

MICROWAVE ASSISTED ALOE VERA COATING ON METALLOCENE
POLYETHYLENE FOR IMPROVING BIOCOMPATIBILITY

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I dedicate this thesis to my lovely family:

My dearest parents, Mr. Balaji Baskaran, Mrs. Bharathi Balaji

&

In memory of my grandfather Mr. Baskaran

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ABSTRACT

Metallocene polyethylene (mPE) is known for its commendable physical and mechanical properties, but the problem of hemocompatibility hampers its clinical application. Therefore, an *Aloe vera* (AV) extract was coated on mPE assisted by microwave to rectify this problem. Initially, the duration of microwave treatment was optimized to 60 s by considering the weight degradation of the samples. Similarly, the coating time of fibrous AV extract was optimized to 12 h (A-12 h-mPE) and 24 h (A-24 h-mPE) based on wettability increment. Fourier transform infrared (FTIR) spectra showed the addition of OH⁻ groups and the vibration characteristic of several active constituents available in the AV coating. The decrease in mean contact angle of pristine mPE (P-mPE) from 88.43° to 32.93° in the A-24 h-mPE sample, depicts an increase in the wettability. Meanwhile, scanning electron microscopy (SEM) images displayed the presence of AV extract. The influence of microwave in enhancing the coating characteristics was investigated through Hirox 3D images, peel test, and degradation studies. In addition, an improvement in average surface roughness (Ra) of P-mPE from 2.069 nm to 7.796 nm for the A-24 h-mPE was interpreted through atomic force microscopy (AFM) analysis. Finally, the *in vitro* coagulation studies indicated a reasonable delay in blood clotting time on the AV coated mPE samples, which was presented by activated partial thromboplastin time (170 s) and prothrombin time (39 s) assay. The coated mPE samples also reduced hemolysis and platelet adhesion insinuating the potential usage of AV coated mPE in permanent and temporary blood contacting devices.

ABSTRAK

Metallocene polietilena (mPE) dikenali dengan sifat-sifat fizikal dan mekanikal yang mengagumkan, namun masalah keserasian dengan darah menghadkan aplikasi klinikal bahan ini. Oleh itu, ekstrak lidah buaya (AV). Disalut ke atas mPE dengan bantuan gelombang mikro untuk mengatasi maseilah ini. Pada permulaanya, tempoh rawatan gelombang mikro telah dioptimumkan kepada 60 saat dengan merujuk kepada kadar degradasi berat sampel. Begitu juga dengan masa penyalutan ekstrak gentian AV telah dioptimumkan kepada 12 jam (A-12 h-mPE) dan 24 jam (A-24 h-mPE) berdasarkan peningkatan ciri kebolehasahan. Spektrum daripada Fourier inframerah (FTIR) menunjukkan pertambahan kumpulan OH⁻ dan ciri getaran bagi beberapa komponen aktif yang terdapat di dalam salutan AV. Purata sudut bersentuhan MPE tulen (P-mPE) menurun secara daripada 88.43° kepada 32.93° untuk sampel A-24 h-mPE menggambarkan peningkatan kebolehasahan. Sementara itu, imej mikroskop elektron pengimbas (SEM) menunjukkan kehadiran ekstrak AV. Pengaruh gelombang mikro dalam peningkatan ciri-ciri penyalutan disiasat melalui imej-imej 3D Hirox, ujian pengupasan, dan kajian degradasi. Tambahan, peningkatan purata kekasaran permukaan (Ra) P-mPE daripada 2.069 nm kepada 7.796 nm untuk A-24 h-mPE telah ditafsirkan melalui analisis mikroskop tenaga atom (AFM). Akhir sekali, kajian koagulasi darah secara *in vitro* menunjukkan kelengahan masa yang wajar bagi pembekuan darah pada sampel mPE yang disaluti AV, yang ditunjukkan oleh masa pengaktifan esei tromboplastin separa (170 s) dan protrombin (39 s). Sampel mPE yang bersalut juga mengurangkan hemolisis dan lekatan platelet menggambarkan potensi penggunaan mPE yang disaluti AV dalam peranti perhubungan darah yang kekal dan sementara.

