

BIOMECHANICAL EVALUATION OF FRACTURE CONSTRUCT FOR  
FRACTURE FIXATION OF THE TIBIA

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*Dedicated to*

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## ABSTRACT

Plate osteosynthesis is one of the methods that can be used by surgeons to treat patients with bone fractures and irregularities. There are various osteosynthesis plates available commercially, but the most suitable implant with optimum screw configurations is highly subjective and remained a topic of debate. The aim of the study is to determine the optimum implant-screws configuration and implant designs which could maintain stability of the construct during bone healing. The tibia bone was chosen for the analyses, and has been divided into three stages – the proximal, diaphyseal and distal part of the bone. Three-dimensional (3D) bone model was reconstructed from computed-tomography (CT) datasets, and the implant models were designed using computer-aided design software. Tibial fractures and deformities were simulated with reference to the orthopaedic literatures. Finite element analysis (FEA) was used with a common loading applied at the proximal tibia. Results showed that the use of Locking Compression Plate (LCP) for fracture fixation provides better stability to the construct despite having a large stress magnitude of 45.5 MPa (p-value<0.001). In terms of screws configurations, placement near the fractured site provides a more rigid fixation. In contrast, placing the screws further away from the fractured site gives flexibility to the fracture construct which may result in callus formation. For the pylon fracture, the Medial Distal Tibial (MDT) plate significantly reduced the displacement and stress magnitudes as compared to the Anterolateral (ATL) plate (p-value<0.001).

## ABSTRAK

Osteosintesis plat merupakan salah satu cara yang digunakan oleh pakar bedah untuk merawat pesakit yang mengalami kepatahan dan kecacatan pada tulang. Kini, pelbagai jenis osteosintesis plat boleh diperolehi secara komersial, tetapi jenis implan dan konfigurasi skru yang terbaik masih menjadi perkara yang subjektif dan topik ini sering dibincangkan. Tujuan kajian ini dilakukan adalah untuk menentukan konfigurasi skru-plat yang optimum dan juga reka bentuk implan yang dapat mengekalkan kestabilan konstruk semasa proses penyembuhan tulang. Tulang tibia telah dipilih untuk kajian ini dan dibahagikan kepada tiga bahagian – *proximal*, *diaphyseal* dan juga bahagian *distal* tulang. Model tulang tiga dimensi (3D) dijana daripada dataset tomografi berkomputer (CT), manakala implan telah direka dengan menggunakan perisian rekaan berpandukan komputer. Kepatahan dan kecacatan pada tulang disimulasikan berdasarkan kajian ortopedik terdahulu. Analisis unsur terhingga (FEA) digunakan dengan mengenakan beban langsung pada bahagian *proximal* tibia. Keputusan menunjukkan bahawa penggunaan *Locking Compression Plate* (LCP) memberikan konstruk yang lebih stabil walaupun mempunyai magnitud tegasan yang tinggi sebanyak 45.5 MPa ( $p\text{-value}<0.001$ ). Selain itu, penetapan yang lebih pegun boleh diperolehi dengan menempatkan skru berdekatan dengan kawasan yang patah. Sebaliknya, dengan menempatkan skru lebih jauh dari kawasan yang patah dapat memberikan lebih fleksibiliti kepada konstruk kepatahan dan seterusnya menggalakkan pertumbuhan *callus*. Bagi kepatahan *pylon*, plat *Medial Distal Tibial* (MDT) memberi kelebihan dengan pengurangan sesaran dan tegasan yang ketara berbanding plat *Anterolateral* (ATL) ( $p\text{-value}<0.001$ ).

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**LIST OF ABBREVIATIONS**

3D	-	Three dimension
AIS	-	Abbreviated injury scale
ANOVA	-	Analysis of variance
AO	-	<i>Arbeitsgemeinschaft für Osteosynthesefragen</i>
ATL	-	Anterolateral
BMD	-	Bone mineral density
CAD	-	Computer-aided design
CT	-	Computed Tomography
CWHTO	-	Closed-wedge high tibial osteotomy
DCP	-	Dynamic Compression Plate
DISP	-	Displacement
EVMS	-	Equivalent von Mises stress
FEA	-	Finite element analysis
HTO	-	High tibial osteotomy
JOT	-	Journal of Orthopaedic Trauma
LC-DCP	-	Limited Contact Dynamic Compression Plate
LCP	-	Locking Compression Plate
LHS	-	Locking head screws
LISS	-	Less invasive stabilize system
MDT	-	Medial distal tibia
MIPO	-	Minimal invasive plate osteosynthesis
mm	-	Millimeter
MPa	-	Mega Pascal
N	-	Newton
NA	-	Neutral axis

No.	-	Number
NTrD	-	National Trauma Database
OTA	-	Orthopaedic Trauma Association
OWHTO	-	Open-wedge high tibial osteotomy
PC-Fix	-	Point Contact fixator
PC-Fix2	-	Point Contact fixator 2
USA	-	United State of America
WBL	-	Weight bearing line

