

FLEXIBLE SKIN-CONTACT ANTENNA WITH ARTIFICIAL MAGNETIC
CONDUCTOR FOR HEALTH MONITORING APPLICATION

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A thesis submitted in fulfilment of the
requirements for the award of the degree of
Doctor of Philosophy

School of Electrical Engineering
Faculty of Engineering
Universiti Teknologi Malaysia

MAY 2022

DEDICATION

To my beloved mom & dad,
Rosadah Abu Bakar & Othman Puteh,
my dearest husband and kids, and my all supportive family members
for their endless love and support

ACKNOWLEDGEMENT

First of all, thank you Allah for the continues blessing, guidance, and for giving me the strength to complete this thesis. In preparing this thesis, I was in contact with many people, researchers, academicians, and practitioners. They have contributed towards my understanding and thoughts.

In particular, I wish to express my sincere appreciation to my main PhD supervisor, Dr. Noor Asmawati Samsuri, whom never stop inspiring me, guiding me, and helping me without prejudice. I am also very thankful to my co-supervisor Ir. Ts. Dr. Kamilia Kamardin for the guidance, advice, and motivation. My utmost thanks to Professor Dr Mohamad Kamal, for the advice, suggestion, and ideas throughout my study from the beginning.

A special gratitude to my fellow labmates at P18 laboratory for a lifetime unforgettable memory. I owe a vote of thanks to my friends for being so supportive during the periods of this study. My sincere appreciation to the Ministry of Higher Education for the scholarship and Universiti Teknologi Malaysia for allowing me to travel along this journey.

Last but not least, I am fully indebted to my loving parents, my handsome husband, my cheeky kids, and my sweetie family members and in-laws for their ultimate support, caring, and sacrifices while I am completing this journey. They all kept me going and survived all the ‘ups and downs’. This thesis would not have been possible without them.

ABSTRACT

Flexible antenna plays a significant role to ensure efficient wireless communication in wearable devices. The choice of the dielectric substrate material of the antenna is one of the important factors to ensure good antenna performance while being tolerant to mechanical deformation. In addition, the size of the antenna becomes the main issue in designing the antenna for on-body applications. Furthermore, the radiation and transmissions performance of the on-body antenna suffers from performance degradation due to several factors such as dielectric properties of the human body as well as line of sight (LOS) and non line of sight (NLOS) transmission conditions. Therefore, this study presents a flexible Skin-Contact Antenna with Artificial Magnetic Conductor surface (SCA-AMC) made from medical-friendly material. Initially, three different types of medical materials which include transdermal cotton patch, semi-transparent film, and self-adhesive bandage were proposed for investigation as the antenna's dielectric substrate. The dielectric properties of the proposed materials were measured prior to the antenna design. For preliminary design investigation, a conventional bowtie antenna was designed using the proposed medical materials and optimized to operate at frequency of 2.4 GHz. To achieve the objectives, the feasibility of medical material usage for the antenna's substrate was explored based on wetness and repeatability test. The proposed SCA is intended for on-body wireless communication devices where there is a significant limitation on the overall size of the antenna. In order to develop a compact flexible antenna, a meandering technique is applied to the conventional bowtie antenna. By employing the meandering technique, the total length of the antenna can be reduced by 20 %. As the body protection against electromagnetic absorption is important, a dipole-like AMC structure was designed at frequency of 2.4 GHz and integrated with the meandered bowtie antenna. The proposed SCA-AMC is made of flexible material for the substrate and conducting parts, making it suitable for wearable applications. Furthermore, the factors that influence the antenna's radiation and transmission performance have been determined. The experiments have been carried out considering various conditions such as body movements and the presence of either human body or obstacle in between the SCA-AMC transmitter and the receiver. The results indicate that the human body introduces an additional 20 dBm power loss when present between the transmitter and receiver. Also, the presence of the book causes 6 dBm reduction in received power while sweatshirts and cotton polo shirts contribute to a small variation of approximately from 0.5 to 1 dBm. Besides, wetness measurements were also carried out using tap water and sweat-like solution. The sweat-like solution had been developed using a mixture of sodium chloride, sodium bicarbonate, and water. The material characterization of the developed sweat-like solution was then performed. The developed sweat-like solution has a measured permittivity and loss tangent of 75.8 and 0.13, respectively at the frequency of 2.4 GHz. The proposed SCA-AMC was also tested in a real-life situation by merging it with an electrocardiogram (ECG) sensor node. The results obtained show that the wireless ECG pattern is comparable to the ECG pattern measured using a conventional ECG machine. The findings in this research have profound implications for future studies to develop an efficient wireless device, especially for on-body applications.

ABSTRAK

Antena yang fleksibel memainkan peranan yang penting untuk memastikan komunikasi tanpa wayar yang cekap dalam peranti boleh pakai. Pemilihan jenis dielektrik antena adalah salah satu faktor penting untuk memastikan prestasi antena yang baik disamping mempunyai ketahanan terhadap ubah bentuk mekanikal. Saiz antena menjadi isu utama dalam mereka bentuk antena untuk aplikasi di atas badan. Tambahan pula, prestasi sinaran dan penghantaran data antena mengalami kemerosotan prestasi disebabkan oleh beberapa faktor seperti sifat dielektrik badan manusia serta keadaan penghantaran garis penglihatan (LOS) dan bukan garis penglihatan (NLOS). Oleh itu, kajian ini bertujuan untuk menghasilkan antena sentuhan kulit bersama permukaan pengalir magnet buatan (SCA-AMC) yang diperbuat daripada bahan mesra perubatan. Tiga jenis bahan perubatan yang berbeza seperti tampalan kapas transdermal, filem separa lutsinar, dan pembalut lekat sendiri dicadangkan untuk penyiasatan sebagai substrat dielektrik antena. Sifat dielektrik bahan yang dicadangkan diukur sebelum reka bentuk antena. Untuk penyiasatan reka bentuk awal, antena tali leher lazim direka menggunakan bahan perubatan yang dicadangkan dan dioptimumkan untuk beroperasi pada frekuensi 2.4 GHz. Untuk mencapai objektif, kebolehlaksanaan penggunaan bahan perubatan untuk substrat antena diterokai berdasarkan ujian kebasahan dan kebolehulangan. SCA-AMC yang dicadangkan bertujuan untuk peranti komunikasi tanpa wayar pada badan di mana terdapat had yang ketara pada saiz keseluruhan antena. Teknik garis berliku digunakan pada antena tali leher lazim untuk membangunkan antena boleh lentur padat. Dengan menggunakan teknik tersebut, jumlah panjang antena boleh dikurangkan sebanyak 20%. Oleh kerana perlindungan badan daripada penyerapan elektromagnet adalah penting, struktur AMC seperti antena dwikutub direka pada frekuensi 2.4 GHz dan disepadukan dengan antena tali leher garis berliku. SCA-AMC yang dicadangkan diperbuat daripada bahan mudah lentur untuk substrat dan bahagian pengalir, menjadikannya sesuai untuk aplikasi mudah alih. Tambahan pula, faktor yang mempengaruhi sinaran antena dan prestasi penghantaran telah ditentukan. Eksperimen telah dijalankan dengan mengambil kira pelbagai keadaan seperti pergerakan badan dan kehadiran tubuh manusia atau halangan di antara penghantar SCA-AMC dan penerima. Keputusan menunjukkan bahawa tubuh manusia menyebabkan kehilangan kuasa sebanyak 20 dBm apabila berada di antara pemancar dan penerima. Selain itu, kehadiran buku menyebabkan pengurangan sebanyak 6 dBm dalam kuasa yang diterima manakala baju peluh dan baju polo kapas menyumbang kepada variasi kecil iaitu antara 0.5 dBm hingga 1 dBm. Selain itu, pengukuran kebasahan juga telah dijalankan menggunakan air paip dan larutan peluh. Larutan peluh dihasilkan dengan menggunakan campuran natrium klorida, natrium bikarbonat, dan air. Larutan peluh yang dihasilkan mempunyai kebolehpercayaan dan tangen kehilangan yang diukur, masing-masing sebanyak 75.8 and 0.13 pada frekuensi 2.4 GHz. SCA-AMC yang dicadangkan juga diuji dalam situasi kehidupan sebenar dengan menggabungkannya dengan nod penerima elektrokardiogram (ECG). Keputusan menunjukkan bahawa corak ECG tanpa wayar menghampiri dengan corak ECG yang diukur menggunakan mesin ECG lazim. Penemuan dalam penyelidikan ini mempunyai implikasi yang mendalam untuk kajian masa depan untuk membangunkan peranti tanpa wayar yang cekap, terutamanya untuk aplikasi pada badan.

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LIST OF ABBREVIATIONS

LOS	-	Line of sight
NLOS	-	Non line of sight
SCA-AMC		Skin-Contact Antenna with AMC
ECG	-	Electrocardiogram
EEG	-	Electroencephalogram
AMC	-	Artificial Magnetic Conductor
VNI	-	Virtual Networking Index
PET	-	Polyethylene terephthalate
PDMS	-	Polydimethylsiloxane
UWB	-	Ultra-wideband
CPW	-	Coplanar waveguide
PMC	-	Perfect Magnetic Conductor
SAR	-	Specific absorption rate
FCC	-	Federal Communications Commission
ICNIRP	-	International Commission on Non-Ionizing Radiation Protection
AUT	-	Antenna under test
EM	-	Electromagnetic
SAM	-	Specific Anthropomorphic Mannequin

LIST OF SYMBOLS

f_r	-	Resonant frequency
ϵ_e	-	Effective permittivity
ϵ_r	-	Relative permittivity
θ	-	Opening angle
μ_0	-	Permeability of free space
ϵ_0	-	Permittivity of free space
η_0	-	Free space impedance
λ	-	Wavelength
σ	-	Conductivity
ρ	-	Mass density

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CHAPTER 1

INTRODUCTION

1.1 Research Background

With the increasing number of monitoring system either in health care, sports or security sector using a wireless area network technology, intense researches are focusing on the development of wearable electronics. Wearable electronics are getting more attention due to the wide range of healthcare, sports, security, and also military applications. These wearable electronics are leading to the creation of wireless devices that is easier to be carried out by the user. The wearable wireless device is usually being attached to the user body or being carried out in the pocket thus improves the user convenience. This phenomenon indicates a strong potential for the wired-communication network to be replaced with wireless communication. Along with this trend, body-centric wireless communication which refers as human-self and human-human networking has received more exposure especially for continuous monitoring applications in the medical sector.

