PREPARATION AND CHARACTERISATION OF BIOCOMPATIBLE POLYETHERSULFONE-BASED HOLLOW FIBRE MEMBRANE FOR HAEMODIALYSIS APPLICATION

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Specially for my mom and dad and for the ummah

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"We act as though comfort and luxury were the chief requirements of life, when all that we need to make us happy is something to be enthusiastic about." Albert Einstein

ABSTRACT

In Malaysia, the number of dialysis patient keeps increasing every year with an estimation of 5,000 new cases of end-stage kidney failure (ESRD) each year. Thus, the development of an efficient haemodialyser is crucial to meet this demand. The objective of this research is to develop a biocompatible asymmetric, ultrafiltration hollow fibre membrane (HFM) for haemodialysis application. Polyethersulfone (PES) was chosen as the main polymer in the fabrication of the haemodialysis HFM due to its outstanding oxidative, thermal and hydrolytic stability as well as good mechanical and film-forming properties. Polyurethane (PU) heparin like structure (range of 0-5wt%) was used as additive in the PES HFM to improve blood compatibility of PES HFM. The HFM of blended PES/PU was fabricated using a dry/wet inversion phase spinning technique and its properties was characterised using a number of physicochemical analyses and in-vitro blood compatibility tests. For the physico-chemical analyses, each of the membrane fabricated showed the desired asymmetry structure, dense area in the inner surface near the lumen and finger-like structure near the end of the outer membrane. The pore size of the membrane is in good agreement with the morphology and the surface roughness of the membrane. A high amount of PU in the membrane resulted in more porous finger-like pore structure, smoother surface, higher hydrophilicity and higher pore size. Based on the in-vitro biocompatibility analysis of the membrane, it is proposed that the membrane incorporated with PU has better anticoagulant properties compared to the control sample. PU incorporation prolonged the clotting time, decreased the formation of thrombin, decreased soluble C3a generation and suppressed platelet adhesion and aggregation. The anionic groups on the membrane surface might bind to coagulation factors (antithrombin) and thus improve anticoagulant ability. Based on both physico-chemical and in-vitro results, 4% loading of PU is the optimum loading for incorporation with PES HFM. The results suggested that the blended PES-PU membranes with good haemocompatibility should be applied in the field of blood purification during haemodialysis process.

ABSTRAK

Di Malaysia, bilangan pesakit yang mengalami kegagalan buah pinggang peringkat akhir (ESRD) semakin meningkat dengan anggaran 5000 pesakit yang didiagnosis positif ESRD setiap tahun. Justeru, pembangunan membran dialisis yang efisien adalah sangat kritikal untuk menampung permintaan ini. Objektif kajian ini adalah untuk membangunkan membran gentian geronggang tidak simetri kultra turasan untuk aplikasi hemodialisis. Polietersulfon (PES) telah dipilih untuk menjadi bahan polimer yang utama dalam pembentukan membran hemodialisis kerana mempunyai ciri oksidatif yang unggul, haba dan hidrolitik yang stabil serta mempunyai ciri mekanikal yang baik dan mampu menghasilkan lapisan nipis. Poliuritan (PU) yang mempunyai ciri-ciri seperti heparin akan disintesis dalam lingkungan 0-5wt% telah digunakan sebagai bahan tambahan dalam PES HFM untuk meningkatkan keserasian darah PES HFM Membran gentian geronggang PES/PU telah dihasilkan melalui proses pembentukan kaedah pemintalan kering/basah dan sifat-sifatnya dicirikan dengan menggunakan beberapa analisis fiziko-kimia dan invitro ujian keserasian darah. Bagi analisis fiziko-kimia, setiap membran yang terhasil menunjukkan ciri-ciri yang dikehendaki iaitu, struktur tidak simetri, kawasan padat di permukaan yang berdekatan lumen dan struktur jejari di bahagian luar membran. Saiz liang membran juga sekata dengan morfologi dan permukaan kasar membran. Kandungan PU yang lebih tinggi di dalam membran menghasilkan struktur membran yang mempunyai lebih banyak liang, permukaan yang lebih licin dan lebih hidrofilik dan saiz liang yang lebih besar. Berdasarkan keputusan dari keserasian membran dengan darah secara in-vitro, membran yang telah diubahsuai dengan PU mempunyai ciri-ciri penggumpalan yang lebih baik berbanding dengan sampel kawalan. PU ini juga mempunyai masa pembekuan yang lebih lama, mengurangkan pembentukan trombin, mengurangkan generasi C3a, dan menghalang lekatan platelet. Kumpulan anionik di permukaan membran mungkin mengikat kepada faktor-faktor pembekuan (antithrombin) dan dengan itu meningkatkan keupayaan antikoagulan. Berdasarkan keputusan fiziko-kimia dan keserasian membran dengan darah secara in-vitro, 4wt% kandungan PU yang dicampurkan dengan PES adalah campuran yang paling ideal. Dapatan kajian menunjukkan bahawa campuran membran PES-PU dengan haemocompatibility mempunyai sifat keserasian yang baik dan seterusnya membenarkan permohonan praktikal dalam bidang pembersihan darah semasa proses hemodialisis.