**LIST OF SYMBOLS**

%	-	Percentage
$E$	-	Elastic Modulus
$^{\circ}$	-	Degree
$\nu$	-	Poisson ratio
$x, y, z$	-	Rectangular coordinates
$\sigma$	-	Stress

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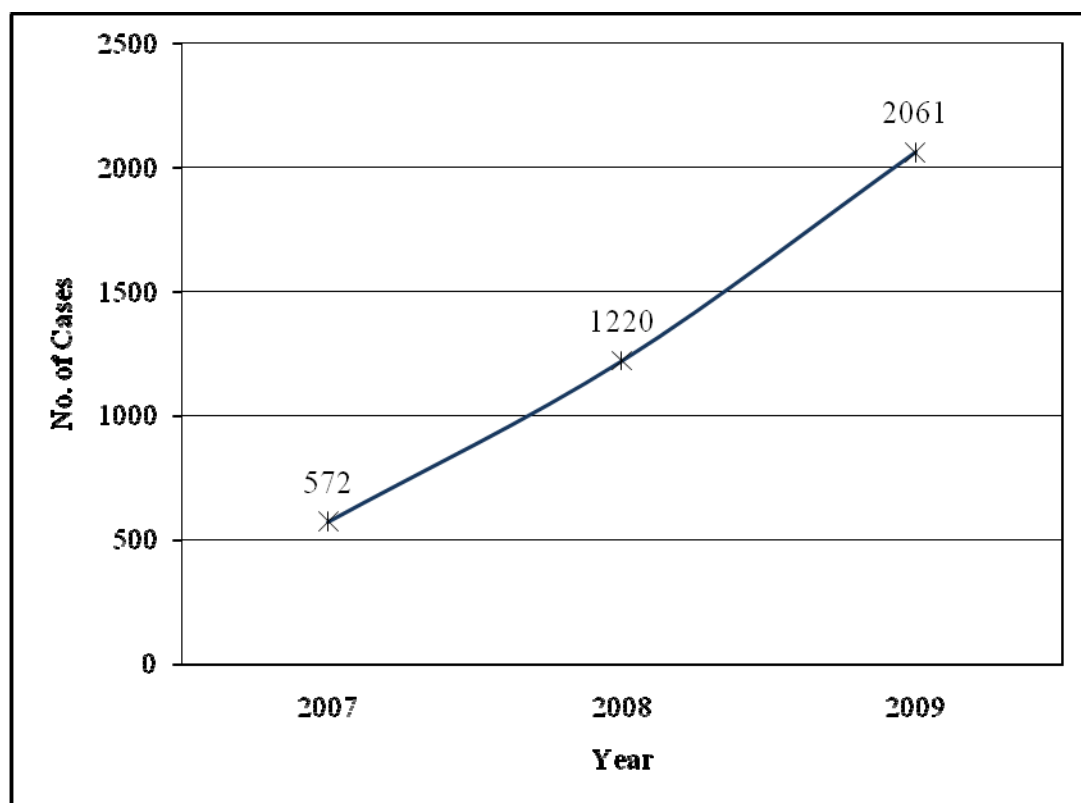


## **CHAPTER 1**

### **INTRODUCTION**

#### **1.1 Project Background**

Trauma can be considered as one of the most common cases attends by surgeon on major medical center around the world. According to the Health Facts 2000 that being document by Ministry of Health, Malaysia, trauma is the third most cases being admit to the medical center [1]. Report by National Trauma Database (NTrD) from January 2007 until December 2009 shows an increasing number of patient with trauma injury being admitted to the medical center (figure 1.1) [2-5]. Bone will fail when large external forces being applied to the bone. Risk for younger patient to experience bone fracture is different from the elderly which osteoporosis can be exclude as one of the factor. Trauma is the fifth contributing to death in Malaysia [2]. Active lifestyle of young patient is one of the factors that contributed to the statistic patient being admitted to the medical center, most of the time the patient suffers broken bones from sport activity. Besides that, accidents can happen anywhere and it also gives away some patient that will suffer some bone fracture.



**Figure 1.1** Number of cases from 2007 till 2009 based on NTrD reports

Condition of the bone also can contribute to bone fracture to occur such low bone mineral density (BMD), osteoporosis or bone cancer which gives weaken the bone and relatively easy to fracture even under a small force being apply directly to the bone. Elderly age around 60 and above are the potential group for bone fracture to occur because of osteoporosis. Gender based statistic shows that female has the tendency to experience bone fracture compared to male because of osteoporosis [6]. Caucasian female age 50 has a risk of forty percent to fracture on hip, spine or distal forearm, while thirteen percent on Caucasian male in similar age [6].

