THREE-DIMENSIONAL COMPUTED TOMOGRAPHY DOSE OPTIMISATION AND IMAGE QUALITY IMPROVEMENT OF ABDOMEN-PELVIS USING ADAPTIVE-ITERATIVE DOSE REDUCTION

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UNIVERSITI TEKNOLOGI MALAYSIA

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To my beloved family, for their endless patience, support, and courage during the hardships in completion of this thesis.

This thesis is dedicated to them.

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ABSTRACT

New development of computed tomography (CT) technology has made CT a versatile and efficient diagnostic modality. This has led to exponentially increased demand in clinical practice with increased risk of radiation exposure to the patients. Most research on CT optimisation concentrates on physical parameters, such as tube potential, tube current and pitch factor. Little research has been done on iterative reconstruction process in dose reduction without compromising image quality in clinical CT examination. Thus, this study investigates dose optimisation and image quality improvement using Adaptive-Iterative Dose Reduction Three-Dimensional (AIDR 3D) reconstruction, compared with conventional filtered back projection (FBP), in abdomen-pelvis CT. In a single-centre cohort study, 100 patients who underwent plain CT abdomen-pelvis using a 80-multidetector CT system were retrospectively analysed. Patients were divided into three groups according to the scanning protocol. Group 1 patients (n = 39) were scanned with 120 kVp standard dose FBP reconstruction. Iterative reconstruction was used for 120 kVp low dose group 2 (AIDR 3D standard, n = 28) and 100 kVp low dose group 3 (AIDR 3D strong, n = 33). Quantitative measures of radiation dose, objective image noise and signal to noise ratio (SNR) were obtained. The results were compared between all groups and correlated to body mass index (BMI). Subjective image quality evaluations were graded by two radiologists. The volume CT dose index (CTDI_{vol}), dose length product (DLP), and effective dose (E) in low dose AIDR 3D studies (group 2 and group 3) were significantly lower than standard dose FBP CT (p < 0.05). Group 3 (100 kVp low dose AIDR 3D strong) obtained highest dose reduction with CTDI_{vol}, DLP and E as low as 3.35 ± 1.04 mGy, 172.05 ± 63.32 mGy.cm and 2.58 ± 0.95 mSv respectively. In objective image quality analysis, group 2 and group 3 achieved significant image noise reduction (41.33% versus 52.62%) and SNR increment (62.25% versus 101.47%) compared to group 1. Subjective image noise, artifacts, sharpness and overall diagnostic confidence were greatly improved by AIDR 3D (group 2 and group 3). Moreover, AIDR 3D strong (group 3) was the most optimal iterative reconstruction to demonstrate fine anatomical structures. AIDR 3D could advance dose optimisation and improved image quality for wide range of BMI in the population. Thus, AIDR 3D is a useful algorithm to optimise scanning protocol and practicable in all routine CT examinations at the lowest radiation exposure.

ABSTRAK

Pembangunan baharu teknologi tomografi berkomputer (CT) telah membuat CT menjadi modaliti diagnostik yang serba guna dan cekap. Ini telah membawa kepada peningkatan pesat permintaan dalam amalan klinikal dengan peningkatan risiko dedahan sinaran terhadap pesakit. Kebanyakan penyelidikan mengenai pengoptimuman CT tertumpu kepada parameter teknikal, seperti keupayaan tiub, arus tiub dan faktor pitch. Segelintir penyelidikan yang dilakukan ke atas proses pembinaan semula lelaran dalam pengurangan dos tanpa menjejaskan kualiti imej dalam pemeriksaan CT klinikal. Oleh itu, kajian ini mengkaji pengoptimuman dos dan peningkatan kualiti imej menggunakan pembinaan semula Adaptive-Iterative Dose Reduction Tiga Dimensi (AIDR 3D), berbanding dengan unjuran tapis semula (FBP) konvensional, dalam CT abdomen-pelvis. Dalam kajian kohort satu pusat ini, 100 pesakit yang menjalani CT abdomen-pelvis menggunakan system CT 80multidetektor telah dianalisis secara retrospektif. Pesakit telah dibahagikan kepada tiga kumpulan berdasarkan protokol pengimbasan. Pesakit kumpulan 1 (n = 39) telah diimbas dengan 120 kVp berdos standard pembinaan semula FBP. Pembinaan semula lelaran digunakan untuk kumpulan 2 iaitu 120 kVp berdos rendah (standard AIDR 3D, n = 28), dan kumpulan 3 iaitu 100 kVp berdos rendah (AIDR 3D kuat, n = 33). Ukuran kuantitatif dos sinaran, hingar imej objektif dan nisbah isyarat kepada hingar (SNR) telah diperolehi. Keputusan tersebut dibandingkan antara semua kumpulan dan dikaitkan dengan indeks jisim badan (BMI). Penilaian kualiti imej subjektif telah dinilai oleh dua pakar radiologi. Indeks dos CT isipadu (CTDIvol), hasil darab dos panjang (DLP), dan dos berkesan (E) dalam kajian AIDR 3D berdos rendah (kumpulan 2 dan kumpulan 3) adalah lebih rendah daripada CT berdos standard FBP (p < 0.05). Kumpulan 3 (100 kVp dos rendah AIDR 3D kuat) memperolehi pengurangan dos tertinggi dengan CTDIvol, DLP dan E masing-masing serendah 3.35 ± 1.04 mGy, 172.05 ± 63.32 mGy.cm dan 2.58 ± 0.95 mSv. Dalam analisis kualiti imej objektif, kumpulan 2 dan kumpulan 3 mengalami pengurangan hingar imej dengan ketara (41.33% berbanding 52.62%) dan kenaikan SNR (62.25% berbanding 101.47%) berbanding dengan kumpulan 1. Hingar imej subjektif, artifak, ketajaman dan keyakinan diagnostik secara keseluruhan telah dipertingkatkan oleh AIDR 3D (kumpulan 2 dan kumpulan 3). Selain itu, AIDR 3D kuat (kumpulan 3) adalah pembinaan semula lelaran yang paling optimum untuk menunjukkan struktur anatomi halus. AIDR 3D boleh memajukan pengoptimuman dos dan meningkatkan kualiti imej untuk populasi yang terdiri dari pelbagai BMI. Oleh itu, AIDR 3D ialah algoritma yang berguna untuk mengoptimumkan protokol pengimbasan dan boleh dilaksanakan dalam semua pemeriksaan CT yang rutin dengan dedahan sinaran yang paling rendah.

TABLE OF CONTENTS

	TITLE	PAGE		
DEC	LARATION	ii		
DED	ICATION	iii		
ACKNOWLEDGEMENT				
ABS	TRACT	V		
ABSTRAK				
TABLE OF CONTENTS				
LIST OF TABLES				
LIST	COF FIGURES	xii		
LIST	XV			
INTI	RODUCTION			
1.1	Background of Study	1		
1.2	Problem Statement	4		
1.3	Research Objectives	7		
1.4	Scope of Study	7		
1.5	Significance of Study	8		
1.6	Research Hypothesis	8		
1.7	Thesis Outline	8		
	DED ACK ABS ABS TAB LIST LIST LIST 1.1 1.2 1.3 1.4 1.5 1.6	DECLARATIONDEDICATIONACKNOWLEDGEMENTACKNOWLEDGEMENTABSTRACTABSTRACTABSTRAKTABLE OF CONTENTSLIST OF TABLESLIST OF TABLESLIST OF FIGURESLIST OF ABBREVIATIONSProblem Statement1.3Research Objectives1.4Scope of Study1.5Significance of Study1.6Research Hypothesis		