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LIST OF ABBREVIATIONS

AFM	-	Atomic Force Microscopy
AMPs	-	Antimicrobial peptides
APTT	-	Activated Partial Thromboplastin Time
ATR	-	Attenuated total reflectance
AV	-	Aloe vera
BSM	-	Bovine submaxillary gland mucin
CT	-	Computed Tomography
DS	-	Dextran sulfate (DS)
ECM	-	Extracellular matrix
EM	-	Electromagnetic
EVA	-	Ethylene-vinyl acetate
FTIR	-	Fourier transform infrared
Hep	-	Heparin
HUVEC	-	Human umbilical vein endothelial cell
LDPE	-	Low density polyethylene
mPE	-	Metallocene polyethylene
NH ₃	-	Ammonia
PBS	-	Phosphate Buffer solution
PCL	-	Polycaprolactone
PDMS	-	Polydimethylsiloxane

PE	-	Polyethylene
PEEK	-	Polyether ether ketone
PEG	-	Polyethylene glycol
PET	-	Polyethyleneterephthalate
PETG	-	Glycol-modified polyethylene terephthalate
PLACL	-	Poly (L-lactic acid)-co-poly (ϵ - caprolactone)
PMMA	-	Polymethylmethacrylate
PP	-	Polypropylene
PPP	-	Platelet poor plasma
PRP	-	Platelet Rich Plasma
PS	-	Polystyrene
PSM	-	Plasma-surface modification
PT	-	Prothrombin Time
PTFE	-	Polytetrafluoroethylene
PU	-	Polyurethane
PVC	-	Polyvinylchloride
RBCs	-	Red Blood Cells
ROS	-	Reactive oxygen species
SEM	-	Scanning Electron Microscope
SPS	-	Segmented polystyrene
Ti	-	Titanium
TPU	-	Thermoplastic polyurethane
USSCs	-	Unrestricted somatic stem cells
UV	-	Ultraviolet
vWF	-	von Willebrand

WBC	-	White blood cells
WHO	-	World Health Organization
WSC	-	Water-soluble chitosan
Z-N	-	Ziegler-Natta

LIST OF SYMBOLS

°C	-	Degree Celsius
μm	-	Micrometer
cm	-	Centimeter
CO ₂	-	Carbon-di-oxide
GHz	-	Gigahertz
He	-	Helium
mg	-	Milligram
MHz	-	Megahertz
ml	-	Milliliter
mm	-	Millimeter
mol%	-	Mole fraction
nm	-	Nanometer
O ₂	-	Oxygen
Si	-	Silicone
μmol	-	Micro moles

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CHAPTER 1

INTRODUCTION

1.1 Overview

Biomaterials are promising materials for an extensive range of utilizations in both diagnostic and therapeutic industries. Scientists have defined it in different perspective based on its rapidly changing outlook [1-3]. Typically, biomaterials can be defined as materials which can provide an environment to assist the rehabilitation of biological systems or replace the entire system itself. Biomaterials have a well-established reputation in the field of tissue engineering, clinical devices, drug delivery, medical implants, biosensors, cosmetics and food industries [4, 5]. Hence, the total market value of biomaterial-based industries is anticipated to exceed \$88.4 billion by 2017 from the current value of \$58.1 billion. Every year, USA alone spend 7-8% of its total global healthcare outgoings exclusively for biomaterial-related usages [6]. Meanwhile, in coming years the demand for promising biomaterials is anticipated to surge radically due to an increasing number of diseased population. It insinuates the need for more research toward improving the properties of existing materials using simple and feasible modification techniques. So, biomaterials have a significant future in both research and commercial fields.