Trauma fixation depends on the severity and the complexity of the injury itself beside the surgeon familiarity and their expertise of handling the case. There are broad number of treatment and implant that can be choosing from. Most of the implant has its own advantages and disadvantages in every aspect for fracture fixation. However, a well known implant that usually being relate to the bone fracture fixation is plate osteosynthesis. Plate osteosynthesis is a method of bone

fracture fixation using a plate and screws as the fixation devices and it also one of the direct method for fracture fixation. The implant will hold the fracture site by maintaining the fracture bones align together in their anatomical place until the bone heal itself. After healing process is complete without any complication, the implant will be leave in the patient body unless there is some complication cause by the implant to the patient. The whole fixation process from identifying the problem until the bone is fully heal need to be done under two separated surgical procedure. Between both surgical procedures, the stability of the implant and the expertise of the surgeon will be tested by the reaction the patient's body with the implant [7]. Stability of the fracture construct is the main aspect that needs to be considers during fracture fixation. The implant need to be able to maintain the fracture construct and endure all physical activity that being done by the patient during healing period of the bone. achieving stable fixation may become a step closer to the fracture fixation common goal which is to achieve boney union [8].

## **1.2 Problem statement**

Since the 1960s, both the techniques and implants used for fracture fixation has evolved in order to improve healing of the bone [9]. Fracture fixation offer a lot of varieties of implant and need a proper planning by the surgeon in detail. Among things that need to be considered by the surgeon are the patient factors, the intended outcome, reduction technique, choice of implant and post operative regime [7].

Varieties choices of implant are wide from the direct to the indirect method of bone healing. Most common implant being used by the orthopedic surgeon for fracture fixation are plate system which include the locking compression plate (LCP), dynamic compression plate (DCP), less-contact dynamic compression plate (LC-DCP), point-contact fixator (PC-Fix) and less invasive stabilize system (LISS). All this plates serve the same purpose which is to achieve boney union but the

approach for each of it is different [8]. Among all the plates, the LCP and DCP are usually being used for fracture fixation. The DCP also referred to as conventional plating, achieves fixation through the friction between the plate and bone [10]. The plate has to be in compression with the fragment bone in order to achieve maximum stability for the fixation [8, 11]. Meanwhile, the LCP does not require the plate to be in contact with the bone mainly because its follows the biomechanical principles of an external fixator [10]. The LCP using the locking head screws (LHS) that will maintaining the stability of the fracture construct and eliminate the need of friction between the plate and the bone. Level of stability of both type of implant in maintaining the fracture fixation is reliable but does not guarantee a correct and successful fixation can be achieved.

Despite the existing of LCP, the DCP is still be using by certain surgeon as their implant of choices even the LCP gives much more biological advantages from the fixation point of view. Comparative study between the LCP and DCP stability still an on-going research. Beside that the combination on the plate itself by manipulating the screw's type, screw's size, plate's length and various combination of screw's placement on the plate can provide a wide option to the surgeon.

### **1.3 Aims and Objective**

Purpose of fracture fixation is to achieve boney union where the bone can function properly. As mention before, the variety of treatment are broad, therefore the correct choice must be made by the surgeon to ensure the fixed bone can achieve their purpose. Plate osteosynthesis technique is one option among all the technique available for fracture fixation. These techniques also offer very wide varieties of plate that can be used for bone fracture fixation. DCP and LCP are common being used because of the stability both implant provide.

Therefore, based from the problem statement, the objective of this study being conduct is to evaluate the fixation construct through the use of Dynamic Compression Plate (DCP) for fracture fixation of lower limb. Besides using only the DCP as the fixator, LCP also be included in this study in order to evaluate the fixation construct through the use of Locking Compression Plate (LCP) using same fracture condition. By having both implants being used for the same fracture construct, comparison between both implant can be determined based on obtained result.

Others than comparing between the different, the LCP alone can provide a different stability by changing the combination on the plate itself. Configuration of the LCP can be change by manipulation of screws numbers being used, length of the screws and the plate length. Each configuration may give stability that need by the surgeon. This study is to investigate the configuration needed by LCP to provide a sufficient stability for fracture fixation.

On the other hand, in order to investigate the effect of different plate with the same locking concept to the stability of the intra-articular fracture or also known as pilon fracture, anterolateral plate (ATL) and medial distal tibia (MDT) will be used for this task. This type of fracture is one of challenging construct to be fixed because of the involvement of multiple fragments. This study will show the effect of the stability on the fracture construct of intra-articular fracture on by using different plate.

#### **1.4 Scope and the Importance of Research**

Traumatology is a wide area which covers almost every area of bone in patient's body that either broken or dislocate. Therefore, for this particular study, the

fixation will take place on the lower limb area, more specifically the femur and tibia bone. Lower limb bear most of the weight from the body during standing and also during high load activities such as climbing, jumping and even running. This study is a three dimensional (3D) computer simulation analysis and the reason is to create more realistic approach in simulating the real condition during the fixation.

Despite the varieties of implant exist for fracture fixation, the LCP and DCP be used in this study as the implant. This study contains three different cases using three different implants. One of the study will used the straight LCP plate with combination screws hole for fixation of tibial shaft. Another cases will used the DCP claw plate that being used as fixator for peri-prosthetic fracture on the proximal femur. The last case in these thesis used the both the DCP and LCP implant concepts that being used for a high tibial osteotomy (HTO) which is the Puddu plate used the DCP concept and the Tomofix plate that using the LCP concept. All the implants created into 3D model using the existing commercially available implant.

