# MATHEMATICAL ANALYSIS OF DISPERSION OF SOLUTES IN BLOOD FLOW USING HERSCHEL-BULKLEY FLUID MODEL THROUGH AN INCLINED UNIFORM ARTERY

INTAN DIYANA BINTI MUNIR

A dissertation submitted in partial fulfilment of the requirements for the award of the degree of Master of Science

> Faculty of Science Universiti Teknologi Malaysia

> > DECEMBER 2020

# DEDICATION

This dissertation is dedicated to both of my parents, who supported me unconditionally in completing my Master's degree.

### ACKNOWLEDGEMENT

In preparing this dissertation, various challenges have been encountered along the way. Many people have helped me in facing those challenges physically and emotionally. In the academic aspect, I wish to express my sincere appreciation to my main supervisor, Dr Nurul Aini Jaafar, for her persistent guidance and constructive criticism in helping me finish my research. She has been patient with my pace and never stopped encouraging me to keep going. I am also very grateful to my cosupervisor Dr Mohammad Faisal Mohd Basir for his continuous supervision and motivational support. Their time and effort spent on helping me have led me to achieve my best possible thesis outcome.

Not to mention my family members who kept pushing me forward when I was having a hard time staying motivated. Their optimistic attitude has thought me to be more resilient in enduring hardship. My fellow friends and acquaintances should also be recognised for their support.

#### ABSTRACT

This study aims to analyse the effect of inclination of the artery on the blood velocity and solute dispersion in an artery when it is inclined to a certain angle. Herschel-Bulkley fluid model is considered in representing the blood flow. The method of integration and perturbation are used to obtain the solution for the velocity of the steady and unsteady blood flow, respectively. The steady convection-diffusion equation is solved for the concentration of the solute using method of integration. Taylor-Aris method has been implemented to obtain the effective and relative axial diffusion. This present work focuses on the effect of arterial inclination angle on the blood flow characteristic in terms of velocity, concentration of solute, effective axial diffusion and relative axial diffusion. Other parameters' effect such as yield stress, gravitational acceleration and power-law index on the behaviour of the blood are also investigated and presented by graph representation. Observation shows that the angle of artery inclination directly influences the gravitational acceleration parameter, which correlates to the resulting blood velocity and solute concentration. 90° and 270° angles of inclination have the highest effect in increasing and decreasing the velocity, concentration of solute and diffusivity, respectively. Meanwhile, 0°, 180° and 360° angles eliminate the gravitational acceleration effect on the blood behaviour and dispersion process. This study concludes that the angle of inclination has a strong impact on blood flow and solute dispersion behaviour.

### ABSTRAK

Kajian ini adalah bertujuan untuk menganalisis kesan kecenderungan arteri pada halaju darah dan penyebaran zat terlarut dalam arteri apabila arteri tersebut cenderung pada sudut-sudut tertentu. Model bendalir Herschel-Bulkley digunakan bagi mewakili aliran darah. Kaedah pengamiran dan usikan, masing-masing digunakan untuk mendapatkan penyelesaian bagi halaju aliran darah yang stabil dan tidak stabil. Persamaan perolakan-penyebaran yang stabil diselesaikan untuk mendapatkan solusi bagi kepekatan zat terlarut menggunakan kaedah pengamiran. Kaedah Taylor-Aris telah digunapakai untuk mendapatkan kemeresapan paksi efektif dan relatif. Kajian ini memberi tumpuan kepada pengaruh sudut kecenderungan arteri pada tingkah laku aliran darah dari segi halaju, kepekatan zat terlarut, kemeresapan paksi efektif dan kemeresapan paksi relatif. Kesan parameter lain seperti tekanan hasil, pecutan graviti dan indeks hukum-kuasa pada tingkah laku bendalir juga disiasat dan dianalisa melalui graf. Pemerhatian menunjukkan bahawa sudut kecenderungan arteri secara langsung mempengaruhi parameter pecutan graviti yang berkorelasi dengan halaju darah dan kepekatan zat terlarut yang dihasilkan. Sudut kecenderungan 90° dan 270° mempunyai kesan tertinggi dalam meningkatkan dan menurunkan halaju, kepekatan zat terlarut dan penyerapan. Sementara itu, sudut kecenderungan 0°, 180° dan 360° menghilangkan kesan pecutan graviti pada tingkah laku aliran darah dan tingkah laku penyebaran zat terlarut. Kajian ini menyimpulkan bahawa sudut kecenderungan mempunyai kesan yang kuat terhadap aliran darah dan tingkah laku penyebaran zat terlarut.

### TABLE OF CONTENTS

### TITLE

]	DECLARATION				
]	DEDICATION				
	ACKNOWLEDGEMENT				
	ABST	RACT	vi		
	ABST	RAK	vii		
,	TABL	E OF CONTENTS	viii		
]	LIST (	OF TABLES	xii		
]	LIST (	OF FIGURES	xiii		
]	LIST (	<b>OF ABBREVIATIONS</b>	xvii		
]	LIST (	OF SYMBOLS	xviii		
]	LIST (	OF APPENDICES	xxi		
CHAPTER	. 1	INTRODUCTION	1		
	1.1	Introduction	1		
	1.2	Problem Statement	5		
	1.3	Research Objectives			
	1.4	Scope of Study			
	1.5	.5 Significance of Study			
CHAPTER	2	LITERATURE REVIEW	9		
:	2.1	Introduction	9		
:	2.2	Blood Rheology	9		
:	2.3	Dispersion by Means of Diffusion and Convection	10		
:	2.4	Dispersion in Non-Newtonian Fluid	11		
:	2.5	Behaviour of a Non-Newtonian Fluid with Inclination in a Pipe	12		
2	2.6	Regular Perturbation Method in Solving for Unsteady Fluid Flow	14		