Conventionally, a medical device for health monitoring such as electrocardiogram (ECG) and electroencephalogram (EEG) use rigid electrodes coupled to the skin via electrolyte gels and affixed with adhesive tapes. Therefore, measuring the bio-signal using the conventional method for everyday life may be tricky due to inconveniences caused by the bulk wire connection of the electrodes and the reliability of the measurement caused by gel drying. Besides, by using the rigid electrodes, the measurement procedure will be limited only to locate the sensor to the flat region of the body such as the forehead or chest. Therefore, flexible antenna comes into play aimed at enhancing the quality of human life by providing comfort during the continuous health monitoring in the medical sector.

1.2 Problem Statements

In the conventional wearable wireless device, a rigid antenna is used to transmit data at 2.4 GHz operating frequency, commonly used for WiFi, Bluetooth, and Zigbee standard. This however limits the positioning of the device on the human body and makes the user uncomfortable for longer usage. Nowadays, there are varieties of wearable antennas made of flexible substrates have been proposed such as fleece, jeans, polymer, and organic paper [1]–[4]. These materials however suffer from serious drawbacks due to high water absorption and pattern distortion due to wrinkles and crumpling. The antenna performance may significantly degrade in wet conditions [5]–[7], experienced poor impedance matching and suffers from a significant reduction of radiation efficiency for up to 26 % due to crumpling effect [8]. In addition, the previously proposed wearable antenna required an additional adhesive element in order to attach to the human body [9]–[11]. The inclusion of additional adhesive elements could change the dielectric properties of the entire substrate material. Thus, affecting the antenna radiation properties. Therefore, suitable flexible materials such as medical patches, bandages, and others that are currently available in the market may be useful for further investigation. This medical-friendly material has proven to be comfort and safe to the user for longer usage. Suitable type of medical-friendly material will be proposed by considering the wet and crumpling effect on the antenna performance. None of these materials has been reported in the literature to be used as the antenna's substrate.

Furthermore, the wearable antenna is required to be located in close proximity to the human body. However, the flexible antenna when operated very close to the human body has been reported to suffer from performance degradation due to the dielectric properties of the body itself [12], [13]. Besides that, electromagnetic power absorption by the human body leads to the tissue heating and present an adverse health effect due to the power absorbed by the body [14]. It is important to evaluate the antenna performance within the human body as well as to minimize the Specific Absorption Rate (SAR). The SAR is the parameter to determine the level of power absorbed by the human body. One of the common technique for reducing the SAR is using a simple ground plane [11], [15]. However, this technique suffers from the out-

of-phase reflection property contributing to decrease in the total efficiency [16]. Other method for SAR reduction using metamaterial such as Artificial Magnetic Conductor (AMC) surface as a shield to the wearable antenna have been considered and studied [17]–[20]. With that being used, the antenna's backward radiation is greatly minimized. As a results, the electromagnetic radiation toward the human body is significantly lowered and improved the antenna performance in term of gain and total efficiency [19], [21]. Therefore, it is expected that integrating flexible AMC surface with flexible antenna will further improved the on-body antenna performance and user's convenient. Since a medical-friendly substrate material will be considered and proposed, the same material will be used as the AMC surface in this study. In addition, none of earlier studies have used or considered AMC using this kind of medical-friendly as the substrate dielectric material. Parametric studies and further optimization will be done in order to design an AMC surface. The proposed flexible antenna will be integrated with the AMC surface made of medical-friendly material for further investigation and analysis.

Besides that, previous works show that antenna in wet conditions experienced performance degradation due to the presence of high permittivity water which in turn alters the dielectric properties of the antenna's substrate. Tap water, rainwater, and seawater have been considered while investigating wetness effect on the antenna performance in their research [5], [6], [22]. Another rational situation that should be considered while designing a wearable antenna is the effect of human sweat. The wearable antenna is believed to be worn on the human body. Thus, there is a tendency for the antenna to exposed to sweat during daily activities especially athlete who is in the recovery process or their daily fitness routine. Human sweat contains additional chemicals that are expected to influence the antenna performance further. Limited research has investigated the human sweat effect on antenna performance [23]. Author in [23] tests the effect of artificial sweat solution on the S_{11} magnitude of the wearable antenna made of denim substrate. The research found that, the resonant frequency is shifted by approximately 10 % when the antenna is exposed to the artificial sweat. Up to date, there is no research reported on the effect of sweat on the transmission performance. Hence, the development of sweat-like liquid using the combination of three different chemical substances is proposed in this study. The developed sweat-like liquid is expected to be suitable for laboratory and small scale investigation. In

addition, the developed sweat-like liquid can be used to further examine and determine the effect of wetness on the antenna radiation and transmission performance in this study.

Moreover, the propagation characteristics of the wearable antenna are greatly affected by several factors such as the human body movements and changes in body posture [24]–[26]. An animated human movement and realistic measurement have been performed in order to study the effect of the body movement on the antenna transmission and propagation characteristics. Previous studies demonstrate that during some daily activities such as exercise, jumping, or even walking, the body dynamic will cause significant degradation on the antenna radiation and transmission performance [25], [27], [28]. However, in these previous works, the antenna alone is used as the transmitter during the characterization. None of the research is found to further investigate and characterize the factors that affect the propagation characteristics of an antenna with the inclusion of an AMC surface. The inclusion of AMC surface may modify the antenna propagation characteristics depending on the position of transmitter and receiver as well as dynamic body movement. Therefore, propagation characteristics of antenna integrated with AMC surface using the proposed medical-friendly material need to be done considering factors such as different height and angle between the transmitter and receiver. Moreover, the effect of human body movement such as degree of turning and bending are considered in this study too. In addition, the presence of additional obstacles in front of the antenna with AMC are likely to influence the transmission and propagation performance. Previous study shows that, the presence of obstacle such as tree in between the transmitter and receiver contribute to the signal attenuation [29]. However, no further research is found to investigate the effect of common obstacles such as book and sweatshirt on the propagation characteristics. These obstacles are commonly found in real situation and present near to the human body. Therefore, it is worth to further characterize and determine the effect of these obstacles on the propagation characteristics. Furthermore, there are limited research presents measurement in the actual home-monitoring setup. Therefore, real home-monitoring setup will be considered in this study to mimic the real situation of in-house monitoring application considering daily routine and activities of the user.

1.3 Research Objectives

The objectives of the current research are:

- i. To propose new substrate material for wearable application
- ii. To design and fabricate flexible antenna and flexible AMC surface using medical-friendly material
- iii. To develop a sweat-like solution in order to investigate the effect of human sweat on the antenna performance
- iv. To examine the off-body transmission and propagation characteristics of the flexible antenna with AMC surface considering the actual home-monitoring environment

1.4 Scope of Research

This study starts with an extensive literature review in order to understand the basic concept of antenna design and the fundamental of AMC working principle. CST Microwave Studio is used as the simulation software to design the antenna with AMC. Antenna performance parameter such as S_{11} magnitude, radiation pattern, gain, and total efficiency are considered in this study. Whilst, the antenna transmission performances are discussed in terms of S_{21} magnitude and received power. The main focuses of this study is to develop a flexible antenna with AMC surface for on-body applications using a medical-friendly material as the dielectric substrate. There are various types of medical materials that are widely available in the market. However, the proposed flexible antenna with AMC surface is targeted for on-body applications where the antenna can be placed directly on the human body. Therefore, this study introduces and investigates the possibilities of three different medical materials (transdermal cotton patch, semi-transparent film, and self-adhesive bandage) to be used as the antenna's substrate. In this study, the flexible antenna and AMC are limited to the operating frequency of 2.4 GHz. Material characterization has been conducted using open-ended probe. Conventional bowtie antenna is designed for the initial

investigation using the proposed substrate materials. Wetness test and repeatability test are conducted to explore the possibilities of the proposed medical material to be used as the antenna substrate. Next, the conventional bowtie antenna is miniaturized using meandering technique. Few series of parametric studies have been conducted to obtain an optimized antenna design at 2.4 GHz. In additions, the AMC surface is designed using the selected substrate materials. The antenna performance above the AMC surface is studied by varying the the AMC array size, the position of the antenna above the AMC surface as well as the separation distance between the antenna and the AMC surface. Finally, an optimum flexible antenna with AMC surface is proposed and denoted as Skin-Contact Antenna with AMC (SCA-AMC).

To further quantify the SCA-AMC performance for on-body conditions, various experiments have been conducted. The factors that contribute to the transmission loss are investigated in terms of the presence of the human body and obstacles in between the transmitter and receiver. Line-of-sight and non-line-of-sight conditions between the transmitter and receiver are also taken into consideration during the measurements. Four different body movements are considered in this study in order to mimic the daily situation. The off-body measurements are conducted in an anechoic chamber with a maximum distance of 300 cm between the transmitter and receiver for two different conditions (with and without the human body). In the measurements, the proposed SCA-AMC is used as the transmitter and wideband horn antenna is used as the receiver. The proposed flexible antenna with AMC surface is integrated with the available wireless ECG sensor kit in order to test its reliability for actual applications.

1.5 Thesis Organization

The thesis consists of seven chapters. Chapter 1 briefly introduces the background of the research, problem statement, research objectives, and the scope of the research.

Chapter 2 discusses the background of the flexible antenna and AMC for wearable applications. Works related to the propagation characteristics of wearable antenna are also reviewed in this chapter.