Impact on bone can break the bone and cause the disturbance in the continuity of the bone and their alignment. Energy level of the impact, direction of the impact and the condition of the bone mineral density all where factor that contributed to the condition of the fracture bone. As in this study, two out three cases using the same type of fracture which is the oblique fracture. According to the Müller AO (*Arbeitsgemeinschaft für Osteosynthesefragen*) classification of fractures for the tibia is 42-A2 for oblique fracture and for articular multi-fragmentary fracture of 43-C3 [12].

Besides the fracture bone, bone deformity correction also being simulated and be analyze. Deformity correction also used the same principal as the fracture fixation which is to restore functionality and union of the bone. As is this thesis, the deformity correction of varus tibia using high tibial osteotomy (HTO) technique being done. With HTO, the tibia will be corrected to be in normal position of the

tibia. The correction will leave a wide gap along the osteotomy line. This gap needs to be stabilized for the bone to be in a normal condition.

Analysis is done in finite element using computer simulation. Computer simulation gives the option of simulate the real condition of the bone and its surrounding. Therefore the result can be trusted and can be as references to the surgeon community for patient's treatment. Results obtain be discussed biomechanically with equivalent von Mises stress (EVMS) and displacement as the parameter to explained the stability of the fracture bone, the efficiency of the implant to maintaining the construct and the effectiveness of the implant to maintain the fracture construct in order to achieved the purpose of fracture fixation.

This study will let us know the stability of the fracture construct after fixation plate place on bone under normal loading condition. Results obtain from the study can gives an overview to surgeon in biomechanical aspect despite the clinical aspect. It also can be as one of the references to the surgeon in determines the best fixation implant that can provide a better stability to the fracture construct and give the functionality and mobility back to the patients.

## REFERENCES

1. Division, I.a.D.U.P.D., *Health Facts 2000*. 2000, Ministry Of Health.
2. Jamaluddin, S.F., *National Trauma Database May 2006 To April 2007 - First Report*. 2008, National Trauma Database And Clinical Research Centre: Malaysia.
3. Jamaluddin, S.F., et al., *National Trauma Database January 2008 To December 2008 - Third Report*. 2010, National Trauma Database And Clinical Research Centre: Malaysia.
4. Jamaluddin, S.F., et al., *National Trauma Database January 2007 To December 2007 - Second Report*. 2009, National Trauma Database And Clinical Research Centre: Malaysia.
5. Jamaluddin, S.F., et al., *National Trauma Database January 2009 To December 2009 - Fourth Report*. 2011, National Trauma Database And Clinical Research Centre: Malaysia.
6. Saag, K.G. Osteoporosis. In: J.H. Klippel, et al. *Primer on the Rheumatic Diseases*. New York: Springer. 576-598; 2008.
7. Szypryt, P. and D. Forward. The use and abuse of locking plates. *Orthopaedics and Trauma*. 2009. 23 (4): 281-290.
8. Miller, D.L. and T. Goswami. A review of locking compression plate biomechanics and their advantages as internal fixators in fracture healing. *Clinical Biomechanics*. 2007. 22 (10): 1049-1062.
9. Miclau, T. and R.E. Martin. The evolution of modern plate osteosynthesis. *Injury*. 1997. 28 (Supplement 1): A3-A6.
10. Smith, W.R., et al. Locking Plates: Tips and Tricks. *J Bone Joint Surg Am*. 2007. 89 (10): 2298-2307.
11. Cronier, P., et al. The concept of locking plates. *Orthopaedics & Traumatology: Surgery & Research*. 2010. 96 (4, Supplement 1): S17-S36.
12. Marsh, J.L., *Fracture and Dislocation Classification Compendium - 2007*, T.F. Slongo, Editor. 2007, Journal of Orthopedic Trauma: Switzerland.
13. Tepic, S. and S.M. Perren. The biomechanics of the PC-Fix internal fixator. *Injury*. 1995. 26 (Supplement 2): B5-B10.