2.7 Taylor-Aris Method in Solving for Concentration 15

CHAPTER 3	<b>RESEARCH METHODOLOGY</b>	19	
3.1	Introduction	19	
3.2	Steady Fluid Flow		
	3.2.1 Mathematical Formulation	20	
	3.2.2 Method of Solution	24	
3.3	Unsteady Fluid Flow	37	
	3.3.1 Mathematical Formulation	37	
	3.3.2 Method of Solution	38	
CHAPTER 4	<b>RESULT AND DISCUSSION</b>	53	
4.1	Introduction	53	
4.2	Validation of Velocity, Concentration and Relative Axial Diffusion	54	
	4.2.1 Steady H-B Fluid Flow	54	
4.3	Non-dimensionalized Velocity Distribution for Steady Blood Flow	57	
	4.3.1 Effect of the angle of inclination of the artery on non-dimensionalized steady velocity	57	
	4.3.2 Effect of power-law index on non- dimensionalized steady velocity	59	
	4.3.3 Effect of gravitational acceleration on non- dimensionalized steady velocity	60	
	4.3.4 Effect of core flow radius on non- dimensionalized steady velocity	61	
4.4	Non-dimensionalized Concentration of Solute Distribution for Steady Blood Flow	62	
	4.4.1 Effect of the angle of inclination of the artery on the non-dimensionalized concentration of solute	62	
	4.4.2 Effect of power-law index on the non- dimensionalized concentration of solute	63	
	4.4.3 Effect of gravitational acceleration on the non- dimensionalized concentration of solute	64	
	4.4.4 Effect of core flow radius on the non- dimensionalized concentration of solute	65	
4.5	Effective Axial Diffusion Distribution for Steady Blood Flow	66	

	4.5.1	Effect of the angle of inclination of the artery on the effective axial diffusion	66
	4.5.2	Effect of power-law index on the effective axial diffusion	67
	4.5.3	Effect of gravitational acceleration on the effective axial diffusion	68
4.6	Relati Flow	ve Axial Diffusion Distribution for Steady Blood	69
	4.6.1	Effect of the angle of inclination of the artery on the relative axial diffusion	69
	4.6.2	Effect of power-law index on the relative axial diffusion	71
4.7	Non-d Unstea	limensionalized Velocity Distribution for ady Blood Flow	72
	4.7.1	Effect of the angle of inclination of the artery on non-dimensionalized unsteady velocity	72
	4.7.2	Effect of power-law index on non- dimensionalized unsteady velocity	74
	4.7.3	Effect of gravitational acceleration on non- dimensionalized unsteady velocity	74
	4.7.4	Effect of core flow radius on non- dimensionalized unsteady velocity	75
	4.7.5	Effect of time on non-dimensionalized unsteady velocity	76
4.8	Conce Blood	entration of Solute Distribution for Unsteady Flow	78
	4.8.1	Effect of the angle of inclination of the artery on the non-dimensionalized concentration of solute	78
	4.8.2	Effect of power-law index on the non- dimensionalized concentration of solute	80
	4.8.3	Effect of gravitational acceleration on the non- dimensionalized concentration of solute	81
	4.8.4	Effect of core flow radius on the non- dimensionalized concentration of solute	81
	4.8.5	Effect of time on the non-dimensionalized concentration of solute	82
4.9	Effect Blood	ive Axial Diffusion Distribution for Unsteady Flow	84

		4.9.1	Effect of the angle of inclination of the artery on the effective axial diffusion	84
		4.9.2	Effect of power-law index on the effective axial diffusion	85
	4.10	Physic	ological Application	86
СНАРТЕ	R 5	CON	CLUSION AND RECOMMENDATIONS	89
	N J	COIN		00
	5.1	Resea	rch Outcomes	89
	5.2	Future	e Works	90
REFERE	NCES			91
APPEND	ICES			96

# LIST OF TABLES

TABLE NO.	TITLE	PAGE
Table 4.1	Effect of time parameter effect on the velocity profile increment at $\theta = 0^{\circ}$ , 90°, 270°.	77
Table 4.2	Radius of various blood vessels (Das & Saha, 2009).	86
Table 4.3	Effective axial diffusion of solute inside different types of blood vessels.	87

### LIST OF FIGURES

FIGURE NO	. TITLE	PAGE
Figure 1.1	(a) Arteries in the circulatory system and (b) the direction of blood flow inside the heart (Huttunen et al., 2019).	2
Figure 1.2	Normal artery and narrowed artery (Hui, n.d.).	3
Figure 2.1	Microscopic image of the blood smear (Hegde et al., 2018).	9
Figure 3.1	Schematic diagram of steady Herschel-Bulkley fluid flow inside an inclined pipe.	20
Figure 4.1	Comparison of non-dimensionalized velocity of Herschel-Bulkley fluid with a power-law index of $m = 1.05$ and core flow radius of $r_c = 0.04$ with the existing result of non-dimensionalized velocity from Jaafar et al. (2017) with similar parameter values.	55
Figure 4.2	Comparison of solute concentration in Herschel-Bulkley fluid with power-law index of $m = 1.05$ , artery radius $\bar{a} = 1$ and core flow radius of $\bar{r}_c = 0.04$ with the existing result from Jaafar et al. (2017) with similar parameter values.	56
Figure 4.3	Comparison of relative axial diffusion of Herschel-Bulkley fluid with power-law index of $m = 0.95$ with the existing result from Jaafar et al. (2017) with similar parameter values.	57
Figure 4.4	Variation of non-dimensionalized velocity of Herschel- Bulkley fluid with fixed values of $m = 1.05$ , $g = 10$ , $r_c = 0.04$ and different values of $\theta$ (a) $\theta = 0^\circ$ , 45°, 90° (b) $\theta = 135^\circ$ , 180°, 225° (c) $\theta = 270^\circ$ , 315°, 360°.	58
Figure 4.5	Variation of non-dimensionalized velocity of Herschel- Bulkley fluid with fixed values of $g = 10$ , $r_c = 0.04$ with different values of $m = 0.95$ , 1, 1.05 at an inclination of $\theta = 0^\circ$ , 90°, 270°.	59
Figure 4.6	Variation of non-dimensionalized velocity of Herschel- Bulkley fluid with fixed values of $m = 1.05$ , $r_c = 0.04$ and different values of $g = 10$ , 15, 20 at an inclination of	
	$\theta = 0^{\circ}, 90^{\circ}, 270^{\circ}.$	60