TABLE OF CONTENTS

| CHAPTER | | | TITLE | PAGE | |
|---------|-------------|---------------------|-------------------------------------|------|--|
| | DECLARATION | | | ii | |
| | DEDICATION | | iii | | |
| | ACK | KNOWI | LEDGEMENTS | iv | |
| | ABS | ABSTRACT ABSTRAK | | | |
| | ABS | | | | |
| | TAB | BLE OF | CONTENTS | vii | |
| | LIST | ΓOFT | ABLES | xiii | |
| | LIST | Г OF FI | GURES | xvi | |
| | LIST | Г OF SY | YMBOLS | xxii | |
| | LIST | Γ OF A | PPENDICES | xxiv | |
| 1 | INT | RODU | CTION | 1 | |
| | 1.1 | Resear | ch Background | 1 | |
| | 1.2 | Proble | m Statement | 3 | |
| | 1.3 | Resear | ch Objectives | 5 | |
| | 1.4 | Scopes | s of Study | 5 | |
| | 1.5 | Signifi | icant of the Study | 6 | |
| 2 | LIT | ERATU | IRE REVIEWS | 8 | |
| | 2.1 | Renal | Failures | 8 | |
| | 2.2 | Haemo | odialysis | 10 | |
| | 2.3 | Haemo | odialyser | 12 | |
| | 2.4 | Conce | pt or Principle in Haemodialyser | 13 | |
| | | 2.4.1 | Blood Compartment | 15 | |
| | | 2.4.2 | Dialysate Compartment | 16 | |
| | 2.5 | Chemi | cal Structures of Dialysis Membrane | 17 | |

| | 2.5.1 | Main Material of the Membrane | 18 |
|------|--------|--------------------------------------|----|
| | 2.5.2 | Hydrophilic Agent/Addictive | 19 |
| 2.6 | Physic | cal Structure of Dialysis Membrane | 20 |
| | 2.6.1 | Homogeneous and Asymmetry | |
| | | Membrane | 20 |
| | 2.6.2 | High Flux and Low Flux Membrane | 22 |
| 2.7 | Chem | ical Structures of Dialysis Membrane | 24 |
| | 2.7.1 | Contact Phase System and Coagulation | |
| | | System Activation | 26 |
| | 2.7.2 | Complement System Activation | 27 |
| | 2.7.3 | Platelets Activation and Aggregation | 28 |
| 2.8 | Chem | ical Structures of Dialysis Membrane | 29 |
| | 2.8.1 | Improvement of Biocompatibility of | |
| | | the Regenerated Cellulose Membrane | 29 |
| | 2.8.2 | Improvement of Biocompatibility of | |
| | | the Synthetic Polymeric Membrane | 31 |
| 2.9 | Polye | thersulfone (PES) | 34 |
| 2.10 | PES N | Addification to Improve Membrane | |
| | Bioco | mpatibility | 35 |
| 2.11 | Polyu | rethane | 37 |
| | | | |
| RES | EARC | H METHODOLOGY | 39 |
| 3.1 | Resea | rch Design | 39 |
| 3.2 | Polyn | ner and Solvent Selection | 41 |
| 3.3 | Polyn | nerisation and Sulphonation of PU | 44 |
| | 3.3.1 | Monomers for PU synthesis | 44 |
| | 3.3.2 | PU Synthesis and Polymerisation | 46 |
| | 3.3.3 | Sulphonation of Polyurethane | 48 |
| 3.4 | Chara | cterisation of PU | 49 |
| | 3.4.1 | Attenuated Total Reflectance Fourier | |
| | | Transform Infrared Spectroscopy | |
| | | (ATR-FTIR) | 49 |
| | 3.4.2 | Nuclear Matrix Resonance (NMR) | 49 |

3

| | 3.4.3 | Matrix A | Assisted Laser Desorption | |
|-----|--------|-------------|--------------------------------|----|
| | | Ionizatio | on Time of Flight (MALDI- | |
| | | TOF) M | ass Spectrometry | 49 |
| 3.5 | Select | ion of Sui | table Spinning Parameter for | |
| | Hollo | w Fibre M | Iembranes Fabrication | 50 |
| | 3.5.1 | Hollow | Fibre Membrane Fabrication | 50 |
| | 3.5.2 | Hydropl | nilic/Hydrophobic Property | |
| | | Analysis | 5 | 54 |
| | 3.5.3 | ATR-F1 | TIR | 54 |
| | 3.5.4 | Adsorpt | ion/Desorption Experiment | 54 |
| | 3.5.5 | Pure Wa | ater Flux | 55 |
| | 3.5.6 | Rejectio | n of the Bovine Serum | |
| | | Albumi | n (BSA) | 55 |
| | 3.5.7 | Scannin | g Electron Microscopy (SEM) | 56 |
| | 3.5.8 | Atomic | Force Microscopic (AFM) | |
| | | Observa | tion | 57 |
| 3.6 | Prepa | ration of H | PES Membrane Incorporation | |
| | with F | ٧U | | 57 |
| | 3.6.1 | Hollow | Fibre Membrane Fabrication | 58 |
| | 3.6.2 | Flat-she | et Membrane Fabrication | 59 |
| 3.7 | Chara | cterisation | n of Hollow Fibre Membranes | 60 |
| | 3.7.1 | Thermo | gravimetric Analysis (TGA) | 60 |
| 3.8 | Chara | cterisation | n of Flat-sheet Membranes | 61 |
| | 3.8.1 | Zeta-pot | tential | 61 |
| 3.9 | Memb | orane Hae | mocompatibility: Materials and | |
| | Reage | nt Prepara | ation | 62 |
| | 3.9.1 | Material | S | 62 |
| | 3.9.2 | Reagent | Preparation | 64 |
| | | 3.9.2.1 | Phosphate Buffered Saline | |
| | | | (PBS) Solution | 64 |
| | | 3.9.2.2 | Sodium Dodecyl sulphate | |
| | | | (SDS) Solution | 64 |
| | | 3.9.2.3 | Glutaraladehyde | 64 |