The method used in this thesis is discussed in detail and presented in Chapter 3. The discussions start with the process to characterize and select the best flexible material to be used in the antenna and AMC design. Then, the method to design and optimize the antenna and AMC operate at 2.4 GHz is discussed. The measurement process to explore the off-body transmission and propagation characteristics is also presented in this chapter too.

In Chapter 4, numerical analysis of the antenna and AMC design is presented. The chapter starts with the introduction of three different flexible materials and processes to determine the suitable flexible material to be used as the antenna's and AMC's dielectric substrate. Then, the miniaturization of the bowtie antenna and AMC design are discussed.

In chapter 5, the antenna performance near the human body with and without the AMC surface is explored. Besides that, off-body transmission and propagation characteristics are discussed. The results are presented in terms of S_{21} and received power, P_r . Several conditions that are expected to affect the transmission and propagation characteristics such as body movement, the effect of water and sweat and also the presence of obstacles close to the human body are also considered and tested.

Chapter 6 presents the possibilities of the proposed flexible SCA-AMC to be integrated with the wireless system. The real-time monitoring ECG signal for in-house monitoring by varying the position and distance between the transmitter and receiver are presented in this chapter.

Chapter 7 summarizes some important conclusions obtained from this research as well as the significance of the research finding. Future works are also suggested.

REFERENCES

- [1] A. Rida, L. Yang, R. Vyas, and M. M. Tentzeris, "Conductive inkjet-printed antennas on flexible low-cost paper-based substrates for RFID and WSN applications," *IEEE Antennas Propag. Mag.*, vol. 51, no. 3, pp. 13–23, 2009.
- [2] C. P. Lin, C. H. Chang, Y. T. Cheng, and C. F. Jou, "Development of a flexible SU-8/PDMS-based antenna," *IEEE Antennas Wirel. Propag. Lett.*, vol. 10, pp. 1108–1111, 2011.
- [3] E. F. Sundarsingh, S. Velan, M. Kanagasabai, A. K. Sarma, C. Raviteja, and M. G. N. Alsath, "Polygon-Shaped Slotted Dual-Band Antenna for Wearable Applications," *IEEE Antennas Wirel. Propag. Lett.*, vol. 13, pp. 611–614, 2014.
- [4] K. Kamardin, M. K. A. Rahim, P. S. Hall, and N. A. Samsuri, "Vertical and horizontal transmission enhancement between antennas using textile artificial magnetic conductor waveguide sheet," *Electron. Lett.*, vol. 51, pp. 671–673, 2015.
- [5] R. Yahya, M. R. Kamarudin, S. Member, and N. Seman, "Effect of Rainwater and Seawater on the Permittivity of Denim Jean Substrate and Performance of UWB Eye-Shaped Antenna," vol. 13, pp. 806–809, 2014.
- [6] B. Ivsic, G. Golemac, and D. Bonafacic, "Performance of wearable antenna exposed to adverse environmental conditions," in *ICECom*, 2013, pp. 1–4.
- [7] K. Kamardin, M. K. A. Rahim, P. S. Hall, N. A. Samsuri, T. A. Latef, and M. H. Ullah, "Textile Artificial Magnetic Conductor Jacket for Transmission Enhancement between Antennas under Bending and Wetness Measurements," *Appl. Phys. A Mater. Sci. Process.*, vol. 122, 2016.
- [8] B. Hu, G. P. Gao, L. Le He, X. D. Cong, and J. N. Zhao, "Bending and On-Arm Effects on a Wearable Antenna for 2.45 GHz Body Area Network," *IEEE Antennas Wirel. Propag. Lett.*, vol. 15, pp. 378–381, 2016.
- [9] M. Tighezza, S. K. A. Rahim, and M. T. Islam, "Flexible Wideband Antenna for 5G Applications," *Microw. Opt. Technol. Lett.*, vol. 60, no. 1, pp. 38–44, 2017.
- [10] R. B. V. B. Simorangkir, D. Le, T. Bjorninen, A. S. M. Sayem, M. Zhadobov, and R. Sauleau, "Washing Durability of PDMS-Conductive Fabric Composite:

- Realizing Washable UHF RFID Tags,” *IEEE Antennas Wirel. Propag. Lett.*, vol. 18, no. 12, pp. 2572–2576, 2019.
- [11] R. B. V. B. Simorangkir, A. Kiourti, and K. P. Esselle, “UWB Wearable Antenna with a Full Ground Plane Based on PDMS-Embedded Conductive Fabric,” *IEEE Antennas Wirel. Propag. Lett.*, vol. 17, no. 3, pp. 493–496, 2018.
- [12] A. Sani *et al.*, “Experimental characterization of UWB on-body radio channel in indoor environment considering different antennas,” *IEEE Trans. Antennas Propag.*, vol. 58, no. 1, pp. 238–241, 2010.
- [13] M. Koohestani, N. Pires, A. K. Skrivervik, and A. A. Moreira, “Performance study of a UWB antenna in proximity to a human arm,” *IEEE Antennas Wirel. Propag. Lett.*, vol. 12, pp. 555–558, 2013.
- [14] A. Zamanian and C. Hardiman, “Electromagnetic radiation and human health: A review of sources and effects,” *EMR Hum. Heal.*, vol. 16, pp. 16–26, 2005.
- [15] L. A. Yimdjo Poffelie, P. J. Soh, S. Yan, and A. E. G. Vandenbosch, “A High-Fidelity All-Textile UWB Antenna with Low Back Radiation for Off-Body WBAN Applications,” *IEEE Trans. Antennas Propag.*, vol. 64, no. 2, pp. 757–760, 2016.
- [16] D. Sievenpiper, L. Zhang, R. F. Jimenez Broas, N. G. Alexöpolous, and E. Yablonovitch, “High-impedance electromagnetic surfaces with a forbidden frequency band,” *IEEE Trans. Microw. Theory Tech.*, vol. 47, no. 11, pp. 2059–2074, 1999.
- [17] J. Lee and J. Lee, “SAR Reduction Using Integration of PIFA and AMC Structure for Pentaband Mobile Terminals,” *Int. J. Antennas Propag.*, 2017.
- [18] S. Il Kwak, D. U. Sim, J. H. Kwon, and Y. J. Yoon, “Design of PIFA with Metamaterials for Body-SAR Reduction in Wearable Applications,” *IEEE Trans. Electromagn. Compat.*, vol. 59, no. 1, pp. 297–300, 2017.
- [19] M. El Atrash, M. A. Abdalla, and H. M. Elhennawy, “A Wearable Dual-Band Low Profile High Gain Low SAR Antenna AMC-Backed for WBAN Applications,” *IEEE Trans. Antennas Propag.*, vol. 67, no. 10, pp. 6378–6388, 2019.
- [20] M. Wang *et al.*, “Investigation of SAR Reduction Using Flexible Antenna With Metamaterial Structure in Wireless Body Area Network,” *IEEE Trans. Antennas Propag.*, vol. 66, no. 6, pp. 3076–3086, 2018.
- [21] B. S. Cook and A. Shamim, “Utilizing wideband AMC structures for high-gain

- inkjet-printed antennas on lossy paper substrate,” *IEEE Antennas Wirel. Propag. Lett.*, vol. 12, pp. 76–79, 2013.
- [22] M. A. R. Osman, M. K. A. Rahim, N. A. Samsuri, M. K. Elbasheer, and M. E. Ali, “Textile UWB Antenna Bending and Wet Performances,” vol. 2012, 2012.
- [23] P. M. Potey and K. R. Tuckley, “Variation in properties of wearable textile antennas due to sweat in erratic climatic conditions,” *IET Conf. Publ.*, vol. 2018, no. CP746, pp. 3–8, 2018.
- [24] K. Turbic, L. M. Correia, and M. Beko, “A Channel Model for Polarized Off-Body Communications with Dynamic Users,” *IEEE Trans. Antennas Propag.*, vol. 67, no. 11, pp. 7001–7013, 2019.
- [25] T. Uusitupa and T. Aoyagi, “Analysis of Dynamic on-Body Communication Channels for Various Movements and Polarization Schemes at 2.45 GHz,” *IEEE Trans. Antennas Propag.*, vol. 61, no. 12, pp. 6168–6179, 2013.
- [26] P. S. Hall, M. Ricci, and D. Hee, “Measurements of On-Body Propagation Characteristics,” *2002 IEEE Antennas Propag. Soc. Int. Symp.*, pp. 310–313, 2002.
- [27] M. Mohamed, M. Cheffena, and A. Moldsvor, “Characterization of the body-to-body propagation channel for subjects during sports activities,” *Sensors (Switzerland)*, vol. 18, 2018.
- [28] P. S. Hall *et al.*, “Antennas and propagation for on-body communication systems,” *IEEE Antennas Propag. Mag.*, vol. 49, no. 3, pp. 41–58, 2007.
- [29] G. Durgin, T. S. Rappaport, and H. Xu, “5.85-GHz Radio Path Loss and Penetration Loss Measurement in and around Homes and Trees,” *IEEE Commun. Lett.*, vol. 2, no. 3, pp. 70–72, 1998.
- [30] S. Lemey, S. Agneessens, and H. Rogier, “Wearable smart objects: microwaves propelling smart textiles: A review of holistic designs for wireless textile nodes,” *IEEE Microw. Mag.*, vol. 19, no. 6, pp. 83–100, 2018.
- [31] N. H. A. Rahman, Y. Yamada, and M. S. A. Nordin, “Analysis on the Effects of the Human Body on the Performance of Electro-Textile Antennas for Wearable Monitoring and Tracking Application,” *Materials (Basel)*, vol. 12, no. 10, pp. 1–17, 2019.
- [32] S. J. Boyes *et al.*, “Measurement and Performance of Textile Antenna Efficiency on a Human Body in a Reverberation Chamber,” vol. 61, no. 2, pp. 871–881, 2013.