Figure 4.7	Variation of non-dimensionalized velocity of Herschel- Bulkley fluid with fixed values of $m = 1.05$ , $g = 10$ and different values of $r_c = 0, 0.05, 0.1, 0.15, 0.2$ at an inclination of $\theta = 0^\circ$ , $90^\circ$ , $270^\circ$ .	61
Figure 4.8	Variation of non-dimensionalized concentration in Herschel-Bulkley fluid with fixed values of $m = 0.95$ , $g = 10$ , $r_c = 0.04$ and different values of $\theta$ (a) $\theta = 0^\circ$ , 45°, 90° (b) $\theta = 135^\circ$ , 180°, 225° (c) $\theta = 270^\circ$ , 315°, 360°.	63
Figure 4.9	Variation of non-dimensionalized concentration in Herschel-Bulkley fluid with fixed values of $g = 10$ , $r_c = 0.04$ with different values of $m = 0.95$ , 1, 1.05 at an inclination of $\theta = 0^\circ$ , 90°, 270°.	64
Figure 4.10	Variation of non-dimensionalized concentration in Herschel-Bulkley fluid with fixed values of $m = 0.95$ , $r_c = 0.04$ and different values of $g = 10$ , 15, 20 at an inclination of $\theta = 0^\circ$ , 90°, 270°.	65
Figure 4.11	Variation of non-dimensionalized concentration in Herschel-Bulkley fluid with fixed values of $m = 0.95$ , $g = 10$ and different values of $r_c = 0.05$ , 0.1, 0.15, 0.2 at an inclination of $\theta = 0^\circ$ , 90°, 270°.	66
Figure 4.12	Variation of effective axial diffusion in Herschel-Bulkley fluid with fixed values of $m = 0.95$ , $g = 10$ and different values of $\theta$ (a) $\theta = 0^{\circ}$ , 45°, 90° (b) $\theta = 135^{\circ}$ , 180°, 225° (c) $\theta = 270^{\circ}$ , 315°, 360°.	67
Figure 4.13	Variation of effective axial diffusion in Herschel-Bulkley fluid with fixed value of $g = 10$ with different values of $m = 0.95$ , 1, 1.05 at an inclination of $\theta = 0^{\circ}$ , 90°, 270°.	68
Figure 4.14	Variation of effective axial diffusion in Herschel-Bulkley fluid with a fixed value of $m = 0.95$ and different values of $g = 10$ , 15, 20 at an inclination of $\theta = 0^\circ$ , 90°, 270°.	69
Figure 4.15	Variation of relative axial diffusion in Herschel-Bulkley fluid with fixed values of $m = 1.05$ , $g = 10$ and different values of $\theta$ (a) $\theta = 0^{\circ}$ , 45°, 90° (b) $\theta = 135^{\circ}$ , 180°, 225° (c) $\theta = 270^{\circ}$ , 315°, 360°.	71
Figure 4.16	Variation of relative axial diffusion in Herschel-Bulkley fluid with a fixed value of $g = 10$ with different values of $m = 0.95$ , 1, 1.05 at an inclination of $\theta = 0^{\circ}$ , 90°, 270°.	72