| | | 3.9.2.4 | C3a Standard Solution | 64 |
|------|--------|--------------------|--------------------------------|----|
| | | 3.9.2.6 | Human TAT Comples | |
| | | | Standard Solution | 65 |
| | | 3.9.2.7 | Bovine Serum Albumin | |
| | | | (BSA) Standard Solution | 66 |
| | | 3.9.2.8 | Fibrinogen (FBG) Standard | |
| | | | Solution | 67 |
| | | 3.9.2.9 | Micro BCA [™] Protein | |
| | | | Working Reagent (WR) | 67 |
| 3.10 | Haemo | ocompatib | ility Analysis of the | 68 |
| | Memb | rane | | |
| | 3.10.1 | Protein | Adsorption | 68 |
| | 3.10.2 | Clotting | gTime | 69 |
| | 3.10.3 | Thromb | ogenic Properties | 71 |
| | 3.10.4 | Comple | ement Activation | 72 |
| | 3.10.5 | Platelet | Adhesion | 73 |
| | | | | |
| RES | ULTS . | AND DIS | CUSSIONS | 75 |
| 4.1 | Charae | cterisation | of Synthesised PU | 75 |
| | 4.1.1 | ATR-FTI | R Analysis of Synthesised PU | 77 |
| | 4.1.2 | ¹ H NMR | Analysis of Synthesised and | |
| | | sulphona | ted PU | 79 |
| | 4.1.3 | MALDI- | TOF Analysis | 80 |
| 4.2 | Effect | of Spinnir | ng Conditions on the | |
| | Proper | ties of Ho | llow Fibre Membrane for | |
| | Haemo | odialysis A | Application | 81 |
| | 4.2.1 | Character | risation of Membrane Spun at | |
| | | Different | Air Gap | 81 |
| | 4.2.2 | Pure Wat | er Flux and BSA Rejection | 84 |
| | 4.2.3 | Morpholo | ogy | 85 |
| 4.3 | Charao | cterisation | of PES/PVP with different | |
| | percen | tage of PU | J Composite Membranes | 93 |
| | 4.3.1 | ATR-FT | IR Analysis | 93 |

4

| | 4.3.2 | Morphology of Composite | |
|-----|--------|--------------------------------------|-----|
| | | PES/PVP/PU Membranes | 95 |
| | 4.3.3 | AFM Analysis | 103 |
| | 4.3.4 | Membrane | |
| | | Hydrophilicity/Hydrophobicity and | |
| | | Surface Charge Analysis | 104 |
| | 4.3.5 | Membrane Thermal Stability | 108 |
| 4.4 | Haem | ocompatibility of Developed PES/PVP | |
| | with I | Different Percentage of PU Composite | |
| | Hollo | w Fibre Membranes via the In-vitro | |
| | Analy | rsis | 110 |
| | 4.4.1 | Protein Adsorption | 110 |
| | 4.4.2 | Platelet Adhesion and Aggregation | 111 |
| | 4.4.3 | Thrombogenic Properties | 113 |
| | 4.4.4 | Clotting Time | 114 |
| | 4.4.5 | Complement Activation | 116 |
| | | | |
| CO | NCLUS | SIONS AND RECOMMENDATIONS | 117 |
| | ~ . | | |

| 5 | CONCLUSIONS AND RECOMMENDATIONS | | |
|---|---------------------------------|-----------------|-----|
| | 5.1 | Conclusions | 117 |
| | 5.2 | Recommendations | 119 |
| | | | |

| REFERENCES | 120 |
|----------------|---------|
| Appendices A-J | 129-147 |

LIST OF TABLES

| TABLE NO. | TITLE | PAGE |
|-----------|---------------------------------------------------------------------------------------------------------------------------|------|
| 1.1 | Stock and flow of renal replacement therapy in Malaysia from year 2005-2014 | 1 |
| 2.1 | Stages of kidney disease and condition of the kidney function based on the estimated glomerular rate (eGFR) reading | 13 |
| 2.2 | Waste product and component inside blood that enter hemodialyser | 16 |
| 2.3 | The normal composition of a dialysate fluid. | 17 |
| 2.4 | Classification of dialysers based on dialysis membrane permeability | 24 |
| 2.5 | Cellulose based membranes that are commonly used during the early invention of the haemodialysis | 31 |
| 2.6 | Synthetic membranes that are used for haemodialysis application | 33 |
| 2.7 | Some examples of PES modification for haemodialysis application and its method of modification | 36 |
| 3.1 | The chemical and physical properties of PES | 42 |
| 3.2 | The chemical and physical properties of PVP | 43 |