- [33] S. L. Cotton, Y. J. Chun, W. G. Scanlon, and G. A. Conway, "Path Loss Models for Indoor Off-Body Communications at 60 GHz," in *EEE Antennas and Propagation Society International Symposium, (APSURSI)*, 2016, pp. 1441–1442.
- [34] K. Turbic, S. J. Ambroziak, and L. M. Correia, "Characteristics of the Polarised Off-Body Channel in Indoor Environments," *Eurasip J. Wirel. Commun. Netw.*, vol. 2017, no. 174, 2017.
- [35] Cisco, "Cisco visual networking index (VNI) global mobile data traffic forecast update, 2017-2022," 2019.
- [36] N. R. Rishani, R. M. Shubair, and G. Aldabbagh, "On the design of wearable and epidermal antennas for emerging medical applications," *2017 Sensors Networks Smart Emerg. Technol. SENSET 2017*, vol. 2017-Janua, pp. 1–4, 2017.
- [37] Y. Chi, S. Member, and F. Chen, "On - body Adhesive - Bandage - like Antenna for Wireless Medical Telemetry Service," vol. 62, no. c, pp. 1–10, 2014.
- [38] N. Ahmed Malik, M. Ur-Rehman, G. Ali Safdar, and Q. H. Abbasi, "Extremely Low Profile Flexible Antenna for Medical Body Area Networks," in *2017 IEEE Asia Pacific Microwave Conference (APMC)*, pp. 5–8.
- [39] X. Lin *et al.*, "Ultrawideband Textile Antenna for Wearable Microwave Medical Imaging Applications," vol. 68, no. 6, pp. 4238–4249, 2020.
- [40] G. A. Conway and W. G. Scanlon, "Compact low-profile antenna for wireless medical vital sign monitors at 868 MHz," *8th Eur. Conf. Antennas Propagation, EuCAP 2014*, pp. 830–832, 2014.
- [41] C. Y. Chiu, S. Shen, and R. D. Murch, "Transparent dual-band antenna for smart watch applications," *2017 IEEE Antennas Propag. Soc. Int. Symp. Proc.*, vol. 2017-Janua, pp. 191–192, 2017.
- [42] B. F. Spencer, M. E. Ruiz-Sandoval, and N. Kurata, "Smart sensing technology: opportunities and challenges," *Struct. Control Heal. Monit.*, vol. 11, no. 4, pp. 349–368, 2004.
- [43] K. Zhao, Z. Ying, and S. He, "Antenna designs of smart watch for cellular communications by using metal belt," *2015 9th Eur. Conf. Antennas Propagation, EuCAP 2015*, vol. 1, no. c, pp. 2–6, 2015.
- [44] H. Lee, J. Tak, Y. Hong, and J. Choi, "Design of an all-textile antenna integrated in military beret for GPS/RFID applications," *ISAP 2016 - Int. Symp. Antennas*

- Propag.*, pp. 982–983, 2017.
- [45] E. D. Ac, “2018 International CET Conference on Control, Communication, and Computing, IC4 2018,” *2018 Int. CET Conf. Control. Commun. Comput. IC4 2018*, vol. 2, pp. 220–223, 2018.
- [46] H. Lee, J. Tak, and J. Choi, “Wearable Antenna Integrated into Military Berets for Indoor/Outdoor Positioning System,” *IEEE Antennas Wirel. Propag. Lett.*, vol. 16, pp. 1919–1922, 2017.
- [47] J. G. and L. Jin, “A Compact Multiband Bow-Tie Dipole Slot Antenna for WLAN and WiMAX Applications,” *Prog. Electromagn. Res. Lett.*, vol. 56, pp. 17–23, 2015.
- [48] A. S. Sayem, K. P. Esselle, and R. M. Hashmi, “Increasing the transparency of compact flexible antennas using defected ground structure for unobtrusive wearable technologies,” *IET Microwaves, Antennas Propag.*, vol. 14, no. 14, pp. 1869–1877, 2020.
- [49] P. Salonen, L. Sydanheimo, M. Keskilammi, and M. Kivikoski, “Small planar inverted-F antenna for wearable applications,” *Int. Symp. Wearable Comput. Dig. Pap.*, pp. 95–100, 1999.
- [50] B. Sanz-Izquierdo, J. C. Batchelor, and M. Sobhy, “UWB wearable button antenna,” *Eur. Sp. Agency, (Special Publ. ESA SP*, vol. 626 SP, pp. 9–12, 2006.
- [51] B. Sanz-Izquierdo, F. Huang, and J. C. Batchelor, “Small size wearable button antenna,” *Eur. Sp. Agency, (Special Publ. ESA SP*, vol. 626 SP, 2006.
- [52] H. Xiaomu, S. Yan, and G. A. E. Vandenbosch, “Wearable button antenna for dual-band WLAN applications with combined on and off-body radiation patterns,” *IEEE Trans. Antennas Propag.*, vol. 65, no. 3, pp. 1384–1387, 2017.
- [53] C. M. Cheng, W. S. Chen, G. Q. Lin, and H. M. Chen, “Four antennas on smart watch for GPS/UMTS/ WLAN MIMO application,” *2017 IEEE Int. Conf. Comput. Electromagn. ICCEM 2017*, pp. 346–348, 2017.
- [54] Y. Wang, J. Zhang, F. Peng, and S. Wu, “A Glasses Frame Antenna for the Applications in Internet of Things,” *IEEE Internet Things J.*, vol. 6, no. 5, pp. 8911–8918, 2019.
- [55] M. Wagih, O. Cetinkaya, B. Zaghari, A. S. Weddell, and S. Beeby, “Real-world performance of sub-1 GHz and 2.4 GHz textile antennas for RF-powered body area networks,” *IEEE Access*, vol. 8, pp. 133746–133756, 2020.
- [56] I. Martinez *et al.*, “Compact , Low-Profile and Robust Textile Antennas With

- Improved Bandwidth for Easy Garment Integration,” *IEEE Access*, vol. 8, pp. 77490–77500, 2020.
- [57] A. K. Biswas and U. Chakraborty, “Compact wearable MIMO antenna with improved port isolation for ultra-wideband applications,” *IET Microwaves, Antennas Propag.*, vol. 13, no. 4, pp. 498–504, 2018.
- [58] R. B. V. B. Simorangkir, Y. Yang, L. Matekovits, and K. P. Esselle, “Dual-Band Dual-Mode Textile Antenna on PDMS Substrate for Body-Centric Communications,” *IEEE Antennas Wirel. Propag. Lett.*, vol. 16, pp. 677–680, 2017.
- [59] Z. G. Liu and Y. X. Guo, “Compact Low-Profile Dual Band Metamaterial Antenna for Body Centric Communications,” *IEEE Antennas Wirel. Propag. Lett.*, vol. 14, pp. 863–866, 2015.
- [60] A. M. Mansour, N. Shehata, B. M. Hamza, and M. R. M. Rizk, “Efficient Design of Flexible and Low Cost Paper-Based Inkjet-Printed Antenna,” *Int. J. Antennas Propag.*, vol. 2015, 2015.
- [61] B. Mohamadzade, R. B. V. B. Simorangkir, R. M. Hashmi, and A. Lalbakhsh, “A conformal ultrawideband antenna with monopole-like radiation patterns,” *IEEE Trans. Antennas Propag.*, vol. 68, no. 8, pp. 6383–6388, 2020.
- [62] H. Abdelrahman *et al.*, “A Transparent and Flexible Polymer-Fabric Tissue UWB Antenna for Future Wireless Networks,” *IEEE Antennas Wirel. Propag. Lett.*, vol. 16, pp. 1333–1336, 2017.
- [63] M. A. S. Tajin, O. Bshara, Y. Liu, A. Levitt, G. Dion, and K. R. Dandekar, “Efficiency measurement of the flexible on- body antenna at varying levels of stretch in a reverberation chamber,” *IET Microwaves, Antennas Propag.*, vol. 14, no. 3, pp. 154–158, 2020.
- [64] F. Wang, T. Arslan, and G. Wang, “Breast cancer detection with microwave imaging system using wearable conformal antenna arrays,” in *IEEE International Conference on Imaging Systems and Techniques (IST)*, 2017.
- [65] W. T. Li, Y. Q. Hei, P. M. Grubb, X. W. Shi, and R. T. Chen, “Inkjet printing of wideband stacked microstrip patch array antenna on ultrathin flexible substrates,” *IEEE Trans. Components, Packag. Manuf. Technol.*, vol. 8, no. 9, pp. 1695–1701, 2018.
- [66] A. T. Castro and S. K. Sharma, “Inkjet-Printed Wideband Circularly Polarized Microstrip Patch Array Antenna on a PET Film Flexible Substrate Material,”

