NUMERICAL SOLUTION OF FOUR DIFFERENT STENOSIS LOCATIONS IN BIFURCATED ARTERY WITH HEAT TRANSFER

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DEDICATION

Special dedication to my beloved parents

Ahmad Jamali Bin Malin

Zaleha binti Amat

To my respectful supervisor and co-supervisor

Dr. Zuhaila Ismail

Prof. Dr. Norsarahaida S. Amin

To my loving siblings and my supportive colleagues

To my friends and seniors

Thank you for everything. Your presence made my journey truly memorable

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ABSTRACT

The development and progression of stenosis with a high probability of rupture can be characterised by changing the temperature distribution in the bifurcated artery. The purpose of this study is to investigate the behaviour of blood flow through four different locations of stenosis under the influence of heat transfer. In this study, the basic step of construction geometries (TYPE I, TYPE II, TYPE III, and TYPE IV that implies four possible morphologies formation of plaque from healthy to disease artery) are shown by using COMSOL Multiphysics 5.2. The blood flow is modelled as laminar, two-dimensional, steady, incompressible, and characterised as a Newtonian fluid. The classical Galerkin Weighted Residual (GWR) method is utilised to discretise the governing equations and boundary conditions. In addition, GWR is a convenient method to compute the solution since this method is compatible with circumventing the Babuska-Brezzi stability conditions. Firstly, a MATLAB source code is developed to solve the problem. Later, the results are compared with COMSOL Multiphysics 5.2 that based on the finite element method. The numerical validations are performed for the lid-driven cavity flow benchmark and the results of the axial velocity profile achieve a good agreement. This investigation focuses on the blood flow characteristics such as the velocity, temperature, pressure, streamline pattern, wall shear stress, and local Nusselt number, which have been discussed graphically and fundamentally. The parameters involved, such as Reynolds and Prandtl numbers, the maximum height of stenosis are very much affect the blood flow characteristics. Besides, TYPE IV shows the highest value of maximum velocity as compare to TYPE II and TYPE III. The backflow is formed in the post-stenotic region near the outer wall surface. Higher Reynolds number has enhanced the magnitudes of the wall shear stress predominantly in the downstream region of stenosis and reduced the pressure at the artery walls to some negative values resulted from the flow reversal. It shows that by increasing the maximum height of stenosis and Reynolds number, the shut of the peak for Nusselt number and also blood flow accelerations will increase rapidly.

ABSTRAK

Pembentukan dan perkembangan stenosis dengan kebarangkalian memecah yang tinggi boleh disifatkan melalui pertukaran taburan suhu di dalam arteri bercabang. Tujuan kajian ini adalah untuk mengkaji sifat aliran darah melalui empat lokasi stenosis yang berbeza di bawah pengaruh pemindahan haba. Dalam kajian ini, langkah-langkah asas pembinaan geometri (JENIS I, JENIS II, JENIS III, dan JENIS IV yang mengimplikasikan empat pembentukan morfologi plak dari arteri yang sihat kepada yang berpenyakit) telah ditunjukkan melalui COMSOL Multiphysics 5.2. Aliran darah dimodelkan sebagai laminar, dua dimensi, mantap, bendalir tak termampat, dan disifatkan sebagai bendalir Newtonian. Kaedah Sisa Berpemberat Galerkin (GWR) digunakan untuk mencerakinkan persamaan menakluk dan syarat sempadan. Tambahan pula, GWR merupakan kaedah yang sesuai untuk mengira penyelesaian kerana kaedah ini dapat mengelakkan syarat kestabilan Babuska-Brezzi. Pertama, kod perisian MATLAB dibangunkan untuk menyelesaikan masalah yang terlibat. Kemudian, keputusan yang dihasilkan dibandingkan dengan COMSOL Multiphysics 5.2, yang berasaskan kaedah unsur terhingga. Pengesahan berangka dilaksanakan mengikut piawaian aliran rongga berpenutup bergerak dan keputusan halaju paksi mencapai persetujuan yang baik. Kajian ini menumpukan kepada sifat aliran darah seperti halaju, suhu, tekanan, corak garis lurus, tegasan ricih dinding, dan nombor Nusselt setempat yang telah dibincangkan secara grafik dan asas. Parameter yang terlibat seperti nombor Reynolds dan Prandtl, ketinggian maksimum stenosis sangat memberi kesan kepada sifat aliran darah. Selain itu, JENIS IV telah menunjukkan nilai halaju maksimum yang tertinggi berbanding dengan JENIS II dan JENIS III. Pembalikan aliran telah terbentuk pada akhir kawasan stenosis berhampiran permukaan dinding luar. Nombor Reynolds yang tinggi telah merangsang magnitud tegasan ricih dinding secara dominasi di kawasan hujung stenosis dan telah mengurangkan tekanan pada dinding arteri kepada beberapa nilai negatif yang terhasil daripada aliran berbalik. Ini menunjukkan bahawa dengan meningkatkan ketinggian maksimum stenosis dan nombor Reynolds, penutupan puncak untuk nombor Nusselt dan juga pecutan aliran darah akan meningkat dengan cepat.