2 LITERATURE REVIEW

2.1	Introduction			
2.2	CT Technology	11		
2.3	3 Radiation Dose and Radiation Risk in CT of			
	Abdomen-pelvis	13		
	2.3.1 CT Dose Quantities	14		
2.4	AIDR 3D in CT Image Quality	16		
2.5	Practical Approaches in Dose Optimisation of Multi			
	Detector CT of Abdomen-pelvis	20		
	2.5.1 AIDR 3D Reconstruction	21		

3 METHODOLOGY

3.1	Introduction 26		
3.2	Study Population	26	
3.3	CT Acquisition Protocol and Image Reconstruction	28	
	3.3.1 K-PACS DICOM Viewer V 1.6.0	29	
3.4	Assessment of Image Quality	31	
	3.4.1 Objective Image Analysis	31	
	3.4.2 Subjective Image Analysis	33	
3.5	Radiation Dose Measurements	35	
3.6	Statistical Analysis 35		
3.7	Operational Framework 36		

4 **RESULTS AND DISCUSSIONS**

4.1	Overview	38
4.2	Patient Characteristics and CT Acquisition Parameter	38
4.3	Radiation Dose	41
4.4	The Correlation between Patient's BMI and CT Dose	54
4.5	Objective Image Quality	61
4.6	The Correlation between Patient's BMI and Objective	
	Image Quality	70
4.7	Subjective Image Quality	82

5 CONCLUSIONS

5.1	Introduction	93
5.2	Recommendations and Future Studies	96

REFERENCES

Appendices A - B	112 - 115
11	

98

LIST OF TABLES

TABLE NO.

TITLE

PAGE

2.1	Highlighted issues regarding AIDR 3D in previous studies	23
3.1	Scan parameters and various image reconstruction setting	29
3.2	Subjective image quality grading scale for general image quality category	34
4.1	Patient characteristic of the study population	39
4.2	Radiation dose parameters for the three groups of patients with different scanning protocol	42
4.3	Comparison between third quartile values of CT dose index volume and dose length product in current study with Malaysia DRLs 2013 and other international DRLs	49
4.4	Comparison of patient radiation dose in multiple AIDR 3D studies	52
4.5	Patient dose data for the three different scanning protocols classified by BMI	55
4.6	Comparison of CT number, objective image noise and SNR in five anatomical structures between group 1, group 2 and group 3	62
4.7	Objective image noise measurements for the three different scanning protocols classified by BMI	71
4.8	Signal to noise ratio measurements for the three different scanning protocols classified by BMI	72
4.9	Subjective image quality analysis	84
4.10	Subjective image quality scores agreement percentage and Kappa analysis between the two radiologists	90

5.1	Radiation dose optimisation using AIDR 3D in CT abdomen-pelvis	95
5.2	Image quality improvement using AIDR 3D in CT abdomen-pelvis	96

LIST OF FIGURES

FIGURE NO.

TITLE

PAGE

1.1	CT coronary angiogram of a 45 years old male with history of chest pain taken in year 2016 using Toshiba Aquilion PRIME 80 CT scanner	2
1.2	The general overview of the research works	6
2.1	Schematic view of a 3rd generation CT scanner (Operation Manual for Whole-Body X-Ray CT Scanner Aquilion, 2004)	12
2.2	Streak artifacts evident in pelvic region of a 50 years old female using routine scanning protocol by Toshiba Aquilion PRIME 80 CT scanner	18
2.3	Multiple rings appearance seen in the center of the CT liver image acquired with 80 kVp abdomen-pelvis CT protocol using Toshiba Aquilion PRIME 80 Ct scanner	19
2.4	Schematic diagram of AIDR 3D advanced operational process	21
3.1	Toshiba Aquilion PRIME 80 CT scanner used in this research study	27
3.2	CT abdomen-pelvis scanogram image that include from bases of lungs to symphysis pubis	28
3.3	K-PACS software for DICOM images viewing and measurement	30
3.4	CT dose report of a 75 years old woman post CT abdomen-pelvis displayed in K-PACS viewer	31

3.5	Detail placement of ROIs in (a) right hepatic lobe, aorta and spleen at the level of main portal vein and placement of ROIs in (b) bladder and both sides of gluteus maximus muscles at tip of greater trochanter level	32
3.6	Schematic diagram of research process	37
4.1	Comparison between CT dose index volume for entire study cohort	44
4.2	Comparison between dose length product for entire study cohort	45
4.3	Effective dose distribution in group 1 patients with protocol 120 kVp standard dose FBP reconstruction	46
4.4	Effective dose distribution in group 2 patients with protocol 120 kVp low dose AIDR 3D standard reconstruction	47
4.5	Effective dose distribution in group 3 patients with protocol 100 kVp low dose AIDR 3D strong reconstruction	47
4.6	Comparison between effective dose for entire study cohort	48
4.7	Relationship between BMI and CTDI _{vol} in (a) group 1, (b) group 2 and (c) group 3 patients	57
4.8	Relationship between BMI and DLP in (a) group 1, (b) group 2 and (c) group 3 patients	58
4.9	Relationship between BMI and E in (a) group 1, (b) group 2 and (c) group 3 patients	59
4.10	Objective image analysis of the CT number measured in liver, aorta, spleen, bladder and gluteus maximus muscle for the entire study cohort	
4.11	Objective image analysis of the image noise measured in liver, aorta, spleen, bladder and gluteus maximus muscle for the entire study cohort	64
4.12	Objective image analysis of the signal to noise ratio measured in liver, aorta, spleen, bladder and gluteus maximus muscle for the entire study cohort	66

4.13	Plain axial CT abdomen-pelvis images at the level of the main portal vein from three sample patients individually scanned with (a) 120 kVp standard dose FBP (b) 120 kVp low dose AIDR 3D standard and (c) 100 kVp low dose	
	AIDR 3D strong	68
4.14	Plain axial CT abdomen-pelvis images at the level of greater trochanteric tip from three sample patients individually scanned with (a) 120 kVp standard dose FBP (b) 120 kVp low dose AIDR 3D standard and (c) 100 kVp low dose AIDR 3D strong	69
4.15	Average objective image noise of all ROIs for imaging parameters in each BMI group	73
4.16	Average signal to noise ratio of all ROIs for imaging parameters in each BMI group	75
4.17	Comparison of (a) group 1, (b) group 2, and (c) group 3 images in patients with normal BMI (BMI range: $20-25 \text{ kg m}^{-2}$)	76
4.18	Comparison of (a) group 1, (b) group 2, and (c) group 3 images in overweight patients (BMI range: $25-30 \text{ kg m}^{-2}$)	77
4.19	Comparison of (a) group 1, (b) group 2, and (c) group 3 images in obese patients (BMI range: $30-35 \text{ kg m}^{-2}$)	78
4.20	Relationship between image noise and BMI	79
4.21	Relationship between signal to noise ratio and BMI for (a) group 1, (b) group 2 and (c) group 3 patients	80
4.22	Axial CT pelvis image with more than average noise and moderate artifacts in (a) 120 kVp standard dose FBP compared to less than average noise and mild artifacts in image performed at (b) 120 kVp low dose AIDR 3D standard and (c) 100 kVp low dose AIDR 3D strong without significant changes in image texture	86
4.23	Subjective assessment of the fine anatomical structures visibility scores in group 1 (FBP), group 2 (AIDR 3D	88
	standard) and group 3 (AIDR 3D strong)	00

