

**MID-RANGE TRANSFORMER BASED WIRELESS POWER TRANSFER  
SYSTEM FOR LOW POWER DEVICES**

**LEONG KAH MENG**

**A thesis submitted in fulfilment of the  
requirements for the award of the degree of  
Master of Engineering (Biomedical)**

**Faculty of Biosciences and Medical Engineering  
Universiti Teknologi Malaysia**

**DECEMBER 2016**

Dedication to my mum and dad,

my brothers and sisters,

and my beloved friends.

## **ACKNOWLEDGEMENT**

First of all, I would like to say thank you to my supervisor, Dr Tan Tian Swee for all his given guidance and assistance throughout my Master study. Countless useful advice had been bestowed by him which were always directing me to the correct path.

Here would also like to express my sincerest gratitude to my senior, Dr Lum Kin Yun who always supportive in my work. He is a helpful person that always teach me and guide me during research work.

At the same time, to all my colleagues and friends from UTM, I am very fortunate to have you in my life for giving me all the beautiful unforgettable memories.

Last but not least, special dedication to my family, for the caring and financial support. They are always my backbone and I am not manage without them. Thank you.

## ABSTRACT

Wireless power transfer technique for biomedical devices has drawn great interest from many researchers in the biomedical domain. Biomedical devices can be powered up either by an external power cord or by batteries. However an external power cord may limit the mobility of a patient and batteries tend to have a very limited power capacity and these methods may pose a high risk of infection towards the patient. Therefore, a wireless power transfer system is proposed to solve the problem. This study attempts to develop a mid-range transformer based wireless power transmission system which is suitable to power biomedical devices. This includes the development of a transmitter circuit, receiver circuit, a pair of transmitter and receiver coils and transformers. This study demonstrates that magnetic coupling technique is a reliable wireless charging technique biomedical devices due to its mid-range transmission and satisfactory efficiency. In order to reduce power loss, an impedance matching method which incorporates a step-up and step-down transformers in the transmitter and receiver circuit is proposed. This study also develops a wireless power charging system that does not emit harmful radiation towards the human body. The frequency for the system is within the range of 700 kHz to 900 kHz which is in accordance to the ICNIRP regulation. Three pairs of round-shaped transmitter and receiver coils pair have been designed and fabricated with the diameter size of 30cm, 40cm, and 50cm. The power supply and frequency generator are connected to the transmitter circuit and an oscilloscope is connected to the load of the receiver circuit. The performance results are recorded using a range from 4 centimeters to 110 centimeters and based on the tabulated results, the mid-range wireless power transfer system managed to supply a transfer efficiency of 60% at a distance of 35cm for the 30cm diameter coil, 62% at a distance of 43cm for the 40cm diameter coil and 46% at a distance of 50cm for the 50cm diameter coil.

## ABSTRAK

Teknik pemindahan kuasa tanpa wayar untuk peranti bioperubatan telah menarik minat ramai penyelidik dalam domain bioperubatan. Peranti bioperubatan boleh dihidupkan sama ada dengan kord kuasa luar atau oleh bateri. Walau bagaimanapun wayar kuasa luar boleh membataskan pergerakan pesakit. Ini boleh memberi risiko jangkitan yang tinggi terhadap pesakit. Oleh itu, sistem pemindahan kuasa tanpa wayar adalah dicadangkan untuk menyelesaikan masalah tersebut. Kajian ini bertujuan untuk membangunkan satu sistem penghantaran kuasa tanpa wayar berdasarkan transformer yang sesuai dalam mengecas peranti bioperubatan. Ini termasuk membangunkan sebuah litar pemancar, litar penerima, sepasang pemancar dan penerima gegelung dan pengubah. Kajian ini menunjukkan bahawa teknik gandingan magnet adalah teknik pengecasan tanpa wayar yang paling cekap dan memuaskan. Dalam usaha untuk mengurangkan kehilangan kuasa, satu teknik padanan impedans yang menggabungkan transformer langkah-naik dan transformer langkah-turun dalam pemancar dan penerima litar juga dicadangkan. Kajian ini juga membangunkan sistem tenaga pengecasan tanpa wayar yang tidak memancarkan radiasi berbahaya terhadap badan manusia. Frekuensi untuk sistem ini adalah dalam julat 700 kHz hingga 900 Hz yang selaras dengan peraturan ICNIRP. Tiga pasang pemancar berbentuk bulat dan penerima pasangan gegelung telah direka dengan saiz diameter 30cm, 40cm, dan 50cm. Bekalan kuasa dan penjana frekuensi disambungkan kepada litar pemancar dan osiloskop disambungkan ke beban litar penerima. Keputusan prestasi direkodkan menggunakan pelbagai dari 4 sentimeter hingga 110 sentimeter dan berdasarkan keputusan yang dijadualkan itu, wayarles sistem pemindahan kuasa pertengahan berjaya membekalkan kecekapan pemindahan sebanyak 60% pada jarak 35 cm bagi gegelung 30cm diameter, 62 % pada jarak 43 cm bagi gegelung 40cm diameter dan 46% pada jarak 50cm untuk gegelung 50cm diameter.