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LIST OF ABBREVIATIONS

CVD	-	Cardiovascular Disease
FEM	-	Finite Element Method
MHD	-	Magnetohydrodynamics
PIV	-	Particle Image Velocimetry
CCA	-	Common Carotid Artery
ICA	-	Internal Carotid Artery
UTM	-	Universiti Teknologi Malaysia
ECA	-	External Carotid Artery
CFD	-	Computational Fluid Dynamics
DOF	-	Degree of Freedom
GWRM	-	Galerkin Weighted Residual Method
CV	-	Control Volume
CS	-	Control Surface
RTT	-	Reynold Transport Theorem

LIST OF SYMBOLS

x	-	Axial coordinate
У	-	Radial coordinate
$R_1(x)$	-	Radii of the outer wall
$R_2(x)$	-	Radii of the inner wall
a	-	Radii of the mother artery
r_1	-	Radii of daughter artery
r_0	-	Radii of curvature for the lateral junction
r_0	-	Radii of curvature for the flow divider
d	-	Onset of the stenosis
l_0	-	Length of the stenosis at distance d from the origin
<i>x</i> ₁	-	Location of the onset and offset of the lateral junction
<i>x</i> ₂	-	Location of the offset of the lateral junction
<i>x</i> ₃	-	Apex
$ au_m$	-	Maximum height of stenosis
β	-	Half of the bifurcation angle
ρ	-	Density of blood
и	-	Axial velocity component
v	-	Radial velocity component
w	-	Tangential velocity component
t	-	Time
μ	-	The respective molecular viscosity coefficient
m	-	Fluid consistency coefficient
Ω	-	Domain
p	-	Pressure
h	-	Length of the inlet
Re	-	Reynold number
Pr	-	Prandtl number
Т	-	Temperature

Nu	-	Nusselt number
${U}_0$	-	Averaged mean inflow velocity
C_p	-	Specific heat
k	-	Thermal conductivity
T_{in}	-	Inlet temperature
T_{wall}	-	Wall temperature
N_{i}	-	Trial function
n	-	The number of degrees of freedom
R	-	Residual
W _m	-	Weight function
<i>W</i> _a	-	Weight function for the momentum equation
W_b	-	Weight function for the continuity equation
τ	-	Tolerance value
e_i	-	Element <i>i</i>
е	-	Internal energy
Re	-	Reynold number
Pr	-	Prandtl number
Ε	-	Energy per unit mass
F(x,t)	-	Body force
P_h	-	Hydrostatic pressure
$F_{surface}$	-	Surface force
P_m	-	Mean pressure
\overline{q}	-	Heat flux vector
$\sigma_{_{ij}}$	-	Stress tensor
${\cal E}_{ij}$	-	Strain rate tensor
$\delta_{_{ij}}$	-	Kronecker Delta
V(t)	-	Material volume

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CHAPTER 1

INTRODUCTION

1.1 Research Background

World Health Organization (WHO 2017) has confirmed that the cardiovascular diseases (CVDs) are the world biggest killer by accounting for more people to die annually compare with any other causes. An estimated number of death of 17 million deaths per year, representing 85% of death is caused by malfunction of organ, heart attack and stroke (World Health Organization, 2018). The understanding of blood flow behaviour is essential to investigate the connection between flow and disease development such as cardiovascular diseases. CVDs disorders of the heart and blood vessels are mainly due to the blockage that prevents blood from flowing to the heart or brain. To understand and discover the genesis of this vascular disease, special attention and interest has been given by many researchers all around the world. Generated knowledge in this area may lead to the design and advances of medical tools, which provide a greater prediction of disease progression and helps to increase the number of patients treated percutaneously.

1.1.1 Blood Composition

Blood is essential to the human body and other animals that delivers substances to the cells. Basically, the blood receives oxygen from the lungs and pushed through the body by the action of rhythmic pump of heart. Blood also transports heat to the skin to help regulate body temperature. Besides, blood is a complex mixture of cells, protein, lipoprotein, and ions. Blood can be classified as connective tissue and consisting the plasma, which is a clear extracellular fluid with the formed elements composed of Erythrocytes, known as red blood cells (RBCs), Leukocytes, known as white blood cells (WBCs), and platelets. These components can be centrifuged in a tube and separate the plasma to form elements according to their density. The total volume of 55% plasma is packed into the top of the tube in the form of pale-yellow colour. RBC makes up 45% of the total volume packed at the bottom of the tube, known as haematocrit. WBCs and platelets will be above RBC with the form of a narrow cream-coloured coat. The details of blood constituent can be referred in (Caro, C.G., Pedley, T.J., Schroter, R.C., 1978).



Figure 1.1 Composition of blood in a human vessel (Health Engine, 2019)

RBCs are small semisolid particles that increase blood viscosity and affect fluid behaviour. Blood is approximately four times more viscous than water. Despite, blood does not exhibit a constant viscosity at all flow rates especially non-Newtonian fluid type in the microcirculatory system. The non-Newtonian behaviour is most evident at meager shear rates when the red blood cells clump together into larger particles, (Ku, 1974). Blood is assumed as non-Newtonian behaviour in small capillaries, where the cell-free skimming layer reduces the effective viscosity through the tube. However, in most arteries, blood exhibits a Newtonian behaviour, and the viscosity is assume to be constant of, four centipoises. Zaman et al., (2015) had concluded that in a large radius of the artery, blood is assumed as a Newtonian fluid for values of a shear rate greater than 100 s⁻¹. Based on this, it clear shows that Newtonian fluid viscosity is always constant with shear rate and has high potential of cardiovascular diseases (Rabby et al., 2014).