- IEEE Antennas Wirel. Propag. Lett.*, vol. 17, no. 1, pp. 176–179, 2018.
- [67] X. Guo, Y. Hang, Z. Xie, C. Wu, L. Gao, and C. Liu, “Flexible and wearable 2.45 GHz CPW-fed antenna using inkjet-printing of silver nanoparticles,” *Microw. Opt. Technol. Lett.*, vol. 59, no. 1, pp. 204–208, 2017.
- [68] P. S. Taylor and J. C. Batchelor, “Small Epidermal UHF RFID Loop Antenna for Passive Oral Cavity Control Applications and Patient Health Monitoring,” *2018 IEEE Antennas Propag. Soc. Int. Symp. Usn. Natl. Radio Sci. Meet. APSURSI 2018 - Proc.*, pp. 687–688, 2018.
- [69] S. Jacobsen, P. R. Stauffer, and D. G. Neuman, “Dual-mode antenna design for microwave heating and noninvasive thermometry of superficial tissue disease,” *IEEE Trans. Biomed. Eng.*, vol. 47, no. 11, pp. 1500–1508, 2000.
- [70] D. E. Anagnostou, A. A. Gheethan, A. K. Amert, and K. W. Whites, “A Direct-Write Printed Antenna on Paper-Based Organic Substrate for Flexible Displays and WLAN Applications,” *J. Disp. Technol.*, vol. 6, no. 11, pp. 558–564, 2010.
- [71] X. Li, J. Siden, H. Andersson, and T. Schon, “A Paper-Based Screen Printed HF RFID Reader Antenna System,” *IEEE J. Radio Freq. Identif.*, vol. 2, no. 3, pp. 118–126, 2018.
- [72] A. Mansour, M. Azab, and N. Shehata, “Flexible Paper-based Wideband Antenna for Compact-size IoT Devices,” in *8th IEEE Annual Information Technology, Electronics and Mobile Communication Conference (IEMCON)*, 2017, pp. 426–429.
- [73] G. Shaker, S. Safavi-Naeini, N. Sangary, and M. M. Tentzeris, “Inkjet printing of ultrawideband (UWB) antennas on paper-based substrates,” *IEEE Antennas Wirel. Propag. Lett.*, vol. 10, pp. 111–114, 2011.
- [74] S. Yang *et al.*, “‘Cut-and-paste’ manufacture of multiparametric epidermal sensor systems communication,” *Adv. Mater.*, vol. 27, pp. 6423–6430, 2015.
- [75] N. A. Elias, N. A. Samsuri, M. K. A. Rahim, C. Panagamuwa, and W. Will, “Bending and crumpling deformation study of the resonant characteristic and SAR for a 2.4 GHz textile antenna,” vol. 10, pp. 17–23, 2015.
- [76] L. Corchia, G. Monti, and L. Tarricone, “Wearable Antennas: Nontextile Versus Fully Textile Solutions,” *IEEE Antennas Propag. Mag.*, vol. 61, no. 2, pp. 71–83, 2019.
- [77] H. A. Damis, N. Khalid, R. Mirzavand, H. J. Chung, and P. Mousavi, “Epidermal loop antenna design at 900 MHz for biotelemetry,” *IET Conf. Publ.*,

- vol. 2018, no. CP741, pp. 2–4, 2018.
- [78] J. C. Costa, F. Spina, P. Lugoda, L. Garcia-Garcia, D. Roggen, and N. Münzenrieder, “Flexible Sensors—From Materials to Applications,” *Technologies*, vol. 7, no. 2, p. 35, 2019.
- [79] M. Mardonova and Y. Choi, “Review of wearable device technology and its applications to the mining industry,” *Energies*, vol. 11, no. 3, 2018.
- [80] S. Shamrao and B. Suryakanth, “A survey on design and development of planar antennas for wireless applications,” *Int. J. Emerg. Technol.*, vol. 6, no. 2, pp. 203–206, 2015.
- [81] S. Liu, Q. Wang, and R. Gao, “A topology optimization method for design of small GPR antennas,” *Struct. Multidiscip. Optim.*, vol. 50, no. 6, pp. 1165–1174, 2014.
- [82] M. Sonkki, Z. Siddiqui, J. Chen, M. E. Leinonen, M. Berg, and A. Parssinen, “Study of planar wideband mm-wave bowtie antennas over PCB ground plane,” *13th Eur. Conf. Antennas Propagation, EuCAP 2019*, no. EuCAP, 2019.
- [83] J. Peng, B. Zhou, Y. Liu, F. Zhao, and Y. Jin, “Design of A Miniature 50 Ω -Printed Bowtie Planar Ultra-Wideband Antenna,” in *2020 IEEE Conference on Telecommunications, Optics and Computer Science, TOCS 2020*, 2020, pp. 272–275.
- [84] A. C. Durgun, C. A. Balanis, C. R. Birtcher, and D. R. Allee, “Design , Simulation , Fabrication and Testing of Flexible Bow-Tie Antennas,” *IEEE Trans. Antennas Propag.*, vol. 59, no. 12, pp. 4425–4435, 2011.
- [85] Y.-L. Chen, C.-L. Ruan, and L. Peng, “A novel ultra-wideband bow-tie slot antenna in wireless communication systems,” *Prog. Electromagn. Res. Lett.*, vol. 1, pp. 101–108, 2008.
- [86] A. C. Durgun, C. A. Balanis, C. R. Birtcher, and D. R. Allee, “Radiation characteristics of a flexible bow-tie antenna,” *IEEE Antennas Propag. Soc. AP-S Int. Symp.*, pp. 1239–1242, 2011.
- [87] J. Rashed and C.-T. Tai, “A new class of resonant antennas,” *IEEE Trans. Antennas Propag.*, vol. 39, no. 9, 1991.
- [88] O. O. Olaode, W. D. Palmer, and W. T. Joines, “Effects of meandering on dipole antenna resonant frequency,” *IEEE Antennas Wirel. Propag. Lett.*, vol. 11, pp. 122–125, 2012.
- [89] L. Deng, S. F. Li, K. L. Lau, and Q. Xue, “Vertical meandering approach for

- antenna size reduction,” *Int. J. Antennas Propag.*, vol. 2012, pp. 1–6, 2012.
- [90] D. K. C. Chew and S. R. Saunders, “Meander line technique for size reduction of quadrifilar helix antenna,” *IEEE Antennas Wirel. Propag. Lett.*, vol. 1, pp. 109–111, 2002.
- [91] M. Ali and S. S. Stuchly, “A Meander-Line Bow-Tie Antenna,” in *IEEE Antennas and Propagation Society International Symposium. 1996 Digest*, 1996, pp. 1566–1569.
- [92] S. Wi, T. Ym, H. Lee, J. P. Yaok, and H. Park, “Bow-tie-shaped Meander Slot Antenna for 5 GHz Application,” in *IEEE Antennas and Propagation Society International Symposium*, 2002, pp. 456–458.
- [93] H. R. Khaleel, “Design and Fabrication of Compact Inkjet Printed Antennas for Integration Within Flexible and Wearable Electronics,” *IEEE Trans. Components, Packag. Manuf. Technol.*, vol. 4, no. 10, pp. 1722–1728, 2014.
- [94] D. Tobjörk and R. Österbacka, “Paper electronics,” *Adv. Mater.*, vol. 23, pp. 1935–1961, 2011.
- [95] M. S. R. Bashri, T. Arslan, and W. Zhou, “Flexible Antenna Array for Wearable Head Imaging System,” in *11th European Conference on Antennas and Propagation (EUCAP) Flexible*, 2017, pp. 172–176.
- [96] S. G. Kirtania *et al.*, “Flexible antennas: A review,” *Micromachines*, vol. 11, 2020.
- [97] S. M. Ali, C. Sovuthy, M. A. Imran, S. Socheatra, Q. H. Abbasi, and Z. Z. Abidin, “Recent advances of wearable antennas in materials, fabrication methods, designs, and their applications: State-of-the-art,” *Micromachines*, vol. 11, no. 10, 2020.
- [98] P. Salonen, Y. Rahmat-Samii, H. Hurme, M. Kivikoski, M. Schaffrath, and M. Kivikoski, “Effect of conductive materials on wearable Antenna performance: A case study of WLAN antennas,” in *IEEE Antennas and Propagation Society Symposium*, 2004, vol. 1, pp. 455–458.
- [99] G. Kaur *et al.*, “Performance analysis of conductive patch materials for the design and fabrication of microstrip patch antennas,” in *Progress in Electromagnetics Research Symposium*, 2017, pp. 502–508.
- [100] C. K. Chiang *et al.*, “Comparison of Two Planar Elliptical Ultra-Wideband PPy Conductive Polymer Antennas Thomas,” in *IEEE International Symposium on Antennas and Propagation*, 2012, pp. 1098–1101.

- [101] C. Occhiuzzi, A. Ajovalasit, M. A. Sabatino, C. Dispenza, and G. Marrocco, "RFID Epidermal Sensor including Hydrogel Membranes for Wound Monitoring and Healing," in *IEEE International Conference on RFID*, 2015, pp. 182–188.
- [102] N. Chahat, M. Zhadobov, S. A. Muhammad, L. Le Coq, and R. Sauleau, "60-GHz textile antenna array for body-centric communications," *IEEE Trans. Antennas Propag.*, vol. 61, no. 4, pp. 1816–1824, 2013.
- [103] S. A. Babale, S. K. A. Rahim, M. Jusoh, and L. Zahid, "Branch-line coupler using PDMS and Shieldit Super fabric conductor," *Appl. Phys. A Mater. Sci. Process.*, vol. 123, no. 2, pp. 1–4, 2017.
- [104] H. R. Raad, A. I. Abbosh, H. M. Al-rizzo, and D. G. Rucker, "Flexible and Compact AMC Based Antenna for Telemedicine Applications," *IEEE Trans. Antennas Propag.*, vol. 61, no. 2, pp. 524–531, 2013.
- [105] M. Mantash, A. C. Tarot, S. Collardey, and K. Mahdjoubi, "Investigation of flexible textile antennas and AMC reflectors," *Int. J. Antennas Propag.*, vol. 2012, 2012.
- [106] S. M. Saeed, C. A. Balanis, C. R. Birtcher, A. C. Durgun, and H. N. Shaman, "Wearable Flexible Reconfigurable Antenna Integrated With Artificial Magnetic Conductor," *IEEE Antennas Wirel. Propag. Lett.*, vol. 16, pp. 2396–2933, 2017.
- [107] D. C. Li, F. Boone, M. Bozzi, L. Perregrini, and K. Wu, "Concept of virtual electric/magnetic walls and its realization with artificial magnetic conductor technique," *IEEE Microw. Wirel. Components Lett.*, vol. 18, no. 11, pp. 743–745, 2008.
- [108] Y. Zhang, J. Von Hagen, M. Younis, C. Fischer, and W. Wiesbeck, "Planar Artificial Magnetic Conductors and Patch Antennas," *IEEE Trans. Antennas Propag.*, vol. 51, no. 10, pp. 2704–2712, 2003.
- [109] K. Agarwal, Y. X. Guo, and B. Salam, "Wearable AMC Backed Near-Endfire Antenna for On-Body Communications on Latex Substrate," *IEEE Trans. Components, Packag. Manuf. Technol.*, vol. 6, no. 3, pp. 346–358, 2016.
- [110] L. O. Nur, A. Kurniawan, Sugihartono, and A. Munir, "Theoretical analysis of resonant frequency for AMC-based absorber composed of square patch array," *Int. J. Electr. Eng. Informatics*, vol. 7, no. 2, pp. 284–296, 2015.
- [111] J. R. Sohn, K. Y. Kim, H. S. Tae, and J. H. Lee, "Comparative study on various