14. Patel, V.A. *Biomechanical Evaluation of Locked and Non-locked Constructs Under Axial And Torsion Loading*. M.Sc. Thesis. Wright State University; 2008.
15. Tortora, G.J. and B. Derrickson. *Principles of Anatomy And Physiology*. United States of America: John Wiley & Sons, Inc. 2009.
16. Bartel, D.L., D.T. Davy, and T.M. Keaveny. *Orthopaedic Biomechanics: Mechanics and Design in Musculoskeletal Systems*. New Jersey: Pearson Prentice Hall. 2006.
17. Netter, F.H. and J.T. Hansen. *Atlas of human anatomy*: Icon Learning Systems. 2003.
18. Bangash, M.Y.H., F.N. Bangash, and T. Bangash. *Trauma - an engineering analysis: with medical case studies investigation*: Springer. 2007.
19. Schmitt, K.U., et al. *Trauma biomechanics: accidental injury in traffic and sports*: Springer. 2007.
20. Hosalkar, H.S., et al. Skeletal Trauma and Common Orthopedic Problems. In: J.S. Khurana. *Bone Pathology*. Humana Press. 159-177; 2009.
21. Tencer, A.F. and K.D. Johnson. *Biomechanics in orthopedic trauma: bone fracture and fixation*. United Kingdom: Martin Dunitz. 1994.
22. Cordey, J., R. Grütter, and R. Johner. The mechanical strength of bones in torsion application to human tibiae. *Injury*. 2000. 31 (Supplement 3): 68-71.
23. Franco, V., et al. Open Wedge High Tibial Osteotomy. *Techniques in Knee Surgery*. 2002. 1 (1): 43-53.
24. Parkinson, R.W. and V. Bhalaiik. (iii) The valgus and varus knee. *Current Orthopaedics*. 2001. 15 (6): 413-422.
25. Macnicol, M.F. Realignment osteotomy for knee deformity in childhood. *The Knee*. 2002. 9 (2): 113-120.
26. Franco, V., et al. (ii) Osteotomy for osteoarthritis of the knee. *Current Orthopaedics*. 2005. 19 (6): 415-427.
27. Rüedi, T.P., R.E. Buckley, and C.G. Moran. *AO principles of fracture management*: Thieme. 2007.
28. Ip, D. Principles of Fracture Fixation. In. *Orthopedic Traumatology — A Resident's Guide*. Heidelberg: Springer Berlin 85-132; 2006.
29. Tan, S.L.E. and Z.J. Balogh. Indications and limitations of locked plating. *Injury*. 2009. 40 (7): 683-691.

30. Duckworth, T. *Lecture notes on orthopaedics and fractures*: Blackwell Science. 1995.
31. Pallister, I. and A. Iorwerth. Indirect reduction using a simple quadrilateral frame in the application of distal tibial LCP: technical tips. *Injury*. 2005. 36 (9): 1138-1142.
32. Faschingbauer, M., et al. Treatment of Distal Lower Leg Fractures: Results with Fixed-Angle Plate Osteosynthesis. *European Journal of Trauma and Emergency Surgery*. 2009. 35 (6): 513-519.
33. Metcalfe, A.J., M. Saleh, and L. Yang. Asymmetrical fracture fixation: stability of oblique fractures is influenced by orientation. *Clinical Biomechanics*. 2005. 20 (1): 91-96.
34. Lerner, A., et al. Complications encountered while using thin-wire-hybrid-external fixation modular frames for fracture fixation: A retrospective clinical analysis and possible support for "Damage Control Orthopaedic Surgery". *Injury*. 2005. 36 (5): 590-598.
35. Lee, T., N.M. Blitz, and S.M. Rush. Percutaneous Contoured Locking Plate Fixation of the Pilon Fracture: Surgical Technique. *The Journal of Foot and Ankle Surgery*. 47 (6): 598-602.
36. Hans, K.U., P. Philippe, and S.B. David. Internal plate fixation of fractures: short history and recent developments. *J Orthop Sci*. 2006. 11 (2): 118-26.
37. Perren, S.M. Evolution Of The Internal Fixation Of Long Bone Fractures: The Scientific Basis Of Biological Internal Fixation: Choosing A New Balance Between Stability And Biology. *J Bone Joint Surg Br*. 2002. 84-B (8): 1093-1110.
38. Stoffel, K.K. *Modern Concepts in Plate Osteosynthesis*. PhD. Thesis. University of Western Australia; 2007.
39. Perren, S.M., et al. The limited contact dynamic compression plate (LC-DCP). *Archives of Orthopaedic and Trauma Surgery*. 1990. 109 (6): 304-310.
40. Miranda, M.A. Locking plate technology and its role in osteoporotic fractures. *Injury*. 2007. 38 (3, Supplement 1): 35-39.
41. Perren, S.M., et al. A dynamic compression plate. *Acta Orthop Scand Suppl*. 1969. 125: 31-41.