1.1.2 Atherosclerotic Plaque

Cardiovascular diseases such as heart attack and stroke that are caused by atherosclerosis. The Atherosclerosis lesion is one of the most widespread diseases in human beings that lead to death in many countries. Typically, the walls of the healthy artery are smooth, which allowing blood to flow through the artery, for transportation of oxygen received from the lung and transmissions of nutrients from the intestine to tissues (Back, L., H., et al., 1977). There is an evidence that vascular fluid dynamics play an essential role in the development and progression of Atherosclerotic arterial, (Chakravarty and Sen, 2005). Atherosclerosis is a condition of the narrowing of the artery lumen as the result of plague deposition, known as stenosis (Zain and Ismail, 2017; Wu, J., et al., 2019). This leads to abnormal pattern of blood flow which severely reduces the flow of blood to the other organs and tissues. In some cases, plaque act differently and may lead to different blood rheology. Plaque might grows to finite size and eventually stops without narrowing the vessel in which the wall artery might resized their external diameter to provide sufficient space for the plaque, (Ikbal et al., 2009). Finally, the silent plaque can only be detected through an intravascular ultrasound device since it never caused any symptoms of the plaque formation that does not even block blood flow. Besides, there is an evidence shows that early atherosclerosis may lead to change in vessel wall size, and deposition of platelet thrombi may occur near the branching entrance. These conditions will disturb a flow where, from a fluid mechanical point of view, this can be related to the formation of eddies and separation of streamlines near the vessel wall (Genuardi et al., 2020).



Figure 1.2 Atherosclerotic plaque build-up causes constriction of the vessel lumen, expose to arterial thrombosis (DPRC Hospital, 2017)

According to Rabby et al., (2014), Alimohamadi et al., (2014), and Jahangiri et al., (2015), as plaque deposition such as cholesterol, fatty substance and smooth muscle cells continues to accumulate. The plaque will be formed on the inner wall of the artery, which is known as the endothelium. This may cause a bleeding when the plaque breaks away into emboli (particles) inside an artery. As a result, blood clots (thrombus) may form around the plaque and blood flow will be blocked and disrupted (Ikbal et al., 2009). As a consequence, patients of this case experience usual symptoms like pain on exertion. In severe cases, the patients will suffer from the neurological system (stroke) and unstable angina or myocardial infarction (heart attack) due to blockage of blood flow in the carotid artery and coronary artery, respectively. The malfunction of the cardiovascular system reveals that people is exposed to these cardiovascular diseases due to lack of awareness is emphasized on controlling their dietary and food intake. The risks such as smoking, high blood pressure and blood cholesterol is eight times more likely to develop atherosclerosis infection than a person without these risk factors. Hence, to elucidate the possible connection between blood flow behaviour and development of thrombosis and atherosclerosis, there is a growing need of work, both experimental and theoretical, to understand basic knowledge of artery disease treatment so that society awareness toward cardiovascular disease will be improved.



Figure 1.3 The carotid artery bifurcation site prone to atherosclerotic plaque deposition in the internal carotid arteries (Mayfield Clinic, 2018)

1.1.3 Arterial Geometry

Apart from that, an essential dynamics of blood flow factor that needs to be considered in current analyses is the arterial geometry. Studying the effect of these factors on the blood flow characteristics with heat transfer will help in a better understanding of the roles of blood dynamical in the development and progression of arterial diseases. Arteries and arterioles that consist of curvatures, junctions, and bifurcations were reported by Rabby et al., (2014), Srinivasacharya and Rao (2017), Zain and Ismail (2017), and Jamali and Ismail (2019). They claimed that the arterial geometry in bifurcation and bend shape exceptionally, would be the initiation of plaque accumulation. This suggests why the flow in certain regions has a high potential to be disturbed by flow disturbances like flow reversal and stagnation. As observed in the previous study, the flow reversal and recirculation zones are formed downstream of stenosis and along the edge of the daughter artery (Zain and Ismail, 2019). It is believed that the existence of flow recirculation in the cardiovascular system can cause danger to the health of a person, especially an atherosclerosis patient since the blood is moving slowly in this zone. The fruitful study has been classified as the geometry of the bifurcated artery according to the angulation between mother and daughter artery and also the location of plaque. T- shaped bifurcated artery is classified when the angulation is greater than 70° and plagued shifting to the bifurcation branched is more difficult. However, Y-shaped bifurcated artery is more pronounced because the angulation of mother to daughter artery is less than 70°, (Lefèvre et al., 2000).



Figure 1.4 Classifications of bifurcations artery according to plaque burden (Lefèvre et al., 2000)

1.1.4 Medical Application

The study of blood flow in the artery has its importance in medical and engineering areas (Sharma et al., 2011). Heat transfer is also an important domain of thermal engineering in blood flow problem. Several literatures have to practice its principles to explore a variety of information on how the body possibly transfers the heat. Interesting to be noted that the heat source produced by the human body supplies to various part of the organs of the body. This energy is utilized for the nutrients metabolism process that ceaselessly takes place. It has been reported by a medical practice that, in a human body at rest, about two-thirds of the total heat is generated by the metabolic activities of the internal organs in the thorax, the abdomen, and the brain. The share of the heat generated in the brain is around 16 % of the total heat generated in the whole body (Sinha et al., 2016).

The mathematical models of heat transfer have been developed and are very useful in the application of modern treatment, such as laser surgery as well as cryosurgery. This physiotherapy technique involves a certain amount of temperature and directly affects the portion of the human body. The normal temperature of human blood is about 37°C. Thus, irreversible ill effects will occur in the proteins of blood, which can cause death after such high fever (Chato, 1980).