Figure 4.17	Variation of non-dimensionalized velocity of unsteady Herschel-Bulkley fluid with fixed values of $m = 1.05$ , $g = 10$ , $t = 1$ , $r_c = 0.04$ and different values of $\theta$ (a) $\theta = 0^{\circ}$ , 45°, 90° (b) $\theta = 135^{\circ}$ , 180°, 225° (c) $\theta = 270^{\circ}$ , 315°, 360°.	73
Figure 4.18	Variation of non-dimensionalized velocity of unsteady Herschel-Bulkley fluid with fixed values of $g = 10$ , $t = 1$ , $r_c = 0.04$ with different values of $m = 0.95$ , 1, 1.05 at an inclination of $\theta = 0^\circ$ , 90°, 270°.	74
Figure 4.19	Variation of non-dimensionalized velocity of unsteady Herschel-Bulkley fluid with fixed values of $m = 1.05$ , $t = 1$ , $r_c = 0.04$ and different values of $g = 10$ , 15, 20 at an inclination of $\theta = 0^\circ$ , 90°, 270°.	75
Figure 4.20	Variation of non-dimensionalized velocity of unsteady Herschel-Bulkley fluid with fixed values of $m = 1.05$ , $g = 10$ , $t = 1$ and different values of $r_c = 0$ , 0.05, 0.1, 0.15, 0.2 at an inclination of $\theta = 0^\circ$ , 90°, 270°.	76
Figure 4.21	Variation of non-dimensionalized velocity of unsteady Herschel-Bulkley fluid with fixed values of $m = 1.05$ , $g = 10$ , $r_c = 0.04$ and different values of $t = 0.1$ , 0.2, 0.5, 1, 2 and $\theta$ (a) $\theta = 0^\circ$ (b) $\theta = 90^\circ$ (c) $\theta = 270^\circ$ .	78
Figure 4.22	Variation of non-dimensionalized concentration in unsteady Herschel-Bulkley fluid with a fixed value of $m = 0.95$ , $g = 10$ , $t = 1$ , $r_c = 0.04$ and different values of $\theta$ (a) $\theta = 0^\circ$ , 45°, 90° (b) $\theta = 135^\circ$ , 180°, 225° (c) $\theta = 270^\circ$ , 315°, 360°.	79
Figure 4.23	Variation of non-dimensionalized concentration in unsteady Herschel-Bulkley fluid with a fixed value of $g = 10$ , $t = 1$ , $r_c = 0.04$ with different values of $m = 0.95$ , 1, 1.05 at an inclination of $\theta = 0^\circ$ , $90^\circ$ , $270^\circ$ .	80
Figure 4.24	Variation of non-dimensionalized concentration in unsteady Herschel-Bulkley fluid with a fixed value of $m = 0.95$ , $t = 1$ , $r_c = 0.04$ and different values of $g = 10$ , 15, 20 at an inclination of $\theta = 0^\circ$ , 90°, 270°.	81
Figure 4.25	Variation of non-dimensionalized concentration in Herschel-Bulkley fluid with a fixed value of $m = 0.95$ , $g = 10$ , $t = 1$ and different values of $r_c = 0.05$ , 0.1, 0.15, 0.2 at an inclination of $\theta = 0^\circ$ , 90°, 270°.	82

Figure 4.26	Variation of non-dimensionalized concentration in unsteady Herschel-Bulkley fluid with a fixed value of $m = 1.05$ , $g = 10$ , $r_c = 0.04$ and different values of $t = 0.5$ ,	
	1, 2, 10 and $\theta$ (a) $\theta = 0^{\circ}$ (b) $\theta = 90^{\circ}$ (c) $\theta = 270^{\circ}$ .	83
Figure 4.27	Variation of effective axial diffusion in unsteady Herschel- Bulkley fluid with a fixed value of $m = 0.95$ , $g = 10$ , $t = 1$ and different values of $\theta$ (a) $\theta = 0^{\circ}$ , $45^{\circ}$ , $90^{\circ}$ (b)	05
	$\theta = 135^{\circ}, 100^{\circ}, 225^{\circ}$ (c) $\theta = 2/0^{\circ}, 315^{\circ}, 360^{\circ}$ .	85

86

Figure 4.28 Variation of effective axial diffusion in unsteady Herschel-Bulkley fluid with a fixed value of g = 10, t = 1 with different values of m = 0.95, 1, 1.05 at an inclination of  $\theta = 0^{\circ}, 90^{\circ}, 270^{\circ}.$ 

# LIST OF ABBREVIATIONS

H-B	-	Herschel-Bulkley
LHS	-	Left-hand side
MHD	-	Magnetohydrodynamics
PDE	-	Partial differential equation
RBC	-	Red blood cell
RHS	-	Right-hand side
UTM	-	Universiti Teknologi Malaysia

# LIST OF SYMBOLS

ā	-	Radius of artery
С	-	Constant of integration
$ar{C}_1$	-	Solute concentration in the core flow region
$C_1$	-	Non-dimensionalized solute concentration in the
		core flow region
$ar{C}_2$	-	Solute concentration in the outer flow region
$C_2$	-	Non-dimensionalized solute concentration in the
		outer flow region
$ar{C}_{c}$	-	Solute concentration in the core flow region
		where the core region is evaluated at $\overline{r} = \overline{r_c}$
$C_c$	-	Non-dimensionalized solute concentration in the
		core flow region where the core region is
		evaluated at $r = r_c$
$\partial \overline{C} / \partial \overline{z}^*$	-	Concentration gradient
$\partial C / \partial z^*$	-	Non-dimensionalized concentration gradient
$ar{D}_m$	-	Constant molecular diffusion
$D_m$	-	Non-dimensionalized constant molecular
		diffusion
$ar{D}_{e\!f\!f}$	-	Effective axial diffusion
$E(r_c)$	-	Measure of the change in Herschel-Bulkley
		dispersion relative to Newtonian fluid
F	-	Body force of gravity in all directions
$\overline{g}$	-	Gravitational acceleration in the downward
		direction
g	-	Non-dimensionalized gravitational acceleration in
		the downward direction
т	-	Power-law index of Herschel-Bulkley fluid

n	-	Vector normal to the control volume
$\overline{p}$	-	Pressure
р		Non-dimensionalized pressure
Pe	-	Peclet number
$Q_{1}, Q_{2}$	-	Integration of the dispersion flow rate in core and
		outer flow regions for a circular pipe
$\overline{q}$	-	Dispersion flow rate
$\overline{r}$	-	Radius
r	-	Non-dimensionalized radius
$\overline{r_c}$	-	Radius of core flow region
r <sub>c</sub>	-	Non-dimensionalized radius of core flow region
S	-	Surface area
dS		Area of a fixed smooth surface of the control
		volume
t	-	Time
t	-	Non-dimensionalized time
V	-	Control volume
$\overline{w}(\overline{z})$	-	Steady velocity at axial direction
$\overline{w}(\overline{z},\overline{t})$	-	Unsteady velocity at axial direction
<i>W</i> <sub>0</sub>	-	First term of the perturbation series of velocity
<i>w</i> <sub>1</sub>	-	Second term of the perturbation series of velocity
$\overline{w}_{c}$	-	Velocity in the core flow region
W <sub>c</sub>	-	Non-dimensionalized velocity in the core flow
		region
$\overline{W}_{o}$	-	Velocity in the outer flow region
W <sub>o</sub>	-	Non-dimensionalized velocity in the outer flow
		region
$\hat{w}_c$	-	Relative velocity in the core flow region
ŵ <sub>o</sub>	-	Relative velocity in the outer flow region
$\overline{W}_m$	-	Mean velocity
w	-	Vector normal to the control volume