2.3	Introduction to Different Wireless Transmission Techniques	11
2.3.1	Radio Frequency	14
2.3.2	Inductive Coupling Wireless Transfer Technique	16
2.3.3	Magnetic Resonant Coupling	18
2.3.4	Comparison and Summary on Three Different Wireless Transfer Technology	19
2.4	Mid-range Wireless Power Transfer Technique via Magnetic Resonant Coupling	23
2.4.1	Two Coils Wireless Power Transfer System	23
2.4.2	Four Coils Wireless Power Transfer System	26
2.4.3	Wireless Power Transfer Systems with Relay Resonators	28
2.4.4	Wireless Power Domino Resonator Systems	29
2.4.5	Summary on Four Types of Magnetic Resonant Coupling Techniques	30
2.5	Safety Exposure Issues	32
2.6	Scattering Parameters	34
<b>3</b>	<b>METHODOLOGY</b>	<b>36</b>
3.1	Implementation Plan	36
3.2	Grand Vision for Mid-Range Wireless Charging System	37
3.3	Hardware Prototyping	41
3.4	Transformer Based Impedance Modeling	43
3.4.1	Analysis of two coil wireless power transfer system without transformer	44
3.4.2	Impedance matching technique for two coils WPT system with transformer	45
3.4.3	Transformer Design in two coils WPT System	49
3.5	System Validation	52
3.6	Two Coil WPT Modeling Simulation	57
3.6.1	Two coil WPT modeling for 30cm Coil Diameter.	57

	3.6.2	Two coil WPT modeling for 40cm Coil Diameter.	58
	3.6.3	Two coil WPT modeling for 50cm Coil Diameter.	60
<b>4</b>		<b>EXPERIMENTAL SETUP</b>	<b>63</b>
<b>5</b>		<b>RESULT AND DISCUSSION</b>	<b>71</b>
	5.1	Qualify Factor of The Transmitter and Receiver Coils	71
	5.1.1	Quality Factor for 30cm Coil	72
	5.1.2	Quality Factor for 40cm Coil	72
	5.1.3	Quality Factor for 50cm Coil	73
	5.2	Simulation Result Comparison Before and After Impedance Matching	74
	5.2.1	Simulation Result for 30cm Coil Diameter.	75
	5.2.2	Simulation Result for 40cm Coil Diameter.	76
	5.2.3	Simulation Result for 50cm Coil Diameter.	78
	5.2.4	Summary for The Three Result Simulation Comparison.	79
	5.3	Result Verification	79
	5.3.1	Comparison Experimental Result and Simulation Result for 30cm Coil Diameter	79
	5.3.2	Comparison Experimental Result and Simulation Result for 40cm Coil Diameter	81
	5.3.3	Comparison Experimental Result and Simulation Result for 50cm Coil Diameter	83
	5.4	Safety Test for Two Coil Wireless Power Transmission System	85
<b>6</b>		<b>CONCLUSION</b>	<b>89</b>
	6.1	Research Outcomes	89



6.2	Contribution to Knowledge	90
6.3	Future Works	91

<b>REFERENCES</b>	<b>92</b>
-------------------	-----------

Appendices A – C	99 – 106
------------------	----------

**LIST OF TABLES**

<b>TABLE NO.</b>	<b>TITLE</b>	<b>PAGE</b>
2.1	Comparison for near-field and far-field wireless transfer technique	10
2.2	Comparison for near-field and far-field wireless transfer technique	12
2.3	Comparison of three wireless power transfer techniques	22
2.4	Comparison for four types of magnetic resonant coupling techniques	31
3.1	Mid-range wireless charging system specifications	41
3.2	Parameters used for equation simulation and $S_{21}$ simulation	56
3.3	Simulation Parameters for 30cm diameter coil	57
3.4	Simulation Parameters for 40cm diameter coil	59
3.5	Simulation Parameters for 50cm diameter coil	61
A.1	Results of 30cm coil	99
B.1	Results of 50cm coil	102
C.1	Results of 50cm coil	106