- artificial magnetic conductors for low-profile antenna,” *Prog. Electromagn. Res.*, vol. 61, pp. 27–37, 2006.
- [112] S. P. Rea, D. Linton, E. Orr, and J. McConnell, “Broadband high-impedance surface design for aircraft HIRF protection,” *IEEE Proceedings- Microwave, Antennas Propag.*, vol. 153, no. 4, pp. 307–313, 2006.
- [113] J. Li, H. Huo, J. Chen, S. Zhu, H. Shi, and A. Zhang, “Miniaturised artificial magnetic conductor and its application in unidirectional circularly polarised slot antenna design,” *IET Microwaves, Antennas Propag.*, vol. 12, no. 12, pp. 1885–1889, 2018.
- [114] O. M. Sanusi, F. A. Ghaffar, A. Shamim, M. Vaseem, Y. Wang, and L. Roy, “Development of 2.45 GHz Antenna for Flexible Compact Radiation Dosimeter Tags,” *IEEE Trans. Antennas Propag.*, vol. 67, no. 8, pp. 5063–5072, 2019.
- [115] A. Y. I. Ashyap and Z. Z. Abidin, “Highly Efficient Wearable CPW Antenna Enabled by EBG-FSS Structure for Medical Body Area Network Applications,” *IEEE Access*, vol. 6, pp. 77529–77541, 2018.
- [116] H. Lago, P. Jack, S. Yan, and G. A. E. Vandenbosch, “Textile antenna integrated with compact AMC and parasitic elements for WLAN / WBAN applications,” *Appl. Phys. A*, vol. 122, no. 12, pp. 1–6, 2016.
- [117] M. Mantash, M. E. De Cos, A. C. Tarot, S. Collardey, K. Mahdjoubi, and F. Las-Heras, “Dual-band textile hexagonal artificial magnetic conductor for WiFi wearable applications,” *Proc. 6th Eur. Conf. Antennas Propagation, EuCAP 2012*, vol. 0, pp. 1395–1398, 2012.
- [118] A. Mersani, L. Osman, and I. Sfar, “Dual-band textile antenna on AMC substrate for wearable applications,” *Mediterr. Microw. Symp.*, vol. 2015-Janua, pp. 1–3, 2015.
- [119] S. Genovesi, F. Costa, F. Fanciulli, and A. Monorchio, “Wearable Inkjet-Printed Wideband Antenna by Using Miniaturized AMC for Sub-GHz Applications,” *IEEE Antennas Wirel. Propag. Lett.*, vol. 15, pp. 1927–1930, 2016.
- [120] X. Liu, Y. Di, H. Liu, Z. Wu, and M. M. Tentzeris, “A Planar Windmill-Like Broadband Antenna Equipped with Artificial Magnetic Conductor for Off-Body Communications,” *IEEE Antennas Wirel. Propag. Lett.*, vol. 15, pp. 64–67, 2016.
- [121] F. Wang and T. Arslan, “A wearable ultra-wideband monopole antenna with

- flexible artificial magnetic conductor,” *2016 Loughbrgh. Antennas Propag. Conf. LAPC 2016*, 2017.
- [122] C. G. Malmberg and A. A. Maryott, “Dielectric constant of water from 0 to 100 C,” *J. Res. Natl. Bur. Stand. (1934)*, vol. 56, no. 1, p. 1, 1956.
- [123] K. Kamardin, M. K. A. Rahim, P. S. Hall, N. A. Samsuri, T. A. Latef, and M. H. Ullah, “Planar textile antennas with artificial magnetic conductor for body-centric communications,” *Appl. Phys. A Mater. Sci. Process.*, 2016.
- [124] J. Lilja, P. Salonen, T. Kaija, and P. De Maagt, “Design and Manufacturing of Robust Textile Antennas for Harsh Environments,” *IEEE Trans. Antennas Propag.*, vol. 60, no. 9, pp. 4130–4140, 2012.
- [125] M. a R. Osman, M. K. a Rahim, N. a Samsuri, H. a M. Salim, and M. F. Ali, “Embroidered Fully Textile Wearable Antenna for Medical Monitoring Applications,” *Prog. Electromagn. Res.*, vol. 117, no. May, pp. 321–337, 2011.
- [126] C. J. Harvey, R. F. Lebouf, and A. B. Stefaniak, “Formulation and stability of a novel artificial human sweat under conditions of storage and use,” *Toxicol. Vitro.*, vol. 24, no. 6, pp. 1790–1796, 2010.
- [127] O. O. Shoewu, L. A. Akinyemi, and L. Oborkhale, “Towards Developing Path loss Models for Dryland and Wetland Environments,” *IEEE AFRICON Conf.*, vol. 2019-Septe, 2019.
- [128] J. A. Dabin, N. Ni, A. M. Haimovich, E. Niver, and H. Grebel, “The effects of antenna directivity on path loss and multipath propagation in UWB indoor wireless channels,” *2003 IEEE Conf. Ultra Wideband Syst. Technol. UWBST 2003 - Conf. Proc.*, pp. 305–309, 2003.
- [129] N. Yohanna, R. Aprilliyani, and R. G. Prabowo, “Path Loss Model Estimation Based on Measurements of Off-Body and On-Body Communication Using Textile Antenna at 2 . 45 GHz,” in *3rd Int. Conf. on Information Tech., Computer, and Electrical Engineering (ICITACEE)*, 2016, pp. 434–438.
- [130] X. Wu, “Antennas and Propagation for Body Area Networks at 60 GHz,” 2013.
- [131] P. Cui, Y. U. Yu, W. Lu, Y. Liu, and H. Zhu, “Measurement and Modeling of Wireless Off-Body Propagation Characteristics Under Hospital Environment at 6-8.5 GHz,” *IEEE Access*, vol. 5, pp. 10915–10923, 2017.
- [132] M. M. Khan, Q. H. Abbasi, A. Alomainy, and Y. Hao, “Study of Line of Sight (LOS) and None Line of Sight (NLOS) Ultra Wideband Off-Body Radio Propagation For Body Centric Wireless Communications in Indoor,” *Proc. 5th*

- Eur. Conf. Antennas Propag.*, pp. 110–114, 2011.
- [133] S. J. Ambroziak *et al.*, “An Off-Body Channel Model for Body Area Networks in Indoor Environments,” *IEEE Trans. Antennas Propag.*, vol. 64, no. 9, pp. 4022–4035, 2016.
- [134] K. Ali, A. Brizzi, S. L. Lee, G. Z. Yang, A. Alomainy, and Y. Hao, “Quantitative analysis of the subject-specific on-body propagation channel based on statistically created models,” *IEEE Antennas Wirel. Propag. Lett.*, vol. 14, pp. 398–401, 2015.
- [135] K. Kamardin, M. K. A. Rahim, N. A. Samsuri, M. E. Jalil, and I. H. Idris, “Textile Artificial Magnetic Conductor Waveguide Jacket for On-Body Transmission Enhancement,” *Prog. Electromagn. Res. B*, vol. 54, pp. 45–68, 2013.
- [136] Y. Rahmat-samii, “Wearable and Implantable Antennas in Body-Centric Communications,” in *The Second European Conference on Antennas and Propagation, EuCAP*, 2007, pp. 6–10.
- [137] R. Rosini and R. D’Errico, “Off-Body Channel Modelling at 2.45 GHz for Two Different Antennas,” *Proc. 6th Eur. Conf. Antennas Propagation, EuCAP 2012*, pp. 3378–3382, 2012.
- [138] S. Dumanli, L. Sayer, E. Mellios, X. Fafoutis, G. S. Hilton, and I. J. Craddock, “Off-Body Antenna Wireless Performance Evaluation in a Residential Environment,” *IEEE Trans. Antennas Propag.*, vol. 65, no. 11, pp. 6076–6084, 2017.
- [139] A. Tsolis, W. G. Whittow, A. A. Alexandridis, and J. Y. C. Vardaxoglou, “Embroidery and related manufacturing techniques for wearable antennas: Challenges and opportunities,” *Electron.*, vol. 3, no. 2, pp. 314–338, 2014.
- [140] S. Patel, H. Park, P. Bonato, L. Chan, and M. Rodgers, “A review of wearable sensors and systems with application in rehabilitation,” *J. Neuroeng. Rehabil.*, vol. 9, no. 1, pp. 1–17, 2012.
- [141] H. Huang, “Flexible wireless antenna sensor: A review,” *IEEE Sens. J.*, vol. 13, no. 10, pp. 3865–3872, 2013.
- [142] A. Arriola, J. I. Sancho, S. Brebels, M. Gonzalez, and W. De Raedt, “Stretchable dipole antenna for body area networks at 2.45 GHz,” *IET Microw. Antennas Propag.*, vol. 5, no. 7, pp. 852–859, 2011.
- [143] M. A. Antoniadou, M. A. B. Abbasi, M. Nikolic, P. Vryonides, and S. Nikolaou,