Z	-	Direction of blood flow
Ζ	-	Non-dimensionalized direction of blood flow
$\overline{Z}^*$	-	Axial coordinate
<b>Z</b> <sup>*</sup>	-	Non-dimensionalized axial coordinate
α	-	Reynolds number
$\overline{ heta}$	-	Angle of pipe inclination
θ	-	Non-dimensionalized angle of pipe inclination
$\overline{\mu}$	-	Viscosity of the fluid
$\overline{\mu}_{\!_H}$	-	Viscosity coefficient of the Herschel-Bulkley
		fluid
$\overline{ ho}$	-	Density of the fluid
ρ	-	Non-dimensionalized density of the fluid
$\sigma$	-	Stress and strain tensor
$\overline{ au}$	-	Shear stress
τ	-	Non-dimensionalized shear stress
$ au_0$	-	First term of the perturbation series of shear stress
$ au_1$	-	Second term of the perturbation series of shear
		stress
$\overline{ au}_{y}$	-	Yield stress
$ au_y$	-	Non-dimensionalized yield stress
$\overline{\psi}$	-	Azimuthal angle of pipe cross-sectional area
		normal to the direction of blood flow

### LIST OF APPENDICES

APPENDIX	TITLE	PAGE
Appendix A	Derivation of Continuity and Momentum Equation	96
Appendix B	Gravitational Acceleration in <i>z</i> Direction	103

### **CHAPTER 1**

#### **INTRODUCTION**

### 1.1 Introduction

This chapter discusses the background of study conducted on the problem concerning the solute dispersion, Herschel-Bulkley fluid model and inclination of the artery. The effectiveness of the solute dispersion is affected by several factors, such as the angle of artery inclination, gravitational acceleration, core flow radius and powerlaw index. This study focuses on blood flow and solute dispersion through an inclined narrow artery.

Many studies have been conducted to formulate an equation describing the blood flow and its relation to the factors affecting the blood flow. The most wellknown equation is the Hagen-Poiseuille equation, which considers the viscosity of the fluid, pressure gradient at the constant cross-section of the pipe, length and diameter of the pipe. The equation was derived independently by Jean Léonard Marie Poiseuille in 1838 and continued by Gotthilf Heinrich Ludwig Hagen in 1839 (Sutera & Skalak, 1993). The ability to mathematically approach the behaviour of blood flow gives many contributions to the medical field in which one of those is the theory of dispersion of solute in blood flow. Many researchers and scientists have explored the study of solute dispersion as it contributes to findings and applications in the medical field. The medical field concerning the circulatory system implements the knowledge of solute dispersion in solving problems related to the transport of solute in the blood circulation system. Since the human circulatory system diverse from one patient to another, studies on solute dispersion are still being extended to further explore problems and solutions under various other conditions. For instance, cardiovascular diseases, specifically atherosclerosis (stenosis) which claims the lives of people, make the study of blood flow through arteries significant as it is closely related to the nature of blood movement and the dynamic behaviour of blood vessel (Ratchagar & Kumar, 2019).

Thus, studies on solute dispersion benefit not only the researchers but also the society who depends on these study developments to live a better life.



Figure 1.1 (a) Arteries in the circulatory system and (b) the direction of blood flow inside the heart (Huttunen et al., 2019).

There are many types of arteries inside the human body, as shown in Figure 1.1. Figure 1.1 illustrates the various inclination of the artery as it branches out from the heart to carry the blood to their specific target body and the anatomy of the heart that generates the pressure to pump blood through the artery. Each artery has its own orientation according to their position in the circulatory system. The velocity of the blood flow and solute dispersion inside those arteries are affected by the angle of artery inclination. Furthermore, an inclined artery coupled with a disease such as atherosclerosis leads to the narrowing of the artery that affects drug delivery through the artery. Figure 1.2 shows a normal artery and an artery with atherosclerosis. The artery with atherosclerosis has a narrowed opening caused by the cholesterol deposit that accumulates at the wall of the artery known as stenoses. The blood in a narrowed artery requires a fluid model that can represent its behaviour flowing through a small radius opening. Therefore, studies on the behaviour of blood flow and solute dispersion inside on the behaviour of blood flow and solute dispersion inside an inclined artery that is narrowed by stenoses are deemed to be significant.



Figure 1.2 Normal artery and narrowed artery (Hui, n.d.).