## LIST OF FIGURES

FIGURE NO.	TITLE	PAGE
2.1	Pacemaker	7
2.2	Implantable cardioverter Defibrillator (ICD)	7
2.3	Thoratec heartmate II	8
2.4	Heartware	9
2.5	Concept for wireless power transmission via RF	14
2.6	Microstrip antenna	16
2.7	Basic inductive coupling system	17
2.8	TET system	17
2.9	Quality factor versus number of turns of 40 cm coils	18
2.10	Equivalent circuit for 2 coils system	25
2.11	Four coils wireless power transfer system	26
2.12	FREE-D system	28
2.13	Examples of domino-resonator arrangements	30
2.14	ICNIRP Reference levels for exposure to time-varying electric and magnetic fields	33
2.15	IEEE Reference levels for exposure to time-varying electric and magnetic fields	33
3.1	Reseach Workflows	37
3.2	Room setting layout	38
3.3	WPT design a	39
3.4	WPT design b	39
3.5	WPT design c	40
3.6	Basic Building Block Of A Proposed Wireless Power Transmission System.	42
3.7	Flows for transformer based impedance modeling	43
3.8	Two coils WPT shematic diagram	44
3.9	Schematic diagram for two coils WPT system with transformers	46
3.10	Transformer coupled wireless power transfer system modeling	46

3.11	Transformer design	51
3.12	Different Size of Transmitter And Receiver Coils pair	53
3.13	Result comparison from equation simulation and $S_{21}$ simulations	56
3.14	Agilent ADS simulation schematics for 30cm diameter coil.	58
3.15	Agilent ADS simulation schematics for 40cm diameter coil.	60
3.16	Agilent ADS simulation schematics for 50cm diameter coil.	62
4.1	Different Size of Transmitter And Receiver Coils pair	63
4.2	Quality Factor Measured of the coil	64
4.3	Fabricated transformer	65
4.4	Transmitter circuit connect to function generator and power source	66
4.5	Connection for power source and transmitter circuit	66
4.6	Receiver circuit connect to LCR meter	67
4.7	Connection for receiver circuit and oscilloscope	68
4.8	Result recorded during the experiment	68
4.9	Safety test using Aaronia Spectrum Analyzers NF-5035	69
4.10	MCS realtime spectrum analyzer software	70
5.1	Quality factor versus number of turns of 30 cm coils	72
5.2	Quality factor versus number of turns of 40 cm coils	73
5.3	Quality factor versus number of turns of 50 cm coils	74
5.4	$S_{21}$ simulation before and after impedance matching for 30cm diameter coil	75
5.5	$S_{21}$ simulation before and after impedance matching for 40cm diameter coil	77
5.6	$S_{21}$ simulation before and after impedance matching for 50cm diameter coil	78
5.7	Comparison for the experimental and simulation results for 30cm diameter coil	80
5.8	Comparison for the experimental and simulation results for 40cm diameter coil	82
5.9	Comparison for the experimental and simulation results for 50cm diameter coil	84
5.10	Safety test perform with Aaronia Spectrum Analyzers	86
5.11	Safety test perform with Aaronia Spectrum Analyzers	87

**LIST OF ABBREVIATIONS**

ADS	-	Advanced Design System
ICD	-	Implantable cardioverter defibrillator
FREE-D	-	Free-Range Resonant Electrical Energy Delivery
LVAD	-	Left ventricular assist device
TET	-	Transcutaneous Energy Transfer
WPT	-	Wireless power transmission
ICNIRP	-	International Commission on Non-Ionizing Radiation Protection

**LIST OF SYMBOLS**

$\omega$	-	Angular frequency
$c$	-	speed of light
$C$	-	Capacitance
$L$	-	Inductance
$f$	-	Resonant frequency
$I$	-	AC Current
$V$	-	AC Voltage
$M$	-	Mutual inductance
$k$	-	Coupling coefficient
$Q$	-	Quality factor
$X$	-	Reactant
$n$	-	Transformer ratio
$N$	-	Number of turns
$A$	-	Cross sectional area
$R$	-	Resistance
$Z$	-	Impedance
$P$	-	Power
$S$	-	Forward gain

**LIST OF APPENDICES**

<b>APPENDIX</b>	<b>TITLE</b>	<b>PAGE</b>
A	Results of 30cm coil	99
B	Results of 40cm coil	102
C	Results of 50cm coil	106

## **CHAPTER 1**

### **INTRODUCTION**

This chapter will briefly discussed about the background study, problem statement, objectives, scope of study and importance of the research for the mid-range wireless charging system for biomedical applications. Mid-range defined as the transmission range can be acheived more than one antenna diameter but less than or equal to 10 antenna diameter. The backgroud study describes the recent trend about the biomedical devices used for patients. The problem statement decrives the obstacles and limitations for recent technologies about biomedical devices. The objectives are set to tackle the problems. The scope of study will serve as a guideline when doing the research. The importance of the mid-range wireless charging system for biomedical devices is also presented.