In general, biomaterials can be classified into three groups based on their origin and applications as (1) synthetic materials, (2) naturally derived, and (3) semisynthetic or hybrid materials. Among the above, synthetic materials like metals, ceramics, polymers and composites are most commonly used for various biomedical applications. The exceptional mechanical properties of metals and their alloys such as

tensile strength, elasticity coefficient and fatigue life makes them attractive materials for many load-bearing biomedical systems. Some of the examples include wires, screws, etc., to fracture fixation plates and artificial joints. Nevertheless, metallic materials are highly prone to corrosion and tend to release harmful side products in the form of ions, chemical compounds and insoluble components which will cause adverse biological reactions. In the meantime, ceramics emerged as desirable biomaterials because of its captivating bioactive, bioinert and biodegradable properties. They have been used in several applications in the dental field; though the poor mechanical characteristics like brittleness and low strength, made them unsuitable for wide exploitation. Later, polymers gained greater attention than other materials because of their versatility and easy to tailor nature. Presently, polymers are reported to be the most promising type of biomaterials.

Common biological substances fall under the second category like collagen, heparin, proteins, peptides, carbohydrates, bio-ceramics, etc., are utilized for both surface coating and material synthesis. Though materials completely made of natural substances possess fascinating biocompatible properties they fail in several aspects because of poor physicochemical and mechanical properties. To avoid that complication, natural materials are coupled with synthetic substances and it falls under the third category [5].

The longevity of an implant/biomaterial inside the human body is dependent on its ability to avoid any adverse reaction or damage to the surrounding environment which chiefly relies on the biocompatibility of materials used. But this crucial property is greatly influenced by its physical, chemical, mechanical and biological characteristics [7]. If analyzed deeply, the existence of interconnections between all these essential properties and the durability of a biomaterial can be inferred. In general, the physicochemical properties such as roughness, hardness, temperature, wettability, surface chemistry, surface reactivity (inert or active) and surface charge, play a crucial role in determining the hemocompatibility of a material by delaying the activation of coagulation pathways, resisting platelets adhesion and avoiding red blood cells (RBCs) damage. On the other hand, mechanical properties such as elasticity, yield stress, ductility, toughness, deformation, fatigue, hardness, and wear resistance will

determine the ability of a material to withstand the dynamism of the internal environment. So, the presence of appropriate surface, mechanical and biological properties will ensure desired function and longevity of an implant [8-13].

Therefore, in this study, the hemocompatibility of mPE is improved by microwave assisted coating of AV extract. This approach not only eliminates the usage of harsh chemicals but also encourage researchers to utilize various natural products, which will ultimately help us to produce cost-effective multifaceted biomaterials.

1.2 Research Background

Polymers have gained a fascinating reputation in the field of biomaterials because of excellent physicochemical and mechanical properties. Basically, a polymer is a large molecule built up by the repetition of small and simple chemical units called monomers. The repetition is either linear, much like a chain or branched. Unlike many products whose structure and reactions were well known before their industrial application, some polymers were produced on an industrial scale long before their chemistry or physics was studied. Traditionally, polymers are synthesized by either simple condensation/step-reaction polymerization methods or addition/chain-reaction polymerization methods. In the biomedical field, polymers like polyurethane (PU), polyethylene (PE), polypropylene (PP), silicone, polytetrafluoroethylene (PTFE) etc., have sealed vital reputations for usage as surgical devices, implants, drug delivery systems, biosensors, bio-adhesives, ocular devices, dental materials, tissue adhesives, cardiac valves, artificial hearts, vascular grafts, breast prosthesis, facial prostheses, kidney and liver parts, tracheal tubes, food preservation, etc., as illustrated in Fig. 1.1 [14-22].