LIST OF ABBREVIATIONS

AAPM	-	American Association of Physicist in Medicine
AIDR 3D	-	Adaptive-Iterative Dose Reduction 3D algorithm
ALARA	-	As low as reasonably achievable
ASIR	-	Adaptive Statistical Iterative Reconstruction
ATCM	-	Automatic Tube Current Modulation
BMI	-	Body mass index
CAT	-	Computed Axial Tomography
CNR	-	Contrast to noise ratio
СТ	-	Computed Tomography
CTDI	-	CT dose index
CTDI100	-	CT dose index from 100 mm
CTDIvol	-	Volume CTDI
CTDIw	-	Weighted CTDI
DICOM	-	Digital Imaging and Communications in Medicine
DLP	-	Dose length product
DRLs	-	Diagnostic reference levels
E	-	Effective dose
FBP	-	Filtered back projection
FC 18	-	Convolution Kernel 18
FDA	-	Food and Drug Administration
HU	-	Hounsfield Unit
IAEA	-	International Atomic Energy Agency
ICRP	-	International Commission on Radiation Protection
IEC	-	International Electrotechnical Commission
IR	-	Iterative reconstruction
IRIS	-	Iterative Reconstruction in Image Space
IVC	-	Inferior vena cava

kVp	-	Kilovoltage peak
MBIR	-	Model-Based Iterative Reconstruction
MDCT	-	Multi Detector Computed Tomography
MPR	-	Multi-planar reconstruction
NaI	-	Sodium Iodide
NMRR	-	National Medical Research Registration
NRPB	-	National Radiological Protection Board
PACS	-	Picture Archiving and Communication System
PMMA	-	Polymethyl methacrylate
ROIs	-	Region of interests
SAFIRE	-	Sonogram-Affirmed Iterative Reconstruction
SD	-	Noise index
SNR	-	Signal to noise ratio
STD	-	Standard deviation
UK	-	United Kingdom
UNSCEAR	-	United Nation Scientific Committee on Effects of
		Atomic Radiations

CHAPTER 1

INTRODUCTION

1.1 Background of Study

The first Nobel Prize in Physics was awarded to Wilhelm Conrad Roentgen, a German physicist, for his discovery of X-rays in 1895. Since the development of X-ray technology, tremendous progress has been made in the field of medical imaging thus enabling detailed visualization of human anatomy and pathology without surgical intervention.

X-rays while being the most common and cheapest examination, lacks the details and resolution provided by other cross-sectional imaging modalities. Among them, Computed Tomography (CT) scanner is one of the most important imaging modality. With the development of multi detector CT (MDCT) in 1998, CT technology has undergone a revolution with the introduction of high resolution and fast CT scanners including 64, 128, 256 and 320 MDCT. These scanners have far higher capability to obtain excellent radiographic resolution compared to conventional radiography. However, in majority of medical diagnosis, single axial image is not sufficient considering the fact of unique structure in human body. Therefore, multiplanar reconstruction (MPR) from volumetric acquisition of CT play an important role in creating coronal, sagittal, or even 3D volume rendering images originally from axial image as in Figure 1.1. Multi-planar reformatted images provide distinct advantage in image interpretation by viewing the extent of the malignancies of diseases as a whole and improve diagnostic accuracy in medical field (Hodel *et al.*, 2009; Honda *et al.*, 2011).

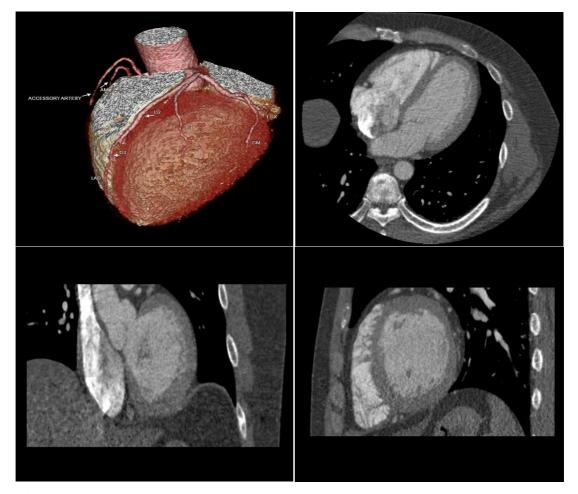


Figure 1.1 CT coronary angiogram image of a 45 years old male with history of chest pain taken in year 2016 using Toshiba Aquilion PRIME CT scanner

CT is a versatile and efficient diagnostic tool that has influenced healthcare industry leading to increased clinical applications throughout the world. It was estimated more than 50,000 clinical CT installations in operation worldwide for the year 2010 (Kalender, 2011). In radiology, CT was not constraint to head imaging alone, but whole body system including chest, abdomen, pelvis, extremities, coronary and functional imaging like perfusion scan. However, this high performance diagnostic tool comes with the price, which is increase in radiation dose to patients. CT uses ionising radiation for its operation that it delivered in far higher doses than conventional X-rays. Thus, the potential of radiation exposure causes health hazards to the patients and has become a concern (Brenner and Hall, 2007; Semelka *et al.*, 2007).

Radiation industries in Malaysia are small sized organisations compared to other countries. They are about 20,000 workers using radiation sources being monitored monthly (Noriah, 2010). Efforts to achieve as low as reasonably achievable (ALARA) doses in this country led to less than 1% of the radiation workers exceed 50 mSv annual dose limit for the last 25 years (Noriah, 2010). Atomic Energy Licensing Board (AELB) and Nuclear Malaysia are the regulatory body that actively involved in promoting radiation safety awareness among radiation workers through a good radiation protection programme at the workplace. However, rapid development and widen application of CT in work requirement may cause increased in average doses. Moreover, study of Karim *et al.* (2016) in organ dose evaluation and radiation risk of routine CT examinations in Johor, Malaysia reported that effective cancer risks of 0 to 1449 cancer cases per one million procedures and the radiation risks from CT exist due to its increase in usage every year. Thus, research in optimising CT doses without compromising image quality is needed in Malaysia.

The issue of radiation-induced cancer is highly relevant (Shah *et al.*, 2014) and the risk is increasing when the dose received exceeded dose reference levels (Rehani *et al.*, 2012; Naumann *et al.*, 2014). Although pediatric patients are at greatest risk and are more radiosensitive to radiation (Valentin 2007; Feng *et al.*, 2010), the stochastic effects from CT radiation in adults are not negligible. Consequently, CT examinations justification and dose optimisation are necessary to reduce radiation exposure. Much attention on technical solutions to reduce radiation dose in CT (McCollough *et al.*, 2009) has become a hot topic in clinical research. Moreover, CT manufacturers had developed number of new dose reduction technologies that promote low radiation dose without degrading image diagnostic quality. Among these latest innovations, the popular techniques that are being used clinically include tube current modulation, dual-energy CT and adaptive noise reduction filters (Gunn and Kohr, 2010).

More recently, renewed interest in iterative reconstruction (IR) are the main focus in CT dose reduction while maintaining high image quality due to limitation of the standard CT reconstruction technique using filtered back projection (FBP) (Renker *et al.*, 2011). Several IR techniques from various vendors were introduced and it was

found that Adaptive-Iterative Dose Reduction 3D algorithm (AIDR 3D) capable to work in both raw and image data domain compared to others (Tomizawa *et al.*, 2012). This promising new technology in conjunction with traditional technical optimisation techniques have potential of producing high quality image with even lower doses of radiation.

