & Physics* 34 (6):681-692.
- Amini, R. (2010). *Iris Biomechanics in Health and Disease*. Doctor of Philosophy, Faculty of the Graduate School, The University Of Minnesota.
- Amini, R., and Barocas, V. (2009). Anterior chamber angle opening during corneoscleral indentation: The mechanism of whole eye globe deformation and the importance of the limbus. *Investigative Ophthalmology & Visual Science* 50 (11):5288-5294.
- Amini, R., and Barocas, V. (2010). Reverse pupillary block slows iris contour recovery from corneoscleral indentation. *Journal of Biomechanical Engineering* 132 (7).
- Anagnoste, S. R., Scott, I. U., Murray, T. G., Kramer, D., and Toledano, S. (2000). Rhegmatogenous retinal detachment in retinoblastoma patients undergoing chemoreduction and cryotherapy. *American Journal of Ophthalmology* 129 (6).
- Anderson, D. R. (1979). Corneal indentation to relieve glaucoma. *American Journal of Ophthalmology* 88 (6):1091-1093.
- Anderson, J. D. (1995). *Computational Fluid Dynamics*. Singapore: McGraw-Hill, INC.
- Argyris, J. H., and Scharpf, D. W. (1970). Finite element formulation of the incompressible lubrication problem. *Nuclear Engineering and Design* 11 (2):225-229.

- Assia, E. I., Levkovich-Verbin, H., and Blumenthal, M. (1995). Management of descemet's membrane detachment. *Journal of Cataract and Refractive Surgery*. 21:714-717.
- Avtar, R., and Srivastava, R. (2006). Modelling the flow of aqueous humor in anterior chamber of the eye. *Applied Mathematics and Computation* 181:1336-1348.
- Baker, A. J. (1974). Finite element solution theory for three-dimensional boundary flows. *Computer Methods in Applied Mechanics and Engineering* 4 (3):367-386.
- Balachandran, R. K. (2010). *Computational Modeling Of Drug Transport In The Posterior Eye*. Doctor of Philosophy, The Faculty of the Graduate School, The University Of Minnesota.
- Batchelor, G. K. (2000). *An Introduction to Fluid Dynamics*. New York: Cambridge University Press.
- Bathe, K. J. (1996). *Finite Element Procedures*. USA: Prentise-Hall, Inc.
- Beavers, G. S., and Joseph, D. D. (1967). Boundary conditions at a naturally permeable wall. *Journal of Fluid Mechanics* 30:197-207.
- Beswick, J. A., and McCulloch, C. (1956). Effect of hyaluronidase on the viscosity of the aqueous humour. . *British Journal of Ophthalmology* 40:545-548.
- Brenner, S. C., and Scott, L. R. (2008). *The Mathematical Theory of Finite Element Methods*. USA: Springer.
- Brezzi, F., and Fortin, M. (1991). *Mixed and Hybrid Finite Element Methods*. New York Springer-Verlag.
- Canning, C. R., Greaney, M. J., Dewynne, J. N., and Fitt, A. D. (2002). Fluid flow in the anterior chamber of a human eye. *IMA Journal of Mathematics Applied in Medicine and Biology*. 19:31-60.
- Carel, R. S., Korczyn, A. D., Rock, M., and Goya, I. (1984). Association between ocular pressure and certain health parameters. *Ophthalmology* 91:311-314.
- Causin, P., Guidoboni, G., Malgaroli, F., Sacco, R., and Harris, A. (2016). Blood flow mechanics and oxygen transport and delivery in the retinal microcirculation: multiscale mathematical modeling and numerical simulation. *Biomech Model Mechanobiol* 15:525-542.
- Cengel, Y. A., and Ghajar, A. J. (2015). *Heat and Mass transfer: Fundamental & Applications*. New York: McGraw-Hill Education.