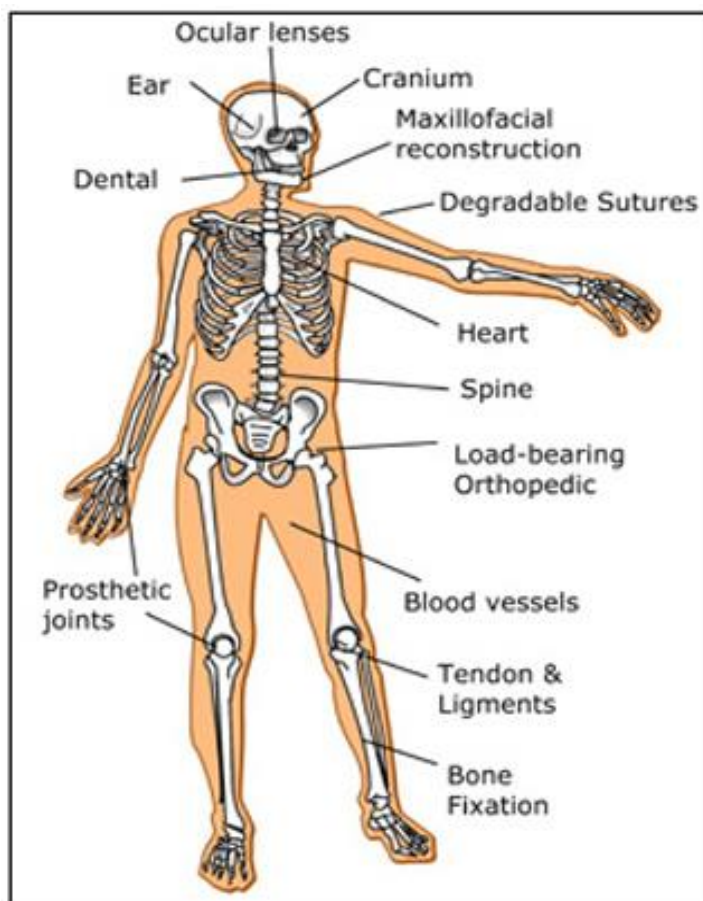


Figure 1.1 Applications of polymeric implants in the human body [2]

The prime advantage of polymers compared to other biomaterials is their ease of manufacture to yield intended shapes like membranes, fibers, gels, capsules, etc., at minimum cost. At present, a variety of biodegradable, bio-adhesive and bio-responsive polymers are mass produced for commercial purposes. Meanwhile, the advent of innovative technologies has created new platforms for exploitation of polymers in the form of hydrogels, nanofibers, nanoparticles, nanocomposites, nanosponges, nanocapsules, etc., [16]. Besides having commendable mechanical and physical properties, polymers fail in numerous cases because of their poor surface characteristics, which ultimately activate undesired host-mediated reactions. Hence, the research on exploring feasible approaches to improve the biocompatibility of polymers is still actively progressing.

The polymer mPE used in this research is one of the rising biomaterials belonging to polyolefin family of polymers synthesized using “metallocene catalyst” [23]. Because of its low density it has been suggested as an effective alternative to commonly used polymers like polyvinylchloride (PVC), for applications including blood bags, syringe tubes, and packaging bottles [12, 23]. In addition, the mPE sheet also offers a number of attractive features such as superior tensile strength, elasticity, toughness, excellent resistance to puncture, impact, blocking and bursting. On top of this, it also inferred to have a better permeability to oxygen when compared with PVC and can also provide an effective barrier against the attack of ammonia [23, 24]. The property of oxygen permeability is not only important for ocular implants, but also for tissue engineering materials since it is reported to facilitate the release of desired biomolecules [11]. Further, the existence of O₂ permeability may also ensure better gas exchange to tissues in contact. However, mPE elicit undesirable reactions when exposed to a biological environment because of poor biocompatibility. Recent efforts have expressed the possibility of enhancing the bioactivity of mPE by subjecting it to various surface modifications [12, 13].