42. Schütz, M. and N.P. Südkamp. Revolution in plate osteosynthesis: new internal fixator systems. *Journal of Orthopaedic Science*. 2003. 8 (2): 252-258.
43. Perren, S.M. Evolution and rationale of locked internal fixator technology: Introductory remarks. *Injury*. 2001. 32 (Supplement 2): 3-9.
44. Frigg, R. Locking Compression Plate (LCP). An osteosynthesis plate based on the Dynamic Compression Plate and the Point Contact Fixator (PC-Fix). *Injury*. 2001. 32 (Supplement 2): 63-66.
45. Smith, T.O., et al. The clinical and radiological outcomes of the LISS plate for distal femoral fractures: A systematic review. *Injury*. 2009. 40 (10): 1049-1063.
46. Schandelmaier, P., et al. Distal femoral fractures and LISS stabilization. *Injury*. 2001. 32 (Supplement 3): 55-63.
47. Kumar, V., et al. Less Invasive Stabilization System for the Management of Periprosthetic Femoral Fractures Around Hip Arthroplasty. *The Journal of Arthroplasty*. 2008. 23 (3): 446-450.
48. Mushtaq, A., et al. Distal Tibial Fracture Fixation with Locking Compression Plate (LCP) Using the Minimally Invasive Percutaneous Osteosynthesis (MIPO) Technique. *European Journal of Trauma and Emergency Surgery*. 2009. 35 (2): 159-164.
49. S. Inc. *Synthes Instrument and implant approved by the AO foundation*. USA. 2003.
50. S. Inc. *Large Fragment LCP Instrument and Implant set*. USA. 2003.
51. Ip, D. Normal and Abnormal Bone Healing. In. *Orthopedic Traumatology — A Resident's Guide*. Heidelberg: Springer Berlin 45-84; 2006.
52. Dimitriou, R., E. Tsiridis, and P.V. Giannoudis. Current concepts of molecular aspects of bone healing. *Injury*. 2005. 36 (12): 1392-1404.
53. Doblaré, M., J.M. García, and M.J. Gómez. Modelling bone tissue fracture and healing: a review. *Engineering Fracture Mechanics*. 2004. 71 (13-14): 1809-1840.
54. Calmar, E.A. and R.J. Vinci. The anatomy and physiology of bone fracture and healing. *Clinical Pediatric Emergency Medicine*. 2002. 3 (2): 85-93.
55. Hounsfield, G.N. Computerized transverse axial scanning (tomography). 1. Description of system. *Br J Radiol*. 1973. 46 (552): 1016-22.

56. Nelissen, E., E. van Langelaan, and R. Nelissen. Stability of medial opening wedge high tibial osteotomy: a failure analysis. *International Orthopaedics*. 2010. 34 (2): 217-223.
57. Gaasbeek, R., et al. Correction accuracy and collateral laxity in open versus closed wedge high tibial osteotomy. A one-year randomised controlled study. *International Orthopaedics*. 2010. 34 (2): 201-207.
58. Chae, D.J., et al. Early complications of medial opening wedge high tibial osteotomy using autologous tricortical iliac bone graft and T-plate fixation. *The Knee*. 2011. 18 (4): 278-284.
59. Hankemeier, S., et al. Accuracy of high tibial osteotomy: comparison between open- and closed-wedge technique. *Knee Surgery, Sports Traumatology, Arthroscopy*. 2010. 18 (10): 1328-1333.
60. Stoffel, K., G. Stachowiak, and M. Kuster. Open wedge high tibial osteotomy: biomechanical investigation of the modified Arthrex Osteotomy Plate (Puddu Plate) and the TomoFix Plate. *Clinical Biomechanics*. 2004. 19 (9): 944-950.
61. Krishna, K.R., I. Sridhar, and D.N. Ghista. Analysis of the helical plate for bone fracture fixation. *Injury*. 2008. 39 (12): 1421-1436.
62. Genta, G. The Finite Element Method. In: G. Genta. *Vibration Dynamics and Control*. US: Springer. 363-400; 2009.
63. Duda, G.N., et al. Mechanical boundary conditions of fracture healing: borderline indications in the treatment of unreamed tibial nailing. *Journal of Biomechanics*. 2001. 34 (5): 639-650.
64. Benli, S., et al. Evaluation of bone plate with low-stiffness material in terms of stress distribution. *Journal of Biomechanics*. 2008. 41 (15): 3229-3235.
65. Blecha, L.D., et al. How plate positioning impacts the biomechanics of the open wedge tibial osteotomy; A finite element analysis. *Computer Methods in Biomechanics and Biomedical Engineering*. 2005. 8 (5): 307 - 313.
66. Chen, G., et al. PREDICTING THE FATIGUE LIFE OF INTERNAL FRACTURE FIXATION PLATES. *Journal of Biomechanics*. 2008. 41 (Supplement 1): S495-S495.
67. Bresina, S.J. and S. Tepic. Finite element analysis (FEA) for the Point contact fixator screw drive, plate design, overcuts. *Injury*. 1995. 26 (Supplement 2): B20-B23.