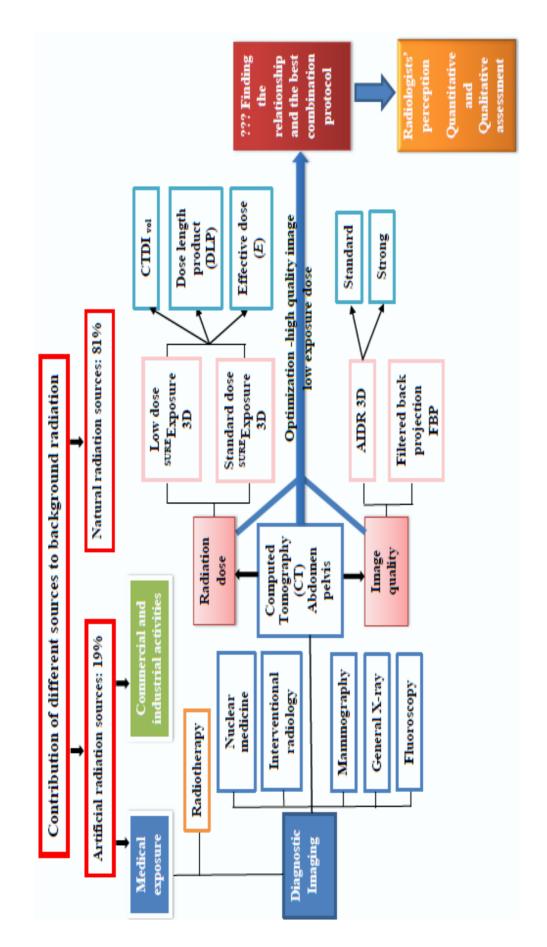
Moreover, limited research has been conducted in Malaysia focusing on AIDR 3D for CT abdomen-pelvis. The feasibility of AIDR 3D in medical imaging has prospective contribution to Malaysia in terms of national radiation safety regulation and may improve the diagnostic reference levels (DRLs) published by Ministry of Health Malaysia in 2013.

This research aimed to assess the benefits of AIDR 3D reconstruction in CT abdomen-pelvis by using low dose technique. This study allowed us to understand the effects of low dose AIDR 3D in image quality and radiation dose compared with standard dose CT using FBP reconstruction technique. Subsequently, the feasibility of further dose reduction without compromising image quality in reduced 100 kVp low dose AIDR 3D strong setting protocol was evaluated.

1.2 Problem Statement

Widespread use of CT has resulted in increase of medical radiation exposure and risks of long-term stochastic effects from ionising radiation (Smith *et al.*, 2009). It was predicted that 29,000 future cancers in United States were caused by CT scans performed in 2007 alone (Berrington *et al.*, 2009). This had alarmed international agencies, medical professionals and even patients regarding radiation safety in CT. Multiple responsible agencies including International Commission on Radiological Protection (ICRP), International Atomic Energy Agency (IAEA), United Nation Scientific Committee on Effects of Atomic Radiations (UNSCEAR), and American Association of Physicist in Medicine (AAPM) are concerned and contributed in radiation safety measurements with recommendations on radiological protection (AAPM Task Group 23, 2008; UNSCEAR, 2010). In Malaysia, there was also a notable increase in the use of CT by 161% from 1990 till 1994, based on a national survey (Ng *et al.*, 1999), which is the only latest data available and reported. One of the ways to reduce radiation dose from CT in the population is to reduce the CT-related dose in individual patients. However, dose optimisation while preserving high image quality in MDCT remain challenging in Malaysia. Direct steps such as using low tube potential, high pitch setting and low tube current had been used, but it compromised the image quality by increasing image noise and artifact due to photon starvation (Han *et al.*, 2011). The introduction of automatic tube current modulation (ATCM) facilitated with iterative reconstruction techniques enabled constant image quality and reasonably low dose with respective of the various attenuation body regions. Despite number of studies shown iterative reconstruction have lower image noise compared to FBP (Gervaise *et al.*, 2012; Joemai *et al.*, 2013; Liu, 2014; Naoum *et al.*, 2015), noise reduction potential of AIDR 3D reconstruction with combination of low dose protocol in abdominal pelvic CT is not well established.

As AIDR 3D is the latest available reconstruction technique in Toshiba MDCT 2010, only limited phantom studies being carried out without conclusive clinically assessment (Kim et al., 2014; Klink et al., 2014). Thus, assessment of image quality in low dose AIDR 3D compared to standard dose FBP in real patients study is required. Since radiation dose is one of the major concerns in conjunction with image in diagnostic level, the effectiveness of dose reduction at reduced tube voltage might obtain comparable image quality with iterative reconstruction (Eller et al., 2013; Kataria and Smedby, 2013; Williams et al., 2013). Although Gervaise et al. (2014) showed promising dose reduction while having similar image quality in low dose AIDR CT, the feasibility of AIDR in strong setting has not been established. Therefore, combination of low dose protocol at reduced tube potential 100 kVp AIDR 3D strong in CT abdomen-pelvis is ever demanding for further dose optimisation in medical imaging. This study aims to give a clear understanding of how to achieve high diagnostic image quality with the lowest possible dose delivered to the patient with the aid from AIDR 3D reconstruction. Figure 1.2 demonstrates the framework of the research that focus on CT abdomen-pelvis and the main variables involved in order to optimise the highest image quality by utilising the lower dose exposure.





1.3 Research Objectives

This study aims to evaluate the benefits of AIDR 3D in clinical work. Specifically, the objectives of the study are;

- i. To verify the image quality improvement using AIDR 3D technique in CT abdomen-pelvis patients study.
- To determine the effectiveness of dose reduction between low dose, reduced 100 kVp low dose and standard dose abdominal pelvic CT scanning protocols with different reconstruction algorithms.
- iii. To optimise the scanning protocol for delivering good diagnostic image quality with the lowest possible radiation dose.

1.4 Scope of Study

This is a retrospective study of 100 patients who underwent CT abdomenpelvis in one hospital in Johor Bahru. Patients were categorized into 3 groups according to the specific scanning tube potential and reconstruction algorithms being used and further subcategorised into 4 different Body Mass Index (BMI) groups for correlation analysis with radiation dose and objective image quality. Based on all data obtained, image quality was assessed for both objective and subjective criteria while dose reports obtained from the CT console were documented and calculated for estimation of dose reduction. Image quality in this study was limited to physical measurements of image noise and signal to noise ratio (SNR) and subjective image quality was graded by radiologist according to their experience and perception of a good image quality. Model observers for detection and measurement of abnormality in specific disease was not available in this work. Results from low dose AIDR 3D standard, reduced 100 kVp low dose AIDR 3D strong and standard dose FBP groups were compared and statistically analysed. Finally, the effects of AIDR 3D reconstruction in radiation dose and image quality were determined.

1.5 Significance of Study

The results of this study provide information on radiation dose and image quality obtained in the plain CT abdomen-pelvis with different dose settings, tube potential and reconstruction techniques. The image quality, which depend on both dose setting, tube voltage and reconstruction algorithm are important for clinical imaging. The optimal protocol obtained can be used as a benchmark in future imaging that involve CT abdomen and pelvis and applicable in various CT examinations. This study enhanced our understanding of the effects of AIDR 3D in dose reduction and image quality improvement, thus introducing a new practicable protocol to conquer the deficiency in current CT abdomen-pelvis practice. The implementation of AIDR 3D in low dose CT improved patient radiation safety and Malaysia healthcare quality.

1.6 Research Hypothesis

It was hypothesized that AIDR 3D reconstruction would obtain good image quality in CT abdomen-pelvis while low dose setting was used. Secondly, reduced tube voltage 100 kVp with combination of iterative reconstruction can further reduce radiation dose with similar image quality compared to 120 kVp standard dose CT.

1.7 Thesis Outline

Five chapters are included in this thesis with each chapter has a different focus of content. Started with chapter 1 about the brief introduction of the study, follow by study background, problem statement involved, research objectives and scope of study follow by research significance and hypothesis.

In chapter 2, the literature reviews the CT technology from past to modern MDCT, radiation dose, radiation risk in CT abdomen-pelvis and dose quantities. Image quality in CT is briefly explained. While the last part of literature discussed

briefly about practical approaches in optimising dose and recent iterative reconstruction techniques, particularly on AIDR 3D for CT abdomen-pelvis.