- “Conformal Wearable Monopole Antenna Backed by a Compact EBG Structure for Body Area Networks,” pp. 164–166, 2017.
- [144] A. D. Johnson, M. W. Nichols, S. Bojja Venkatakrishnan, and J. L. Volakis, “Reconfigurable log-periodic dipole array on textile,” *IET Microwaves, Antennas Propag.*, vol. 14, pp. 1791–1794, 2020.
- [145] A. Note, “Agilent Basics of Measuring the Dielectric Properties of Materials.”
- [146] A. Godio, D. Politecnico, and C. Duca, “Open ended-coaxial Cable Measurements of Saturated Sandy Soils Open ended-coaxial Cable Measurements of Saturated Sandy Soils,” no. June, 2014.
- [147] D. M. Hagl, D. Popovic, S. C. Hagness, J. H. Booske, and M. Okoniewski, “Sensing volume of open-ended coaxial probes for dielectric characterization of breast tissue at microwave frequencies,” *IEEE Trans. Microw. Theory Tech.*, vol. 51, no. 4 I, pp. 1194–1206, 2003.
- [148] A. La Gioia *et al.*, “Open-Ended Coaxial Probe Technique for Dielectric Measurement of Biological Tissues : Challenges and Common Practices,” 2018.
- [149] M. A. R. Osman, “The development of textile ultra wide-band antennas for wearable applications,” 2012.
- [150] H. A. Rahim *et al.*, “Measurement of Dielectric Properties of Textile Substrate,” *J. Teknol.*, vol. 1, pp. 1–6, 2015.
- [151] Keysight Technologies, “Keysight 85070E dielectric probe kit 200 MHz to 50 GHz: Technical overview,” 2014.
- [152] K. Kamardin, “Artificial Magnetic Conductor Waveguide Sheet for Transmission Enhancement Between Antennas for Body Centric Communications,” Universiti Teknologi Malaysia, 2014.
- [153] P. M. Meaney, A. P. Gregory, J. Seppala, and T. Lahtinen, “Open-Ended Coaxial Dielectric Probe Effective Penetration Depth Determination,” *IEEE Trans. Microw. Theory Tech.*, vol. 64, no. 3, pp. 915–923, 2016.
- [154] S. Sankaralingam and B. Gupta, “Use of electro-textiles for development of wibro antennas,” *Prog. Electromagn. Res. C*, vol. 16, no. August, pp. 183–193, 2010.
- [155] F. Long *et al.*, “Implementation and Wireless Readout of Passive UHF RFID Strain Sensor Tags based on Electro-Textile Antennas.”
- [156] Z. Hamouda *et al.*, “Dual-band elliptical planar conductive polymer antenna printed on a flexible substrate,” *IEEE Trans. Antennas Propag.*, 2015.

- [157] M. K. Elbasheer, M. A. R. Osman, A. Abuelnuor, M. K. A. Rahim, and M. E. Ali, "Conducting Materials Effect on UWB Wearable Textile Antenna," vol. I, 2014.
- [158] "3M Fabric Tape CN-3190 Nickel on Copper-Plated Polyester Fabric," 2008.
- [159] K. N. Paracha, S. K. A. Rahim, P. J. Soh, and M. Khalily, "Wearable Antennas: A Review of Materials, Structures, and Innovative Features for Autonomous Communication and Sensing," *IEEE Access*, vol. 7, pp. 56694–56712, 2019.
- [160] G. Measurement, "15 : Measurement," in *Pipeline Rules of Thumb Handbook*, 2014, p. 562.
- [161] S. Agneessens, S. Lemey, T. Vervust, and H. Rogier, "Wearable, Small, and Robust: The Circular Quarter-Mode Textile Antenna," *IEEE Antennas Wirel. Propag. Lett.*, vol. 14, pp. 1482–1485, 2015.
- [162] M. K. A. Rahim, M. Z. A. A. Aziz, and C. S. Goh, "Bow-tie microstrip antenna design," in *IEEE International Conference on Networks*, 2005, pp. 17–20.
- [163] W. S. Kaswiati and J. Suryana, "Design and realization of planar bow-tie dipole array antenna with dual-polarization at 2.4 GHz frequency for Wi-Fi access point application," in *2012 7th International Conference on Telecommunication Systems, Services, and Applications, TSSA 2012*, 2012.
- [164] D. Chang, J. Lee, and S. Lee, "The Study of Wideband Bowtie Antenna for ITDAMS," in *International Conference on Microwave and Millimeter Wave Technology*, 2004, pp. 54–57.
- [165] J. Rashed and C.-T. Tai, "A New Class of Resonant Antennas," *IEEE Trans. Antennas Propag.*, vol. 39, no. 9, pp. 14–16, 1991.
- [166] Vikram P, Dr. H.V Kumaraswamy, and R.K Manjunath, "Design and Simulation of Meander Line Antenna for RFID Passive Tag," *Int. J. Adv. Res. Comput. Commun. Eng.*, vol. 4, no. 8, pp. 119–122, 2015.
- [167] O. O. Olaode, w. D. Palmer, and W. T. Joines, "Characterization of Meander Dipole Antennas With a geometry-based, frequency-independent Lumped Element Model," *IEEE Antennas Wirel. Propag. Lett.*, vol. 11, no. 0704, pp. 346–349, 2012.
- [168] K. Noguchi and M. Mizusawa, "Increasing the Bandwidth of a Meander Line Antenna Consisting of Two Strips," pp. 2198–2201, 1997.
- [169] T. J. Warnagiris, S. Member, and T. J. Minardo, "Performance of a Meandered Line as an Electrically Small Transmitting Antenna," vol. 46, no. 12, pp. 1797–

1801, 1998.

- [170] B. Bonnet, F. Guitton, Y. Raingeaud, and D. Magnon, “Resonant frequency, bandwidth and gain of meander line antenna,” *ANTEM 2005 - 11th Int. Symp. Antenna Technol. Appl. Electromagn. Conf. Proc.*, pp. 6–9, 2005.
- [171] A. Geogiadis, H. Rogier, and L. Rosella, *Microwave and Millimeter Wave Circuits and Systems: Emerging Design, Technologies and Applications*. WILEY, 2012.
- [172] Wwww.cst.com, “Application note:Periodic Arrays,” pp. 1–14, 2006.
- [173] A. P. Feresidis, G. Goussetis, S. Wang, and J. C. Vardaxoglou, “Artificial magnetic conductor surfaces and their application to low-profile high-gain planar antennas,” *IEEE Trans. Antennas Propag.*, vol. 53, no. 1 I, pp. 209–215, 2005.
- [174] D. Yan, Q. Gao, C. Wang, and N. Yuan, “Strip-type AMC structure and analysis to its band-gap characteristic,” in *PIERS 2005 - Progress in Electromagnetics Research Symposium, Proceedings*, 2005, vol. 2, pp. 505–509.
- [175] “Guidelines for limiting exposure to electromagnetic fields (100 kHz to 300 GHz),” *Health Phys.*, vol. 118, no. 5, pp. 483–524, 2020.
- [176] C. Kwok and D. L. Means, “Evaluating Compliance with FCC Guidelines for Human Exposure to Radiofrequency Electromagnetic Fields,” 2001.
- [177] S. N. Mahmood *et al.*, “Recent Advances in Wearable Antenna Technologies: a Review,” *Prog. Electromagn. Res. B*, vol. 89, no. July, pp. 1–27, 2020.
- [178] “FCC Rules and Regulations.”
- [179] R. Dewan, M. K. A. Rahim, M. R. Hamid, H. A. Majid, M. F. . Yusoff, and M. E. Jalil, “Reconfigurable antenna using capacitive loading to artificial magnetic conductor (AMC),” *Microw. Opt. Technol. Lett.*, vol. 58, no. 10, pp. 2422–2429, 2016.
- [180] H. T. Friis, “A note on a simple transmission formula,” in *Proceedings of the IRE*, 1946, no. 5, pp. 254–256.
- [181] S. K. Yoo, S. L. Cotton, Y. J. Chun, W. G. Scanlon, and G. A. Conway, “Channel characteristics of dynamic off-body communications at 60 GHz under line-of-sight (LOS) and non-LOS conditions,” *IEEE Antennas Wirel. Propag. Lett.*, vol. 16, pp. 1553–1556, 2017.
- [182] R.-G. Garcia-Serna, C. Garcia-Pardo, and J.-M. Molina-Garcia-Pardo, “Effect of the receiver attachment position on untrawideband off-body channels,” *IEEE*

- Antennas Wirel. Propag. Lett.*, vol. 14, pp. 1101–1104, 2015.
- [183] J. Lee, M. D. Kim, H. K. Chung, and J. Kim, “Non-line-of-sight path loss model for low-height terminals in urban street grid environments,” *IEEE Antennas Propag. Soc. AP-S Int. Symp.*, vol. 2015-Octob, pp. 1792–1793, 2015.
- [184] M. M. Khan, Q. H. Abbasi, A. Alomainy, Y. Hao, and C. Parini, “Experimental characterisation of ultra-wideband off-body radio channels considering antenna effects,” *IET Microwaves, Antennas Propag.*, vol. 7, no. 5, pp. 370–380, 2013.
- [185] D. B. Smith, D. Miniutti, and L. W. Hanlen, “Characterization of the body-area propagation channel for monitoring a subject sleeping,” *IEEE Trans. Antennas Propag.*, vol. 59, no. 11, pp. 4388–4392, 2011.
- [186] K. Kamardin *et al.*, “Investigation of Transmission Performance Between Antennas with Textile Artificial Magnetic Conductor Jacket on Male and Female Subjects,” no. December, pp. 11–13, 2016.
- [187] K. Kamardin, M. K. A. Rahim, N. A. Samsuri, M. E. Jalil, and H. A. Majid, “Transmission enhancement using textile artificial magnetic conductor with coplanar waveguide monopole antenna,” *Microw. Opt. Technol. Lett.*, 2015.
- [188] R. G. Garcia-Serna, C. Garcia-Pardo, and J. M. Molina-Garcia-Pardo, “Effect of the receiver attachment position on ultrawideband off-body channels,” *IEEE Antennas Wirel. Propag. Lett.*, vol. 14, pp. 1101–1104, 2015.
- [189] K. G. Tan and T. A. Rahman, “Receiving antenna height dependence of radio propagation path loss in fixed wireless access environment,” in *Asia Pacific Microwave Conference. APMC’99. Microwaves Enter the 21st Century. Conference Proceedings*, 1999, pp. 797–800.
- [190] A. Alomainy, Y. Hao, C. G. Parini, and P. S. Hall, “Comparison between two different antennas for UWB on-body propagation measurements,” *IEEE Antennas Wirel. Propag. Lett.*, vol. 4, no. 1, pp. 31–34, 2005.
- [191] D. E. Townsend, S. S. Ditchkoff, and S. D. Fuhlendorf, “Transmitter height influences error of ground-based radio-telemetry,” *Wildlife Biol.*, vol. 13, no. 1, pp. 98–101, 2007.
- [192] T. Chrysikos, I. Zisi, and S. Kotsopoulos, “Channel modeling and path loss characterization for in-body propagation at MICS and ISM bands,” *Wirel. Telecommun. Symp.*, vol. 2016-May, 2016.
- [193] O. P. Pasquero and R. D. Errico, “A spatial model of the UWB off-body channel in indoor environments,” *IEEE Trans. Antennas Propag.*, vol. 64, no. 9, pp.