Drugs are commonly administrated through the vein via intravenous injection. However, the practice of administrating drugs through the artery known as the intraarterial injection is sometimes performed for a specific treatment and situation. Administrating drugs intravenously requires knowledge of the dispersion rate of the drug solutes in the blood since many drugs are therapeutic at low concentrations and harmful at high concentrations (Rana & Murthy, 2016). This knowledge also applies to drug administration through the artery, but more caution is needed as the risk of developing complications is higher. Increased risk of complications is due to the nature of the artery having a higher blood pressure compared to the veins and could potentially damage the tissue surrounding it as the drug is injected into the artery. Not to mention, the high blood pressure inside the artery could lead to heavy bleeding when the artery is punctured by the needle. The method of administrating drugs through the artery has a high risk of developing clinical trauma such as paraesthesia, severe pain, motor dysfunction, compartment syndrome, gangrene and limb loss (Sen et al., 2005). Nevertheless, in the event of intravenous cannulation (injection) is impossible and intraosseous access is considered too invasive, cannulation through the artery might be an alternative (Fikkers et al., 2006). Therefore, studies on behaviour of blood flow and solute dispersion inside an inclined artery are vital to reduce the risk of complications from an intra-arterial injection. An extensive study on solute dispersion inside an artery helps doctors and pharmacists in deciding the dose and distribution rate of medication to patients with less risk of causing toxicity and bleeding.

In representing the physiology of blood flowing inside an inclined artery, a circular pipe with various inclination is used to represent the inclined artery and non-Newtonian fluid is used to represent the blood. The primary concern of this study is

the dispersion of solute in blood flow, especially in an inclined pipe as many ducts in a physiological system have some inclination rather than being horizontal (Prasad & Radhakrishnamacharya, 2008). Thus, adding an inclination to the study gives insights on the blood behaviour when gravity is considered.

A vast number of researches have been conducted to study the blood flow and solute dispersion behaviour due to the various type of fluid models being used to represent the blood properties known as Newtonian and non-Newtonian fluids. The viscosity of a Newtonian fluid is independent of the shear rate, while the viscosity of a non-Newtonian fluid is dependent on the shear rate. Blood has a viscosity that decreases with shear stress, and this shear-thinning property is closely related to the dynamics and mutual interactions of red blood cells (Lanotte et al., 2016). Since blood exhibits a shear-thinning property, non-Newtonian fluid sare more suitable to represent the blood in studies involving haemodynamics. Non-Newtonian fluid such as Casson, Carreau, Carreau-Yasuda and Herschel-Bulkley has been proven to be useful in haemodynamics and to be applied in the study of the solute dispersion process in blood flow (Rana & Liao, 2019).

Nevertheless, for a low shear rate of blood flow with high yield stress in a very narrow artery, the Herschel–Bulkley fluid model is more suitable (Sankar & Hemalatha, 2007). An appropriate choice of a parameter for the power-law index of the Herschel-Bulkley fluid model can reduce it to other non-Newtonian fluid models such as power law and Bingham model. Therefore, Herschel-Bulkley fluid model is more fitting to describe the blood property flowing in a narrow artery.

In previous studies, non-Newtonian Herschel-Bulkley fluid is widely used in representing blood when it comes to solving problems related to solute dispersion in blood flow, mainly in small circular channel since blood vessels are relatively small. However, the study on solute dispersion using Herschel-Bulkley fluid in an inclined pipe has not yet been explored. Therefore, this present study focuses on the effect of pipe inclination on the behaviour of the Herschel-Bulkley fluid model and dispersion of solute to extend the study of previous researches and obtain results under different conditions. In this study, the application of fluid mechanics knowledge helps to measure the velocity profile, the concentration of solute, the rate of dispersion and the transport coefficients for the Herchel-Bulkley model in an inclined pipe.

### **1.2 Problem Statement**

Solute dispersion occurs when solutes are injected into a circular pipe containing fluid that is flowing. This can be seen in the medical field when a doctor injects the drug into patients. However, the concentration of the drug being injected must be carefully calculated to avoid overdosing or damage to the blood vessel. Factors such as the velocity of the blood, the radius of the blood vessel and the rate of dispersion of the drugs should be considered in determining the dosage of medicine to be injected. Thus, the study of solute dispersion in a pipe contributes to understanding the dispersion process. Many researchers used the Newtonian fluid in representing the blood in studying its flow in a large diameter artery. However, in a real-life problem, certain artery has a narrow diameter due to underlying medical conditions. Thus, it is significant to study the blood flow in a narrow artery at a low shear rate to give a lifelike description of blood flow. A fluid model of Herschel-Bulkley is used to represent the blood in a narrow diameter artery.

Not to mention, studies that used a horizontal pipe can deviate from a close representation of the real-life situation as blood flowing in the artery is not always or never in a perfect horizontal state. Therefore, the inclination of the pipe has been considered to study the blood flow in the real-life situation.

### **1.3 Research Objectives**

The objectives of this present study are:

(a) To formulate the fluid flow model of the Hershel-Bulkley through an inclined uniform artery.

- (b) To solve the momentum and constitutive equations for finding the velocity using the method of integration for steady blood flow and perturbation method for unsteady blood flow.
- (c) To solve the steady dispersion analytically for finding effective and relative axial diffusion using the Taylor-Aris method.
- (d) To analyse the graphical data of velocity profile, solute concentration, effective axial diffusion and relative axial diffusion at various angles of inclination and under the influence of different values of power-law index, gravitational acceleration and core flow radius.

### 1.4 Scope of Study

The scope of the study is limited to solving for the fluid velocity, solute concentration, effective axial diffusion and relative axial diffusion of steady dispersion of solute in a steady and unsteady, laminar, fully-developed Herschel-Bulkley flow in an inclined pipe. The governing equations are solved analytically for both momentum and convection-diffusion equations. The data of the velocity of Herschel-Bulkley fluid flow, the concentration of solute, the effective axial diffusion and relative axial diffusion are obtained using *Mathematica* software.