- Chang, P. Y., Yang, C. M., Yang, C. H., Huang, J. S., Ho, T. C., Lin, C. P., Chen, M. S., Chen, L. J., and Wang, J. Y. (2005). Clinical characteristics and surgical outcomes of pediatric rhegmatogenous retinal detachment in Taiwan. *American Journal of Ophthalmology* 139 (6):1067-1072.
- Charles, M. W., and Brown, N. (1975). Dimensions of the human eye relevant to radiation protection. *Physics in Medicine and Biology* 20:202-218.
- Chignell, A. H. (1974). Retinal detachment surgery without drainage of subretinal fluid. *American Journal of Ophthalmology* 77 (1):1-5.
- Chung, T. J., and Chiou, J. N. (1976). Analysis of unsteady compressible boundary layer flow via finite elements. *Computers & Fluids* 4 (1):1-12.
- Cicekli, U. (2003). *Computational Model For Heat Transfer In The Human Eye Using The Finite Element Method*. Master of Science, Civil Engineering, Louisiana State University.
- Clemens, S., Kroll, P., Stein, E., Wagner, W., and Wriggers, P. (1987). Experimental studies on the disappearance of subretinal fluid after episcleral buckling procedures without drainage. *Graefe's Archive for Clinical and Experimental Ophthalmology* 225:16-18.
- Cook, B., Lewis, G. P., Fisher, S. K., and Adler, R. (1995). Apoptotic photoreceptor degeneration in experimental retinal-detachment. *Investigative Ophthalmology & Visual Science* 36 (6):990-996.
- Couch, S. M., and Baratz, K. H. (2009). Delayed, bilateral descemet's membrane detachments with spontaneous resolution: Implications for nonsurgical treatment. *Cornea* 28:1160-1163.
- Cowper, G. R. (1973). Gaussian quadrature formulas for triangles. *International Journal for Numerical Methods in Engineering* 7 (3):405-408.
- Crawford, K. S., Kaufman, P. L., and Bitto, L. Z. (1990). The role of the iris in accommodation of rhesus monkeys. *Investigative Ophthalmology & Visual Science* 31:2185-2190.
- Daniel, A. B., and Wilkinson, C. P. (2009). *Retinal Detachment : Principles and Practice: Principles and Practice*. USA: Oxford University Press.
- Darren, E. (2014). *Locally Optimal Delaunay-refinement and Optimisation-based Mesh Generation*. Doctor of Philosophy, School of Mathematics and Statistics, The University of Sydney.
- David, P., and Chaim, G. (1992). *Fluid Mechanics* UK: Cambridge University Press.

- David, T., Smye, S., Dabbs, T., and James, T. (1998). A model for the fluid motion of vitreous humour of the human eye during saccadic movement. *Physics in Medicine and Biology* 43 (6):1385.
- Davies, A. J. (2011). *The Finite Element Method*. (2). New York: Oxford University Press.
- Davson, H. (1949). *The physiology of the eye*. London: J. & A. Churchill Ltd.
- Davson, H. (1980). *Physiology of the Eye*. (Fourth). New York: Elsevier Science.
- Davson, H. (1984). *The eye, vegetative physiology and biochemistry*. (3). Vol. 1A. New York: Academic Press.
- Davson, H. (1990). *Physiology of the eye*. (5): Pergamon press.
- Downs, J. C., Ensor, M. E., and Bellezza, A. J. e. a. (2001). Posterior scleral thickness in perfusion-fixed normal and early-glaucoma monkey eyes. *Investigative Ophthalmology & Visual Science* 42:3202-3208.
- Dunavant, D. A. (1985). High degree efficient symmetrical gaussian quadrature rules. *International Journal for Numerical Methods in Engineering* 21:1129-1148.
- Dyson, R., Fitt, A. D., Jensen, O., Mottram, N., Miroshnychenko, D., Naire, S., Ocone, R., Siggers, J., and Smith, A. (2004). Post Re-attachment Retinal Re-detachment. In UK Mathematics in Medical Study Group Strathclyde 2004, edited by F. Alistair. Glasgow: University of Strathclyde.