| 3.3 | Physical properties of DMAc | 44 |
|------|-------------------------------------------------------------------------------------------------------------------------------------------------------------------------|----|
| 3.4 | The chemical and physical properties of MDI | 45 |
| 3.5 | The chemical and physical properties of DMPA | 46 |
| 3.6 | Spinning parameters for different air gap distance, different dope extrusion rate (DER), bore fluid flow rate (BFFR) and speed during membrane collection (CD) | 53 |
| 3.7 | Composition of each component in the dope solution | 58 |
| 3.8 | Spinning parameter for HFMs fabrication | 59 |
| 3.9 | Reagents list and its manufacturer | 62 |
| 3.10 | Kits list and its manufacturer | 62 |
| 3.11 | Instruments list and its manufacturer | 63 |
| 3.12 | Consumables list and its manufacturer | 63 |
| 3.13 | List of two-fold dilution series for Human TAT complex standard solution | 66 |
| 3.14 | List of two-fold dilution series for BSA standard solution | 66 |
| 3.15 | List of two-fold dilution series for FBG standard solution | 67 |
| 3.16 | Normal range of APTT and PT test | 70 |
| 4.1 | Physical properties of the membranes spun at different air gap distance | 84 |
| 4.2 | Water permeability and protein rejection of the hollow fibre membrane | 85 |

| 4.3 | The OD and ID of the membrane with different air | |
|-----|--------------------------------------------------------------------------------------------------------|-----|
| | gap lengths | 86 |
| 4.4 | The OD and ID of the membrane with different dope extrusion rate (DER) and bore fluid flow rate (BFFR) | 89 |
| 4.5 | Surface roughness of the hollow fibre membrane | 93 |
| 4.6 | Surface roughness of the hollow fibre membrane | 103 |

LIST OF FIGURES

| TABLE NO. | TITLE | PAGE |
|-----------|--------------------------------------------------------------------------------------------------------------------------------------------|------|
| 2.1 | The gross anatomy of normal kidney and chronic renal failure kidneys | 9 |
| 2.2 | Simplified haemodialysis circuit | 10 |
| 2.3 | Mechanism of blood and dialysate flow through semipermeable membrane | 12 |
| 2.4 | Graphic illustration of water and solute movement across the semipermeable membrane | 14 |
| 2.5 | Chemical structure of natural (cellulose) and synthetic polymer membrane | 18 |
| 2.6 | Types of membrane. (a) homogeneous membrane, (b) asymmetric membrane-porous structure, (c) asymmetric membrane-finger-like structure | 20 |
| 2.7 | Movement of uremic toxins, albumin and water molecules across asymmetric membrane | 21 |
| 2.8 | Comparison of homogeneous and heterogeneous membrane | 22 |
| 2.9 | Haemodialysis and haemofiltration principles | 23 |
| 2.10 | The effect of protein adsorption and its activation cascade | 25 |

| 2.11 | Blood purification across the glomerular | 26 |
|------|---------------------------------------------------|----|
| 2.12 | The contact pathway activation mechanism induces | |
| | by negatively charged material | 27 |
| 2.13 | Three pathway of complement system | 28 |
| 2.14 | SEM images of platelet adhesion during resting | |
| | state, non-thrombotic state (R), and 4 different | |
| | stages of platelet spreading or pseudopodia | |
| | formation; dendritic (D), spread-dendritic (SD), | |
| | spread (S) and fully spread (FS) | 29 |
| 2.15 | The SEM findings of cross-sectional structure of | |
| | cellulose triacetate (CTA) | 30 |
| 2.16 | The structural formulas of PES and PSf | 34 |
| 2.17 | The SEM findings of cross-sectional structural of | |
| | PES | 35 |
| 3.1 | Experimental stages flow chart of this research | |
| | study | 40 |
| 3.2 | The molecular structure of (a)heparin and | |
| | (b)modified polyurethane | 41 |
| 3.3 | Chemical structure of PES, Veradel® A-301 | |
| | (n = number of unit) | 41 |
| 3.4 | Chemical structure of PVP, K90 | 42 |
| 3.5 | Chemical structure of MDI, Sigma-aldrich | 45 |
| 3.6 | The schematic diagram of PU polymerisation | |
| | laboratory apparatus preparation | 47 |