Chapter 3, research methodology provides methods and materials used in this study. The details how the image quality evaluated in both objective and subjective methods and its criteria for scoring are explained. Radiation dose measurement, calculation and validation further explained, including software for image viewing and measurement. Lastly, data comparison and statistical analysis involved are described.

Results and discussions are presented in Chapter 4 with supporting figures and tables. Subtopic results of patient characteristics, CT acquisition parameter, radiation dose measurements and image quality assessment are discussed and compared to previous literatures.

Chapter 5 includes conclusion of the present research. It summarise the main findings to address each objectives. Suggestions of future works are included for research improvement.

REFERENCES

- AAPM Task Group 23. (2008). AAPM Report No. 96 The Measurement, Reporting and Management of Radiation Dose in CT. Virginia. AAPM.
- Ashburn, D. D., & Reed, M. J. (2010). Gastrointestinal system and obesity. *Critical Care Clinics*, 26(4), 625-627.
- Berrington, D. G. A., Mahesh, M., Kim, K. P., Bhargavan, M., Lewis, R., Mettler, F., & Land, C. (2009). Projected Cancer Risks from Computed Tomographic Scans Performed in the United States in 2007. Archives of Internal Medicine, 169(22), 2071-2077.
- Boedeker, K. L., & McNitt-Gray, M. F. (2007). Application of the noise power spectrum in modern diagnostic MDCT: part II. Noise power spectra and signal to noise. *Physics in Medicine and Biology*, 52(14), 4047.
- Bongartz, G. S. J. G., Golding, S. J., Jurik, A. G., Leonardi, M., Van Persijn Van Meerten, E., Rodríguez, R., Schneider, K., Calzado, A., Geleijns, J., Jessen, K.A., & Panzer, W. (2004). European guidelines for multislice computed tomography. *European Commission*.
- Boning, G., Schafer, M., Grupp, U., Kaul, D., Kahn, J., Pavel, M., Maurer, M., Denecke, T., Hamm, B., & Streitparth, F. (2015). Comparison of applied dose and image quality in staging CT of neuroendocrine tumor patients using standard filtered back projection and adaptive statistical iterative reconstruction. *European Journal of Radiology*, 84(8), 1601-1607.

- Boos, J., Lanzman, R. S., Meineke, A., Heusch, P., Sawicki, L. M., Antoch, G., & Kröpil, P. (2015). Dose monitoring using the DICOM structured report: assessment of the relationship between cumulative radiation exposure and BMI in abdominal CT. *Clinical Radiology*, 70(2), 176-182.
- Brenner, D. J., & Hall, E. J. (2007). Computed tomography—an increasing source of radiation exposure. *New England Journal of Medicine*, *357*(22), 2277-2284.
- Buzug, T. M. (2008). Computed Tomography: From Photon Statistics to Modern Cone-Beam CT. Springer Science & Business Media.
- Chen, C. M., Lin, Y. Y., Hsu, M. Y., Hung, C. F., Liao, Y. L., & Tsai, H. Y. (2016). Performance of adaptive iterative dose reduction 3D integrated with automatic tube current modulation in radiation dose and image noise reduction compared with filtered-back projection for 80-kVp abdominal CT: Anthropomorphic phantom and patient study. *European Journal of Radiology*, 85(9), 1666-1672.
- Deak, P. D., Smal, Y., & Kalender, W. A. (2010). Multisection CT protocols: Sex-and age-specific conversion factors used to determine effective dose from doselength product 1. *Radiology*, 257(1), 158-166.
- Desai, G. S., Uppot, R. N., Elaine, W. Y., Kambadakone, A. R., & Sahani, D. V. (2012). Impact of iterative reconstruction on image quality and radiation dose in multidetector CT of large body size adults. *European Radiology*, 22(8), 1631-1640.
- Eller, A., May, M. S., Scharf, M., Schmid, A., Kuefner, M., Uder, M., & Lell, M. M. (2012). Attenuation-based automatic kilovolt selection in abdominal computed tomography: effects on radiation exposure and image quality. *Investigative Radiology*, 47(10), 559-565.
- Eller, A., Wuest, W., Scharf, M., Brand, M., Achenbach, S., Uder, M., & Lell, M. M. (2013). Attenuation-based automatic kilovolt (kV)-selection in computed tomography of the chest: effects on radiation exposure and image quality. *European Journal of Radiology*, 82(12), 2386-2391.

- Feng, S. T., Law, M. W. M., Huang, B., Ng, S., Li, Z. P., Meng, Q. F., & Khong, P. L. (2010). Radiation dose and cancer risk from pediatric CT examinations on 64-slice CT: a phantom study. *European Journal of Radiology*, 76(2), 19-23.
- Flohr T. Multidetector Row CT: Recent Developments, Radiation Dose and Dose Reduction Techniques. In: Tack D, Kalra MK, Gevenois PA, eds. *Radiation Dose from Multidetector CT*. 2nd ed. New York, NY: Springer. 3–19; 2012.
- Gervaise, A., Naulet, P., Beuret, F., Henry, C., Pernin, M., Portron, Y., & Lapierre-Combes, M. (2014). Low-dose CT with automatic tube current modulation, adaptive statistical iterative reconstruction, and low tube voltage for the diagnosis of renal colic: impact of body mass index. *American Journal of Roentgenology*, 202(3), 553-560.
- Gervaise, A., Osemont, B., Lecocq, S., Noel, A., Micard, E., Felblinger, J., & Blum, A. (2012). CT image quality improvement using adaptive iterative dose reduction with wide-volume acquisition on 320-detector CT. *European Radiology*, 22(2), 295-301.
- Gervaise, A., Osemont, B., Louis, M., Lecocq, S., Teixeira, P., & Blum, A. (2014).
 Standard dose versus low-dose abdominal and pelvic CT: comparison between filtered back projection versus adaptive iterative dose reduction 3D. *Diagnostic and Interventional Imaging*, 95(1), 47-53.
- Ginsburg, M., Obara, P., Wise, L., Wroblewski, K., Vannier, M. W., & Dachman, A. H. (2013). BMI-based radiation dose reduction in CT colonography. *Academic Radiology*, 20(4), 486-492.
- Goceri, E., Shah, Z. K., Layman, R., Jiang, X., & Gurcan, M. N. (2016). Quantification of liver fat: A comprehensive review. *Computers in Biology and Medicine*, 71, 174-189.
- Goldman, L. W. (2007). Principles of CT and CT technology. Journal of Nuclear Medicine Technology, 35(3), 115-128.

- Gordic, S., Desbiolles, L., Stolzmann, P., Gantner, L., Leschka, S., Husarik, D. B., & Alkadhi, H. (2014). Advanced modelled iterative reconstruction for abdominal CT: qualitative and quantitative evaluation. *Clinical Radiology*, 69(12), 497-504.
- Greffier, J., Fernandez, A., Macri, F., Freitag, C., Metge, L., & Beregi, J. P. (2013). Which dose for what image? Iterative reconstruction for CT scan.*Diagnostic* and Interventional Imaging, 94(11), 1117-1121.
- Greffier, J., Macri, F., Larbi, A., Fernandez, A., Khasanova, E., Pereira, F., Mekkaoui,
 C., & Beregi, J. P. (2015). Dose reduction with iterative reconstruction:
 Optimization of CT protocols in clinical practice. *Diagnostic and Interventional Imaging*, 96(5), 477-486.
- Gunn, M. L., & Kohr, J. R. (2010). State of the art: technologies for computed tomography dose reduction. *Emergency Radiology*, 17(3), 209-218.
- Han, B. K., Lindberg, J., Grant, K., Schwartz, R. S., & Lesser, J. R. (2011). Accuracy and safety of high pitch computed tomography imaging in young children with complex congenital heart disease. *The American Journal of Cardiology*, 107(10), 1541-1546.
- Hart, D., Wall, B. F., Hillier, M. C., & Shrimpton, P. C. (2010). Frequency and Collective Dose for Medical and Dental X-Ray Examination in the UK, 2008 (p. 52). Chilton, UK: Health Protection Agency.
- Hausleiter, J., Martinoff, S., Hadamitzky, M., Martuscelli, E., Pschierer, I., Feuchtner, G. M., Catalán-Sanz, P., Czermak, B., Meyer, T. S., Hein, F. & Bischoff, B. (2010). Image quality and radiation exposure with a low tube voltage protocol for coronary CT angiography: results of the PROTECTION II Trial. *JACC: Cardiovascular Imaging*, *3*(11), 1113-1123.
- Hodel, J., Zins, M., Desmottes, L., Boulay-Coletta, I., Jullès, M. C., Nakache, J. P., & Rodallec, M. (2009). Location of the transition zone in CT of small-bowel obstruction: added value of multiplanar reformations. *Abdominal Imaging*, 34(1), 35-41.