- Eisner, G. (1976). The anatomy and biomicroscopy of the vitreous body. *Documenta Ophthalmologica Proceedings Series. New Development in Ophthalmology*:87-104.
- Ern, A., and Guermond, J. L. (2004). *Theory and Practice of Finite Elements*. New York: Springer-Verlag.
- Erturk, E., Corke, T. C., and Gokcol, C. (2005). Numerical solutions of 2-D steady incompressible driven cavity flow at high Reynolds numbers. *International Journal for Numerical Methods in Fluids* 48:747-774.
- Erwan, H. K. (2012). *Mixed formulations for Navier Stokes equations with magnetic effect in rectangular channel*. Master of Engineering, Civil Engineering, Universiti Teknologi Malaysia.
- Ethier, C. R., Johnson, M., and Ruberti, J. (2004). Ocular biomechanics and biotransport. *Annual Review of Biomedical Engineering* 6:249-273.
- Fang, W., and Heow-Pueh, L. (2007). Biomechanical effect of segmental scleral buckling surgery. *Current Eye Research* 32:133-142.

- Fatt, I., and Shantinath, K. (1971). Flow conductivity of retina and its role in retinal adhesion. *Experimental Eye Research* 12 (2):218-226.
- Favero, J. L., Secchi, A. R., Cardozo, N. S. M., and Jasak, H. (2010). Viscoelastic flow analysis using the software OpenFOAM and differential constitutive equations. *Journal of Non-Newtonian Fluid Mechanics* 165 (23–24):1625-1636.
- Fitt, A. D., and Gonzalez, G. (2006). Fluid mechanics of the human eye: Aqueous humour flow in the anterior chamber. *Bulletin of Mathematical Biology* 68 (1):53-71.
- Fontana, S. T., and Brubaker, R. F. (1980). Volume and dimensions of the anterior chamber of the normal aging human eye. *Archives of Ophthalmology* 98:1803-1808.
- Forbes, M. (1966). Gonioscopy with corneal indentation. *Archives of Ophthalmology* 76 (4):488-492.
- Forrester, J. V., Dick, A. D., McMenemy, P. G., and Roberts, F. (2008). *Anatomy of the eye and orbit. In: The eye: basic sciences in practice*: WB Saunders Co.
- Foster, W. J., Dowla, N., Joshi, S. Y., and Nikolaou, M. (2010). The fluid mechanics of scleral buckling surgery for the repair of retinal detachment. *Graefe's Archive for Clinical and Experimental Ophthalmology* 248 (1):31-36.
- France, P. W. (1975). An improved finite element technique for the analysis of free surface flow problems. *Computers & Fluids* 3 (2–3):149-153.
- Francesco, B. (2010). Scleral buckling biomaterials and implants for retinal detachment surgery. *Medical Engineering & Physics* 32:945-956.
- Frey, P. J., and George, P. L. (2008). *Mesh Generation*. US: John Wiley & Sons, Inc.
- Gartling, D. K., and Becker, E. B. (1976a). Finite element analysis of viscous, incompressible fluid flow: Part 1 : Basic methodology. *Computer Methods in Applied Mechanics and Engineering* 8 (1):51-60.
- Gartling, D. K., and Becker, E. B. (1976b). Finite element analysis of viscous, incompressible fluid flow: Part 2: Applications. *Computer Methods in Applied Mechanics and Engineering* 8 (2):127-138.
- Ghia, U., Ghia, K. N., and Shin, C. T. (1982). High-Re solutions for incompressible flow using the Navier-Stokes equations and a multigrid method. *Journal of Computational Physics* 48:387-411.
- Girault, V., and Raviart, P. A. (1980). *Finite Element Methods For Navier-Stokes Equations*. Berlin: Springer-Verlag.

- Gonzalez, G. (2004). *The mathematical modelling of human eye*. PhD, School of Mathematics University of Southampton.
- Gray, W. H., and Schnurr, N. M. (1975). A comparison of the finite element and finite difference methods for the analysis of steady two dimensional heat conduction problems. *Computer Methods in Applied Mechanics and Engineering* 6 (2):243-245.