#### **1.1 BACKGROUND STUDY**

A medical device may refer to any instrument or apparatus to be used on human beings for the purpose of diagnosis, prevention monitoring, treatment or alleviation of disease. Medical implant devices are getting popular and critical in today and future healthcare market due to the ability to locally stimulate internal organs and communicate the internal important data to the outside world (Li *et al.*, 2012; RamRakhyani *et al.*, 2011). Riding on the advances in integrated circuit (IC) technology today, the electronic system can be made completely implantable (Chandrakasan *et al.*, 2008). For the past four decades, there is a significant development and implementation for implantable medical devices. The examples of medical implantable devices are pacemakers, defibrillators, circulatory assist devices, artificial hearts, cochlear implants, neuromuscular stimulators, and analog sensors (Sanni *et al.*, 2012).These implantable devices or low-power biosensors serve as devices for identification, monitoring and treatment of patients (Fowler *et al.*, 2012;



Zhu *et al.*, 2011). Besides that, it can also perform therapeutic, prosthetic, and diagnostic functions (Liu *et al.*, 2009b). Some research data show that the global medical device market yielded around \$209 billion during year 2006.

However, these electronic devices are not self-powered. It is greatly depending on the electricity from the battery which is coupled together with the devices. Early implantable devices such as pacemakers are powered by small lithium ion batteries (Laskovski *et al.*, 2009). Even though the battery is coupled together with the implanted devices is able to supply stable electrical energy, the limitation in energy storage is still hindering its application and durability (Hu *et al.*, 2005). The internal battery has the disadvantages of limited life time, large volume and leakage possibility, hence it is not a preferable solution in this area of interest (Cha *et al.*, 2012; Li *et al.*, 2012; Samad *et al.*, 2006).

Devices such as the implanted extendable rod for the treatment of adolescent idiopathic scoliosis or as growing prosthesis for young patients with bone cancer, it requires several watts of electric power to drive the electric motor (Jiang *et al.*, 2010). For this high power demand device, a more frequent recharging of battery or replacement is required. This increases the risk of operation. Otherwise, a transcutaneous power cord has to be made out from the patient's skin in order to charge the devices. According to a research, there are about 40 percent of patients who are infected due to this opening and require re-hospitalization. In some extreme case, the patients might die from it. In order to reduce the fatality rate of patients, which is the objective of medication, a continuous supply of energy is crucial in order for the devices to operate continuously and reliably (RamRakhyani *et al.*, 2011; Zhu *et al.*, 2011).

As a result, it is a meaningful study in order to power these implanted devices efficiently (Liu *et al.*, 2009b; Si *et al.*, 2007). Moreover, due to the space constraint, real-time energy supplying system can save a lot of space as well Laskovski *et al.* (2009). If these problems can be solved by getting rid of the cable, the human made devices can be a good alternative for the patients to recover.

## 1.2 PROBLEM STATEMENT

As mentioned in the background study, the power supply for the implantable devices can only be obtained mainly through two processes, which are the battery replacement or via external power cord charging.

The energy supply is crucial in the functionality of biomedical devices. Hence, an efficient, continuous and stable supply of energy is required. These devices must receive energy supply externally or harvest the ambient energy. For non-implantable devices, batteries can be easily replaced or recharged. For the patient's benefit, it is also not recommended to do it frequently. One of the examples is the behind-the-ear cochlear instrument which has to be charged everyday. However, the batteries in implantable devices can only be replaced or recharged by surgery. Therefore, an alternative solution such as wireless power charging may be a viable solution (Chandrakasan *et al.*, 2008).

An alternative method to use is transcutaneous power cable. Generally, the percutaneous link across the body skin is used to recharge the internal battery (RamRakhyani *et al.*, 2011). However, it may pose infection risks to the patients and the wire is also somehow entangled and causes restriction in mobility (Samad *et al.*, 2006; Si *et al.*, 2007). The power cord also restricts the patient to perform activities related to water. Since human is an individual which required motion and freedom, the constantly charging also make them have to stick to a place for certain amount of time periodically. These will cause low mobility and not productive for the patients to carry out their works.

So, if the electric supply for the implant devices can be solve, certainly it will make the biomedical implant devices more applicable and help to save more life.

## 1.3 OBJECTIVE

This research has proposed the use of wireless power charging technology to charge the battery of biomedical devices. The objectives for this research are outlined as follow:

1. To develop a mid-range wireless power transmission system to charge the biomedical devices.
2. To design a transformer based wireless power transmission system.
3. To evaluate the safety performance of developed wireless power transfer system.