- 3981–3989, 2016.
- [194] D. Chizhik, J. Ling, and R. A. Valenzuela, “The Effect of Electric Field Polarization on Indoor Propagation .,” in *IEEE Universal Personal International Conference on Communications*, 1998, pp. 1–4.
- [195] R. Yoshimura *et al.*, “Effect of vegetation on radio wave propagation in 920-MHz and 2.4-GHz bands,” in *Asia-Pacific Microwave Conference Proceedings, APMC*, 2016, vol. 0, pp. 2–5.
- [196] H.-S. Zhang, S.-L. Chai, K. Xiao, and L. F. Ye, “Numerical and Experimental Analysis of Wideband E-Shape Patch Textile Antenna,” *Prog. Electromagn. Res. C*, vol. 45, no. November, pp. 163–178, 2014.
- [197] H. P. Schwan, R. J. Sheppard, and E. H. Grant, “Complex permittivity of water at 25 °C,” *J. Chem. Phys.*, vol. 64, no. 5, pp. 2257–2258, 1976.
- [198] P. U. In and H. E. P. Hys, “International Commission on Non-Ionizing Radiation Protection Icnirp Guidelines for Limiting Exposure To,” 2020.
- [199] C. Gabriel, “Body tissue dielectric parameters,” *U.S. Air Force Report AFOSR-TR-96*. .
- [200] “MySignals HW (eHealth Medical Development Shield for Arduino).” .
- [201] O. Yakut, S. Solak, and E. D. Bolat, “Measuring ECG Signal Using e-Health Sensor Platform,” in *International Conference on Chemistry, Biomedical and Environment Engineering (ICCBEE’14)*, 2014, pp. 65–69.
- [202] R. Araz, “Pocket Guide to ECG Interpretation,” 2017.
- [203] M. Abri, H. Badaoui, and Z. Berber, “A Bow-Tie Bluetooth/Wimax Antenna Design for Wireless Networks Applications,” *Int. J. Inf Netw. Secur.*, vol. 1, no. 3, pp. 207–215, 2012.
- [204] Y. Tawk, K. Y. Kabalan, A. El-Hajj, C. G. Christodoulou, and J. Costantine, “A simple multiband printed bowtie antenna,” *IEEE Antennas Wirel. Propag. Lett.*, vol. 7, pp. 557–560, 2008.
- [205] M. Fallahpour and R. Zoughi, “Antenna miniaturization techniques-A review of topology and material-based method,” *IEEE Antennas Propag. Mag.*, vol. 60, pp. 38–50, 2018.
- [206] P. Salonen and Y. Rahmat-samii, “Wearable Antennas in the Vicinity of Human Body,” pp. 467–470.
- [207] Sankaralingam Subramaniam and Bhaskar Gupta, “Design and development of flexible fabric antenna for body-worn applications and its performance study

- under flat and bent positions,” *Microw. Opt. Technol. Lett.*, vol. 54, no. 12, pp. 2781–2784, 2012.
- [208] L. Deias, G. Mazzarella, G. Montisci, and G. A. Casula, “Synthesis of artificial magnetic conductors using structure-based evolutionary design,” *Int. J. Antennas Propag.*, vol. 2013, 2013.
- [209] L. Yao *et al.*, “Miniaturization and electromagnetic reliability of wearable textile antennas,” *Electronics*, vol. 10, no. 9, 2021.
- [210] Z. H. Jiang, D. E. Brocker, P. E. Sieber, and D. H. Werner, “A compact, low-profile metasurface-enabled antenna for wearable medical body-area network devices,” *IEEE Trans. Antennas Propag.*, vol. 62, no. 8, pp. 4021–4030, 2014.
- [211] A. R. Eldamak, S. Thorson, and E. C. Fear, “Study of the dielectric properties of artificial sweat mixtures at microwave frequencies,” *Biosensors*, vol. 10, no. 6, pp. 1–13, 2020.
- [212] Q. Spencer, M. Rice, B. Jeffs, and M. Jensen, “Indoor wideband time/angle of arrival multipath propagation results,” *IEEE Veh. Technol. Conf.*, vol. 3, pp. 1410–1414, 1997.
- [213] N. Agarwal, A. Mittal, and R. Bhattacharjee, “Angle and time of arrival statistics for indoor UWB communication,” *Proc. 16th Natl. Conf. Commun. NCC 2010*, no. 1, pp. 15–18, 2010.
- [214] N. Amini, W. Xu, Z. Li, M. Huang, and M. Sarrafzadeh, “Experimental Analysis of IEEE 802.15.4 for On/Off Body Communications,” in *22nd International Symposium on Personal, Indoor and Mobile Radio Communications*, 2011, pp. 2138–2142.
- [215] “Statistics on Causes of Death, Malaysia 2019,” 2019.
- [216] I. Romero *et al.*, “Motion artifact reduction in ambulatory ECG monitoring: An integrated system approach,” in *Proceedings - Wireless Health 2011, WH'11*, 2011, pp. 1–8.
- [217] K.-I. Wong and M. M. S. Ho, “Wearable Biosignal Monitoring Nodes for Real-Time Electrocardiogram and Motion Measurement,” in *2008 5th International Summer School and Symposium on Medical Devices and Biosensors*, pp. 190–193.
- [218] M. A. Ahamed, M. A. U. Ahad, M. H. A. Sohag, and M. Ahmad, “Development of Low Cost Wireless Biosignal Acquisition System for ECG EMG and EOG,” in *International Conference on Electrical Information and Communication*

Technologies, EICT 2015, pp. 195–199.

- [219] I. Villanueva-Miranda, H. Nazeran, and R. Martinek, “CardiaQloud: A remote ECG monitoring system using cloud services for eHealth and mHealth applications,” in *2018 IEEE 20th International Conference on e-Health Networking, Applications and Services, Healthcom 2018*, pp. 1–6.
- [220] T. Morrison, J. Silver, and B. Otis, “A Single-chip Encrypted Wireless 12-Lead ECG Smart Shirt for Continuous Health Monitoring,” pp. 6–7, 2014.
- [221] Y. Tian, Z. Tang, and Y. Yu, “Third-order channel propagation model-based indoor adaptive localization algorithm for wireless sensor networks,” *IEEE Antennas Wirel. Propag. Lett.*, vol. 12, pp. 1578–1581, 2013.
- [222] G. Hwang, K. Shin, S. Park, and H. Kim, “Measurement and comparison of wi-fi and super wi-fi indoor propagation characteristics in a multi-floored building,” *J. Commun. Networks*, vol. 18, no. 3, pp. 476–483, 2016.

Appendix A

LIST OF PUBLICATIONS

Journal

- [1] N. Othman, N. A. Samsuri, M. K. A. Rahim, K. Kamardin “Low specific absorption rate and gain-enhanced meandered bowtie antenna utilizing flexible dipole-like artificial magnetic conductor for medical application at 2.4 GHz” *Microw Opt Technol Lett.* pp 1– 9, 2020
- [2] N. Othman, N. A. Samsuri, M. K. A. Rahim, N. H. Sulaiman “Water ageing effect on wearable antenna made of medical-friendly and transdermal material at 2.4 GHz” *J. Phys.: Conf. Ser.* 1502 012011, 2019
- [3] N. Othman, N. A. Samsuri, M. K. A. Rahim, K. Kamardin, H. A. Majid “Meander bowtie antenna for wearable application” *TELKOMNIKA*, Vol.16, No.4, pp. 1522-1526, 2018
- [4] N. Othman, N. A. Samsuri, M. K. A. Rahim, K. Kamardin,” Design and analysis of flexible bow-tie antenna for medical application” *Journal of Electrical Engineering*, Vol.16, No.1, pp. 17-21, 2017

Conference & Proceeding

- [1] N. Othman, N. A. Samsuri, “Performance of Skin-Contact Meandered Bowtie Antenna with AMC Exposed to Sweat-like Liquid for Health Monitoring” *International Conference on UK-China Emerging Technologies (UCET)*, August 2020, Tele-presentation
- [2] N. Othman, N. A. Samsuri, M. K. A. Rahim, K. Kamardin, “Transmission Characteristic of Meandered Bowtie Antenna at 2.4 GHz in proximity to human body” *IEEE Asia-Pacific Conference on Antennas and Propagation (APCAP)*,

August 2018, New Zealand

Awards

- [1] Best Student Paper Award - 2020 International Conference on UK-China Emerging Technologies (UCET) with paper titled “Performance of Skin-Contact Meandered Bowtie Antenna with AMC Exposed to Sweat-like Liquid for Health Monitoring”.

- [2] Gold Medal - 2020 Industrial Art and Technology Exhibition (INATEX 2020) product title “Skin-Contact Transdermal Patch Antenna for Perpetual Health Monitoring Application”.

Patent

- [1] Skin Contact Flexible Antenna Assembly Utilizing Transdermal Patch For Continuous Health Monitoring