| | •• |
|-----|-----|
| V V | 711 |
| ΛV | 11 |
| | |

| 3.7 | The flow chart of the procedure for polymerisation and sulphonation of PU | 48 |
|------|----------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------|----|
| 3.8 | Schematic diagram of dry/wet inversion spinning technique | 51 |
| 3.9 | Glass plate and glass rod used for flat-sheet membrane casting | 60 |
| 3.10 | C3a standard solution | 65 |
| 3.11 | The summary procedure of protein adsorption | 69 |
| 3.12 | The summary procedure of APTT and PT testing | 70 |
| 3.13 | The summary procedure of sample preparation for TAT, C3a and C5a complement activation | 71 |
| 3.14 | Schematic diagram for platelet adhesion procedure | 74 |
| 4.1 | Mechanism of synthesis of sulphonated PU by polymerisation and sulphonation | 76 |
| 4.2 | ATR-FTIR spectra for synthesised PU | 78 |
| 4.3 | ATR-FTIR spectra for sulphonated PU | 78 |
| 4.4 | The ¹ H NMR spectra of the sulphonated polyurethane. | 79 |
| 4.5 | Maldi-TOF spectra for synthesised PU | 80 |
| 4.6 | Maldi-TOF spectra for sulphonated PU | 81 |
| 4.7 | Contact angle measurement for hollow fibre spun with different air gap between spinneret and coagulation bath and constant DER (3 cm ³ /min) and BFFR (1 cm ³ /min) | 82 |

| 4.8 | ATR-FTIR analysis for hollow fibre spun with | |
|------|------------------------------------------------------|----|
| | different air gap between spinneret and coagulation | |
| | bath and constant DER (3 cm^3/min) and BFFR (1 | |
| | cm^{3}/min). | 83 |
| 4.9 | The SEM images of hollow fibre membrane spun at | |
| | different air gap | 87 |
| 4.10 | The SEM images of hollow fibre membrane with | |
| | different dope extrusion rate (DER) and bore fluid | |
| | flow rate (BFFR) spun at air gap 50 cm. | 90 |
| 4.11 | Cross sectional SEM pictures of sample A-2-1 | |
| | hollow fibre membrane spun at 50cm air gap region | |
| | and DER and BFFR ratio of 1:1 | 91 |
| 4.12 | AFM images of hollow fibre membrane spun at | |
| | different air gap distance | 92 |
| 4.13 | ATR-FTIR spectra for neat PES/PVP membrane | 94 |
| 4.14 | ATR-FTIR spectrum series for PES/PVP with | |
| | different PU loading | 95 |
| 4.15 | SEM image for PES/PVP/PU4%, dense skin layer | |
| | near the inner surface of the membrane and porous | |
| | finger-like structure near the edge of the membrane. | 96 |
| 4.16 | SEM images for hollow fibre membrane spun from | |
| | 0% - 5% of PU cross-sectional region at different | |
| | magnification. (a)PES/PVP, (b)PES/PVP/PU1%, | |
| | (c)PES/PVP/PU2%, (d) PES/PVP/PU3%, | |
| | (e)PES/PVP/PU4%, (f)PES/PVP/PU5%. | |
| | Magnification: 1500x. | 97 |
| 4.17 | SEM images for hollow fibre membrane spun from | |
| | 0% - 5% of PU surface region at different | |

| | magnification. (a)PES/PVP, (b)PES/PVP/PU1%, | |
|------|------------------------------------------------------|-----|
| | (c)PES/PVP/PU2%, (d) PES/PVP/PU3%, | |
| | (e)PES/PVP/PU4%, (f)PES/PVP/PU5%. | |
| | Magnification: 5000x. | 99 |
| 4.18 | SEM image for PES/PVP/PU4%, dense skin layer | |
| | near the inner surface of the membrane and porous | |
| | finger-like structure near the edge of the membrane. | 100 |
| 4.19 | SEM images for flat-sheet membrane spun from 0% | |
| | - 5% of PU cross-sectional region at different | |
| | magnification. (a)PES/PVP, (b)PES/PVP/PU1%, | |
| | (c)PES/PVP/PU2%, (d) PES/PVP/PU3%, | |
| | (e)PES/PVP/PU4%, (f)PES/PVP/PU5%. | |
| | Magnification: 500x. | 101 |
| 4.20 | SEM images for hollow fibre membrane spun from | |
| | 0% - 5% of PU surface region at different | |
| | magnification. (a)PES/PVP, (b)PES/PVP/PU1%, | |
| | (c)PES/PVP/PU2%, (d) PES/PVP/PU3%, | |
| | (e)PES/PVP/PU4%, (f)PES/PVP/PU5%. | |
| | Magnification: 2000x | 102 |
| 4.21 | AFM images of hollow fibre membrane spun at | |
| | different air gap distance | 104 |
| 4.22 | Contact angle measurement of the composite | |
| | hollow fibre membrane | 105 |
| 4.23 | Contact angle measurement of the flat-sheet | |
| | membrane | 106 |
| 4.24 | Surface charge of the membranes against pH | 107 |
| 4.25 | Thermal analysis of PES/PU blend hollow fibre | |
| | membranes with different concentration of PU | 109 |

| 4.26 | Thermal analysis of PES/PU blend flat-sheet | |
|------|--------------------------------------------------|-----|
| | membranes with different concentration of PU | 109 |
| 4.27 | Adsorption results of BSA and FBG on the | |
| | membrane surface of PES/PVP with different PU | |
| | loading | 111 |
| 4.28 | SEM images of platelet adhesion on flat-sheet | |
| | membrane (a)PES/PVP, (b)PES/PVP/PU1%, | |
| | (c)PES/PVP/PU2%, (d)PES/PVP/PU3%, | |
| | (e)PES/PVP/PU4%, (f) PES/PVP/PU5% | 112 |
| 4.29 | TAT activation for PES/PVP with different PU | |
| | loading Complement Activation | 114 |
| 4.30 | APTTs coagulation time analysis for PES/PVP with | |
| | different PU loading | 115 |
| 4.31 | PTs coagulation time analysis for PES/PVP with | |
| | different PU loading | 115 |
| 4.32 | C3a complement activation for PES/PVP | |
| | incorporated with different PU percentage | 116 |
| | | |