- Honda, O., Yanagawa, M., Inoue, A., Kikuyama, A., Yoshida, S., Sumikawa, H., Tobino, K., Koyama, M., & Tomiyama, N. (2011). Image quality of multiplanar reconstruction of pulmonary CT scans using adaptive statistical iterative reconstruction. *The British Journal of Radiology*, 84(1000), 335–341.
- Hosch, W., Stiller, W., Mueller, D., Gitsioudis, G., Welzel, J., Dadrich, M., Buss, S.
 J., Giannitsis, E., Kauczor, H. U., Katus, H. A. & Korosoglou, G. (2012).
 Reduction of radiation exposure and improvement of image quality with BMIadapted prospective cardiac computed tomography and iterative reconstruction. *European Journal of Radiology*, *81*(11), 3568-3576.
- Hricak, H., Brenner, D. J., Adelstein, S. J., Frush, D. P., Hall, E. J., Howell, R. W., McCollough, C. H., Mettler, F. A., Pearce, M. S., Suleiman, O. H., & Thrall, J. H. (2011). Managing radiation use in medical imaging: a multifaceted challenge. *Radiology*, 258(3), 889-905.
- Hsiao, E. M., Rybicki, F. J., & Steigner, M. (2010). CT coronary angiography: 256slice and 320-detector row scanners. *Current Cardiology Reports*, 12(1), 68-75.
- Husarik, D. B., Alkadhi, H., Puippe, G. D., Reiner, C. S., Chuck, N. C., Morsbach, F., Szucs-Farkas, Z. & Schindera, S. T. (2015). Model-based iterative reconstruction for improvement of low-contrast detectability in liver CT at reduced radiation dose: ex-vivo experience. *Clinical Radiology*, 70(4), 366-372.
- International Electrotechnical Commission. (2002). Medical Electrical Equipment Part 2-44: Particular Requirements for the Safety of X-Ray Equipment for Computed Tomography. Geneva, Switzerland.
- International Electrotechnical Commission. (2011). Evaluation and Routine Testing in Medical Imaging Departments. Part 3–5: Acceptance Tests–Imaging Performance of Computed Tomography X-Ray Equipment. IEC Publication, 61223-3.

- Irwan, R., Nakanishi, S., & Blum, A. (2012). AIDR 3D–Reduces Dose and Simultaneously Improves Image Quality. *Toshiba Medical Systems Whitepaper*.
- Jessen, K. A., Panzer, W., Shrimpton, P. C., Bongartzm, G., Geleijns, J., Golding, S., Jurik, A. G., Leonar, M., & Tosi, G. (2000). EUR 16262: European guidelines on quality criteria for computed tomography. *Luxembourg: Office for Official Publications of the European Communities*.
- Joemai, R. M., Veldkamp, W. J., Kroft, L. J., Hernandez-Giron, I., & Geleijns, J. (2013). Adaptive iterative dose reduction 3D versus filtered back projection in CT: evaluation of image quality. *American Journal of Roentgenology*, 201(6), 1291-1297.
- Juri, H., Matsuki, M., Itou, Y., Inada, Y., Nakai, G., Azuma, H., & Narumi, Y. (2013). Initial experience with adaptive iterative dose reduction 3D to reduce radiation dose in computed tomographic urography. *Journal of Computer Assisted Tomography*, 37(1), 52-57.
- Kalender, W. A. (2011). *Computed Tomography: Fundamentals, System Technology, Image Quality, Applications.* John Wiley & Sons. Erlangen, Germany.
- Kalmar, P. I., Quehenberger, F., Steiner, J., Lutfi, A., Bohlsen, D., Talakic, E., Hassler,
 E. M., & Schollnast, H. (2014). The impact of iterative reconstruction on image quality and radiation dose in thoracic and abdominal CT. *European Journal of Radiology*, *83*(8), 1416-1420.
- Kalra, M. K., Maher, M. M., Kamath, R. S., Horiuchi, T., Toth, T. L., Halpern, E. F., & Saini, S. (2004). Sixteen–Detector Row CT of Abdomen and Pelvis: Study for Optimization of Z-Axis Modulation Technique Performed in 153 Patients. *Radiology*, 233(1), 241-249.
- Kalra, M. K., Maher, M. M., Toth, T. L., Kamath, R. S., Halpern, E. F., & Saini, S. (2004). Comparison of z-axis automatic tube current modulation technique with fixed tube current CT scanning of abdomen and pelvis. *Radiology*, 232, 347-353.

- Kalra, M. K., Sodickson, A. D. & Mayo-Smith, W. W. (2015). CT Radiation: key concepts for gentle and wise use. *Radiographics*, 35(6), 1706-1721.
- Karim, M. K. A., Hashim, S., Bakar, K. A., Muhammad, H., Sabarudin, A., Ang, W. C., & Bahruddin, N. A. (2016, March). Establishment of multi-slice computed tomography (MSCT) reference level in Johor, Malaysia. In *Journal of Physics: Conference Series* (Vol. 694, No. 1, p. 012033). IOP Publishing.
- Karim, M. K. A., Hashim, S., Sabarudin, A., Bradley, D. A., & Bahruddin, N. A. (2016). Evaluating organ dose and radiation risk of routine CT examinations in Johor, Malaysia. *Sains Malaysiana*, 45(4), 567-573.
- Kataria, B., & Smedby, O. (2013). Patient dose and image quality in low-dose abdominal CT: a comparison between iterative reconstruction and filtered back projection. *Acta Radiologica*, 54(5), 540-548.
- Khawaja, R. D. A., Singh, S., Blake, M., Harisinghani, M., Choy, G., Karosmangulu,
 A., Padole, A., Do, S., Brown, K., Thompson, R. & Morton, T. (2015). Ultralow dose abdominal MDCT: using a knowledge-based Iterative Model Reconstruction technique for substantial dose reduction in a prospective clinical study. *European Journal of Radiology*, 84(1), 2-10.
- Kim, M., Lee, J. M., Yoon, J. H., Son, H., Choi, J. W., Han, J. K., & Choi, B. I. (2014). Adaptive iterative dose reduction algorithm in CT: effect on image quality compared with filtered back projection in body phantoms of different sizes. *Korean Journal of Radiology*, 15(2), 195-204.
- Klink, T., Obmann, V., Heverhagen, J., Stork, A., Adam, G., & Begemann, P. (2014). Reducing CT radiation dose with iterative reconstruction algorithms: the influence of scan and reconstruction parameters on image quality and CTDI_{vol}. *European Journal of Radiology*, 83(9), 1645-1654.
- Lam, D., Wootton-Gorges, S. L., McGahan, J. P., Stern, R., & Boone, J. M. (2011, January). Abdominal Pediatric Cancer Surveillance Using Serial Computed Tomography: Evaluation of Organ Absorbed Dose and Effective Dose. In Seminars in Oncology (Vol. 38, No. 1, pp. 128-135). Elsevier.