#### **1.4 SCOPE**

The area of interest of this research is limited to the following scope:

1. The research focuses on the development of transmitter circuit and receiver circuit. This include the transmitter and receiver coils pair design and the impedance matching for the system.
2. This wireless energy transfer system is only implemented for biomedical applications.
3. The viable range for charging the devices should be within 1meter.
4. The target power of biomedical devices is from 1 watt to 5 watt.
5. The range of frequency used should be lower than 1MHz

#### **1.5 IMPORTANCE OF RESEARCH**

This system is expected to contribute to the advancement of biomedical technology for more patients to benefit from it especially for those who need the biomedical devices to sustain their life. The increasing usability of cables for charging purposes towards the biomedical devices will limit the mobility of patients during the charging process. In addition, when replacing the batteries of some implantable biomedical devices in human body, it will increase risk of several infection during the operation surgery. Hence, the wireless power charging system is a better solution for those problems.

## 1.6 Thesis Organisation

Chapter 1 introduces the background of the study. It gives a brief introduction on the problems related to the biomedical devices. In addition, it also list out the objectives and the scope of this study.

Chapter 2 presentes the literature review for this research. It includes a history of recent wireless charging technology and its founder. Comparisons between three different techniques of wireless charging technologies, namely inductive transfer, magnetic resonant coupling and radio frequency energy transfer are described. Magnetic resonant coupling technique is used in this research and for further elaboration. The technical review on magnetic resonant coupling for two coil transfer system, four coil transfer systema and resonators are presented in this chapter. A short discussion on mid-range wireless charging system can improve patients life is presented in this chapter. The available evaluation methods are discussed based on the suitability and effectiveness and how the results are statistically compared is also introduced in this chapter.

Chapter 3 present the methodology used in this study. It describes the quality factor of transmitter and receiver coils pair being measured and fabricated, the impedance matching apply to the system to improved efficiency, the system machanism of the system works, and measurement, tabulation and verification of results.

Chapter 4 present the experiment set up for the study. It shows the procedures and preparations for the experiment and equipment used.

Chapter 5 presents the result and discussion section. It shows the quality factor measured for each different transmitter and receiver coils. It also compares the result from the experimental and simulation result and provides some discussions and also compares with the preformance current wireless technologies with others researches.

Chapter 6 summarises the conclusion and the contributions of this research. The future works are also presented at the end of this chapter.

## REFERENCES

- (????).
- Agbinya, J. I. (2012). Techniques for Optimal Wireless Power Transfer Systems. *Wireless Power Transfer*, 201.
- AlTawy, R. and Youssef, A. M. (2016). Security Tradeoffs in Cyber Physical Systems: A Case Study Survey on Implantable Medical Devices. *IEEE Access*. 4, 959–979.
- Baarman, D. W. and Schwannecke, J. (2015). White paper: Understanding Wireless Power. *Fulton Innovation*. Retrieved January. 3.
- Bawa, G. and Ghovanloo, M. (2008). Active high power conversion efficiency rectifier with built-in dual-mode back telemetry in standard CMOS technology. *IEEE transactions on biomedical circuits and systems*. 2(3), 184–192.
- Bawa, G., Huang, A. Q. and Ghovanloo, M. (2010). An efficient 13.56 MHz active back-telemetry rectifier in standard CMOS technology. In *Proceedings of 2010 IEEE International Symposium on Circuits and Systems*. IEEE, 1201–1204.
- Beasley, J. S. (2010). Modern electronic communication.
- Boys, J. *et al.* (1998). Inductive power transfer across an extended gap. *WO*. 98, 50993.
- Budhia, M., Boys, J. T., Covic, G. A. and Huang, C.-Y. (2013). Development of a single-sided flux magnetic coupler for electric vehicle IPT charging systems. *IEEE Transactions on Industrial Electronics*. 60(1), 318–328.
- Budhia, M., Covic, G. A. and Boys, J. T. (2011). Design and optimization of circular magnetic structures for lumped inductive power transfer systems. *IEEE Transactions on Power Electronics*. 26(11), 3096–3108.
- Cha, H.-K., Park, W.-T. and Je, M. (2012). A CMOS rectifier with a cross-coupled latched comparator for wireless power transfer in biomedical applications. *IEEE Transactions on Circuits and Systems II: Express Briefs*. 59(7), 409–413.
- Chandrakasan, A. P., Verma, N. and Daly, D. C. (2008). Ultralow-power electronics for biomedical applications. *Biomedical Engineering*. 10.
- Chen, C.-J., Chu, T.-H., Lin, C.-L. and Jou, Z.-C. (2010). A study of loosely coupled coils for wireless power transfer. *IEEE Transactions on Circuits and Systems II:*