Figure 1.5 Hyperthermia surgery and Cryosurgery Machine

Moreover, hypothermia or hyperthermia is widely used for many purposes such as open-heart surgeries and cancer treatment. The role of the temperature is substantially essential, refer to Figure 1.5. For a rising of 1°C, the time of cure is reduced to half for a particular biological result like the decrease of cancer cells of a tumor (Lin, Yen, Chen, Jin, and Shieh, 1999). The objective of hyperthermia in cancer therapy is to raise the temperature of cancerous tissue above a therapeutic value 42° C, while maintaining the surrounding normal tissue at a suitable temperature value. The heat exchange between the living tissues and the blood network that passes through it depends on the geometry of the blood vessels, the blood flow through it, and the properties of the blood and surrounding tissue, (Chato, 1980). Furthermore, the observed effects of heat transfer in blood flow influence the stenosis deformation and may disturb the flow behaviour. From medical point of view, the presence of stenosis in the artery may lead to blood flow acceleration (velocity increase), and the heat transfer coefficient is increases at the stenotic region and drop as the flow pass through the offset of stenosis (Audaa and Ph, 2018). Therefore, the presence of stenosis in artery enhances the rate of heat transfer. Formulation and analysis of mathematical models on heat transfer during blood flow have been found to be very useful.

1.2 Problem Statements of Research

Atherosclerosis is one of the important and common causes of death and disability throughout the world (WHO). Atherosclerosis refer to physiological problem due to the malfunction of cardiovascular system and have close relationship with flow characteristics of blood deformability of the vessel wall.

Heat transfer is one of the crucial parameters that needs to be considered in blood flow investigation. Lack of a proper analysis of this factor will cause an irreversible effect in the proteins of blood and may lead to fatality. The abnormal growth that happens in the bifurcated artery, known as stenosis, increase blood flow and blood temperatures in the artery. Therefore, the energy equation needs to be considered in order to determine the behaviour of heat transfer by calculating the blood temperature in the bifurcated artery. The existence of stenosis at various possible location in the artery, especially in the bifurcated lesion, will change the artery size at the specific location. So far, the existing literature investigated the flow structure and characteristic of heat transfer on Newtonian and non-Newtonian fluid models. The fluid behaves as a strong non-Newtonian characteristic in the small artery at a low shear rate (Zaman et al., 2015). However, it has been confirmed that the Newtonian model is considered as a good approximation as the shear rates are more than 100 s⁻¹ (reciprocal seconds), which have tendency to occur in a large artery.

Another important factor in haemodynamic analysis is the geometry of the artery. The arterial geometry in bifurcation and the shape of the bend will exceptionally, be the initiation of plaque accumulation since it has a sudden change on area and curvature. Various locations of stenosis in the bifurcation artery give a huge considerable effect to the blood characteristic and flow structure. It is believed that the existence of flow recirculation in the cardiovascular system can cause danger to the health of a person, especially atherosclerosis patients since the blood is moving slowly in this zone. Studying the effect of different location stenosis with heat transfer will help in better understanding of the development and arterial disease progression.

A numerical method is needed since the bifurcated artery geometry itself isin irregular shape and small scale. The finite element method (FEM) is proposed in this study to obtain the numerical results of the flow. This method has been demonstrated as one of the suitable numerical methods since it is easily applied to domains with complex geometry, film properties, and boundary conditions. The governing equation is discretized by using the Galerkin weighted residual (GWR) method, which is sufficient for computation the result in a large scale of convergence.

1.3 Objectives of Research

The main objective of this research is to develop the mathematical model of blood flow under the influence of heat transfer with the effect of different location of stenosis. This includes the construction of suitable mathematical models of the flow by considering appropriate governing equations and boundary conditions. The resulting governing equations are then solved using a Galerkin weighted residual (GWR). Specifically, the objectives are:

- 1. To develop appropriate governing equations that describe the blood flow through the bifurcated artery with the influence of heat transfer.
- 2. To generate MATLAB code based on the numerical discretization that has been performed using the Galerkin Weighted Residual method (GWR).
- To investigate the effect of heat transfer at different locations of stenosis on the blood flow characteristics, such as velocity, streamlines, wall shear stress, and pressure drop.
- 4. To investigate the effect parameters such as Reynold number, Prandtl number, the maximum height of stenosis, and local Nusselt number inside the streaming blood.

1.4 Scope of Research

The fluid flow with heat transfer in the stenosed bifurcated artery is analyzed. Only four different types of stenosis location are considered. The fluid is considered as an incompressible Newtonian fluid. The Navier-Stokes equation is modelled with few assumptions imposed, which are the flow is steady, laminar, and two-dimension by considering a rigid wall with the no-slip condition. The geometry of arteries forming bifurcations is not symmetrical about the trunk axis, and bifurcated circular cylinders of finite length contain the stenosis at the outer wall and inner wall. As a numerical technique, the finite element method (FEM) is developed by using the Cartesian coordinate system to tackle the convergence rate for even large-scale transient simulation. The GWR method is utilized to discretize the governing equations and boundary conditions. In addition, the classical Galerkin weighted residual is a convenient method to compute the resulting governing equations since this method is compatible with circumventing the Babuski-Brezzi stability conditions. A MATLAB source code is developed to solve the problem. Then, the results are compared with COMSOL Multiphysics 5.2, a software based on the FEM. The comparison is found in satisfactory agreement with previous literature work.