- Greven, C. M., Wall, A. B., and Slusher, M. M. (1999). Anatomic and visual results in asymptomatic clinical rhegmatogenous retinal detachment repaired by sclera. *American Journal of Ophthalmology* 128 (5):618-620.
- Hammer, M. E. (1981). Retinal re-attachment forces created by absorption of subretinal fluid. *Docum. Ophthalm. PrOf. Series*, 25:61-75.
- Heys, J. J., and Barocas, V. H. (2002). A Boussinesq model of natural convection in the human eye and the formation of Krukenberg's spindle. *Annals of Biomedical Engineering* 30:392-401.
- Hirano, K., Sugita, J., and Kobayashi, M. (2002). Separation of corneal stroma and descemet's membrane during deep lamellar keratoplasty. *Cornea* 21 (2):196-199.
- Isakova, K., Pralits, J. O., Repetto, R., and Romano, M. R. (2014). Mechanical models of the dynamics of vitreous substitutes. *BioMed research international* 2014.
- Ismail, Z. (2013). *The Mathematical Modelling of Flow and Deformation in the Human Eye*. Doctor of Philosophy, School of Mathematics, University of Southampton.
- Ismail, Z., Fitt, A. D., and Please, C. P. (2012). A fluid mechanical explanation of the spontaneous reattachment of a previously detached Descemet membrane. *Mathematical Medicine and Biology* 30:339-355.
- Jaluria, Y. (1980). *Natural Convection Heat and Mass Transfer*. London: Pergamon Press.
- Jichun, L., and Yi-Tung, C. (2008). *Computational Partial Differential Equations Using MATLAB*. Boca Raton: CRC Press.
- Jouzani, S. (2013). *Biomechanical Characterization and Computational Modeling of the Anterior Eye*. Doctor Of Philosophy, The Faculty of the Graduate School, The University Of Minnesota.
- Kara, R., ed. 2011. *The eye : the physiology of human perception*. New York: Britannica Educational Publishing.

- Karampatzakis, A., and Samaras, T. (2010). Numerical model of heat transfer in the human eye with consideration of fluid dynamics of the aqueous humour. *Physics in Medicine and Biology* 55:5653-5665.
- Karen, S. (2002). *Beginning Functional Analysis*. New York: Springer-Verlag.
- Karimi, A., Razaghi, R., Navidbakhsh, M., Sera, T., and Kudo, S. (2016a). Computing the stresses and deformations of the human eye components due to a high explosive detonation using fluid–structure interaction model. *International Journal of the Care of the Injured* 47:1042-1050.
- Karimi, A., Razaghi, R., Navidbakhsh, M., Sera, T., and Kudo, S. (2016b). Quantifying the injury of the human eye components due to tennis ball impact using a computational fluid–structure interaction model. *Sports Engineering* 19:105-115.
- Kathawate, J. (2006). *Numerical Solution of Flow Resistance in Outflow Pathway and Intravitreal Drug Delivery in Vitrectomised Eyes*. Master of Science, Mechanical Engineering, Louisiana State University
- Kawamorita, T., Shimizu, K., and Shoji, N. (2016). Effect of hole size on fluid dynamics of a posterior-chamber phakic intraocular lens with a central perforation by using computational fluid dynamics. *Graefe's Archive for Clinical and Experimental Ophthalmology* 254:739-744.
- Keeling, S. L., and Prospt, G. (2009). A mathematical model for the deformation of the eyeball by an elastic band. *Mathematical Medicine and Biology* 26:165-185.
- Kolb, H. (2003). How the retina works. *American scientist*.
- Kumar, S. (2003). *Numerical solution of ocular fluid dynamics*. Master of Science, Mechanical Engineering, Louisiana State University.
- Kumar, S., Acharya, S., Beuerman, R., and Palkama, A. (2006). Numerical solution of ocular fluid dynamics in a rabbit eye: Parametric effects. *Annals of Biomedical Engineering* 34 (3):530-554.