68. Zhim, F., et al. Biomechanical stability of high tibial opening wedge osteotomy: Internal fixation versus external fixation. *Clinical Biomechanics*. 2005. 20 (8): 871-876.
69. Spahn, G. and R. Wittig. Primary stability of various implants in tibial opening wedge osteotomy: a biomechanical study. *Journal of Orthopaedic Science*. 2002. 7 (6): 683-687.
70. Fan, Y., et al. Biomechanical and histological evaluation of the application of biodegradable poly-l-lactic cushion to the plate internal fixation for bone fracture healing. *Clinical Biomechanics*. 2008. 23 (Supplement 1): S7-S16.
71. Peleg, E., et al. A short plate compression screw with diagonal bolts: A biomechanical evaluation performed experimentally and by numerical computation. *Clinical Biomechanics*. 2006. 21 (9): 963-968.
72. Kim, S.-H., S.-H. Chang, and H.-J. Jung. The finite element analysis of a fractured tibia applied by composite bone plates considering contact conditions and time-varying properties of curing tissues. *Composite Structures*. 2010. 92 (9): 2109-2118.
73. KazImoglu, C., et al. Which is the best fixation method for lateral cortex disruption in the medial open wedge high tibial osteotomy? A biomechanical study. *The Knee*. 2008. 15 (4): 305-308.
74. Sonoda, N., et al. Biomechanical analysis for stress fractures of the anterior middle third of the tibia in athletes: nonlinear analysis using a three-dimensional finite element method. *Journal of Orthopaedic Science*. 2003. 8 (4): 505-513.
75. Cordey, J., M. Borgeaud, and S.M. Perren. Force transfer between the plate and the bone: relative importance of the bending stiffness of the screws and the friction between plate and bone. *Injury*. 2000. 31 (Supplement 3): 21-28.
76. Jacobi, M., P. Wahl, and R. Jakob. Avoiding intraoperative complications in open-wedge high tibial valgus osteotomy: technical advancement. *Knee Surgery, Sports Traumatology, Arthroscopy*. 2010. 18 (2): 200-203.
77. Niemeyer, P. and N.P. Sudkamp. Principles and clinical application of the locking compression plate (LCP). *Acta Chir Orthop Traumatol Cech*. 2006. 73 (4): 221-8.

78. Gong, H., Y.B. Fan, and M. Zhang. Computational Simulation for Osteoporosis at the Basic Multicellular Unit Level. In: Y. Peng and X. Weng. *7th Asian-Pacific Conference on Medical and Biological Engineering*. Heidelberg: Springer-Berlin 182-185; 2008.
79. Meneghini, R., et al. Stem diameter and rotational stability in revision total hip arthroplasty: a biomechanical analysis. *Journal of Orthopaedic Surgery and Research*. 2006. 1 (1): 1-7.
80. Augat, P., et al. Shear movement at the fracture site delays healing in a diaphyseal fracture model. *Journal of Orthopaedic Research*. 2003. 21 (6): 1011-1017.
81. Will, R., et al. Locking plates have increased torsional stiffness compared to standard plates in a segmental defect model of clavicle fracture. *Archives of Orthopaedic and Trauma Surgery*. 2010: 1-7.
82. Cheng, H.-Y.K., et al. Biomechanical evaluation of the modified double-plating fixation for the distal radius fracture. *Clinical Biomechanics*. 2007. 22 (5): 510-517.
83. Aro, H.T. and E.Y. Chao. Bone-healing patterns affected by loading, fracture fragment stability, fracture type, and fracture site compression. *Clin Orthop Relat Res*. 1993 (293): 8-17.
84. Gorsse, S. and D.B. Miracle. Mechanical properties of Ti-6Al-4V/TiB composites with randomly oriented and aligned TiB reinforcements. *Acta Materialia*. 2003. 51 (9): 2427-2442.
85. Taylor, W.R., et al. Tibio-femoral loading during human gait and stair climbing. *Journal of Orthopaedic Research*. 2004. 22 (3): 625-632.
86. Kim, S.-H., S.-H. Chang, and H.-J. Jung. The finite element analysis of a fractured tibia applied by composite bone plates considering contact conditions and time-varying properties of curing tissues. *Composite Structures*. In Press, Corrected Proof.
87. Bachus, K.N., M.T. Rondina, and D.T. Hutchinson. The effects of drilling force on cortical temperatures and their duration: an in vitro study. *Medical Engineering & Physics*. 2000. 22 (10): 685-691.
88. Matthews, L.S. and C. Hirsch. Temperatures Measured in Human Cortical Bone when Drilling. *The Journal of Bone and Joint Surgery*. 1972. 54 (2): 297-308.