### 1.5 Significance of Study

Research on solute dispersion in blood flow through an inclined artery has many benefits in the science field such as medical, pharmaceutical and bioengineering fields. In the medical field, the study on solute dispersion helps doctors in deciding the suitable dosage of medicine to be given to patients. The findings of this present study can also help to depict a realistic description of solute dispersion through an inclined artery for future researchers in extending studies related to circulatory system or cardiovascular diseases. Therefore, the significance of this study are:

- (a) In-depth insight on the flow and dispersion characteristics of the Herschel-Bulkley model in an inclined pipe may help future studies in extending research revolving the Herschel-Bulkley fluid model.
- (b) The result of this research can help doctors in understanding the behaviour of the dispersion process of solute in treating diseases that involves injecting drugs into the artery by observing the behaviour of blood flow and solute dispersion under the influence of artery inclination.

#### REFERENCES

- Abbas, Z., Shabbir, M. S., & Ali, N. (2017). Analysis of rheological properties of Herschel-Bulkley fluid for pulsating flow of blood in ω-shaped stenosed artery. *AIP Advances*, *7*(10), 105123.
- Achab, L., Mahfoud, M., & Benhadid, S. (2016). Numerical study of the non-Newtonian blood flow in a stenosed artery using two rheological models. *Thermal Science*, 20(2), 449-460.
- Aris, R. (1956). On the dispersion of a solute in a fluid flowing through a tube. Proceedings of the Royal Society of London. Series A. Mathematical and Physical Sciences, 235(1200), 67-77.
- Bakheet, A., Alnussaiyri, E. A., Ismail, Z., & Amin, N. (2016). Blood flow through an inclined stenosed artery. *Applied Mathematical Sciences*, *10*(5), 235-254.
- Bali, R., Gupta, N., & Mishra, S. (2016). Dispersion Characteristics of non-Newtonian fluid during transportation of nanoparticles in permeable capillary. *Applications & Applied Mathematics*, 11(2).
- Bird, R. B., Stewart, W. E., & Lightfoot, E. N. (1960). Transport Phenomena John Wiley & Sons. *New York*, 413.
- Das, K., & Saha, G. C. (2009). Arterial MHD pulsatile flow of blood under periodic body acceleration. *Bulletin of Society of Mathematicians Banja Luka*, 16, 21-42.
- Debnath, S., Saha, A. K., Mazumder, B. S., & Roy, A. K. (2017). Hydrodynamic dispersion of reactive solute in a Hagen–Poiseuille flow of a layered liquid. *Chinese journal of chemical engineering*, *25*(7), 862-873.
- Fikkers, B. G., Wuis, E. W., Wijnen, M. H., & Scheffer, G. J. (2006). Intraarterial injection of anesthetic drugs. *Anesthesia & Analgesia*, *103*(3), 792-794.
- Hegde, R. B., Prasad, K., Hebbar, H., & Sandhya, I. (2018). Peripheral blood smear analysis using image processing approach for diagnostic purposes: A review. *Biocybernetics and Biomedical Engineering*, 38(3), 467-480.
- Hui, F. *Hypertension*. Dr. Fred Hui. Retrieved 15 September 2020, from http://drhui.com/articles-by-dr-hui/articles-by-dr-hui-2/hypertension/.

- Huttunen, J. M., Kärkkäinen, L., & Lindholm, H. (2019). Pulse transit time estimation of aortic pulse wave velocity and blood pressure using machine learning and simulated training data. *PLoS computational biology*, *15*(8), e1007259.
- Jaafar, N. A., Yatim, Y. M., & Sankar, D. S. (2014). Mathematical modeling of shear augmented dispersion of solute in blood flow. *AIP Conference Proceedings*, 1605(1), 374-379.
- Jaafar, N. A., Yatim, Y. M., & Sankar, D. S. (2017). Effect of chemical reaction in solute dispersion in Herschel-Bulkley fluid flow with applications to blood flow. *Advances and Applications in Fluid Mechanics*, *20*(2), 279-310.
- Johnston, B. M., Johnston, P. R., Corney, S., & Kilpatrick, D. (2004). Non-Newtonian blood flow in human right coronary arteries: steady state simulations. *Journal of biomechanics*, *37*(5), 709-720.
- Kumagai, T., Takeda, N., Fukase, S., Koshu, H., Inoue, A., Ibuchi, Y., & Yoneoka, Y. (2003). Intra-arterial chemotherapy for malignant tumors of head and neck region using three types of modified injection method. *Interventional Neuroradiology*, 9(Suppl. 1), 113-123.
- Kumar, S. R., & Ahmed, A. (2013). Magnetohydrodynamic couple stress peristaltic flow of blood through porous medium in a flexible channel at low Reynolds number. *International Interdisciplinary Reasearch Journal*, *3*(6), 157-166.
- Kumari, S. V. H. N. K., Murthy, M. V., Reddy, M. C. K., & Kumar, Y. V. K. R. (2011). Peristaltic pumping of a magnetohydrodynamic Casson fluid in an inclined channel. *Advances in Applied Science Research*, 2(2), 428-436.
- Lanotte, L., Mauer, J., Mendez, S., Fedosov, D. A., Fromental, J. M., Claveria, V., Nicoud, F., Gompper, G., & Abkarian, M. (2016). Red cells' dynamic morphologies govern blood shear thinning under microcirculatory flow conditions. *Proceedings of the National Academy of Sciences*, 113(47), 13289-13294.
- Lentine, M., Aanjaneya, M., & Fedkiw, R. (2011). Mass and momentum conservation for fluid simulation. *Proceedings of the 2011 ACM SIGGRAPH/Eurographics Symposium on Computer Animation*, 91-100.
- Mandin, P., Cense, J. M., Georges, B., Favre, V., Pauporté, T., Fukunaka, Y., & Lincot, D. (2007). Prediction of the electrodeposition process behavior with the gravity or acceleration value at continuous and discrete scale. *Electrochimica acta*, 53(1), 233-244.