1.5 Significances of Research

Cardiovascular diseases are the number one killer disease in the world. More than 786,641 deaths of all 2515458 deaths are approximately caused by stroke, heart attack and other cardiovascular diseases (Mozaffarian, Benjamin, Go, Arnett, Blaha, and Howard, 2015). Therefore, the application of computational fluid dynamics is essential and economical in biomedical engineering to predict the roles of fluid dynamical factors in the development and progression of arterial diseases in various types of physiological artery geometries.

This research may help in better understanding the behaviour of blood flow in arterial bifurcation with stenosis under the effect of heat transfer. Hypothermia or hyperthermia is widely used for many purposes, such as open-heart surgeries and cancer treatment. The temperature is also substantially critical. Here, the numerical source code for the solution of Newtonian blood flow in arterial bifurcation will be established. The establishment of a numerical library can be used for validation purposes against future experimental and numerical results. This study can be beneficial for analyzing the behavior of temperature distribution inside the artery during hyperthermia and cryosurgery.

1.6 Outline of the Thesis

This thesis contains seven chapters. Chapter 1 contains general introduction of the research background to understand the connection between human blood flow and cardiovascular diseases. Explanation to human blood flow allows us to understand cardiovascular diseases such as heart attacks and strokes. This chapter also highlight problem, statement research objectives, scope, and the significance of the study. The literature review of the interesting problems is elaborated and provided in Chapter 2. It consists of discussions of some basic rheology of blood, heat transfer, and types of the stenosed artery, particularly with the location of stenoses. The achievements of researchers of all existing problems in blood flow, as well as the method used to accomplish their study are presented. The finite element method is implemented, as a solving method for the proposed problem. The fundamental steps of using the finite element method are provided in Chapter 3. Triangular Taylor-Hood element is proposed in this chapter where the domain with the shape of triangular or rectangular is discretized to solve the nonlinear equation by applying the iteration manner. Subsequently, the computer implementation of the finite element method has been explored in this chapter as well. Chapter 4 will provide basic knowledge of how to create geometry in COMSOL Multiphysics 5.2. Then, the procedure is continued by collecting the nodes from the constructed geometry from COMSOL and transferred into MATLAB.

The investigation on the effect of different morphologies of the stenosed bifurcated artery with heat transfer is presented in Chapter 5. The finite element method is validated with the integrated software COMSOL Multiphysics 5.2 and previous works for the axial velocity over the specific location of the artery. The alteration of the fluid flow inside different artery geometry with involving parameters, such as Reynold number, Prandtl number and occlusion of stenosis as well as Nusselt number, are explored and discussed. The blood flow characteristics, such as velocity, streamlines, wall shear stress, temperature and pressure drop are scrutinized in this chapter. Chapter 6, the last chapter, consists of a summary of the study and several suggestions for future work.

REFERENCES

- Abdullah, I., and Amin, N. (2010) 'A micropolar fluid model of blood flow through a tapered artery with a stenosis', *Mathematical Methods in the Applied Sciences*, 33(16), 1910–1923.
- Achaba, L., Mahfouda, M., and Benhadida, S. (2016) 'Numerical study of the non-Newtonian blood flow in a stenosed artery using two rheological models', *Thermal Science*, 20(2), 449-460.
- Alimohamadi, H., Imani, M. and Forouzandeh, B. (2015) 'Computational analysis of transient non-newtonian blood flow in magnetic targeting drug delivery in stenosed carotid bifurcation artery', *International Journal of Fluid Mechanics Research*, 42(2), 149–169.
- Argyris, J. H., and Scharpf, D. W. (1970) 'Finite element formulation of the incompressible lubrication problem', *Nuclear Engineering and Design*, 11(2), 225-229.
- Audaa, K., and Ph, J. (2018) 'Numerical study of Blood Hemodynamic and Heat Transfer in Catheterized Multiple Stenosis Artery', Association of Arab Universities Journal of Engineering Sciences 25(5), 302–323.
- Bakheet, A., Alnussaiyri, E. A., Ismail, Z., and Amin, N. (2016) 'Blood flow through an inclined stenosed artery', *Applied Mathematical Sciences*, 5(10), 235–254.
- Barozzi, G. S., and Dumas, A. (1991) 'Convective heat transfer coefficients in the circulation', *Journal of Biomechanical Engineering*, 113(3), 308–313.
- Basri, A. A., Khader, S. M. A., Johny, C., Pai, R., Zuber, M., Ahmad, K. A., and Ahmad, Z. (2018) 'Numerical study of haemodynamics behaviour in normal and single stenosed renal artery using fluid - structure interaction', *Journal of Advanced Research in Fluid Mechanics and Thermal Sciences*, 51(1), 91–98.
- Bertolotti, C. and Deplano, V. (2000) 'Three-dimensional numerical simulations of flow through a stenosed coronary bypass', *Journal of Biomechanics*, 8(33), 1011–1022.
- Bessonov, N., Sequeira, A., Simakov, S., Vassilevskii, Y., and Volpert, V. (2016) 'Methods of blood flow modelling', *Mathematical Modelling of Natural Phenomena*, 11(1), 1–25.
- Bose, S. and Banerjee, M. (2015) 'Magnetic particle capture for biomagnetic fluid flow

in stenosed aortic bifurcation considering particle–fluid coupling', *Journal of Magnetism and Magnetic Materials*, 385(2015), 32–46.