- Express Briefs*. 57(7), 536–540.
- Cheon, S., Kim, Y.-H., Kang, S.-Y., Lee, M. L., Lee, J.-M. and Zyung, T. (2011). Circuit-model-based analysis of a wireless energy-transfer system via coupled magnetic resonances. *IEEE Transactions on Industrial Electronics*. 58(7), 2906–2914.
- Christ, A., Douglas, M. G., Roman, J. M., Cooper, E. B., Sample, A. P., Waters, B. H., Smith, J. R. and Kuster, N. (2013). Evaluation of wireless resonant power transfer systems with human electromagnetic exposure limits. *IEEE Transactions on Electromagnetic Compatibility*. 55(2), 265–274.
- DiMarco, J. P. (2003). Implantable cardioverter–defibrillators. *New England Journal of Medicine*. 349(19), 1836–1847.
- Fowler, A. G., Moheimani, S. R. and Behrens, S. (2012). A 3-DoF MEMS ultrasonic energy harvester. In *Sensors, 2012 IEEE*. IEEE, 1–4.
- Gozalvez, J. (2007). WiTricity-the wireless power transfer [Mobile radio]. *IEEE Vehicular Technology Magazine*. 2(2), 38–44.
- Guo, S. and Lee, H. (2009). An efficiency-enhanced CMOS rectifier with unbalanced-biased comparators for transcutaneous-powered high-current implants. *IEEE Journal of Solid-State Circuits*. 44(6), 1796–1804.
- Harrist, D. W. (2004). *Wireless battery charging system using radio frequency energy harvesting*. Ph.D. Thesis. University of Pittsburgh.
- Ho, S., Wang, J., Fu, W. and Sun, M. (2011). A comparative study between novel witricty and traditional inductive magnetic coupling in wireless charging. *IEEE Transactions on Magnetics*. 47(5), 1522–1525.
- Hu, S.-K., Chou, T.-C. and Hwang, B.-J. (2005). Effect of cathode structure on cell performance in wireless charging process. *Journal of power sources*. 146(1), 606–610.
- Hui, S. Y. R., Zhong, W. and Lee, C. K. (2014). A critical review of recent progress in mid-range wireless power transfer. *IEEE Transactions on Power Electronics*. 29(9), 4500–4511.
- Imura, T. and Hori, Y. (2011). Maximizing air gap and efficiency of magnetic resonant coupling for wireless power transfer using equivalent circuit and Neumann formula. *IEEE Transactions on Industrial Electronics*. 58(10), 4746–4752.
- Islam, M. T., Shakib, M. N. and Misran, N. (2009). Broadband E-H shaped microstrip patch antenna for wireless systems. *Progress In Electromagnetics Research*. 98, 163–173.

- Jang, B.-J., Lee, S. and Yoon, H. (2012). HF-band wireless power transfer system: Concept, issues, and design. *Progress in electromagnetics research*. 124, 211–231.
- Jiang, H., Zhang, J. M., Liou, S. S., Fechter, R., Hirose, S., Harrison, M. and Roy, S. (2010). A high-power versatile wireless power transfer for biomedical implants. In *2010 Annual International Conference of the IEEE Engineering in Medicine and Biology*. IEEE, 6437–6440.
- Jow, U.-M. and Ghovanloo, M. (2007). Design and optimization of printed spiral coils for efficient transcutaneous inductive power transmission. *IEEE Transactions on Biomedical Circuits and Systems*. 1(3), 193–202.
- Kalathiya, R. J., Chaisson, J. M., Stevens, G. R., Sciortino, C. M., Shah, A. S., Whitman, G. J., Russell, S. D. and Tedford, R. J. (2014). Cardiac Index Declines During Long-term LVAD Support. *Circulation*. 130(Suppl 2), A18178–A18178.
- Karalis, A., Joannopoulos, J. D. and Soljačić, M. (2008). Efficient wireless non-radiative mid-range energy transfer. *Annals of Physics*. 323(1), 34–48.
- Kiani, M. and Ghovanloo, M. (2012). The circuit theory behind coupled-mode magnetic resonance-based wireless power transmission. *IEEE Transactions on Circuits and Systems I: Regular Papers*. 59(9), 2065–2074.
- Kim, Y.-H., Kang, S.-Y., Cheon, S., Lee, M.-L. and Zyung, T. (2011). Wireless charging technology using magnetically coupled resonators. In *2011 IEEE 33rd International Telecommunications Energy Conference (INTELEC)*. IEEE, 1–3.
- Kim, Y.-H., Kang, S.-Y., Cheon, S., Lee, M.-L., Zyung, T. *et al.* (2010). Optimization of wireless power transmission through resonant coupling. In *SPEEDAM 2010*. IEEE, 1069–1073.
- Kurs, A. (2007). *Power transfer through strongly coupled resonances*. Ph.D. Thesis. Massachusetts Institute of Technology.
- Kurs, A., Karalis, A., Moffatt, R., Joannopoulos, J. D., Fisher, P. and Soljačić, M. (2007). Wireless power transfer via strongly coupled magnetic resonances. *science*. 317(5834), 83–86.
- Laskovski, A. N., Yuce, M. R. and Dissanayake, T. (2009). *Wireless power technology for biomedical implants*. INTECH Open Access Publisher.
- Lee, C. K., Zhong, W. and Hui, S. (2012). Effects of magnetic coupling of nonadjacent resonators on wireless power domino-resonator systems. *IEEE Transactions on Power Electronics*. 27(4), 1905–1916.
- Leong Kah Meng, L. K. Y., Tan Tian Swee (2014). Wireless power transfer using microstrip antenna]. *American Journal of Applied Sciences*. 11(2), 195–201.