LIST OF SYMBOLS

| γ | - | Gamma |
|----------------------------|---|---------------------------------------------------------|
| δt | - | Solubility coefficient (MPa ^{1/2}) |
| Δx | - | thickness selectivity of the membrane (μm) |
| L | - | thickness of the support layer (µm) |
| \mathbf{K}_{uf} | - | ultrafiltration coefficient of the membrane (mL/h/mmHg) |
| K _d | - | Dialyser clearance (mL/min) |
| $\mathbf{M}_{\mathbf{w}}$ | - | Molecular weight (g/mol) |
| Tg | - | Glassy temperature (°C) |
| С | - | Carbon |
| Н | - | Hydrogen |
| Ν | - | Nitrogen |
| 0 | - | Oxygen |
| R | - | Extrusion ratio |
| Ao | - | Initial cross-sectional area of the spinneret |
| A_{f} | - | final cross-sectional area of the spinneret |
| V | - | volume of permeation (L) |

| Α | - | total area of the hollow fibres (m ²) |
|----------------------------|---|----------------------------------------------------------------|
| t | - | time taken (h). |
| C_P | - | permeate concentrations (wt%) |
| $C_{\scriptscriptstyle F}$ | - | feed concentrations (wt%) |
| R_{a} | - | mean surface roughness |
| DER | - | Dope extrusion rate (cm ³ /min) |
| BFFR | - | Bore fluid flow rate (cm ³ /min) |
| LER | - | Linear extrusion rate (cm ³ /min) |
| CD | - | Collection drum (Hz) |
| CaCl ₂ | - | Calcium chloride |
| C3a | - | Complement 3a |
| C5a | - | Complement 5a |
| C5b-9 | - | Complement 5b, 6, 7, 8, 9 (complement membrane attack complex) |

xxiii

LIST OF APPENDICES

| APPENDIX | TITLE | PAGE | |
|----------|----------------------------------------------------------------------------------------------------------------------------------|------|--|
| А | List of Publication | 129 | |
| В | Membrane Fabrication | 130 | |
| С | Flow Chart of the Polymerisation and Sulphonation Process of Synthesised Polyurethane | 131 | |
| D | Calculation of Estimated Dope Extrusion Rate to Bore Fluid Flow Rate Ration | 132 | |
| Ε | Calculated Molecular Weight according to Structural Formula | 133 | |
| F | Scanning Electron Microscopic (SEM) Images for Hollow Fibre Membrane and Flat-sheet Membrane at Different Magnification | 134 | |
| G | Elemental Composition Analysis based on Energy- dispersive X-ray (EDX) Spectroscopy of Membrane Fabricated | 137 | |
| Н | ATR-FTIR Spectrum for Synthesised PU, Sulphonated PU and all the Fabricated PES/PVP Membrane with Different PU Percentage. | 139 | |
| I | Determination of Membrane Thermal Stability based on the TGA Curve Analysis and Estimation of | | |

| Polymer Degradation based on Membrane Weight | 143 |
|------------------------------------------------|-----|
| Loss | |
| The Flow Chart of Human Complement Fragment 3a | |
| (C3a) ELISA Assay Procedure | 147 |

I

CHAPTER 1

INTRODUCTION

1.1 Research Background

In recent years, there has been a crucial rise of kidney failure notably chronic kidney disease (CKD) caused by disease or condition impairs kidney function, causing kidney damage to worsen over several months or years as reported by National Kidney Foundation Malaysia (Yam et al., 2016). The recent statistic from National Kidney Foundation Malaysia reveals worrying figures where the total number of haemodialysis patients increases from 12,182 patients in year 2005 to 31,497 patients in year 2014 (Table 1.1). Renal patients need to undergo this treatment for 3 to 4 hours at least three times a week (Hakim et al., 2016). This treatment could be burden in term of finance especially to the people from middle class and poor background. Resulting in the urge to search for better and more efficient and low cost ultrafiltration system.