- Kundu, P. K., Cohen, I. M., and Dowling, D. R. (2012). *Fluid Mechanics*. USA: Academic Press.
- Lakawicz, J. M., and Bottega, W. J. (2015). An analysis of the mechanical behaviour of a detaching retina *Mathematical Medicine and Biology* 32:137-161.
- Lanchares, E., del Buey, M. A., Cristobal, J. A., Calvo, B., Ascaso, F. J., and Malve, M. (2016). Computational simulation of scleral buckling surgery for

- rhegmatogenous retinal detachment: On the effect of the band size on the myopization. *Journal of Ophthalmology* 2016.
- Lewis, G. P., Charteris, D. G., Sethi, C. S., and Fisher, S. K. (2002). Animal models of retinal detachment and reattachment: identifying cellular events that may affect visual recovery. *Eye* 16 (4):375-387.
- Lewis, R. W., Nithiarasu, P., and Seetharamu, K. (2008). *Fundamentals of the Finite Element Method for Heat and Fluid Flow*: Wiley.
- Liversedge, S. P., and Findlay, J. M. (2000). Saccadic eye movements and cognition. *Trends in Cognitive Sciences* 4 (1):6-14.
- Mackool, R. J., and Holtz, S. J. (1977). Descemet membrane detachment. *Archives of Ophthalmology* 95:459-463.
- Mahmood, R., Sajid, M., and Nadeem, A. (2011). Finite element solution for heat transfer flow of a third order fluid between parallel plates. *Advanced Studies in Theoretical Physics* 5 (3):107-120.
- Marcon, A. S., Rapuano, C. J., Jones, M. R., Laibson, P. R., and Cohen, E. J. (2002). Descemet's membrane detachment after cataract surgery: management and outcome. *Ophthalmology* 109 (12):2325-2330.
- Martin, S., Raimund, A. S., and George, T. T. (1996). A novel method for measuring saccade profiles using the scanning laser ophthalmoscope. *Vision Research* 36 (13):1987-1994.
- Masselos, K., Bank, A., Francis, I. C., and Stapleton, F. (2009). Corneal indentation in the early management of acute angle closure. *Ophthalmology* 116 (1):25-29.
- Matsunaga, K., Ito, K., Esaki, K., Sugimoto, K., Sano, T., Miura, K., Sasoh, M., and Uji, Y. (2004). Evaluation of eyes with relative pupillary block by indentation ultrasound biomicroscopy gonioscopy. *American Journal of Ophthalmology* 137 (3):552-554.
- Meinhard, T. S. (2010). *Fluid Mechanics for Engineers*. USA: Springer-Verlag Berlin Heidelberg.
- Menezo, V., Choong, Y. F., and Hawksworth, N. R. (2002). Reattachment of extensive Descemet's membrane detachment following uneventful phaco-emulsification surgery. *Eye* 16 (6):786-788.
- Meskauskas, J., Repetto, R., and Siggers, J. H. (2011). Oscillatory motion of a viscoelastic fluid within a spherical cavity. *Journal of Fluid Mechanics* 685:1-22.

- Meskauskas, J., Repetto, R., and Siggers, J. H. (2012). Shape change of the vitreous chamber influences retinal detachment and reattachment processes: Is mechanical stress during eye rotations a factor? *Investigative Ophthalmology & Visual Science* 53 (10):6271-6281.
- Modarreszadeh, A., and Abouali, O. (2014). Numerical simulation for unsteady motions of the human vitreous humor as a viscoelastic substance in linear and non-linear regimes. *Journal of Non-Newtonian Fluid Mechanics* 204:22-31.
- Modarreszadeh, S., Abouali, O., Ghaffarieh, A., and Ahmadi, G. (2014). Physiology of aqueous humor dynamic in the anterior chamber due to rapid eye movement. *Physiology & behavior* 135:112-118.
- Morrison, F. A. (2013). *An Introduction to Fluid Mechanics*. USA: Cambridge University Press.