- Li, X., Zhang, H., Peng, F., Li, Y., Yang, T., Wang, B. and Fang, D. (2012). A wireless magnetic resonance energy transfer system for micro implantable medical sensors. *Sensors*. 12(8), 10292–10308.
- Liu, X., Zhang, F., Hackworth, S. A., Sciabassi, R. J. and Sun, M. (2009a). Modeling and simulation of a thin film power transfer cell for medical devices and implants. In *2009 IEEE International Symposium on Circuits and Systems*. IEEE, 3086–3089.
- Liu, X., Zhang, F., Hackworth, S. A., Sciabassi, R. J. and Sun, M. (2009b). Wireless power transfer system design for implanted and worn devices. In *2009 IEEE 35th Annual Northeast Bioengineering Conference*. IEEE, 1–2.
- Lo, E., Truong, H., Elnatan, L., Mar, A., Nguyen, H. and Kwok, R. (2005). Wireless Battery Charger. *EE 198B Final Report Dec. 2*.
- Mandal, S. and Sarpeshkar, R. (2007). Low-power CMOS rectifier design for RFID applications. *IEEE Transactions on Circuits and Systems I: Regular Papers*. 54(6), 1177–1188.
- McCarthy, P. M., Schmitt, S. K., Vargo, R. L., Gordon, S., Keys, T. F. and Hobbs, R. E. (1996). Implantable LVAD infections: implications for permanent use of the device. *The Annals of thoracic surgery*. 61(1), 359–365.
- Mur-Miranda, J. O., Fanti, G., Feng, Y., Omanakuttan, K., Ongie, R., Setjoadi, A. and Sharpe, N. (2010). Wireless power transfer using weakly coupled magnetostatic resonators. In *2010 IEEE Energy Conversion Congress and Exposition*. IEEE, 4179–4186.
- Parks, T. J. and Register, D. S. (1995). *Inductive coupling system for power and data transfer*. US Patent 5,455,466.
- Patel, D., Hasselblad, V., Patel, C., Pokorney, S., Zeitler, E., Rogers, J., Daubert, J., Khazanie, P., Sun, A., Mentz, R. *et al.* (2016). The Role Of Implantable Cardioverter Defibrillators (ICDS) In Patients With A Left Ventricular Assist Device (LVAD): A Systematic Review and Meta-analysis. *Journal of the American College of Cardiology*. 67(13\_S), 700–700.
- Pinuela, M., Yates, D. C., Lucyszyn, S. and Mitcheson, P. D. (2013). Maximizing DC-to-load efficiency for inductive power transfer. *IEEE transactions on power electronics*. 28(5), 2437–2447.
- RamRakhyani, A. K., Mirabbasi, S. and Chiao, M. (2011). Design and optimization of resonance-based efficient wireless power delivery systems for biomedical implants. *IEEE Transactions on Biomedical Circuits and Systems*. 5(1), 48–63.
- Samad, N. A., Vaithianathan, T., Aziz, S. M. and Brander, C. E. (2006). Design of a