- Prasad, K. M., & Radhakrishnamacharya, G. (2008). Flow of Herschel–Bulkley fluid through an inclined tube of non-uniform cross-section with multiple stenoses. *Archives of Mechanics*, *60*(2), 161-172.
- Nadeem, S., & Ijaz, S. (2016). Theoretical Analysis of shear thinning hyperbolic tangent fluid model for blood flow in curved artery with stenosis. *Journal of Applied Fluid Mechanics*, 9(5), 2217-2227.
- Nagarani, P., & Sebastian, B. T. (2017). Effect of flow unsteadiness on dispersion in non-Newtonian fluid in an annulus. *J. Appl. Math. & Inform*, *35*(3-4), 241-260.
- Rajashekhar, C., Manjunatha, G., Vaidya, H., Divya, B., & Prasad, K. (2018). Peristaltic flow of Casson liquid in an inclined porous tube with convective boundary conditions and variable liquid properties. *Frontiers in Heat and Mass Transfer (FHMT)*, 11(35), 1-8.
- Rana, J., & Murthy, P. V. S. N. (2016). Unsteady solute dispersion in Herschel-Bulkley fluid in a tube with wall absorption. *Physics of Fluids*, *28*(11), 111903.
- Rana, J., & Murthy, P. V. S. N. (2017). Unsteady solute dispersion in small blood vessels using a two-phase Casson model. *Proceedings of the Royal Society A: Mathematical, Physical and Engineering Sciences*, 473(2204), 20170427.
- Rana, J., & Liao, S. (2019). A general analytical approach to study solute dispersion in non-Newtonian fluid flow. *European Journal of Mechanics-B/Fluids*, 77, 183-200.
- Ratchagar, N. P., & Kumar, R. V. (2019). Dispersion of solute with chemical reaction in blood flow. Bulletin of Pure & Applied Sciences-Mathematics and Statistics, 38(1), 385-395.
- Rohlf, K., & Tenti, G. (2001). The role of the Womersley number in pulsatile blood flow: a theoretical study of the Casson model. *Journal of biomechanics*, 34(1), 141-148.
- Saltzman, J., Nachbar, R., Panorchan, P., Stone, J., & Khan, A. (2010). Applying regular perturbation analysis to HCV viral load equations. Proceedings of the 2009 SIAM Conference on "Mathematics for Industry" The Art of "Mathematics for Industry", 73-83.
- Sankar, D. S., & Hemalatha, K. (2007). Pulsatile flow of Herschel–Bulkley fluid through catheterized arteries–A mathematical model. *Applied Mathematical Modelling*, 31(8), 1497-1517.

- Sankar, D. S., & Ismail, A. I. M. (2010). Effect of periodic body acceleration in blood flow through stenosed arteries—A theoretical model. *International Journal of Nonlinear Sciences & Numerical Simulation*, 3(5), 7-9.
- Sankar, D. S., & Hemalatha, K. (2007). Non-linear mathematical models for blood flow through tapered tubes. *Applied Mathematics and Computation*, *188*(1), 567-582.
- Sankar, D. S. (2015). Perturbation analysis for pulsatile flow of Carreau fluid through tapered stenotic arteries. *International Journal of Biomathematics*, 9(04), 1650063.
- Sankar, D. S., & Lee, U. (2016). Influence of slip velocity in Herschel-Bulkley fluid flow between parallel plates-A mathematical study. *Journal of Mechanical Science and Technology*, 30(7), 3203-3218.
- Sen, S., Chini, E. N., & Brown, M. J. (2005, June). Complications after unintentional intra-arterial injection of drugs: risks, outcomes, and management strategies. *Mayo Clinic Proceedings*, 80(6), 783-795.
- Sharp, M. K. (1993). Shear-augmented dispersion in non-Newtonian fluids. *Annals of biomedical engineering*, *21*(4), 407-415.
- Shaw, S., Ganguly, S., Sibanda, P., & Chakraborty, S. (2014). Dispersion characteristics of blood during nanoparticle assisted drug delivery process through a permeable microvessel. *Microvascular Research*, 92, 25-33.
- Sucharitha, G., Vajravelu, K., Sreenadh, S., & Lakshminarayana, P. (2017). Peristaltic flow and heat transfer of a Herschel-Bulkley fluid in an inclined non-uniform channel with wall properties. In *IOP Conference Series: Materials Science and Engineering*, *263*(6), 062026.
- Sutera, S. P., & Skalak, R. (1993). The history of Poiseuille's law. *Annual review of fluid mechanics*, 25(1), 1-20.
- Tan, J., Thomas, A., & Liu, Y. (2012). Influence of red blood cells on nanoparticle targeted delivery in microcirculation. *Soft matter*, *8*(6), 1934-1946.
- Taylor, G. I. (1953). Dispersion of soluble matter in solvent flowing slowly through a tube. Proceedings of the Royal Society of London. Series A. Mathematical and Physical Sciences, 219(1137), 186-203.
- Veena, B. S., & Warke, A. S. (2015). Study of blood flow in one half of cosine shaped stenosis in the presence of magnetic field. *International Journal of Experimental and Computational Biomechanics*, 3(2), 121-136.

Verma, S. R., & Srivastava, A. (2013). Effect of magnetic field on steady blood flow through an inclined circular tube. *International Journal of Engineering Research and Applications*, 3(4), 428-432.