89. Rosson, J., et al. Bone weakness after the removal of plates and screws. Cortical atrophy or screw holes? *J Bone Joint Surg Br.* 1991. 73-B (2): 283-286.
90. Fouad, H. Assessment of function-graded materials as fracture fixation bone-plates under combined loading conditions using finite element modelling. *Medical Engineering & Physics.* 2011. 33 (4): 456-463.
91. Stoffel, K., et al. Biomechanical testing of the LCP - how can stability in locked internal fixators be controlled? *Injury.* 2003. 34 (Supplement 2): 11-19.
92. Cordey, J., S.M. Perren, and S.G. Steinemann. Stress protection due to plates: myth or reality? A parametric analysis made using the composite beam theory. *Injury.* 2000. 31 (Supplement 3): 1-13.
93. Duda, G.N., et al. Mechanical conditions in the internal stabilization of proximal tibial defects. *Clinical Biomechanics.* 2002. 17 (1): 64-72.
94. Cheal, E.J., et al. Stress analysis of a simplified compression plate fixation system for fractured bones. *Computers & Structures.* 1983. 17 (5-6): 845-855.
95. Ehlinger, M., P. Adam, and F. Bonnomet. Minimally invasive locking screw plate fixation of non-articular proximal and distal tibia fractures. *Orthopaedics & Traumatology: Surgery & Research.* 2010. 96 (7): 800-809.
96. Ellis, T., C.A. Bourgeault, and R.F. Kyle. Screw Position Affects Dynamic Compression Plate Strain in an In Vitro Fracture Model. *Journal of Orthopaedic Trauma.* 2001. 15 (5): 333-337.
97. Bone, L.B., et al. Displaced isolated fractures of the tibial shaft treated with either a cast or intramedullary nailing. An outcome analysis of matched pairs of patients. *J Bone Joint Surg Am.* 1997. 79 (9): 1336-41.
98. Merchant, T.C. and F.R. Dietz. Long-term follow-up after fractures of the tibial and fibular shafts. *J Bone Joint Surg Am.* 1989. 71 (4): 599-606.
99. Ahmad, M., et al. Biomechanical testing of the locking compression plate: When does the distance between bone and implant significantly reduce construct stability? *Injury.* 2007. 38 (3): 358-364.
100. Gautier, E., S.M. Perren, and J. Cordey. Effect of plate position relative to bending direction on the rigidity of a plate osteosynthesis. A theoretical analysis. *Injury.* 2000. 31 (Supplement 3): 14-20.

101. Fouad, H. Effects of the bone-plate material and the presence of a gap between the fractured bone and plate on the predicted stresses at the fractured bone. *Medical Engineering & Physics*. 32 (7): 783-789.
102. Seebeck, J., et al. Effect of cortical thickness and cancellous bone density on the holding strength of internal fixator screws. *Journal of Orthopaedic Research*. 2004. 22 (6): 1237-1242.
103. Seebeck, J., et al. Mechanical behavior of screws in normal and osteoporotic bone. *Osteoporosis International*. 2005. 16 (0): S107-S111.
104. French, B. and P. Tornetta, 3rd. High-energy tibial shaft fractures. *Orthop Clin North Am*. 2002. 33 (1): 211-30, ix.
105. Egol, K.A., R. Dolan, and K.J. Koval. Functional outcome of surgery for fractures of the ankle. A prospective, randomised comparison of management in a cast or a functional brace. *J Bone Joint Surg Br*. 2000. 82 (2): 246-9.
106. Boer, P.d. and R. Metcalfe. (iv) Pilon fractures of the tibia. *Current Orthopaedics*. 2003. 17 (3): 190-199.
107. Ronga, M., et al. Percutaneous Plating of Ankle Fractures. In: A. Saxena. *International Advances in Foot and Ankle Surgery*. London: Springer. 163-168; 2012.
108. Clare, M.P. and R.W. Sanders. Percutaneous ORIF of Periarticular Distal Tibia Fractures. In: G.R. Scuderi and A.J. Tria. *Minimally Invasive Surgery in Orthopedics*. New York: Springer. 515-522; 2010.
109. Ronga, M., et al. Percutaneous Osteosynthesis of Distal Tibial Fractures Using Locking Plates Minimally Invasive Surgery of the Foot and Ankle. In: N. Maffulli and M. Easley. London: Springer. 357-361; 2011.
110. Kim, H.-J., S.-H. Kim, and S.-H. Chang. Bio-mechanical analysis of a fractured tibia with composite bone plates according to the diaphyseal oblique fracture angle. *Composites Part B: Engineering*. 2011. 42 (4): 666-674.
111. Kim, S.-H., S.-H. Chang, and D.-S. Son. Finite element analysis of the effect of bending stiffness and contact condition of composite bone plates with simple rectangular cross-section on the bio-mechanical behaviour of fractured long bones. *Composites Part B: Engineering*. 2011. 42 (6): 1731-1738.
112. Anglen, J.O. Early Outcome of Hybrid External Fixation for Fracture of the Distal Tibia. *Journal of Orthopaedic Trauma*. 1999. 13 (2): 92-97.



113. Grose, A., et al. Open Reduction and Internal Fixation of Tibial Pilon Fractures Using a Lateral Approach. *Journal of Orthopaedic Trauma*. 2007. 21 (8): 530-537
114. Chowdhry, M. and K. Porter. The pilon fracture. *Trauma*. 2010. 12 (2): 89-103.
115. Kanchanomai, C., V. Phiphobmongkol, and P. Muanjan. Fatigue failure of an orthopedic implant - A locking compression plate. *Engineering Failure Analysis*. 2008. 15 (5): 521-530.
116. Kao, F.C., et al. Treatment of distal tibial fractures by minimally invasive percutaneous plate osteosynthesis of three different plates: Results and cost-effectiveness analysis. *Formosan Journal of Musculoskeletal Disorders*. 2010. 1 (1): 35-40.
117. Krackhardt, T., et al. Fractures of the distal tibia treated with closed reduction and minimally invasive plating. *Archives of Orthopaedic and Trauma Surgery*. 2005. 125 (2): 87-94.