- Caro, C.G., Pedley, T.J., Schroter, R.C., and S. W. A. (1978) 'The Mechanics of the Circulation. *Oxford University Press*.
- Chakravarty, S. and Mandal, P. K. (1994) 'Mathematical modelling of blood flow through an overlapping arterial stenosis', *Mathematical and Computer Modelling*, 19(1), 59–70.
- Chakravarty, S., and Sen, S. (2005) 'Dynamic response of heat and mass transfer in blood flow through stenosed bifurcated arteries', *Korea Australia Rheology Journal*, *17*(2), 47–62.
- Chato, J. C. (1980) 'Heat Transfer to Blood Vessels', *Journal of Biomechanical* Engineering, 102(2), 110–118.
- Chinyoka, T., and Makinde, O. D. (2014) 'Computational Dynamics of Arterial Blood Flow in the Presence of Magnetic Field and Thermal Radiation Therapy', *Advances in Mathematical Physics*, 2014, 1-9.
- Clough, R. W. (1960) 'The finite element method in plane stress analysis', *Proceedings* of 2nd ASCE Conference on Electronic Computation, Pittsburgh Pa.
- Consiglieri, L., dos Santos, I., and Haemmerich, D. (2003) 'Theoretical analysis of the heat convection coefficient in large vessels and the significance for thermal ablative therapies', *Physics in Medicine & Biology*, 24(48), 4125.
- Craciunescu, O. I., and Clegg, S. T. (2001) 'Pulsatile blood flow effects on temperature distribution and heat transfer in rigid vessels', J. Biomechanical. Eng., 123(5), 500-505.
- Darren, E. (2014). Locally Optimal Delaunay-refinement and Optimisation-based Mesh Generation. Doctor of Philosophy, School of Mathematics and Statistics, The University of Sydney.
- Davies, A. J. (2011). The Finite Element Method. (2). New York: Oxford University Press.
- Dennis B. H. (2000). Simulation and Optimization of electomagnetohydrodynamic flows. Doctor of Philosophy, School of Mathematics and Statistics, The Pennsylvania State University.
- Erwan, H. K. (2012) Mixed formulations for Navier Stokes equations with magnetic effect in rectangular channel. Master of Engineering, Civil Engineering, Universiti Teknologi Malaysia.

- Erturk, E., Corke, T. C., and Gokcol, C. (2005) 'Numerical solutions of 2-D steady incompressible driven cavity flow at high Reynolds numbers'. *International Journal for Numerical Methods in Fluids*, 48, 747-774.
- Friedman, M. H., O'Brien, V., and Ehrlich, L. W. (1975), 'Calculations of pulsatile flow through a branch: implications for the hemodynamics of atherogenesis', *Circulation Research*, 36(2), 277–285.
- Ghia, U., Ghia, K. N., and Shin, C. T. (1982) 'High-Re solutions for incompressible flow using the Navier-Stokes equations and a multigrid method', *Journal of Computational Physics*, 48, 387-411.
- Gray, W. H., and Schnurr, N. M. (. (1975) 'A comparison of the finite element and finite difference methods for the analysis of steady two dimensional heat conduction problems', *Computer Methods in Applied Mechanics and Engineering*, 6(2), 243–245.
- Huh, H. K., Ha, H. and Lee, S. J. (2015) 'Effect of non-Newtonian viscosity on the fluid-dynamic characteristics in stenotic vessels', *Experiments in Fluids*, 56(8), 1–12.
- Iakovou, I., Ge, L., and Colombo, A. (2005) 'Contemporary stent treatment of coronary bifurcations', *Journal of the American College of Cardiology*, *46*(8), 1446–1455.
- Ikbal, A., Chakravarty, S., Wong, K. K. L., Mazumdar, J., and Mandal, P. K. (2009) 'Journal of Computational and Applied Unsteady response of non-Newtonian blood flow through a stenosed artery in magnetic field', *Journal of Computational* and Applied Mathematics, 230(1), 243–259.
- Jahangiri, M., Saghafian, M. and Sadeghi, M. R. (2015) 'Numerical study of turbulent pulsatile blood flow through stenosed artery using fluid-solid interaction', *Computational and Mathematical Methods in Medicine*, 2015(51561), 1–10.
- Jamali, M. S. A., and Ismail, Z. (2019) 'Simulation of heat transfer on blood flow through a stenosed bifurcated artery', *Journal of Advanced Research in Fluid Mechanics and Thermal Sciences*, 60(2).
- Kefayati, S., Holdsworth, D. W., and Poepping, T. L. (2014) 'Turbulence intensity measurements using particle image velocimetry in diseased carotid artery models: Effect of stenosis severity, plaque eccentricity, and ulceration', *Journal of Biomechanics*, 47(1), 253–263.

Ku, D. N. (1974). 'Blood flow in arteries', Annual Review of Fluid Mechanics, 29(1).

Kumar, D., Vinoth, R., and Raviraj Adhikari, V. S. (2017) 'Non-Newtonian and

Newtonian blood flow in human aorta: a transient analysis', *Biomedical Research*, 28(7), 3194–3203.