- Larobina, M., & Murino, L. (2014). Medical Image File Formats. *Journal of Digital Imaging*, 27(2), 200–206.
- Lin, E. C. (2010, December). Radiation risk from medical imaging. In Mayo Clinic Proceedings (Vol. 85, No. 12, pp. 1142-1146). Elsevier.
- Litmanovich, D. E., Tack, D. M., Shahrzad, M., & Bankier, A. A. (2014). Dose reduction in cardiothoracic CT: review of currently available methods. *Radiographics*, 34(6), 1469-1489.
- Liu, L. (2014). Model-based iterative reconstruction: a promising algorithm for today's computed tomography imaging. *Journal of Medical Imaging and Radiation Sciences*, 45(2), 131-136.
- Macari, M., Spieler, B., Kim, D., Graser, A., Megibow, A. J., Babb, J. & Chandarana,
 H. (2010). Dual-source dual-energy MDCT of pancreatic adenocarcinoma: initial observations with data generated at 80 kVp and at simulated weighted-average 120 kVp. *American Journal of Roentgenology*, *194*(1), 27-32.
- Matsuki, M., Murakami, T., Juri, H., Yoshikawa, S., & Narumi, Y. (2013). Impact of adaptive iterative dose reduction (AIDR) 3D on low-dose abdominal CT: comparison with routine-dose CT using filtered back projection. Acta Radiologica, 54(8), 869-875.
- McCollough, C. H., Leng, S., Yu, L., Cody, D. D., Boone, J. M. & McNitt-Gray, M.F. (2011). CT dose index and patient dose: they are not the same thing. *Radiology*, 259(2), 311-316.
- McCollough, C. H., Primak, A. N., Braun, N., Kofler, J., Yu, L., & Christner, J. (2009). Strategies for reducing radiation dose in CT. *Radiologic Clinics of North America*, 47(1), 27-40.
- McHugh, M. L. (2012). Interrater reliability: the kappa statistic. *Biochemia Medica*, 22(3), 276-282.
- McNitt-Gray, M. F. (2002). AAPM/RSNA Physics Tutorial for Residents: Topics in CT: Radiation Dose in CT 1. *Radiographics*, 22(6), 1541-1553.

- Ministry of Health Malaysia. *Guidelines in Malaysia Diagnostic Reference Levels in Medical Imaging (Radiology).* Putrajaya: Ministry of Health Malaysia. 2013.
- Mirsadraee, S., Weir, N. W., Connolly, S., Murchison, J. T., Reid, J. H., Hirani, N., Connell, M. & van Beek, E. J. (2015). Feasibility of radiation dose reduction using AIDR-3D in dynamic pulmonary CT perfusion. *Clinical Radiology*, 70(8), 844-851.
- Nakamoto, A., Kim, T., Hori, M., Onishi, H., Tsuboyama, T., Sakane, M., Tatsumi, M. & Tomiyama, N. (2015). Clinical evaluation of image quality and radiation dose reduction in upper abdominal computed tomography using model-based iterative reconstruction; comparison with filtered back projection and adaptive statistical iterative reconstruction. *European Journal of Radiology*, 84(9), 1715-1723.
- Naoum, C., Blanke, P., & Leipsic, J. (2015). Iterative reconstruction in cardiac CT. *Journal of Cardiovascular Computed Tomography*, 9(4), 255-263.
- Naumann, D. N., Raven, D., Pallan, A., & Bowley, D. M. (2014). Radiation exposure during paediatric emergency CT : Time we took notice ? *Journal of Pediatric Surgery*, 49(2), 305–307.
- Ng, K. H., Abdullah, B. J., & Sivalingam, S. (1999). Medical radiation exposures for diagnostic radiology in Malaysia. *Health Physics*, 77(1), 33-36.
- Nitta, N., Ikeda, M., Sonoda, A., Nagatani, Y., Ohta, S., Takahashi, M., & Murata, K. (2014). Images acquired using 320-MDCT with adaptive iterative dose reduction with wide-volume acquisition: visual evaluation of image quality by 10 radiologists using an abdominal phantom. *American Journal of Roentgenology*, 202(1), 2-12.
- Noriah, M. A. (2010). Challenges in strengthening radiation safety and security programme in Malaysia (IAEA-CN-18). International Atomic Energy Agency (IAEA)

- Ogden, C. L., Carroll, M. D., Kit, B. K., & Flegal, K. M. (2012). Prevalence of obesity and trends in body mass index among US children and adolescents, 1999-2010. *JAMA*, 307(5), 483-490.
- *Operation Manual for Whole-Body X-Ray CT Scanner Aquilion.* (2004). Toshiba Medical Systems Corporation.
- Pan, Y. N., Li, A. J., Chen, X. M., Wang, J., Ren, D. W., & Huang, Q. L. (2016). Coronary Computed Tomographic Angiography at Low Concentration of Contrast Agent and Low Tube Voltage in Patients with Obesity:: A Feasibility Study. *Academic Radiology*, 23(4), 438-445.
- Paul, N. S., Kashani, H., Odedra, D., Ursani, A., Ray, C., & Rogalla, P. (2011). The influence of chest wall tissue composition in determining image noise during cardiac CT. *American Journal of Roentgenology*, 197(6), 1328-1334.
- Pontana, F., Duhamel, A., Pagniez, J., Flohr, T., Faivre, J. B., Hachulla, A.L., Remy,
 J. & Remy-Jardin, M. (2011). Chest computed tomography using iterative reconstruction vs filtered back projection (Part 2): image quality of low-dose CT examinations in 80 patients. *European Radiology*, 21(3), 636-643.
- Prakash, P., Kalra, M. K., Kambadakone, A. K., Pien, H., Hsieh, J., Blake, M. A., & Sahani, D. V. (2010). Reducing abdominal CT radiation dose with adaptive statistical iterative reconstruction technique. *Investigative Radiology*, 45(4), 202-210.
- Rehani, M. M., Ciraj-Bjelac, O., Al-Naemi, H. M., Al-Suwaidi, J. S., El-Nachef, L., Khosravi, H. R., Kharita, M. H., Muthuvelu, P., Pallewatte, A. S., Juan, B. Y. C. S., Shaaban, M., & Zaman, A. (2012). Radiation protection of patients in diagnostic and interventional radiology in Asian countries: impact of an IAEA project. *European Journal of Radiology*, 81(10), 982–989.
- Renker, M., Nance Jr, J. W., Schoepf, U. J., O'Brien, T. X., Zwerner, P. L., Meyer, M., Kerl, J. M., Bauer, R. W., Fink, C., Vogl, T. J., & Henzler, T. (2011). Evaluation of heavily calcified vessels with coronary CT angiography: comparison of iterative and filtered back projection image reconstruction. *Radiology*, 260(2), 390-399.