Table 1.1Stock and flow of renal replacement therapy in Malaysia from year2005-2014 (Yam et al., 2016)

| Year | 2005 | 2006 | 2007 | 2008 | 2009 | 2010 | 2011 | 2012 | 2013 | 2014 |
|------------------------|--------|--------|--------|--------|--------|--------|--------|--------|--------|--------|
| New dialysis patients | 3,167 | 3,709 | 4,103 | 4,640 | 4,952 | 5,305 | 6,073 | 6,690 | 6,985 | 7,055 |
| New transplants | 172 | 151 | 112 | 131 | 141 | 128 | 127 | 107 | 98 | 81 |
| Dialysis deaths | 1,515 | 1,820 | 1,987 | 2,191 | 2,601 | 3,047 | 3,292 | 3,645 | 4,001 | 4,015 |
| Transplant deaths | 49 | 58 | 47 | 59 | 49 | 48 | 55 | 64 | 56 | 45 |
| Dialysing at 31st | 13,356 | 15,080 | 17,084 | 19,388 | 21,590 | 23,709 | 26,328 | 29,223 | 32,026 | 34,767 |
| December | | | | | | | | | | |
| Functioning transplant | 1,716 | 1,771 | 1,788 | 1,808 | 1,852 | 1,881 | 1,907 | 1,891 | 1,870 | 1,844 |
| at 31st December | | | | | | | | | | |

Haemodialysis is one of the prominent treatments for chronic kidney disease (CKD) and end stage renal disease (ESRD). Haemodialysis helps to filtrate out low and middle molecular weight uremic toxins from the blood and helps to balance the pH value in the body. Barzin et al. (2004) stated that uremic toxins such as urea and creatinine range from size 10,000-55,000 Da needs to be excreted out from the blood, while, proteins such as albumin (66,000 Da) need to be retained. In order for these secretion and retention to be worked, the design of the membrane needs to fulfil certain criteria. The membrane produced is preferred to be high flux, asymmetric, micro porous ultrafiltration hollow fibre membrane.

One of the most important components in blood purification application that need to be considered thoroughly is the membrane of the haemodialysis. The membrane of the haemodialysis is potted inside a module and is known as haemodialyser, which is the heart of the haemodialysis system. The implementation of membrane technology in blood purification applications has proven vital. In hollow fibre ultrafiltration system, blood purification is achieved by regulating impure blood flow through the lumen of hollow fibre membrane as the dialysate flows countercurrently outside the lumen (Dahe et al., 2011). Uremic toxins like urea, creatinine etc. are filtered out from the blood through the porous structure of the membrane. The membrane facilitates the filtration without the loss of important blood proteins such as albumin (Dahe et al., 2011). Desirable characteristics of such hollow fibre membranes include high flux, selectivity and biocompatibility (Clark et al., 2002). However, clinical complications such as neutropenia, hypersensitivity reactions, oxidative stress, contact and complement activation, have repeatedly associated with the commercially available and widely used polysulfone haemodialysis membrane (Urbani et al., 2012). This causes the decrease in quality of life, life expectancy and mortality of haemodialysis patients and has limited the success rates of such membranes. Thus, the selection of membrane used for haemodialysis needs to be chosen wisely in order to prevent any bio-incompatibility due to the interaction between blood and the new haemodialysis membranes.

Functionalisation of polymer membranes has been studied as one of the methods to improve polymer properties. The surface of membranes has been modified

and grafted using several of functional groups like hydroxyl, ketone and carboxylic acid groups. The chemical bonding between substrates and adhesives is able to be improved by adding functional groups to the polymer. Through functionalisation method, properties such as hydrophilicity, hydrophobicity, biocompatibility, antifouling, and antibacterial properties etc. can be enhanced, while some of membrane native properties and its core structure are still remained (Dahe et al., 2011).

1.2 Problem Statement

Currently, polysulfone (PSf) and polyethersulfone (PES) are among the most available and commercial haemodialysis membranes that have been used as the main polymer in the fabrication of asymmetric hollow fibre haemodialysis membrane. However, these membranes have been associated with numerous of clinical complications which include hypersensitivity reactions, neutropenia, oxidative stress, and complement activation.

Hydrophobic property of PES membrane is the main disadvantage of this polymer. Many studies have concluded that the material hydrophobicity is the causes of membrane fouling. Membrane fouling happens when protein adsorbs on the surface of the membrane (Khulbe et al., 2010). However, Zhao et al. (2013) has been reported the opposite findings. He stated that the adsorption of nonpolar solutes, hydrophobic particles or bacteria is the cause of membrane fouling. Membrane fouling is a serious problem in membrane filtration, resulting in a higher energy demand, shorter membrane lifetime, and unpredictable separation performance (Agenson et al., 2007; Su et al, 2011). The most desirable property of a biomaterial is the biocompatibility of the material towards body. Biologically compatible means that in contact of foreign material with human body mechanism will not produce a toxic, injurious and immunological response in living tissues or blood (Dahe et al., 2011). The most commonly accepted mode of improving hollow fibre membranes biocompatibility is the modification of surface chemistry. Thus, in order to improve the hydrophilicity of

PES hollow fibre membrane used in haemodialysis, PES is modified by hydrophilic polymers.