- Ledesma, J. M., Riahi, D. N., & Roy, R. (2013) 'Two-Phase Flow In A Catheterized Artery With Atherosclerosis', *Journal of Theoretical and Applied Mechanics*. 5(2), 409–418.
- Lefèvre, Thierry, Yves Louvard, Marie-Claude Morice, Pierre Dumas, Christophe Loubeyre, Abdeljabbar Benslimane, Rajendra Kumar Premchand, Niels Guillard, and J. P. (2000) 'Stenting of bifurcation lesions: classification, treatments, and results', *Catheterization and Cardiovascular Interventions*, 49(2), 274-283.
- Lewis, R. W., Nithiarasu, P., and Seetharamu, K. (2008) 'Fundamentals of the Finite Element Method for Heat and Fluid Flow', Wiley.
- Frey, P. J., and George, P. L. (2008) 'Mesh Generation', US, John Wiley & Sons, Inc.
- Li, J., and Huang, H. (2010) 'Effect Of Magnetic Field On Blood Flow And Heat Transfer Through A Stenosed Artery', *Bmei*, 2028–2032.
- Lin, W.L., Yen, J.Y., Chen, Y.Y., Jin, K.W., and Shieh, M. J. (1999) 'Relationship Between Acoustic Aperture Size and Tumor Conditions for External Ultrasound Hyperthermia' *Medical Physics*, 26(5), 818–824.
- Lim, Y.J., (2017). Finite Element Method For Fluid Flow Of Modelling Of The Descemet Membrane Detachment And Rhematogeneous Retinal Detachment. Doctor of Philosophy, Universit Teknologi Malaysia.
- Lou, Z. and Yang, W. –J. (1993) 'A computer simulation of the non-Newtonian blood flow at the aortic bifurcation', *J. Biomechanics*, *26*(1), 37–49.
- Mahmood, R., Sajid, M., and Nadeem, A. (2011) 'Finite element solution for heat transfer flow of a third order fluid between parallel plates', *Advanced Studies in Theoretical Physics*, 5(3), 107–120.
- Mekheimer, K. S., and El Kot, M. A. (2015) 'Suspension model for blood flow through catheterized curved artery with time-variant overlapping stenosis', *Engineering Science and Technology, an International Journal*, 3(18), 452–462.
- Misra, J. C., and Pal, B. (1990). A mathematical model for the study of the pulsatile flow of blood under an externally imposed body acceleration. *Mathematical and Computer Modelling*, 1(29), 89–106.
- Mozaffarian, D., Benjamin, E. J., Go, A. S., Arnett, D. K., Blaha, M. J., C., & M., and Howard, V. J. (2015). Heart Disease and Stroke Statistics—2016 Update A Report from the American Heart Association. *Circulation, CIR-131(4.*

- Mu, L., Wang, J., and Ye, X. (2014). A stable numerical algorithm for the Brinkman equations by weak Galerkin finite element methods. *Journal of Computational Physics*, 0(273), 327–342.
- Nadeem, S., Akbar, N.S., Hayat, T., and Hendi, A.A. (2012) 'Influence of Heat and Mass Transfer on Newtonian Biomagnetic Fluid of Blood Flow Through a Tapered Porous Arteries with a Stenosis', *Transport in Porous Media*, 91(1), 81– 100.
- Ogulu, A., and Abbey, T. M. (2005). 'Simulation of heat transfer on an oscillatory blood flow in an indented porous artery', *International Communications in Heat and Mass Transfer*, *32*(7), 983–989.
- Papafaklis, M. I. and Lampros, K. M. (2012). 'Intravascular Imaging and Haemodynamics: The Role of Shear Stress in Atherosclerosis and In-Stent Restenosis, in Intravascular Imaging. In: Tsakanikas, V. D., Michalis, L. K., Fotiadis, D. I., Naka, K. K. and Bourantas, C. V. (Ed.)', *Current Applications and Research Developments*, (pp. 326-348). Hershey, PA, USA: IGI Global.
- Pedley, T. J. (1980). *The Fluid Mechanics of Large Blood Vessels*. Cambridge University Press.
- Rabby, M. G., Shupti, S. P., and Molla, M. (2014) 'Pulsatile Non-Newtonian Laminar Blood Flows through Arterial Double Stenoses', *Journal of Fluids*, (757902), 1– 13.
- Rahbari, A., Fakour, M., Hamzehnezhad, A., Vakilabadi, M. A., and Ganji, D. D. (2017) 'Heat transfer and fluid flow of blood with nanoparticles through porous vessels in a magnetic field: A quasi-one dimensional analytical approach', *Mathematical Biosciences*, (283), 38–47.
- Rajesh, V., Bég, O. A., and Mallesh, M. P. (2016) 'Transient nanofluid flow and heat transfer from a moving vertical cylinder in the presence of thermal radiation: Numerical study', *Proceedings of the Institution of Mechanical Engineers, Part N: Journal of Nanomaterials, Nanoengineering and Nanosystems*, 230(1), 3–16.
- Riahi, D. N., Roy, R. and Cavazos, S. (2011) 'On arterial blood flow in the presence of an overlapping stenosis', *Mathematical and Computer Modelling*, 54(11–12), 2999-3006.
- Riahi, D. N., & Garcia, A. E. (2014). 'Blood Flow in an Artery with Multi Stenosis', Mathematics and Computers in Biology and Biomedical Informatics, 45–48.
- Roy, M., Sikarwar, B. S., Bhandwal, M., and Ranjan, P. (2017) 'Modelling of blood

flow in stenosed arteries', Procedia Computer Science, 115(2), 821-830.