1.3 Problem statement

Though mPE has excellent physical and mechanical properties, they often lead to clot formation because of poor blood compatibility [12]. As mentioned, blood compatibility is a crucial factor which determines the quality of a polymer and its performance in various applications. It precisely reflects the ability of a material to function in the desired region without triggering an appropriate host reaction. In general, a series of events will be triggered when blood comes in contact with the polymer after implementation, which is collectively called blood mediated reactions [21]. Based on those subsequent reactions, a material is said to possess good or poor blood compatibility. In general, if the blood contacts the poorly compatible material it will lead to the complications such as: (1) Adsorption of plasma proteins and platelets on the material surface, (2) Release of clotting factors from activated platelets and initiation of coagulation cascades, (3) Interaction of RBCs with poorly compatible surface will be followed by the upset in cell integrity and leads to lysis [22]. To solve

these issues, several surface modification techniques have been explored but most of them are complicated and limited to a certain family of polymers. Nowadays, millions of investment have been directed towards advanced biomaterial research which involves in the exploration of new alternatives [25]. But to cater the future demand, more research need to be encouraged to improve the properties of existing medical materials using a feasible, eco-friendly and affordable modification technique [26, 27]. So in this study, the problem of poor blood compatibility reported in the medical usage of mPE is rectified by microwave assisted coating of AV extract.

1.4 Research objectives

1. To prepare AV extract and coat them on mPE samples pre-treated with microwaves.
2. To assess the physicochemical changes induced on the surface of mPE after coating with AV extract.
3. To determine the hemocompatibility of pristine and AV extract coated mPE samples.

1.5 Scope of the study

Initially, the semi-transparent gel was separated from fresh, succulent leaves of AV and was blended into a thick fibrous extract. Then, the mPE sheet was cut into square samples of dimension $2 \times 2 \text{ cm}^2$ and treated with microwaves for an optimized period of 60 s. Later, the microwave treated mPE samples were coated with the prepared AV extract for selected periods of 12 h and 24 h respectively. The coating process was carried out using a rocking shaker. After coating, the samples were dried and utilized for physicochemical studies includes FTIR, contact angle assay, SEM, Hirox 3D microscopy analysis and AFM to determine the alterations in surface chemistry, wettability and surface roughness of AV coated mPE samples. Moreover, the coating properties like thickness and strength were also determined, using Hirox

3D microscopy, peel test, and degradability test. Finally, the influence of the physicochemical changes in delaying the clotting time, resisting platelet adhesion and avoiding RBC's damage was displayed through *in vitro* blood compatibility assays like activated partial thromboplastin time (APTT), prothrombin time (PT), platelet adhesion studies and hemolysis assay respectively.

1.6 Significance of the study

Usage of plant extract for improving the biocompatibility of polymers not only opens the gate for a spectrum of medical utilization but also offer a nurturing environment for cells to proliferate. Most of the available approaches are complicated, expensive, and not eco-friendly because of usage of harsh chemicals and limited to a particular material or application. Therefore, this research is anticipated to encourage more studies on developing surface modification tools for multifaceted biomaterials.

1.7 Thesis outline

This thesis is divided into five main chapters. In Chapter 1, a brief explanation about the biomaterials and the research background of this study is elaborated. Further, the objectives of this study have been presented in the context of rectifying clinical complications caused by implants. Finally, the importance of the proposed method and its influence in encouraging future research is also projected.

In Chapter 2, key characteristic features of mPE and the problem of biocompatibility associated with polymers is explained in the context of blood interaction and related responses. In addition, the importance of surface modification techniques in improving the physicochemical properties of materials and its ability to act as a coating tool was described in detail. Lastly, a brief discussion of the medical history of AV, its chemical constituents, and biomaterial usages is also framed.

In Chapter 3, the research methodology and characterization studies followed in this thesis are given in detail. The discussions mainly cover the details of materials used, procedures followed in the optimization of parameters and the need for the reported characterization studies.

In Chapter 4, the results obtained from proposed characterization studies have been elaborated and compared with previously reported work. This section is the heart of the thesis since it reflects the achievement and the effectiveness of the study.

In Chapter 5, a short summary of the whole work and its efficacy in eliminating a number of existing problems are projected. Moreover, some suggestion for future research is also presented.

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