Polyurethane (PU) has been reported to be used in blood-contacting application due to its excellent mechanical properties and relatively good blood compatibility (Agenson et al., 2007; Li et al, 2012). Meanwhile, PU, with a Hansen solubility coefficient $\delta t = 20.5$ MPa^{1/2}, showed good miscibility with PES ($\delta t = 21.3$ MPa^{1/2}), the miscibility has also been proved by using the cloud point measurements, and all of these showed similar results (Yin et al., 2014). The excellent miscibility ensured a homogeneous blend between the PU and the PES, and inhibited the macro phase separation. Therefore, the blending of PU would not affect the morphology and the surface roughness of the PES membrane significantly.

However, limited number of research works has been done on the grafting functional group or functional molecules to PU, such as hydroxyl group, carboxyl group, and sulphonic group. Therefore, in this study, PU polymerisation and sulphonation will be tested, which it is expected that the modified PU could minimise protein adsorption and prolong blood coagulation time. The aim of this study is to introduce hydroxyl, carboxyl and sulphonic groups onto the molecular chains of PU and to synthesize a polyurethane with good blood compatibility, which later on will be used for the modification of PES haemodialysis membrane. Positive result will not only give benefits to the university but also to the biomaterial field of research.

1.3 Research Objectives

The general aim of this proposed project is to fabricate a haemocompatible PES based hollow fibre membrane for haemodialysis. The specific objectives of this study are:

- To synthesise and functionalise hydrophilic PU heparin like structure as biocompatible additive for haemodialysis membrane.
- To fabricate and characterise physico-chemical properties of the asymmetric PES/PU hollow fibre membrane.
- 3) To study the blood compatibility of PES hollow fibre membrane that incorporated with modified PU in haemodialysis application.

1.4 Scopes of Study

In order to achieve the objective of this research, the following scopes are outlined: -

- 1) Modifying PU molecular structure by first synthesising it from methylene diphenyl diisocynate (MDI) and dimethylolpropionic acid (DMPA) at temperature 80° C for 6 hours and then functionalising it by sulphonating with concentrated H₂SO₄ for 16 hours.
- Determining PU characterisation by analysing the attenuated total reflectancefourier transform infrared (ATR-FTIR), nuclear matrix resonance (NMR) and matrix assisted laser desorption ionisation time of flight (MALDI-TOF) analysis.
- 3) Investigating suitable spinning conditions (air gap distance, dope extrusion rate, bore fluid flow rate and the take-up speed) to produce an asymmetric, micro porous ultrafiltration hollow fibre specifically for haemodialysis membrane.
- Preparing a dope solution that, made of different loadings of PU (0-5%wt) in PES blended with polyvinylpyrrolidone (PVP) solution.

- 5) Fabricating polymeric hollow fibre membrane via dry/wet spinning technique using the preliminary identified spinning parameters (50 cm air gap, 3 cm³/min of dope extrusion rate, and 1 cm³/min bore fluid flow rate) and PVP as the pore modifier.
- 6) Observing the hollow fibre membrane morphology, membrane molecular orientation, membrane hydrophobicity/hydrophilicity, membrane porosity and thermal transition and stability using scanning electron microscopy (SEM), ATR-FTIR, contact angle measurement, zeta-potential and thermagravimetric analysis (TGA) test respectively.
- 7) Evaluating PES/PU membrane haemocompatibility by assessment in protein adsorption, platelet adhesion, thrombogenic properties, coagulation and complement activation.

1.4 Significant of the Study

Over the past 15 years, the figure of patients experiencing chronic kidney diseases has increased dramatically. Such kidney diseases render the incapable of kidney to filter and remove body waste from the bloodstream. The most widely accepted extracorporeal treatment used to filter and purify blood is haemodialysis. According to Malaysia's National Renal Registry, it has been reported that the total number of people underwent haemodialysis had risen from 6689 in 2000 to 21159 in 2009. The number did not stop there. The latest report dated March 2013 mentioned the increase of dialysis patients to 26159 people (Yam et al., 2016).

The main component of haemodialysis machine is the dialyser, where a semipermeable membrane is used as the filter. As the paramount component for haemodialysis system, the development of membrane continues to attain the best of it. Due to bio-incompatibility and low performance of cellulose-based membranes, fully synthetic membrane was introduced and became favourable until very recent times. These synthetic membranes are made up of a variety of hydrophobic polymers as the main component to serve as hosts. The rationale and significance of this current

7

research are to explore the formation and development of modified PES hollow fibre membranes blended with hydrophilic addictive PU for haemodialysis application. Physicochemical properties of PU have been proven to be reliable blood compatible biomaterials. Thus the blending of PU with PES is expected to enhance the haemocompatibility of the fabricated membrane when contacting with blood.

In Malaysia, very few researches on haemodialysis membranes have been conducted. There is no large-scale initiative to utilise local expertise in membrane for haemodialysis application. Until now, Malaysia is still depending on imported dialysers for haemodialysis treatments in either government or private hospitals. The information constraint in this field is the main cause of this problem. The impact of this matter includes unnecessary expenditure due to high cost of dialysers. Therefore, this research's long-term target is to develop a locally made dialyser equipped with a highly efficient membrane in order to sustain current demand especially in Malaysia. Furthermore, this research study may lead to a new finding that can possibly be a basis for the next move in fabricating high performance haemodialysis membrane. Positive result can benefit to the membrane field of research especially in membrane technology for haemodialysis application.

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