- Moses, R. A. (1975). "Intraocular pressure," in *Adler's Physiology of the Eye*. St. Louis: C. V. Mosby Company.
- Moustafa, E. S., and Elmaboud, Y. A. (2005). On the fluid flow in the anterior chamber of a human eye with slip velocity. *International Communications in Heat and Mass Transfer* 32:1104-1110.
- Mu, L., Wang, J., and Ye, X. (2014). A stable numerical algorithm for the Brinkman equations by weak Galerkin finite element methods. *Journal of Computational Physics* 273 (0):327-342.
- Mulhern, M., Barry, P., and Condon, P. (1996). A case of Descemet's membrane detachment during phacoemulsification surgery. *British Journal of Ophthalmology* 80 (2):185-186.
- Nam-Ho, K. (2015). *Introduction to Nonlinear Finite Element Analysis*. New York: Springer.
- Nouri, M., Pineda, R. J., and Azar, D. (2002). Descemet membrane tear after cataract surgery. *Seminars in Ophthalmology* 17:115-119.
- O'Connor, P. R. (1973). Absorption of subretinal fluid after external scleral buckling without drainage. *American Journal of Ophthalmology* 76 (1):30-34.
- Ockendon, H., and Ockendon, J. R. (1995). *Viscous Flow*. USA: Cambridge University Press.
- Olsen, T. W., Aaberg, S. Y., Geroski, D. H., and Edelhauser, H. F. (1998). Human sclera: Thickness and surface area. *American Journal of Ophthalmology* 125:237-241.

- Ooi, E. H. (2009). *Studies of Ocular Heat Transfer using the Boundary Element Method*. Doctor of Philosophy, School of Mechanical and Aerospace Engineering, Nanyang Technological University.
- Ooi, E. H., and Ng, E. Y. K. (2008). Simulation of aqueous humor hydrodynamics in human eye heat transfer. *Computers in Biology and Medicine* 38:252-262.
- Ooi, E. H., and Ng, E. Y. K. (2011). Effects of natural convection within the anterior chamber on the ocular heat transfer. *International Journal for Numerical Methods in Biomedical Engineering* 27:408-423.
- Patterson, C. A. (1992). *The lens*. In: *Adler's physiology of the eye*: Mosby-Year Book.
- Pavlin, C., Harasiewicz, K., and Foster, F. (1992). Ultrasound biomicroscopy analysis of the anterior segment in normal and glaucomatous eyes. *American Journal of Ophthalmology* 113:381-389.
- Pepose, J. S., and Ubels, J. L. (1992). *The cornea*. In: *Adler's physiology of the eye*. . St. Louis, MO, USA: Mosby Year Book.
- Pepper, D. W., and Heinrich, J. C. (2006). *The Finite Element Method*. US: CRC Press.
- Pirenne, H. (1967). *Vision and the Eye (2)*: Chapman and Hall.
- Pissanetzky, S. (1984). *Sparse Matrix Technology*. Great Britain: Academic Press.
- Porte, H. S. (2004). Slow horizontal eye movement at human sleep onset. *Journal of Sleep Research* 13 (3):239-249.
- Potter, J., and Zalatio, N. (2005). Descemet's membrane detachment after cataract extraction. *Optometry* 76 (12):720-724.
- Quarteroni, A., and Valli, A. (2008). *Numerical Approximation of Partial Differential Equations*. Springer-Verlag: Berlin.
- Quintyn, J. C., and Brasseur, G. (2004). Subretinal fluid in primary rhegmatogenous retinal detachment physiopathology and composition. *Survey Ophthalmol* 49 (1):96-108.
- Reddy, J. N. (2003). *Mechanics of Laminated Composite Plates and Shells*. USA: CRC Press.
- Reddy, J. N. (2005). *An Introduction to Nonlinear Finite Element Analysis*. Oxford: Oxford University Press.
- Reddy, J. N. (2006). *An Introduction to the Finite Element Method*. Singapore: McGraw-Hill Education (Asia).