- Rubin, G. D. (2014). Computed tomography: revolutionizing the practice of medicine for 40 years. *Radiology*, 273(2S), 45-74.
- Sagara, Y., Hara, A. K., Pavlicek, W., Silva, A. C., Paden, R. G., & Wu, Q. (2010). Abdominal CT: comparison of low-dose CT with adaptive statistical iterative reconstruction and routine-dose CT with filtered back projection in 53 patients. *American Journal of Roentgenology*, 195(3), 713-719.
- Semelka, R. C., Armao, D. M., Elias, J., & Huda, W. (2007). Imaging strategies to reduce the risk of radiation in CT studies, including selective substitution with MRI. *Journal of Magnetic Resonance Imaging*, 25(5), 900-909.
- Shah, A., Das, P., Subkovas, E., Buch, A. N., Rees, M., & Bellamy, C. (2015). Radiation dose during coronary angiogram: relation to body mass index. *Heart, Lung and Circulation*, 24(1), 21-25.
- Shah, D. J., Sachs, R. K., & Wilson, D. J. (2014). Radiation-induced cancer: a modern view. *The British Journal of Radiology*, 85(1020), 1166–1173.
- Shrimpton, P. C. *Protection of the Patient in X-ray Computed Tomography*. National Radiological Protection Board (NRPB). Chilton: NRPB. 3(4); 1992.
- Shrimpton, P. C., Hillier, M. C., Lewis, M. A., & Dunn, M. Doses from Computed Tomography (CT) Examinations in the UK–2003 Review. Chilton, UK: National Radiological Protection Board. 2005.
- Shrimpton, P. C., Hillier, M. C., Meeson, S., & Golding, S. J. Doses from computed tomography (CT) examinations in the UK-2011 review. Chilton, UK: Public Health England Centre for Radiation, Chemical and Environmental Hazards. 2014.
- Shuman, W. P., Chan, K. T., Busey, J. M., Mitsumori, L. M., Choi, E., Koprowicz, K. M., & Kanal, K. M. (2014). Standard and reduced radiation dose liver CT images: adaptive statistical iterative reconstruction versus model-based iterative reconstruction—comparison of findings and image quality. *Radiology*, 273(3), 793-800.

- Singh, S., Kalra, M. K., Hsieh, J., Licato, P. E., Do, S., Pien, H. H., & Blake, M. A. (2010). Abdominal CT: comparison of adaptive statistical iterative and filtered back projection reconstruction techniques. *Radiology*, 257(2), 373-383.
- Smith-Bindman, R., Lipson, J., Marcus, R., Kim, K. P., Mahesh, M., Gould, R., de Gonzalez, A. B., & Miglioretti, D. L. (2009). Radiation dose associated with common computed tomography examinations and the associated lifetime attributable risk of cancer. *Archives of Internal Medicine*, 169(22), 2078-2086.
- Sokolovskaya, E., & Shinde, T. (2016). Comparison of utilization rate of CT scans of the abdomen and pelvis in patients with elevated BMI compared to patients with normal BMI presenting to the ER with gastrointestinal symptoms. *Radiography*, 22(1), 21-24.
- Sun, G., Hou, Y. B., Zhang, B., Yu, L., Li, S. X., Tan, L. L., & Chen, D. J. (2015). Application of low tube voltage coronary CT angiography with low-dose iodine contrast agent in patients with a BMI of 26–30 kg/m 2. *Clinical Radiology*, 70(2), 138-145.
- Sun, Z. (2007). Multislice CT angiography in aortic stent grafting: relationship between image noise and body mass index. *European Journal of Radiology*, 61(3), 534-540.
- The International Commission on Radiation Units and Measurements. (2012).
 Radiation Dose and Image-Quality Assessment in Computed Tomography (Vol. 12). USA: Oxford University Press.
- Tomizawa, N., Nojo, T., Akahane, M., Torigoe, R., Kiryu, S., & Ohtomo, K. (2012). Adaptive iterative dose reduction in coronary CT angiography using 320-row CT: assessment of radiation dose reduction and image quality. *Journal of Cardiovascular Computed Tomography*, 6(5), 318-324.
- Trattnig, S., Welsch, G. H., Juras, V., Szomolanyi, P., Mayerhoefer, M. E., Stelzeneder, D., Mamisch, T. C., Bieri, O., Scheffler, K. & Zby, S. (2010).
 23Na MR Imaging at 7 T after Knee Matrix–associated Autologous Chondrocyte Transplantation Preliminary Results 1. *Radiology*, 257(1), 175-184.

- Tsapaki, V., Rehani, M., & Saini, S. (2010). Radiation Safety in Abdominal Computed Tomography. In *Seminars in Ultrasound, CT, and MRI, 1*(31), 29-38.
- UNSCEAR. (2010). Report of the United Nations Scientific Committee on the Effects of Atomic Radiation. *United Nations Assembly in 2011, New York*.
- Valentin, J. The 2007 recommendations of the International Commission on Radiological Protection. International Commission on Radiological Protection. Oxford, UK: Elsevier. 2007.
- Vardhanabhuti, V., Riordan, R. D., Mitchell, G. R., Hyde, C., & Roobottom, C. A. (2014). Image comparative assessment using iterative reconstructions: clinical comparison of low-dose abdominal/pelvic computed tomography between adaptive statistical, model-based iterative reconstructions and traditional filtered back projection in 65 patients. *Investigative Radiology*, 49(4), 209-216.
- Verdun, F. R., Racine, D., Ott, J. G., Tapiovaara, M. J., Toroi, P., Bochud, F. O., Veldkamp, W. J. H., Schegerer, A., Bouwman, R. W., Giron, I. H., & Marshall, N. W. (2015). Image quality in CT: From physical measurements to model observers. *Physica Medica*, *31*(8), 823-843.
- Wang, A. J., Goldsmith, Z. G., Wang, C., Nguyen, G., Astroza, G. M., Neisius, A., Iqbal, M. W., Neville, A. M., Lowry, C., Toncheva, G. & Yoshizumi, T. T. (2013). Obesity triples the radiation dose of stone protocol computerized tomography. *The Journal of Urology*, 189(6), 2142-2146.
- Williams, M. C., Weir, N. W., Mirsadraee, S., Millar, F., Baird, A., Minns, F., Uren, N. G., McKillop, G., Bull, R. K., van Beek, E. J. R. & Reid, J. H. (2013). Iterative reconstruction and individualized automatic tube current selection reduce radiation dose while maintaining image quality in 320-multidetector computed tomography coronary angiography. *Clinical Radiology*, 68(11), 570-577.
- Wilting, J. E., Zwartkruis, A., van Leeuwen, M. S., Timmer, J., Kamphuis, A. G., & Feldberg, M. (2001). A rational approach to dose reduction in CT: individualized scan protocols. *European Radiology*, 11(12), 2627-2632

- Xu, J., Mahesh, M., & Tsui, B. M. (2009). Is Iterative Reconstruction Ready for MDCT? Journal of the American College of Radiology, 6(4), 274-276.
- Yamada, Y., Jinzaki, M., Hosokawa, T., Tanami, Y., Sugiura, H., Abe, T., & Kuribayashi, S. (2012). Dose reduction in chest CT: comparison of the adaptive iterative dose reduction 3D, adaptive iterative dose reduction, and filtered back projection reconstruction techniques. *European Journal of Radiology*, 81(12), 4185-4195.
- Yamamura, S., Oda, S., Imuta, M., Utsunomiya, D., Yoshida, M., Namimoto, T., Yuki,
 H., Kidoh, M., Funama, Y., Baba, H., & Yamashita, Y. (2016). Reducing the
 Radiation Dose for CT Colonography: Effect of Low Tube Voltage and
 Iterative Reconstruction. *Academic Radiology*, 23(2), 155-162.
- Yoon, J. H., Lee, J. M., Hur, B. Y., Baek, J., Shim, H., Han, J. K., & Choi, B. I. (2015). Influence of the adaptive iterative dose reduction 3D algorithm on the detectability of low-contrast lesions and radiation dose repeatability in abdominal computed tomography: a phantom study. *Abdominal Imaging*, 40(6), 1843-1852.
- Yoshimura, N., Sabir, A., Kubo, T., Lin, P. J. P., Clouse, M. E., & Hatabu, H. (2006). Correlation between image noise and body weight in coronary CTA with 16row MDCT. *Academic Radiology*, 13(3), 324-328.
- Zarb, F., Rainford, L., & McEntee, M. F. (2010). Image quality assessment tools for optimization of CT images. *Radiography*, 16(2), 147-153.