- wireless power supply receiver for biomedical applications. In *APCCAS 2006-2006 IEEE Asia Pacific Conference on Circuits and Systems*. IEEE, 674–677.
- Sanni, A., Vilches, A. and Toumazou, C. (2012). Inductive and ultrasonic multi-tier interface for low-power, deeply implantable medical devices. *IEEE transactions on biomedical circuits and systems*. 6(4), 297–308.
- Sazonov, E. and Neuman, M. R. (2014). *Wearable Sensors: Fundamentals, implementation and applications*. Elsevier.
- Shetawy, S. A., Abdallah, E. A. and Abdel-Aziz, D. (2008). Slotted ground plane of rectangular patch microstrip antenna with enhanced bandwidth and size reduction. In *WSEAS International Conference. Proceedings. Mathematics and Computers in Science and Engineering*. 12. World Scientific and Engineering Academy and Society.
- Shinohara, N. (2014). *Wireless Power Transfer via Radiowaves*, ISTE Ltd. and John Wiley & Sons. inc., Great Britain and United States.
- Si, P., Hu, A., Hsu, J., Chiang, M., Wang, Y., Malpas, S. and Budgett, D. (2007). Wireless power supply for implantable biomedical device based on primary input voltage regulation. In *2007 2nd IEEE Conference on Industrial Electronics and Applications*. IEEE, 235–239.
- Singh, V., Kukde, A., Warty, C. and Wagh, S. (2014). Wireless Power Transfer using microstrip antenna assigned with graded index lenses for WSN. In *Advances in Computing, Communications and Informatics (ICACCI, 2014 International Conference on)*. IEEE, 1664–1669.
- Slaughter, M. S. and Myers, T. J. (2010). Transcutaneous energy transmission for mechanical circulatory support systems: history, current status, and future prospects. *Journal of cardiac surgery*. 25(4), 484–489.
- Solbach, K. (1982). Microstrip-franklin antenna. *IEEE Transactions on Antennas and Propagation*. 30(4), 773–775.
- Sun, T., Xie, X. and Wang, Z. (2013). *Wireless power transfer for medical microsystems*. Springer.
- Sweeney, M. O., Hellkamp, A. S., Ellenbogen, K. A., Greenspon, A. J., Freedman, R. A., Lee, K. L., Lamas, G. A. *et al.* (2003). Adverse effect of ventricular pacing on heart failure and atrial fibrillation among patients with normal baseline QRS duration in a clinical trial of pacemaker therapy for sinus node dysfunction. *Circulation*. 107(23), 2932–2937.

- Syms, R., Solymar, L., Young, I. and Floume, T. (2010). Thin-film magneto-inductive cables. *Journal of Physics D: Applied Physics*. 43(5), 055102.
- Tan, Y. K. (2013). *Energy harvesting autonomous sensor systems: design, analysis, and practical implementation*. CRC Press.
- Valtchev, S. S., Baikova, E. N. and Jorge, L. R. (2012). Electromagnetic field as the wireless transporter of energy. *Facta Universitatis Series: Electronics and Energetics*. 25(3), 171–181.
- Waffenschmidt, E. and Staring, T. (2009). Limitation of inductive power transfer for consumer applications. In *Power Electronics and Applications, 2009. EPE'09. 13th European Conference on*. IEEE, 1–10.
- Wang, B., Hu, A. P. and Budgett, D. (2013). Autonomous synchronous rectifier for heart pump applications. In *Industrial Technology (ICIT), 2013 IEEE International Conference on*. IEEE, 481–486.
- Waters, B. H., Sample, A. P., Bonde, P. and Smith, J. R. (2012). Powering a ventricular assist device (VAD) with the free-range resonant electrical energy delivery (FREE-D) system. *Proceedings of the IEEE*. 100(1), 138–149.
- Waters, B. H., Smith, J. R. and Bonde, P. (2014). Innovative free-range resonant electrical energy delivery system (FREE-D system) for a ventricular assist device using wireless power. *ASAIO Journal*. 60(1), 31–37.
- Wilson, W., Goldraich, L., Parry, D., Cusimano, R., Rao, V. and Horlick, E. (2014). Cardiac arrest secondary to sudden LVAD failure in the setting of aortic valve fusion successfully managed with emergent transcatheter aortic valve replacement. *Int J Cardiol*. 171, e40–e41.
- Wong, K. K., Tu, J., Sun, Z. and Dissanayake, D. W. (2013). *Methods in research and development of biomedical devices*. World Scientific.
- Yetisen, A. K., Martinez-Hurtado, J., da Cruz Vasconcellos, F., Simsekler, M. E., Akram, M. S. and Lowe, C. R. (2014). The regulation of mobile medical applications. *Lab on a Chip*. 14(5), 833–840.
- Zhang, F., Hackworth, S. A., Fu, W., Li, C., Mao, Z. and Sun, M. (2011). Relay effect of wireless power transfer using strongly coupled magnetic resonances. *IEEE Transactions on Magnetics*. 47(5), 1478–1481.
- Zhang, F., Hackworth, S. A., Fu, W. and Sun, M. (2010). The relay effect on wireless power transfer using witrlicity. In *Electromagnetic Field Computation (CEFC), 2010 14th Biennial IEEE Conference on*. IEEE, 1–1.
- Zhong, W., Lee, C. K. and Hui, S. (2012). Wireless power domino-resonator

systems with noncoaxial axes and circular structures. *IEEE Transactions on Power Electronics*. 27(11), 4750–4762.

Zhong, W., Lee, C. K. and Hui, S. R. (2013). General analysis on the use of Tesla's resonators in domino forms for wireless power transfer. *IEEE Transactions on Industrial Electronics*. 60(1), 261–270.

Zhu, Y., Moheimani, S. R. and Yuce, M. R. (2011). A 2-DOF MEMS ultrasonic energy harvester. *IEEE Sensors journal*. 11(1), 155–161.