- Reddy, J. N., and Gartling, D. K. (2010). *The Finite Element Method in Heat Transfer and Fluid Dynamics, Third Edition*: Taylor & Francis.

- Remington, L. A. (2005). *Clinical Anatomy of the Visual System*. St. Louis: Elsevier.
- Repetto, R. (2006). An analytical model of the dynamics of the liquefied vitreous induced by saccadic eye movements. *Meccanica* 41 (1):101-117.
- Repetto, R., Siggers, J. H., and Stocchino, A. (2010). Mathematical model of flow in the vitreous humor induced by saccadic eye rotations: effect of geometry. *Biomechanics and Modeling in Mechanobiology* 9 (1):65-76.
- Repetto, R., Stocchino, A., and Cafferata, C. (2005). Experimental investigation of vitreous humour motion within a human eye model. *Physics in Medicine and Biology* 50 (19):4729.
- Roberts, P. A., Gaffney, E. A., Luthert, P. J., Foss, A. J. E., and Byrne, H. M. (2016). Mathematical and computational models of the retina in health, development and disease. *Progress in Retinal and Eye Research*.
- Rohen, J. (1979). Scanning electron microscopic studies of the zonular apparatus in human and monkey eyes. *Investigative Ophthalmology & Visual Science* 18:133-144.
- Root, T. (2009). *OphthoBook*: CreateSpace Independent Publishing Platform.
- Rottach, K. G., Das, V. E., Wohlgemuth, W., Zivotofsky, A. Z., and Leigh, R. J. (1998). Properties of horizontal saccades accompanied by blinks. *Journal of Neurophysiology* 79 (6):2895-2902.
- Scott, J. A. (1988). A finite element model of heat transport in the human eye. *Physics in Medicine and Biology* 33:227-241.
- Sebag, J. (1992). "The vitreous," in *Adler's Physiology of the Eye*. St. Louis: Mosby
- Sevillano, C., Viso, E., and Millan-Rodriguez, A. C. (2008). Descemet's membrane detachment as a complication of cataract surgery. *Archivos de la Sociedad Española de Oftalmología*. 83:549-552.
- Shunmugam, M., Shah, A. N., Hysi, P. G., and Williamson, T. H. (2014). The pattern and distribution of retinal breaks in eyes with rhegmatogenous retinal detachment. *American Journal of Ophthalmology* 157 (1):221-226
- Siebinga, I., Vrensen, G. F. J. M., DeMul, F. F. M., and Greve, J. (1991). Age-related changes in local water and protein content of human eye lenses measured by raman microspectroscopy. *Experimental Eye Research* 53:233-239.
- Sit, A. J., Nau, C. B., McLaren, J. W., Johnson, D. H., and Hodge, D. (2008). Circadian variation of aqueous dynamics in young healthy adults. *Investigative Ophthalmology & Visual Science* 49:173-1479.

- Smith, S. L., and Brebbia, C. A. (1975). Finite-element solution of navier-stokes equations for transient two-dimensional incompressible flow. *Journal of Computational Physics* 17 (3):235-245.
- Sodhi, A., Leung, L. S., Do, D. V., Gower, E. W., Schein, O. D., and Handa, J. T. (2008). Recent trends in the management of rhegmatogenous retinal detachment. *Survey Ophthalmol* 53 (1):50-67.
- Som, S. K. (2008). *Introduction to Heat Transfer*. New Delhi: PHI Learning Private Limited.
- Stephen, A. W., and Allen, L. (2004). Management of corneal abrasions. *American Family Physician* 70 (1):123-128.
- Stocchino, A., Repetto, R., and Cafferata, C. (2007). Eye rotation induced dynamics of a Newtonian fluid within the vitreous cavity: the effect of the chamber shape. *Physics in Medicine and Biology* 52:2021-2034.
- Sváček, P., Louda, P., and Kozel, K. (2014). On numerical simulation of three-dimensional flow problems by finite element and finite volume techniques. *Journal of Computational and Applied Mathematics* 270 (0):451-461.