- Singh, A. K. (2012). 'Effects of Shape Parameter and Length of Stenosis on Blood Flow through Improved Generalized Artery with Multiple Stenoses', *Advances in Applied Mathematical Biosciences* 3(1), 41–48.
- Sinha, A., Misra, J. C., and Shit, G. C. (2016) 'Effect of heat transfer on unsteady MHD flow of blood in a permeable vessel in the presence of non-uniform heat source', *Alexandria Engineering Journal*, 55(3), 2023–2033.
- Srikanth, D., Reddy, J. R., Jain, S., and Kale, A. (2015) 'Unsteady polar fluid model of blood flow through tapered ω-shape stenosed artery: Effects of catheter and velocity slip', *Ain Shams Engineering Journal*, *3*(6), 1093–1104.
- Srinivasacharya, D. and Rao, G. M. (2017) 'Micropolar fluid flow through a stenosed bifurcated artery', *Nonlinear Analysis : Modelling and Control*, 22(2), 147–159.
- Srivastava, V. P. and Rastogi, R. (2010) 'Blood flow through a stenosed catheterized artery : Effects of hematocrit and stenosis shape', *Computers & Mathematics with Applications*, 59(4), 1377–1385.
- Srivastava, N. (2018) 'Herschel-Bulkley Magnetized Blood Flow Model for an Inclined Tapered Artery for an Accelerated Body', *Journal of Science and Technology*, 10(1), 53–59.
- Stroud, J. S., Berger, S. A. and Saloner, D. (2002) 'Numerical analysis of flow through a severely stenotic carotid artery bifurcation', *Journal of Biomechanical Engineering*, 24(1), 9–20.
- Sváček, P., Louda, P., and Kozel, K. (2014) 'On numerical simulation of threedimensional flow problems by finite element and finite volume techniques', *Journal of Computational and Applied Mathematics*, (270), 451–461.
- Taylor, C., and Hood, P. (1973) 'A numerical solution of the Navier-Stokes equations using the finite element technique', *Computers & Fluids* 1(1),73-100.
- Tang L. Q., Tsang T. H., (1993) ' A least squres finite element method for time dependent incompressible flows with thermal convection', *International Journal for Numerical Methods in fluidS*, 17, 271-289.
- Tungjitkusolmun, S., Staelin, S. T., Haemmerich, D., Tsai, J. Z., Cao, H., Webster, J. G., and Vorperian, V. R. (2002) 'Three-dimensional finite-element analyses for radio-frequency hepatic tumor ablation', *IEEE Transactions on Biomedical Engineering*, 49(1), 3–9.

- Varshney, G., Katiyar, V.K., and Kumar, S. (2010) 'Numerical Modeling of Pulsatile Flow of Blood through a Stenosed Tapered Artery under Periodic Body Acceleration', *Journal of Mechanics in Medicine and Biology*, 10(2), 251–272.
- Victor, S. A., and Shah, V. L. (1976) 'Steady state heat transfer to blood flowing in the entrance region of a tube', *International Journal of Heat and Mass Transfer*,19(7), 777–783.
- Weddell, J. C., Kwack, J. H., Imoukhuede, P. I. and Masud, A. (2015) 'Hemodynamic analysis in an idealized artery tree: differences in wall shear stress between Newtonian and non-Newtonian blood models', *PLos ONE*, 19(4), 1–23.
- Young, D. F. (1968) 'Effects of a Time-Dependent Stenosis of Flow through a Tube', Journal of Engineering and Industrial, 90(2), 248–254.
- Zain, N. M., and Ismail, Z. (2017) 'Modelling of Newtonian blood flow through a bifurcated artery with the presence of an overlapping stenosis', *Malaysian Journal* of Fundamental and Applied Sciences, 13(2017). 304–309.
- Zain, N. M., and Ismail, Z. (2019) 'Hartmann and Reynolds Numbers Effects in the Newtonian Blood Flow of a Bifurcated Artery with an Overlapping Stenosis', *MATEMATIKA*, 35(2), 213–227.
- Zaman, A., Ali, N., Bég, O. A., and Sajid, M. (2016) 'International Journal of Heat and Mass Transfer Heat and mass transfer to blood flowing through a tapered overlapping stenosed artery', *International Journal of Heat and Mass Transfer*, 95(2016), 1084–1095.
- Zaman, A., Ali, N., Sajid, M., & Hayat, T. (2015) 'Effects of unsteadiness and non-Newtonian rheology on blood flow through a tapered time-variant stenotic artery', *AIP Advances*, 5(3), 1-13
- Zarins, C. K., Giddens, D. P., Bharadvaj, B. K., Sottiurai, V. S., Mabon, R. F. and, and Glagov, S. (2015) 'Carotid bifurcation atherosclerosis quantitative correlation of plaque localization with flow velocity profiles and wall shear stress', *Journal of the American Heart Association*, 53(4), 502–514.

LIST OF PUBLICATIONS AND PAPERS PRESENTED

The findings from this research have been published or presented in conferences as listed below:

Published Papers and Proceedings in Conference

- Jamali, M. S. A., and Ismail, Z. (2019) 'Simulation of Heat Transfer on Blood Flow through a Stenosed Bifurcated Artery', *Journal of Advanced Research in Fluid Mechanics and Thermal Sciences* 60, 2(2019), 310-323.
- Jamali, M. S. A. and Ismail, Z. (2019) 'Generalized Power Law Model of Blood Flow in a Stenosed Bifurcated Artery', *Annals of Mathematical Modeling*, 1(2). Retrieved from <u>https://ejournal.ressi.id/index.php/aam/article/view/26</u>
- Muhammad Sabaruddin Ahmad Jamali, Zuhaila Ismail and Norsarahaida Saidina Amin. 'Heat Transfer of Newtonian Blood Flow in a stenosed Bifurcated Artery', *Proceedings of 6th International Graduate Conference on Engineering, Science and Humanities 2018 (IGCESH 2018).* August 13-15, 2018. Johor Bahru, 598-600.