- Tanner, R. I., Nickell, R. E., and Bilger, R. W. (1975). Finite element methods for the solution of some incompressible non-newtonian fluid mechanics problems with free surfaces. *Computer Methods in Applied Mechanics and Engineering* 6 (2):155-174.
- Taylor, C., and Hood, P. (1973). A numerical solution of the Navier-Stokes equations using the finite element technique. *Computers & Fluids* 1 (1):73-100.
- Thompson, H. S. (1992). "The pupil," in *Adler's Physiology of the Eye*. Chicago: Mosby Year Book.
- Thompson, J. F., Soni, B. K., and Weatherill, N. P., eds. 1999. *Handbook of Grid Generation*. USA: CRC Pree.
- Ünlü, K., and Aksünger, A. (2000). Descemet membrane detachment after viscocanalostomy. *American Journal of Ophthalmology* 130 (6):833-834.
- Van de Put, M. A. J., Hooymans, J. M. M., and Los, L. I. (2013). The incidence of rhegmatogenous retinal detachment in the Netherlands. *Ophthalmology* 120 (3):616-622.
- Vaughan, D., Cook, T., and Asbury, R. (1965). *General Ophthalmology*: LangeMedical Publications.

- Villamarin, A., Roy, S., Hasballa, R., Vardoulis, O., Reymond, P., and Stergiopoulos, N. (2012). 3D simulation of the aqueous flow in the human eye. *Medical Engineering & Physics* 34:1462-1470.
- Wadhwa, N., Venkatesh, P., Sampangi, R., and Garg, S. (2008). Rhegmatogenous retinal detachments in children in India: clinical characteristics, risk factors, and surgical outcomes. *Journal of AAPOS* 12 (6):551-554.
- Wang, S., and Linsenmeier, R. A. (2007). Hyperoxia improves oxygen consumption in the detached feline retina. *Investigative Ophthalmology & Visual Science* 48 (3):1335-1341.
- Weidenthal, D. T. (1967). Retinal reattachmnet without release of subretinal fluid. *American Journal of Ophthalmology* 63 (1):108-112.
- Wong, J. C. F. (2007). On the use of the consistent splitting scheme for double-diffusive convection flows in mixed finite element formulations. *International Journal of Computer Mathematics* 84 (11):1683-1700.
- Wong, J. C. F., and Chan, M. K. H. (2006). A consistent splitting scheme for unsteady incompressible viscous fows I. Dirichlet boundary condition and applications. *International Journal for Numerical Methods in Fluids* 51:384-424.
- Wong, J. C. F., and Yuan, P. (2006). Numerical convergence studies of the mixed finite element method for natural convection flow in a fluidsaturated porous medium. *International Journal of Computational Fluid Dynamics* 20 (10):657-671.
- Wong, T., Tielsch, J. M., and Schein, O. D. (1999). Racial difference in the incidence of retinal detachment in singapore. *Archives of Ophthalmology* 117 (3):379-383.
- Wyatt, H. J. (1996). Ocular pharmacokinetics and convectional flow: evidence from spatio-temporal analysis of mydriasis. *Journal Of Ocular Pharmacology* 12 (4):441-459.
- Yang, S. N., and McConkie, G. W. (2001). Eye movements during reading: a theory of saccade initiation times. *Vision Research* 41 (25–26):3567-3585.
- Young, K. W., and Hyochoong, B. (1997). *The Finite Element Method Using MATLAB*. United States of America: CRC Press LLC.
- Zhou, W. (2008). *Perfusion Studies Of Trabecular Outflow*. Doctor of Philosophy, Department of Pharmacology, The University Of Arizona.

Zienkiewicz, O. C., Taylor, R. L., and Nithiarasu, P. (2013). *The Finite Element Method for Fluid Dynamics*: Elsevier Science.

Zienkiewicz, O. C., Taylor, R. L., and Zhu, J. Z. (2005). *The Finite Element Method: Its Basis and Fundamentals: Its Basis and Fundamentals*: Elsevier Science.